

1 **Manuscript (with author details)**

2 **Review**

3 **Metal nanoparticle hybrid hydrogels: the state-of-the-art of combining hard and soft**  
4 **materials to promote wound healing <sup>1</sup>**

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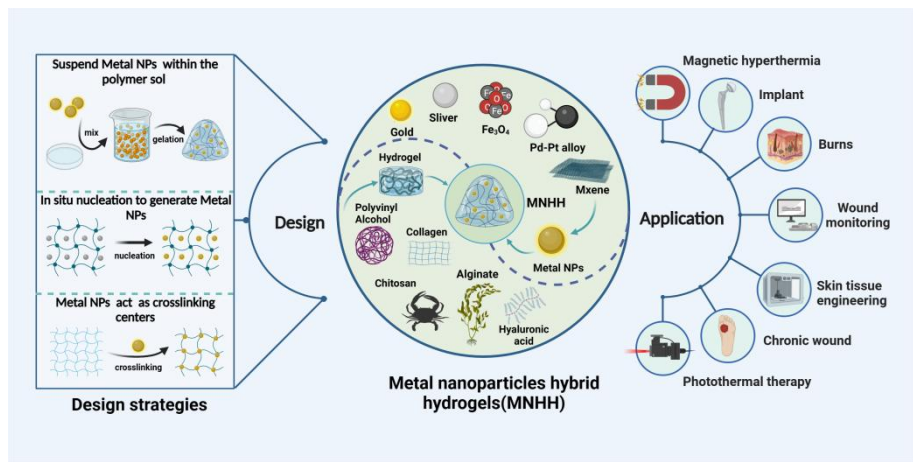
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20  
21 Abstract: Wounds represent a grave affliction that profoundly impacts human well-being.  
22 Establishing barriers, preventing infections, and providing a conducive microenvironment  
23 constitute the crux of wound therapy. Hydrogel, a polymer with an intricate three-dimensional  
24 lattice, serves as a potent tool in erecting physical barriers and nurturing an environment  
25 conducive to wound healing. This enables effective control over exudation, hemostasis,  
26 accelerated wound closure, and diminished scar formation. As a result, hydrogels have gained  
27 extensive traction in the realm of wound treatment. Metallic nanoparticle carriers, characterized by  
28 their multifaceted responses encompassing acoustics, optics, and electronics, have demonstrated  
29 efficacy in wound management. Nevertheless, these carriers encounter challenges associated with  
30 swift clearance and nonuniform effectiveness. The hybridization of metallic nanoparticle carriers  
31 with hydrogels overcomes the shortcomings inherent in metallic nanoparticle-based wound  
32 therapy. This amalgamation not only addresses the limitations but also augments the mechanical  
33 robustness of hydrogels. It confers upon them attributes such as environmental responsiveness and  
34 multifunctionality, thereby synergizing strengths and compensating for weaknesses. This

integration culminates in the precise and intelligent management of wounds. This review encapsulates the structural classifications, design strategies, therapeutic applications, and underlying mechanisms of metal nanoparticle hybrid hydrogels in the context of acute and chronic wound treatment. The discourse delves into the generation of novel or enhanced attributes arising from hybridization and how the current paradigm of wound therapy leverages these attributes. Amidst this continually evolving frontier, the potential of metal nanoparticle hybrid hydrogels to revolutionize wound treatment is underscored.

**Keywords:** Metal nanoparticles; Hydrogels; Wound healing; Skin tissue engineering; Biomaterials

**Running title:** Metal nanoparticle hybrid hydrogels



**Figure 1.** The design strategies and applications of MNHH. MNHH combining the advantages of hydrogel and metal nano have been widely used in the fields of wound healing. (Created with BioRender.com)

## 50 1. Introduction

51 A wound refers to the impairment of the skin's barrier function caused by external forces or  
 52 internal diseases. Based on the healing timeline, wounds can be classified as acute or chronic[1].  
 53 Burn injuries and diabetic foot ulcers (DFUs) stand as two archetypal instances of compromised  
 54 skin barrier function [1]. Burns are common acute wounds, signifying the most severe forms of  
 55 damage and trauma. Based on data from the World Health Organization, it has been determined  
 56 that approximately 180,000 individuals experience fatal outcomes due to burns on a yearly basis  
 57 [2]. This occurrence is predominantly prevalent in countries with low to middle income levels. In  
 58 the specific case of India, more than 1 million individuals suffer from moderate to severe burns  
 59 annually. Similarly, approximately 173,000 Bangladeshi children experience moderate to severe  
 60 burns each year. The financial burden associated with providing direct care for burns varies  
 61 significantly, but generally leans towards being costly. A systematic review conducted in 2014  
 62 revealed an average total healthcare cost per burn patient of US\$ 88,218 [3]. Concurrently, chronic  
 63 wounds induced by diabetes present a prominent challenge in wound management and stand as a  
 64 leading cause of mortality in diabetic patients [4]. Presently, the global diabetic population stands  
 65 at 537 million and is projected to reach 783 million by 2045 [4]. Approximately 25% of diabetic  
 66 patients are at risk of chronic nonhealing wounds, exemplified by diabetic foot ulcers (DFUs) [5].  
 67 In addressing the impediments to wound healing and infection, the swift establishment of a  
 68 provisional skin barrier proves pivotal. Traditional wound dressings predominantly encompass  
 69 regular gauze and petrolatum-infused gauze. While these materials shield wounds from  
 70 contamination, their efficacy in fluid absorption and infection resistance remains limited.  
 71 Additionally, they fail to provide the requisite mildly moist environment necessary for optimal  
 72 wound healing. Moreover, they necessitate frequent replacement within a short span, inflicting  
 73 considerable discomfort upon patients [6,7]. Biological materials such as allogeneic skin,  
 74 xenogeneic skin, and amnion serve as ideal temporary wound coverings. These materials foster a  
 75 mildly moist wound environment, accelerate wound healing, and alleviate the anguish associated  
 76 with frequent dressing changes. However, they are encumbered by constraints, including  
 77 insufficient skin sources, inconvenient preservation and usage, and suboptimal infection resistance  
 78 [8,9]. Hence, contemporary wound dressings should inherently embody the following attributes:  
 79 provision of a mildly moist wound environment; reduction of wound exudation; potent infection  
 80 resistance; diminished dressing change frequency; and alleviated patient discomfort.

81 Hydrogels possess distinct physicochemical and mechanical properties, including water  
 82 absorption and retention, biodegradability, and tunable viscoelasticity, thereby providing effective  
 83 barriers that absorb wound exudates, reduce wound moisture evaporation and prevent bacterial  
 84 infiltration [10–13]. Thus, hydrogels foster a microenvironment conducive to healing [14–17].  
 85 Furthermore, hydrogels, as extracellular matrix (ECM), are capable of supporting and enhancing

cell migration and proliferation to facilitate tissue repair [16,18–20]; as a result, hydrogels are composed of a soft and hydrophilic three-dimensional network of crosslinked polymers [21–23].

Given these attributes, hydrogels have emerged as promising novel wound healing dressings [14,24]. However, additional limitations in wound dressings include singular functionality, inferior mechanical strength, susceptibility to physiological degradation, limited resistance to multidrug-resistant bacteria, which fails to meet the requirements of processing and shaping, frequent and everlasting exposure to bacteria and free mobility around wound tissue. Hence, these challenges highlight the importance of developing modifications and adaptations of hydrogels as wound dressings in terms of structure and function.

Nanomaterials have a wide range of biological activities, of which metal nanoparticles are outstanding representatives [25–30]. Metal nanoparticles are three-dimensional crystalline materials with diameters ranging from 1 to 100 nm. They possess a high surface area-to-volume ratio and come in various sizes, shapes, and physicochemical activities [31]. Therefore, they serve as drug delivery vehicles and carriers owing to their strong stability, high loading capacity, specific targeting, and trigger release capabilities. Metal nanoparticles are notably extended to be utilized in wound healing as a result of reducing mitochondrial membrane potential, triggering neutrophil apoptosis and consequently reducing cytokine production [6]. Furthermore, photothermal effects induced by metal nanoparticles stimulate the proliferation and migration of epidermal cells and fibroblasts, expediting wound healing [32] and eliminating bacteria [33,34]. Moreover, metal nanoparticles inhibit microorganisms through actions such as penetrating bacterial membranes, inducing intracellular damage, and generating intracellular reactive oxygen species (ROS), thus exhibiting superior antibacterial performance [33]. However, metal nanoparticles exhibit certain toxicity toward normal tissue cells [34], while they are easily oxidized or degraded due to oxygen or pH fluctuations [35] and cleared by macrophages [32]. Hence, modifications and upgrades to metal nanoparticles in wound treatment are imperative to address high toxicity, poor stability, and short circulation.

Metal nanoparticle hybrid hydrogels (MNHHs) represent a significant advancement in biomedical materials, resulting from the fusion of metal nanoparticles with hydrogels. This innovative hybrid hydrogel not only enhances the stability and circulation time of metal nanoparticles, thereby mitigating their toxicity, but also exhibits responsiveness to a wide range of physicochemical stimuli, including acoustic, light, and electric stimuli. Furthermore, the distribution of metal nanoparticles within the hydrogel enhances its physical and mechanical properties, such as stretchability and rheology, effectively meeting the diverse requirements for wound healing. The versatile nature of MNHHs has led to their widespread application in various biomedical contexts, encompassing antimicrobial wound dressings [36], environmentally responsive therapies [37], tissue engineering scaffolds [38], and biosensing detection [39–41]. Nevertheless, the application of MNHHs in wound treatment is not without challenges. Current issues include the environmental impact of large-scale production, the high cost hindering clinical

adoption, and the potential long-term toxic effects of accumulated metal nanoparticles in the human body. In this emerging field of MNHH, although there have been some reviews discussing the application progress of specific types of MNHH (e.g., silver, ZnO), to our knowledge, there is currently no comprehensive and systematic overview of the types, design strategies, and mechanisms of action of MNHH in wound healing. Hence, there is a need for a comprehensive summary and analysis of the research progress of MNHH, its potential applications, and challenges in the field of wound healing.

In this review, we introduce common design strategies, research advancements, and challenges related to MNHH for wound healing applications. We briefly explain the gelation mechanism and loading methods of MNHH, outline their functional characteristics, and comprehensively elaborate on the mechanisms by which MNHH promotes wound healing. Through this review, we present the latest progress, challenges, and prospects of MNHH, which may inspire the design of advanced composite hydrogel materials and provide valuable insights for the clinical translation of these emerging materials for wound healing purposes.

## **2. The design strategies of MNHH**

Hydrogels are crosslinked through physical mechanisms such as ionic bonds or chemical methods such as Schiff's base bonds. Metal nanoparticles can be loaded into hydrogels using various approaches. For instance, metal nanoparticle precursor ions can be adsorbed onto the polymer matrix and then reduced in situ to form nanoparticles, thus integrating them into the hydrogel [42–45]. Although the metal nanoparticles are uniformly dispersed within the hydrogel matrix using this approach, it is typically employed for polymer systems or reactions involving reduction. Alternatively, colloidal suspensions containing metal nanoparticles can be mixed with the polymer solution before gelation, effectively immobilizing the nanoparticles within the hydrogel matrix [46,47]. The blending process is straightforward and results in the formation of stable networks. However, initiation of polymerization requires the use of an initiator or an external system, such as a photoinitiator with light, HRP (Horse radish peroxidase) with  $H_2O_2$ , or even temperature. Finally, the polymer solution can be initially gelled into the primary hydrogel structure, and subsequently, metal nanoparticles can be incorporated through covalent chelation, physical embedding, or electrostatic interactions after gelation [48-50], representing a comprehensive strategy for the formation of a double or multi-network. The majority of the formed networks may be reversible, allowing them to adapt to the extracellular matrix (ECM) due to the transformable bonding between polymer chains and metal nanoparticles. Notably, metal nanoparticles can serve as crosslinking centers through various mechanisms, significantly enhancing the mechanical and physicochemical properties of the hydrogel. Metal nanoparticles act as physical crosslinkers by forming interparticle interactions and increasing the entanglement of polymer chains. Additionally, modified or metal nanoparticles themselves possess functional groups on their surfaces that can react with the polymer chains, leading to the formation of covalent bonds. For example, gold nanoparticles tend to bind and cap to sulfur groups due to the

strong ionic and covalent bonds of Au-S. Leveraging the dynamic exchangeability of Au-S, thiol end group ligands modified polymers can be attached to thiolated Au nanoparticles, such as polyethylene glycol (PEG) [51-53]. Initially, the focus of metal nanoparticle hybrid hydrogels (MNHH) was primarily on enhancing the mechanical strength of composite hydrogel materials. Today, MNHHs exhibit a wider range of functionalities. First, the multi-responsive nature of metal nanoparticles—responsive to stimuli such as sound, light, and electricity—imparts the hydrogel with precise disease diagnostics and treatment capabilities. Second, the environmental sensitivity of hydrogel structures alters the optical, chemical, or electronic properties of embedded metal nanoparticles. Furthermore, the distribution of metal nanoparticles within the hydrogel's spatial network structure leads to the creation of materials with super-performance or composites featuring enhanced modified nanocarriers. For instance, hydrogels loaded with metal nanoparticles can be employed to develop multifunctional wound dressings that combat drug-resistant pathogens and promote wound healing [34,54–56]. They can also serve as components of smart wound dressing systems [35,57,58], providing scaffolds for cell differentiation, manipulation, and proliferation, integrated with real-time monitoring and on-demand therapy to overcome the limitations of traditional wound management [39,41]. As such, MNHHs exhibit enhanced mechanical properties and multifunctionality, offering effective interventions for wound management. This advancement holds promise for improving wound healing processes and patient outcomes.

### **3. The mechanism by which the enhancement function of MNHH**

#### **3.1. How metal nanoparticles improve the properties of hydrogels.**

Metal nanoparticles can indeed enhance the mechanical strength and stability of hydrogels. The integration of metal nanoparticles as structural components promotes the physical or chemical crosslinking of hydrogels, leading to improved mechanical and rheological properties. For instance, research has demonstrated the use of TiO<sub>2</sub> nanoparticles to enhance the physicochemical and rheological properties of hydrogels [59]. The formation of localized microstructures and permeation leads to changes in the gel structure, resulting in an increase in viscoelastic modulus and a decrease in frequency dependency, resembling more solid-like behavior [59]. Furthermore, a composite material, gelatin/CS/Ag, was obtained by in situ reduction of silver nanoparticles using gelatin as a reducing and stabilizing agent mixed with chitosan [60]. This composite hydrogel exhibited excellent mechanical properties, water absorption, and moisture retention, along with good biocompatibility [60]. In another example, cobalt nanoparticles were crosslinked into a poly(hydroxyethyl methacrylate) (pHEMA) hydrogel, resulting in improved loading efficiency and reduced leaching effects. The resulting composite material demonstrated muscle-like movement and flexibility [61]. The incorporation of metal nanoparticles can significantly enhance the mechanical properties and overall performance of hydrogels, making them promising materials for various biomedical applications.

The self-healing ability of hydrogels often arises from reversible noncovalent interactions between polymer chains, and interactions between polymer chains and metal ions can also drive the self-healing of composite materials [62]. As colloids in solution, the surface ligands, morphology, and size of metal nanoparticles determine their interfacial interactions. Metal nanoparticle-loaded hydrogels can utilize the self-assembly behavior and optical activity of metal nanoparticles for self-repair. For instance, research has indicated that azobenzene-functionalized gold nanoparticles can undergo photoisomerization under ultraviolet light. Combining this nanomaterial with a hydrogel imparts the hydrogel with the ability to self-heal under photothermal stimulation [63]. Additionally, the coordination between polymers and metal surfaces typically remains unchanged due to local environmental ion variations [64]. Therefore, the introduction of metal nanoparticles can enhance the robustness of hydrogel self-healing performance. In a study, gelatin modified with dopamine was used as a biomimetic template to synthesize a composite hydrogel material called Gel-DA @ Ag nanoparticles. This material exhibited good mechanical properties, injectability, and excellent self-healing capabilities [65]. The incorporation of metal nanoparticles into hydrogels not only enhances their mechanical and responsive properties but also adds a self-healing dimension to their functionalities, making them even more promising for advanced biomedical applications.

Furthermore, metal nanoparticle hybrid hydrogels (MNHH) have the potential to enhance the drug delivery system within hydrogels and refine the form of drug release. Due to the propensity of hydrogels to degrade in wound environments and their inherent mechanical instability, the sustained stability of their drug delivery systems is compromised. The incorporation of metal nanoparticles as structural components induces physical cross-linking, thereby improving the mechanical properties of hydrogels, enhancing their stability as drug delivery systems, and prolonging the drug release duration. For instance, the integration of Ag nanoparticles end-capped with benzotriazole maleimide into furfural-modified gelatin, alongside the addition of chondroitin sulfate (CS), yields mechanically stable MNHH [49]. Although the introduction of Ag nanoparticles might diminish the overall loading capacity of hydrogel systems for hydrophilic drugs, the augmentation of mechanical stability leads to an extended drug release period [49,66]. Additionally, metal nanoparticles endowed within MNHH with active or passive stimulus-responsive capabilities, encompassing responsiveness to external photothermal stimulation and localized environmental cues at wound sites, facilitate precise, intelligent, and targeted drug release. The local biological stimuli at wound sites generally encompass pH, temperature, and ion concentration. For instance, when the metal nanoparticles within MNHH are consistently exposed to specific wavelengths of light, their temperature rapidly rises, thus effectuating photothermal therapeutic (PTT) effects. Simultaneously, the incorporation of metal nanoparticles into MNHH to realize PTT can be employed to modulate drug release through the thermal-responsive deformation of hydrogels [67]. For instance, composite hydrogels containing polydopamine (PDA)-coated gold nanoparticles (Au NPs) and doxorubicin (DOX) firmly

anchored within the hydrogel matrix through PDA and amide interactions can achieve PTT and controlled DOX release upon near-infrared (NIR) light irradiation [68]. Similarly, MNHH can achieve drug modulation akin to photothermal effects through magneto-thermal responses [69].

In addition to enhancing and refining the inherent properties of hydrogels, metal nanoparticles can also bestow upon them entirely novel characteristics, including environmental responsiveness, biomarker monitoring, and imaging capabilities. These attributes are not independent but rather interconnected and mutually influencing, collectively propelling the application of composite materials in wound treatment. Environmentally responsive hydrogels, also known as smart hydrogels, are hydrogel materials that exhibit the ability to perceive intrinsic or extrinsic environmental stimuli and enact moderate responses accordingly. The introduction of metal nanoparticles grants hydrogels an entirely new environmental responsiveness, encompassing light sensitivity, magnetic field sensitivity, and conductivity, among others [70]. Research reports have described the design of a chemically cross-linked polyacrylamide hydrogel containing carboxyl-modified Au metal nanoparticle (AuC)-stabilized liposomes for pH-responsive local antibacterial delivery [71]. This hydrogel effectively sustains the release of AuC liposomes for up to 7 days, and in the acidic environment associated with skin infections (pH 4.5), the released liposomes exhibit responsive fusion with bacterial membranes, achieving localized bactericidal effects. Highly ordered layer-by-layer metal nanoparticle-loaded hydrogels were synthesized through alternating deposition of gold nanoparticles and poly(diallyl dimethylammonium chloride) (PDDA), leading to enhanced drug release rates when subjected to a magnetic field stimulus within the range of 40 to 110 Hz [72]. Natural hydrogels serve as ideal substitutes for the extracellular matrix (ECM) in tissue and cell engineering, yet their lack of conductivity limits their applications [22]. Cellular activity and functionality are dependent on the conduction of intercellular electrical signals. Metal nanoparticles can provide the conductivity that hydrogels lack, significantly augmenting their ability to promote various cellular functions [73]. For instance, the combination of gold nanorods with hydrogels effectively enhances cell adhesion and intercellular communication, elevating the volumetric conductivity and mechanical rigidity of the hydrogel scaffold. This leads to increased expression of cardiac cell phenotypes and maturity, holding significant implications for the construction of tissue-engineered skin and its application in wound treatment [73–75].

Furthermore, the environmental responsiveness of MNHH enables the monitoring of wound microenvironments and microorganisms. MNHH based on label-free surface-enhanced resonance Raman scattering (SERRS) can be utilized to monitor wound infections caused by *Pseudomonas aeruginosa* [41]. By incorporating uniformly dispersed Au nanorods, Au nanospheres, and Au nanostars within the hydrogel, forming distinct sensitivities and spatial resolutions, pyocyanin can be quantified, and its spatial distribution within biofilms can be imaged using the SERRS composite. Additionally, reports have demonstrated that Au nanostars and Pt nanospheres can bestow electrochemiluminescent immunosensing capabilities upon hydrogels for detecting human



chorionic gonadotropin (HCG) [76]. This method functionalizes HCG antibodies onto complexes based on Pt nanocarriers and sandwich-captured hormones between antibodies functionalized on Au nanocarriers. Under voltage stimulation, electrochemiluminescent signals are generated. These complexes can effectively detect changes in the steady state of wound microenvironments, aiding in predicting and guiding disease treatments. Metal nanoparticle composite hydrogels have been designed to construct a series of systems for monitoring steady-state changes, including variations in temperature, pH, and hydrogen peroxide concentration [77–80]. Changes in wound pH values are closely linked to infection, often presenting an acidic environment (reduced pH) during skin infections. Research has discovered that by incorporating conductive Au metal nanoparticles, precise pH determination of hydrogels composed of dimethyl aminoethyl methacrylate (DMAEMA) and 2-hydroxyethyl methacrylate (HEMA) was achieved [81]. Natural DMAEMA/HEMA hydrogels exhibit strong pH-responsive characteristics upon swelling but lack electrical conductivity. The introduction of gold nanocarriers imparts a pH-related electrochemical response to the hydrogel: as the pH shifts from acidic to neutral, the hydrogel swells, increasing interparticle distance and reducing the composite's conductivity, thereby accurately identifying pH changes [81].

In conclusion, MNHH effectively enhances the hydrogel structure, elevating its mechanical and self-healing properties, thereby rendering the hydrogel more malleable and pliable. This expansion in the capabilities of hydrogel dressings in wound care is attributed to MNHH. Moreover, MNHH represents a modifiable and controllable drug release system, enabling precise and intelligent drug delivery. Importantly, metal nanoparticle carriers bestow novel functional attributes upon hydrogels. These composites not only respond to local environmental changes but also allow triggering through external stimuli such as light, heat, and magnetism. They enable the construction of multifunctional composite hydrogels equipped with automatic sensing, real-time monitoring, and controllable intervention. Therefore, MNHHs possessing these new attributes transcend being merely dressings for infection control and wound healing promotion. They have emerged as intelligent and adaptable interfaces for wound management, paving the way for precise and intelligent wound treatments.

Table 1. The mechanism by which the enhancement function of MNNH

The enhancement function	Types of hydrogels	Specific performance	Refs.
Mechanical properties of hydrogels	SSG-TiO <sub>2</sub> hydrogels	It reduced the zeta potential of SSG-TiO <sub>2</sub> hydrogel, increased its density (from 47.1 g/ml to 50.15 g/ml), and particle size (from 277 nm to 764 nm), altering its surface tension.	[59]
Mechanical properties of hydrogels	Gelatin/CS/Ag hydrogels	The Young's modulus increased from $1.89 \pm 0.62$ MPa to $2.36 \pm 0.54$ MPa; the tensile strength increased from $1.62 \pm 0.56$ MPa to $1.92 \pm 0.06$ MPa; the fracture elongation (100%) increased from $29.23 \pm 2.11$ to $37.27 \pm 1.65$ .	[60]
Mechanical properties of hydrogels	Cobalt nanoparticle magnetic crosslinked pHEMA hydrogel	Enhancing the thermal stability of the hydrogel, the ignition point increased from 228°C to 420°C; improving mechanical stability and flexibility, it can be stretched to 123% of its initial length.	[61]
Self-healing properties of hydrogels	Gel-DA@Ag hydrogel	The hydrogel is capable of self-healing within 5 minutes; when subjected to alternating high (500%) and low (1%) strains with amplitude oscillations, the hydrogel demonstrates a reversible gel-sol-gel transition, indicating a remarkable self-healing ability.	[65]
Stability and durability of drug release	AuC-liposome polyacrylamide hydrogel	Carboxyl-modified gold nanoparticles were employed as stabilizers for cationic liposomes, enabling the hydrogel to steadily release AuC-loaded liposomes over a span of 7 days.	[71]

The enhancement function	Types of hydrogels	Specific performance	Refs.
Controlled release	PNAm-PDAAu-DOX hydrogel	Hydrogels exhibit the capability of mediating photothermal effects and controlled DOX release through intermittent near-infrared light irradiation.	[68]
Enlargement of drug release	layer-by-layer gold nanoparticle-loaded PDDA hydrogels	Under the stimulation of a magnetic field within the range of 40 to 110 Hz, the drug release rate from the hydrogel accelerates.	[72]
Conductivity of hydrogels	CS-GNP hydrogels	The incorporation of gold nanoparticles (GNPs) imparts electrical conductivity to the hydrogel, promoting active metabolism, migration, and proliferation of MSCs (mesenchymal stem cells).	[73]
Environmental responsiveness	Au@pNIPAM hydrogels	The formation of Au nanoparticle carriers results in distinct sensitivities and spatial resolutions, enabling the quantification of pyocyanin and allowing its spatial distribution within the biofilm to be imaged on the SERRS (surface-enhanced resonance Raman scattering) composite. schematic representation of wound contraction.	[41]
Environmental responsiveness	Au nanoparticles within dT-DMAEMA/HEMA hydrogels	The incorporation of gold nanoparticle carriers imparts pH-responsive electrochemical characteristics to the hydrogel: as the pH shifts from acidic to neutral, the hydrogel swells, increasing interparticle spacing and decreasing the conductivity of the composite, allowing for precise detection of pH changes.	[81]

The enhancement function	Types of hydrogels	Specific performance	Refs.
Biocompatibility of the metal nanoparticles	Dex-G5-Ag hydrogel	G5 dendritic polymers exhibit pH-responsive Ag release and mitigate Ag tissue toxicity: When the gel is immersed in a pH 5.0 buffer solution, approximately 17.6% of Ag is released from the gel within 24 hours, whereas when immersed in a pH 7.4 buffer solution, this value decreases to only 6%.	[82]
Biocompatibility of the metal nanoparticles	Ag-PEG- Heparin hydrogel	A multilayer hydrogel system can mitigate Ag hemolytic activity and reduce damage to normal tissues.	[83]
Long-term stability	Cu NPs-Starch hydrogel	Copper nanoparticles (Cu NPs) are encapsulated within the hydrogel matrix, safeguarding Cu NPs from the influence of reactive oxygen species (ROS) while preserving their antibacterial activity.	[84]

### 3.2 Hydrogels enhance the functionality of metal nanoparticles.

Metal nanoparticles have been widely employed in wound healing applications [33,85,86]. However, their application still faces numerous drawbacks, such as inadequate biocompatibility, a tendency to aggregate over time, impacting their biological performance, susceptibility to protein fouling and subsequent macrophage clearance, and toxicity due to accumulation within tissues [15,16,87]. Moreover, metal nanoparticles often fail to distinguish between different bacterial strains, potentially harming beneficial microorganisms essential for ecological balance. For example, studies by Hussain *et al.* revealed that even low-level exposure to Ag nanoparticles induced oxidative stress and mitochondrial dysfunction in rat liver cells [88]. Another investigation demonstrated the toxic impact of Ag nanoparticles on cytokine proliferation and expression in peripheral blood mononuclear cells [89]. In contrast, hydrogels provide a means to address these shortcomings of metal nanoparticles. Firstly, stimulus-responsive hydrogels can alleviate the potential toxicity associated with metal nanoparticles. When loaded within hydrogels, metal nanoparticles can release slowly, reducing tissue accumulation and subsequent toxicity. Research reports the synthesis of a pH-responsive Ag-nanoparticle dendritic polymer system that releases drugs in response to infection-induced pH changes, displaying excellent antibacterial activity alongside minimal cell toxicity [82]. Further studies suggest that incorporating Ag nanoparticles into a multilayer hydrogel system with PEG and heparin reduces hemolytic activity and minimizes damage to normal tissues [83]. Additionally, hydrogels can enhance the long-term stability of metal nanoparticles [90]. Copper nanoparticles can generate antibacterial effects similar to those of Ag<sup>+</sup> ions, but reduced oxidative activity compromises their stability and antibacterial efficacy. Incorporating Cu nanoparticles within a hydrogel matrix shields their surface from ROS impact while retaining antibacterial activity [84]. Thus, metal nanoparticle hybrid hydrogels can effectively mitigate limitations associated with metal nanoparticles for wound healing applications, leveraging their advantages while promoting wound healing. However, it is important to note that despite the reduced tissue accumulation and toxicity facilitated by hydrogels, there remains a possibility of prolonged deposition and toxic effects in organs such as the skin, liver, and kidneys with prolonged usage [33,35]. Therefore, further research into degradable metal materials is warranted to enhance the biocompatibility of metal nanoparticle-loaded hydrogels.

### 3.3 The synergy between hydrogels and metal nanoparticles

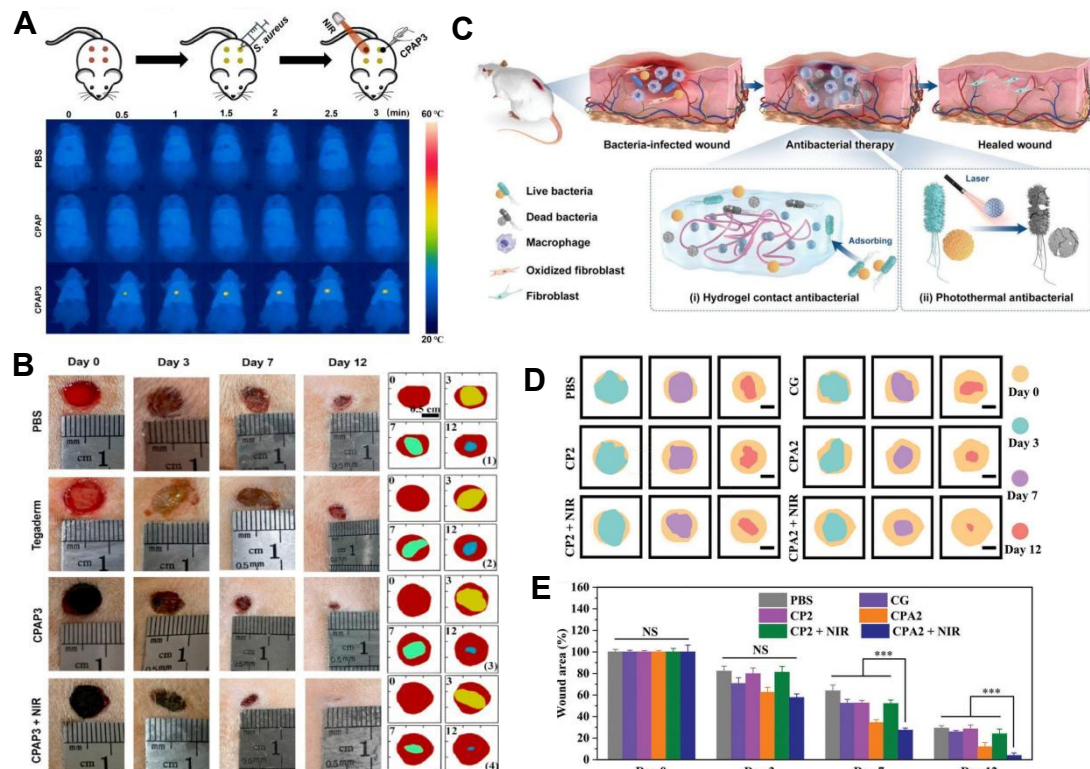
The combination of hydrogels and metal nanoparticles not only compensates for each other's deficiencies but also generates a powerful synergistic effect, such as synergistic antibacterial and wound healing properties.

The collaboration between hydrogels and metal nanoparticles exhibits a robust synergistic antibacterial function, which is illustrated in Figure 2. Hydrogels efficiently capture bacteria and, when combined with metal nanoparticles, achieve precise pathogen eradication. Moreover, encapsulating metal nanoparticles within hydrogel matrices significantly enhances their

343 photothermal capability, leading to synergistic antibacterial activity. For instance, by employing a  
344 reduction deposition method, Ag nanoparticles grown on the surface of polydopamine (PDA)  
345 nanoparticles displayed a remarkable increase in photothermal conversion efficiency to 36.1%  
346 (PDA @ Ag). Further embedding PDA@Ag nanoparticles into a polysaccharide (cationic guar  
347 gum, CG) network produced CG/PDA@Ag hydrogels [91]. As shown in Figure 2, the PDA@Ag  
348 nanoparticles were uniformly dispersed without aggregation, and the photothermal conversion  
349 efficiency of the designed CG/PDA@Ag system increased from 36.1% to 38.2% [91].  
350 Additionally, CG polysaccharide hydrogels, rich in functional hydroxyl and quaternary  
351 ammonium groups, interact with bacteria through electrostatic forces, van der Waals forces, and  
352 hydrophobic interactions, leading to nonselective capture and elimination of both gram-positive  
353 and gram-negative bacteria [91]. This provided supplementary antibacterial effects.

354 Furthermore, hydrogels and metal nanoparticles synergistically promote wound healing.  
355 Hydrogels effectively absorb wound exudate, prevent infection, and create a favorable  
356 microenvironment for healing [16,18–20]. They support and accelerate cell migration,  
357 proliferation, and tissue repair [21–23]. Metal nanoparticles, offering nanoenzyme activities  
358 similar to glucose oxidase and catalase, enhance the wound microenvironment. Their combined  
359 action significantly advances wound healing. For example, a combination of silver nanoparticles  
360 and epigallocatechin gallate synergistically regulated the expression of growth factors at injury  
361 sites, improving wound healing outcomes [92]. Additionally, composite materials combining gold  
362 nanoparticles with natural hydrogels have been shown to promote fibroblast migration and  
363 granulation formation and reduce inflammatory factors [37,93]. Studies have also demonstrated  
364 that an alloy of Au-Pt nanoparticles combined with oxidized hyaluronic acid (OHA) and  
365 carboxymethyl chitosan (CMCS) exhibited outstanding antibacterial and self-healing properties in  
366 hydrogel dressings (OHCs). The Au-Pt alloy nanoparticles acted as simulated glucose oxidase and  
367 catalase, enhancing wound microenvironment modulation [93]. Composite hydrogel dressings  
368 significantly improved wound microenvironments and accelerated the healing of diabetic wounds.  
369 It is important to note that while metal nanoparticles often endow hydrogels with excellent  
370 photothermal capabilities, appropriate temperatures can effectively promote wound  
371 microcirculation, elevate local oxygen levels, and accelerate wound healing.

372 The combination of metal nanoparticle-hydrogel complexes shows robust synergistic  
373 antibacterial and wound healing capabilities. They release potent metal ions for antibacterial  
374 effects, establish temporary barriers against pathogen invasion, regulate cell proliferation and  
375 differentiation, and achieve precise pathogen eradication through photothermal effects. As a  
376 potential solution to antibiotic resistance, composite antibacterial hydrogels hold promising  
377 prospects in the field of wound healing.



**Figure 2.** Metal nanoparticle hybrid hydrogels for treating infected wounds. (A) Schematic diagram of in vivo wound treatment evaluation of CPAP/PDA@Cu hydrogel photothermal performance, along with infrared thermographic images; (B) Photographic images and schematic illustration of wound contraction during the treatment of *Staphylococcus aureus*-infected wounds from Day 0 to Day 12: (1) PBS, (2) Tegaderm, (3) CPAP3 and (4) CPAP3 + NIR. Reproduced with permission from [94]. Copyright 2022, Elsevier.

(C) Schematic representation of the fabrication of the CG/PDA@Ag hydrogel and its application as a photothermal antibacterial platform for wound dressings. (D) Schematic diagram depicting wound contraction from Day 0 to Day 12 with different treatments for *Staphylococcus aureus*-infected wounds. (E) Wound area for each group (n = 3, \*\* p < 0.01, \*\*\* p < 0.001, NS indicates not significant). Reproduced with permission from [91]. Copyright 2022, Wiley-VCH GmbH.

#### 4. Various Types of MNHH

As shown in Table 2, various types of metal nanoparticles or nanomaterials containing metal components have been utilized in the preparation of MNHH. These include silver nanoparticles, gold nanoparticles, copper nanoparticles, and more. These hydrogels exhibit excellent mechanical properties, antimicrobial capabilities, and wound healing promotion, making them extensively applied in clinical wound management. The following sections will describe the characteristics and potential applications of different types of MNHH based on the types of metals used.

##### 4.1 MNHH based on Monometallic Nanoparticles

###### 4.1.1 Silver nanoparticle hybrid hydrogel

Throughout history, silver has been recognized for its antibacterial properties. Silver nanoparticles (Ag NPs) exhibit potent antimicrobial activity against a wide range of microorganisms, including drug-resistant bacteria, fungi, and viruses. Ag NPs utilize various mechanisms for antibacterial action, although a definitive mechanism is still under debate. The integration of silver nanoparticle carriers with hydrogels effectively prevents pathogenic colonization at wound sites. While the antibacterial mechanisms of Ag NPs remain contentious, their robust broad-spectrum antibacterial efficacy is undeniable. Currently, the antibacterial mechanisms of Ag NPs can be categorized into six types: cell membrane disruption, inhibition of the bacterial respiratory chain, induction of bacterial genetic toxicity, interference with bacterial protein synthesis and folding, induction of oxidative stress and ROS production, and light-induced damage to bacterial proteins [33,95].

Research indicates that the primary mechanism of antibacterial action of Ag NPs (silver nanoparticles) is the release of silver ions ( $\text{Ag}^+$ ). Composite materials of silver nanoparticle carriers and hydrogels exhibit potent antibacterial effects, effectively inhibiting common wound pathogens such as *Escherichia coli* and *Pseudomonas aeruginosa* while promoting wound healing. For instance, Baukum and colleagues employed solvent casting to create SA/gelatin hydrogels with crosslinked silver nanoparticle carriers using varying concentrations of calcium chloride ( $\text{CaCl}_2$ ) [96]. These doped Ag NPs significantly enhanced the mechanical properties of the hydrogel and endowed it with excellent antibacterial activity against *Staphylococcus aureus*, *Pseudomonas aeruginosa*, and *Escherichia coli* [96]. As illustrated in Figure 3, a composite PB@PDA@Ag containing silver nanoparticle carriers was prepared to treat MRSA (methicillin-resistant *Staphylococcus aureus*) infections in a diabetic model with laser assistance [97]. This combination strategy demonstrated synergistic effects in combating MRSA through cell membrane disruption, ROS production, ATP reduction, and oxidative GSH reduction, effectively accelerating wound healing in diabetic MRSA-infected wounds. Silver nanoparticle-hybrid hydrogels can establish physical barriers, prevent microbial invasion, reduce infection risks, and support fibroblast migration, thereby accelerating wound healing. For instance, Masood *et al.* reported the preparation of an Ag nanoparticle carrier-chitosan-polyethylene glycol (PEG) composite hydrogel. Compared to pure hydrogels, this Ag nanoparticle carrier hydrogel exhibited



improved mechanical strength and physical properties. It better maintained a microenvironment conducive to wound healing, accelerating wound healing in diabetes-induced rabbit models[98]. Moreover, hydrogels can enhance the stability of silver nanoparticles, thus prolonging their antimicrobial activity. For example, Obradovic *et al.* optimized a freeze–thaw technique based on alginate, polyvinyl alcohol (PVA), and poly(N-vinylpyrrolidone) (PVP) to produce Ag nanoparticle-loaded composite alginate microsphere hydrogels. This approach suppressed the tendency of silver nanoparticle carriers to aggregate, ensuring their stability[99]. Furthermore, silver nanoparticle-hybrid hydrogels exhibit superior mechanical properties and physicochemical characteristics compared to natural hydrogels [100].

Silver nanoparticle hybrid hydrogels possess numerous advantages, including antimicrobial properties, tissue regeneration promotion, and excellent mechanical performance, making them highly promising multifunctional wound dressings for enhancing wound healing. However, the clinical application of silver nanoparticle-hybrid hydrogels still faces challenges. First, the inhibition of gram-positive bacteria by silver nanoparticle carriers is inferior to their effect on gram-negative bacteria, possibly due to the stronger resistance of gram-positive bacteria's peptidoglycan cell walls. Second, silver nanoparticle carriers are cytotoxic to normal cells as well, and their accumulation in natural environments or human tissues such as skin, liver, and kidneys can pose potential toxicity risks in the long term. Last, despite the rarity of bacterial resistance to silver ions, with the increasing clinical use of silver nanoparticle-hybrid hydrogel materials, this issue remains worthy of attention. In designing silver nanoparticle carrier hydrogel composites, several aspects should be considered: enhancing the antibacterial capacity against gram-positive bacteria, prolonging the release time of antibacterial components, minimizing cytotoxicity to cells, and developing environmentally friendly in situ synthesis processes to avoid potential environmental and health concerns [7,32,90,101].

#### 4.1.2 Gold nanoparticle hybrid hydrogel

Although gold is generally considered biologically inert, gold nanoparticle carriers exhibit various biological functions and have been widely applied in the medical field. Compared to other metal nanoparticle carriers, such as silver and copper, gold nanoparticle carriers have minimal toxicity to human tissues and cells [71]. Gold nanoparticle carriers can be designed in different sizes or shapes, and when combined with hydrogels, they create biomaterials with enhanced mechanical properties, environmental responsiveness, biocompatibility, conductivity, and antimicrobial performance for wound management [102–106].

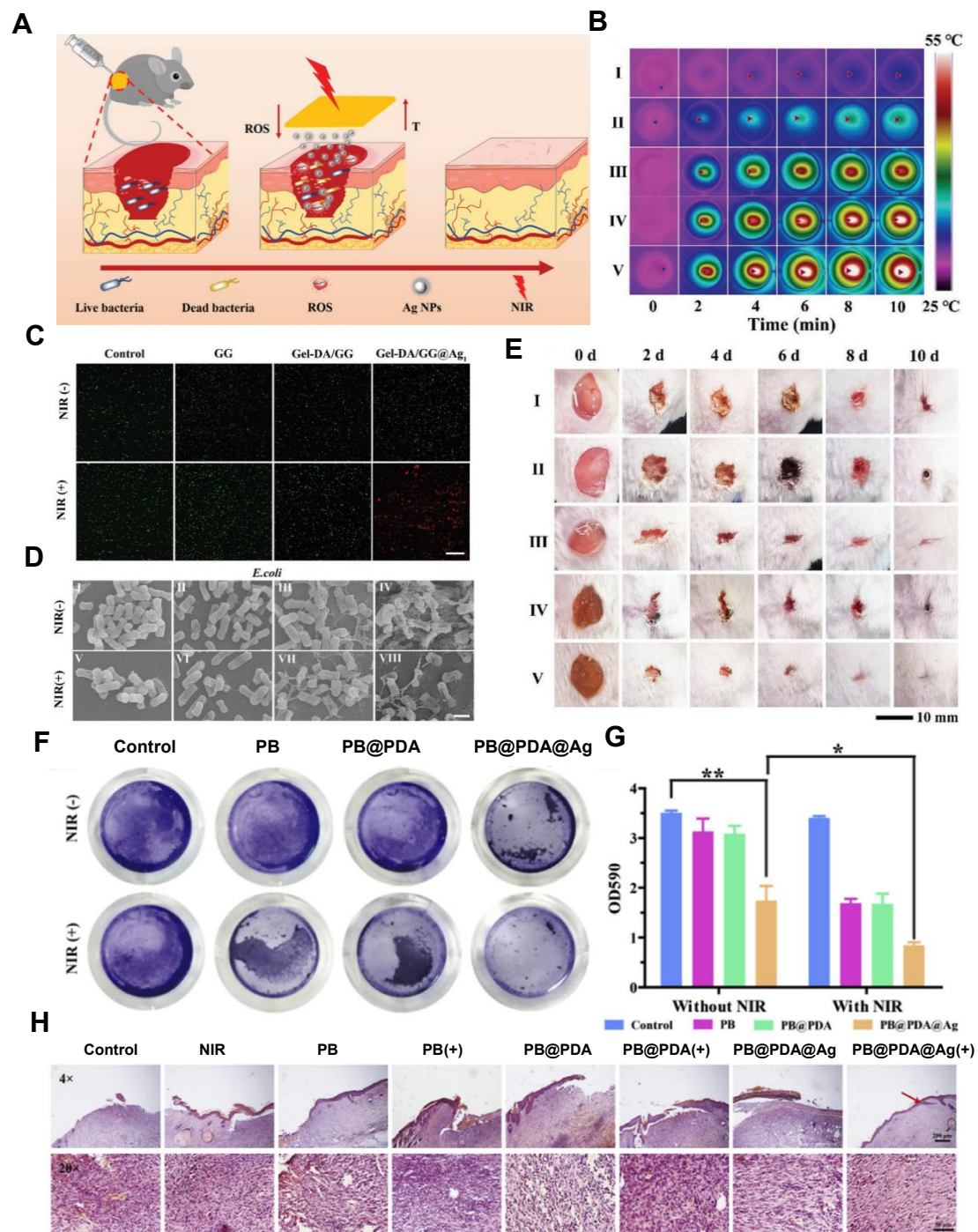
Most hydrogel scaffolds themselves are nonconductive, requiring additives to facilitate intercellular signal transmission, thus limiting their applications in the field of biotechnology [107]. Metal nanocarriers offer hydrogel conductivity enhancement while concurrently augmenting their mechanical performance, significantly advancing the applicability of hydrogel scaffolds in tissue engineering. Research has revealed that embedding gold nanocarriers within chitosan hydrogels generates scaffolds with electrical conductivity akin to cardiac tissue [108,109]. Furthermore, the

concentration of gold nanocarriers directly impacts scaffold conductivity and mechanical rigidity, thereby augmenting the phenotype expression and maturity of cardiac cells [108,109]. This composite material has been shown to enhance the regenerative capacity of myocardial cells post myocardial infarction, a finding of paramount significance for constructing engineered skin tissues in vitro [108,109]. Beyond the fortification of mechanical and conductive attributes, gold nanocarriers can also promote wound healing by inhibiting the growth of bacteria and fungi or stimulating the release of wound healing factors. Research has demonstrated that the antibacterial mechanism of gold nanocarriers against *Escherichia coli* involves hindering ATPase activity to disrupt membrane potential, concurrently suppressing the connection between ribosomal subunits and tRNA [110]. Gold nanocarriers can attach to bacterial membranes, leading to leakage of bacterial contents or permeation through the outer membrane and peptidoglycan layer, resulting in bacterial demise. Zahra and colleagues reported a composite of gold nanocarrier hydrogel synthesized through sunlight-assisted green methods, which exhibited heightened antibacterial activity. Moreover, this composite elevated the levels of the transcription factor NANOG and transmembrane adhesive protein CD34 in mouse wound sites, consequently promoting wound healing [55]. Furthermore, research has unveiled noticeable variations in antibacterial activity between gold nanocarriers of distinct shapes. Gold nanostars and gold nanoflowers exhibited greater antibacterial activity than gold nanospheres, with rod-shaped nanocarriers more effectively disrupting pathogenic biofilms. This observation may be attributed to the distinctive shapes of gold nanocarriers providing higher surface area-to-mass ratios and facilitating interaction with cell membranes [111,112].

Apart from their inherent antibacterial capabilities, gold nanogels can also be utilized for photothermal therapy (PTT) to combat bacterial infections. PTT, an effective strategy for treating bacterial infections using photothermal materials under visible light or near-infrared radiation, leverages tunable surface plasmon resonance effects under near-infrared radiation. Gold can be shaped into specific configurations and widely employed for PTT therapy [113]. Research has developed a novel soy protein-based hydrogel by utilizing oxidized dextran as a crosslinker and loading it with gold nanocarriers [114]. This hydrogel exhibited robust mechanical performance and photothermal antibacterial abilities against *Escherichia coli* and *Staphylococcus aureus* [114]. While photothermal therapy effectively counters bacterial infections, overheating may inadvertently damage nearby host cells or tissues. Therefore, Chen and collaborators devised a localized precise photothermal antibacterial strategy termed Thermal Destruction-Induced Relief of Interface [115]. This strategy involves a flexible base of polydimethylsiloxane with microchannels and a temperature-sensitive PNIPAm hydrogel loaded with gold nanocarriers [115]. The PNIPAm hydrogel undergoes contraction under near-infrared radiation, confining the heat generated by gold within the microchannels, thus achieving precise therapeutic aims [115].

Although the current antibacterial efficacy of gold nanocarriers may not match that of silver nanocarriers, gold nanocarriers possess unique advantages, bestowing upon gold nanogels a broad

505 spectrum of antibacterial properties, low cytotoxicity, superior conductivity, and mechanical  
506 strength. As a potentially influential adjunct, gold nanogel scaffolds have the potential to facilitate  
507 wound healing intelligently and precisely. When designing composite materials involving silver  
508 nanocarrier hydrogels, it is imperative to consider the following: enhancing antibacterial efficacy  
509 against gram-positive bacteria, prolonging the release duration of antibacterial agents, minimizing  
510 cytotoxicity, and developing environmentally and health-friendly in situ synthesis methods, as  
511 suggested by the literature [7,32,90,101].



**Figure 3.** MNHH based on monometallic nanoparticles is used for wound treatment. (A) Application of the Gel-DA/GG@Ag hydrogel to wound healing. (B) Photothermal effects of the Gel-DA/GG@Ag hydrogels. (C) Fluorescence images of *S. aureus* treated with different hydrogels. (D) Morphologies of *E. coli* treated with I) Control, II) GG, III) Gel-DA/GG, IV) Gel-DA/GG@Ag<sub>1</sub>, V) control + NIR, VI) GG + NIR, VII) Gel-DA/GG + NIR, and VIII) Gel-DA/GG@Ag<sub>1</sub> + NIR. Irradiation time: 10 min. Scale bars, 1  $\mu$ m. (E) Photographs of *S. aureus*-infected wounds with different treatments. I) Control, II) GG, III) Gel-DA/GG, IV)

520 Gel-DA/GG@Ag1, and V) Gel-DA/GG@Ag1 + NIR. Reproduced with permission from [116].  
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522 (F) Photographs of crystal violet-stained MRSA biofilms treated with different samples, including  
523 normal saline, NIR, PB, PB + NIR, PB@PDA, PB@PDA + NIR, PB@PDA@Ag, and  
524 PB@PDA@Ag + NIR. (G) Relative MRSA biofilm biomass treated with different materials.  
525 MRSA biofilm biomass was determined by measuring the absorbance at 590 nm. (H)H&E  
526 staining images of infected wound tissue after various treatments for 8 days. Reproduced with  
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## 4.2 MNHH based on metal oxide nanoparticles

Metal oxides refer to binary compounds composed of oxygen and another metallic chemical element, encompassing alkaline oxides, acidic oxides, amphoteric oxides, and more. Compared to elemental metals, metal oxides often possess greater stability, and when nanosized, they exhibit various catalytic activities (Figure 4).

Beyond inert metals such as silver and gold, other metal nanoparticles can also combine with hydrogels in the form of oxides. These nanoparticles release metal ions continuously on wounds, achieving antimicrobial and wound healing effects. These metal compounds include ZnO, CuO, iron oxides, MnO<sub>2</sub>, and more [86,117,118].

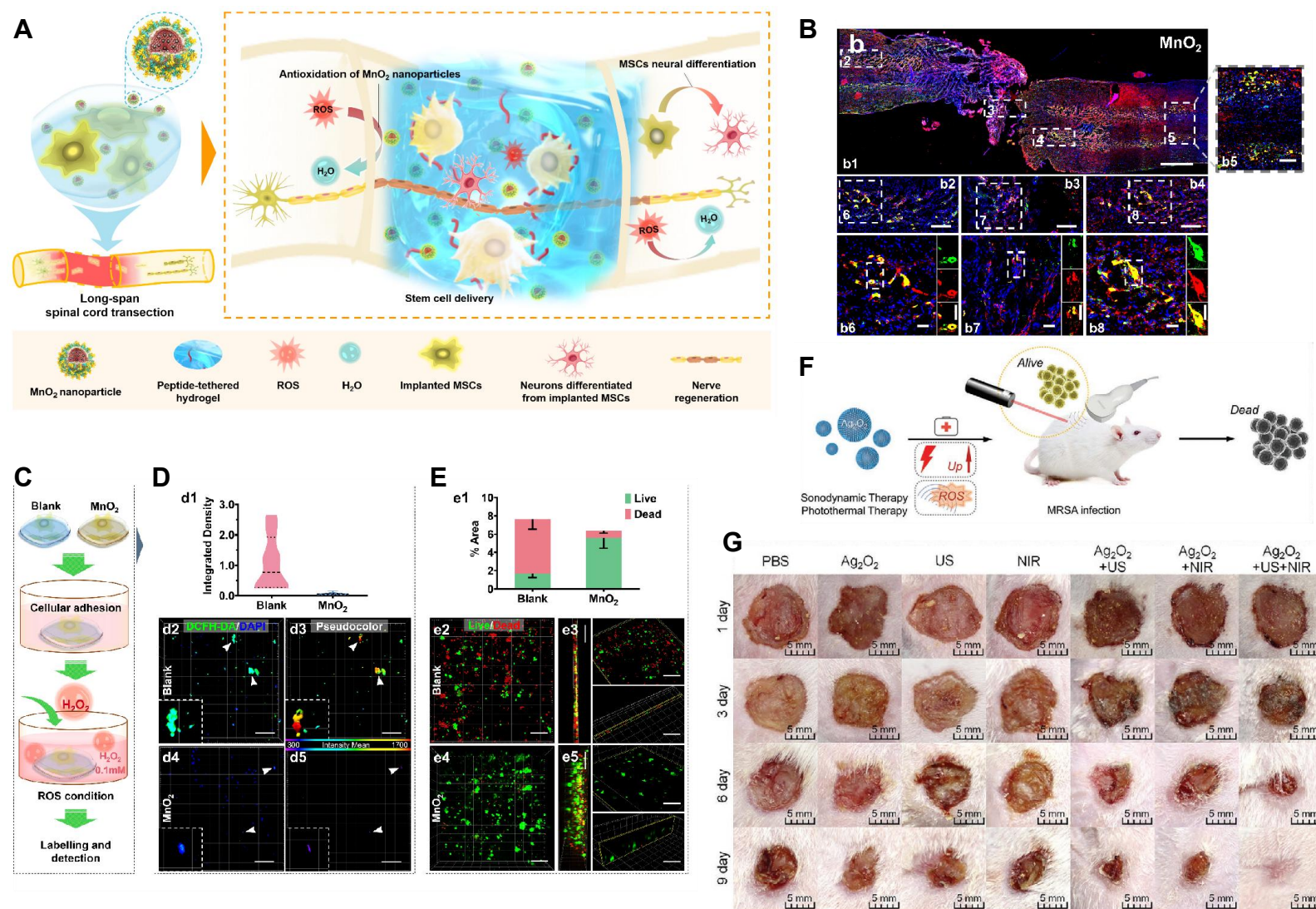
Zinc, as the most commonly used antibacterial agent, employs several mechanisms against microorganisms. ZnO nanoparticles exhibit antibacterial activity at suitable concentrations without cytotoxicity, making them widely used in cosmetic production. ZnO hydrogels demonstrate great potential in drug delivery and wound healing promotion. CMC-Zn-MEL composites containing ZnO nanoparticles exhibit antibacterial activity against both gram-positive and gram-negative bacteria, making them excellent wound dressing materials [119]. Despite relatively weaker antibacterial efficacy, ZnO nanoparticles possess low cytotoxicity, suggesting their potential for broader clinical applications. Moreover, research indicates that ZnO nanoparticles can facilitate bone tissue regeneration, implying their potential for tissue engineering applications [120,121].

Copper nanoparticles exhibit a bacterial killing efficiency comparable to that of silver nanoparticles. Although the antibacterial effect of hydrogels containing copper nanoparticles (Cu-nano/CuO-nano) is weaker than that of Ag-nano, they show broader spectrum antibacterial activity against fungi and bacteria [122–124]. Recent studies on CMC/CuO-nano composite hydrogels and CS hydrogels loaded with copper particles have demonstrated excellent antibacterial effects against *E. coli* and *S. aureus* without inducing toxicity [125,126]. In wound environments, copper nanoparticles are prone to oxidation, which reduces their stability and antibacterial efficacy. Incorporating copper nanoparticles into hydrogels can protect them from ROS effects, maintaining their antibacterial activity [127,128]. In addition to releasing copper ions for bactericidal effects, copper nanoparticle hydrogels can utilize the local surface plasmon resonance (LSPR) effect for photothermal pathogen elimination. Researchers have developed Cu nanoparticles using a polyol method and then incorporated them into biocompatible polysaccharide hydrogels, enhancing the stability of Cu nanoparticles. These hybrid hydrogels exhibit rapid self-healing capabilities and exceptional photothermal antibacterial performance [129]. Other studies have reported the in-situ formation of copper nanoparticles on polydopamine surfaces, followed by introduction into precursor polyelectrolyte hydrogels (CPAPs) to prepare hybrid hydrogels CPAP/PDA@Cu. This composite material prevents nanoparticle aggregation, demonstrating excellent photothermal antibacterial properties (PCE 55.4%) and electrostatic adsorption capacity for bacterial capture [94]. Such adaptive and potent antibacterial dressings hold significant potential for treating infected wounds [94].

Other metal oxide hydrogel composites also exhibit various biological functions, including antibacterial properties, stimuli-responsive drug release, and tissue regeneration promotion. Recent reports have indicated that hydrogels containing magnesium oxide nanoparticles also combat microorganisms through multiple mechanisms [130–132]. Hesaveh *et al.* incorporated MgO nanoparticles into hydrogels derived from hydroxypropyl  $\kappa$ -carrageenan to control drug delivery in gastrointestinal studies [133]. Furthermore, research has employed chitosan hydrogel microbeads containing superparamagnetic iron oxide nanoparticles (SPIONs) for stimulus-responsive release of vancomycin [134]. Metal oxides can also confer characteristics such as magnetic heating to hydrogels, further expanding the application scope in wound management, artificial skin, and more. Research has embedded GO-Fe<sub>3</sub>O<sub>4</sub> nanoparticles in poly(N-isopropylacrylamide), alginate-interpenetrated polymer hydrogels, developing an innovative nanocomposite hydrogel microcapsule drug delivery system [135].

These metal nanoparticle hybrid hydrogels (MNHHs) offer multiple effective pathways to combat infections, with few reported cases of bacterial resistance. They prove to be efficient strategies against antibiotic-resistant microorganisms. The stability of metal nanoparticles ensures sustained antimicrobial effects, even after release from dead cells, allowing them to continue eradicating other microbial cells. Furthermore, composite materials can achieve pathogen eradication through photothermal effects and offer controlled drug delivery systems locally through stimulus-responsive behaviors. Last, such composite materials exhibit superior biocompatibility, enhanced mechanical strength, flexibility, and self-healing properties, making them ideal candidates for creating wound coverings.





587 **Figure 4.** Applications of metal oxide nanoparticles. (A)  $\text{MnO}_2$  NPs improve the survival, integration and neural differentiation of transplanted MSCs and promote



588 nerve tissue regeneration by mitigating the oxidant microenvironment. (B) Nerve fibers were significantly regenerated by the MnO<sub>2</sub> nanoparticle (NP)-dotted  
 589 hydrogel across the whole tissue (b1) with integrated MSCs (green) colocalizing with NF (red), the marker of mature neurons. MSCs integrating into the distant (b2)  
 590 and adjacent (b4) regions exhibited a larger total amount of 21 wells and a higher proportion of neural differentiation compared to those sustained in the lesion site  
 591 (b3). Caudal distant segments of the tissue (b5) showed the same result as that in the rostral side (b2). Micrographs in (b6-b8) show magnified views of the boxed  
 592 fields in (b2-b4). Separated NF and GFP-MSC channels of the boxed cells in (b6-b8) are shown in detail and presented on the right of each micrograph. Scale bar, 1  
 593 mm (b1), 200  $\mu$ m (b2-b5), 50  $\mu$ m (b6-b8). (C). MSCs were encapsulated in the hydrogels and allowed to adhere overnight before being exposed to the ROS  
 594 microenvironment-simulating medium containing 0.1 mM H<sub>2</sub>O<sub>2</sub>. (D) After 24 h, the intracellular ROS levels of MSCs were quantified (d1) in the blank (d2, d3) and  
 595 MnO<sub>2</sub> NP-dotted (d4, d5) hydrogels after dichlorodihydrofluorescein diacetate (DCFH-DA) labeling (n=3), demonstrating the effective antioxidant impact of the  
 596 MnO<sub>2</sub> NP-dotted hydrogel on MSCs. Green, DCFH-DA; blue, DAPI. The fluorescence of DCFH-DA in (d2, d4) was analyzed using pseudocolor (d3, d5) according  
 597 to mean intensities to further show more detailed differences. € Cytoviability of the MSCs after 24 h of incubation was analyzed by Live/Dead assay. Numbers of  
 598 live cells (green) and dead cells (red) were quantified in terms of stained areas (e1). Data in the graph are presented as the average  $\pm$  SD (n= 9 views). Representative  
 599 images of the cells in the blank (e2, e3) and MnO<sub>2</sub> NP-dotted (e4, e5) hydrogels are presented, with n= 3 hydrogels for each group. Scale bar, 100  $\mu$ m (D and E).  
 600 Reproduced with permission from [136]. Copyright 2019, American Chemical Society.

601 (F) Schematic illustration of the combined antibacterial sonodynamic and photothermal therapy in an MRSA-infected murine model with Ag<sub>2</sub>O<sub>2</sub> NPs. (G)  
 602 Representative images of wounds infected with MRSA in seven different treatment groups on days 1, 3, 6, and 9. Reproduced with permission from [137]. Copyright  
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#### 4.3 MNHH based on multiple metal materials

In addition to loading single-metal nanoparticle hydrogels, there is also research focused on creating composite hydrogels containing two or more types of metal nanoparticles. Compared to hydrogels with single-metal nanoparticles, the synergistic effects arising from alloy interactions introduce many pleasantly surprising new properties to these composite materials: enhanced antimicrobial efficiency, reduced cytotoxicity, and heightened stimulus-responsive capabilities [85,138–140].

Multimetal nanoparticle composites can be utilized to enhance antimicrobial efficiency while simultaneously reducing their toxicity to cells. Research has been conducted using gold-silver nanoparticles with an average size of 10 nm loaded into chitosan to create CS-Au-Ag wound dressings [85]. CS-Au-Ag wound dressings exhibited faster, higher, and more sustained release of silver ions compared to chitosan dressings loaded with the same silver content (CS-Ag), thus demonstrating enhanced antimicrobial activity [85]. These findings suggest that reducing the silver content can mitigate the cell toxicity that limits further applications of silver nanoparticles, making them a promising material for wound dressings [85]. Multimetal composites have also exhibited good antimicrobial activity against multidrug-resistant bacteria [141]. Research has employed biopolymer starch as a reducing and capping agent for the environmentally friendly, repeatable, and simple synthesis of Ag/Au bimetallic nanoparticles. These nanoparticles demonstrated excellent antimicrobial performance against multidrug-resistant *Escherichia coli* and methicillin-resistant *Staphylococcus aureus*, promoting wound healing and reducing scar formation [142]. Furthermore, Imran *et al.* utilized zinc oxide (ZnO) coverage on biogenic gold nanoparticles obtained from Hibiscus plant extracts to synthesize Au@ZnO core-shell nanocomposites [140]. The synthesized nanocomposites aided in generating reactive oxygen species (ROS), exhibiting antibacterial and antibiofilm activities against *Staphylococcus aureus* and methicillin-resistant *Staphylococcus aureus* (MRSA) [140]. Simultaneously, these nanocomposites reduced their toxicity toward mouse fibroblasts under normal and high glucose conditions, promoting wound healing [140]. Similarly, research designed Ag/CaO nanocomposites (NCs) that demonstrated effective antibacterial activity against *Staphylococcus aureus* and MRSA [143]. The formation of NCs maintained the antibacterial efficacy of silver nanoparticles while decreasing their toxicity to mammalian cells [143].

Alloy interactions can also enhance metal-stimulus responsiveness. It has been found that combining silver nanoparticles with iron oxide confers new magnetic responsiveness to the material [144]. The presence of iron imparts magnetic responsiveness to Ag/Fe<sub>3</sub>O<sub>4</sub> NCs, allowing them to penetrate and disrupt biofilms under a magnetic field, effectively inhibiting wound infections [144]. Compared to pure silver nanoparticles, Ag/Fe<sub>3</sub>O<sub>4</sub> NCs exhibit lower silver release, less ROS generation, lower cell toxicity, and higher antibacterial efficacy [144]. This presents a potential avenue for developing novel treatment strategies for chronic wound infections.

641 Additionally, studies have reported combining silver with nanomaterials such as ZnO and MgO,  
642 resulting in superior photocatalytic and antibacterial activities [145–147].

643 Therefore, multimetal nanoparticle hybrid hydrogels can introduce new environmental  
644 responsiveness for precise therapeutic applications. Through their synergistic effects, diverse  
645 physicochemical properties, and varied mechanisms, bimetallic nanocomposite hydrogels,  
646 synthesized by combining two distinct metals, showcase enhanced antibacterial efficiency and  
647 lower tissue toxicity compared to monometallic hydrogels. They have emerged as effective tools  
648 to combat emerging drug-resistant bacteria and promote wound healing.

649 Table 2. Hybrid hydrogels loaded with different kinds of metal nanoparticles

Metal Nano Types		Hydrogel Types	Functions	Refs.
Noble metal	Ag	SA/gelatin hydrogel; Polyacrylamide (PAM)/Polyvinyl alcohol (PVA); Composite alginate hydrogel; Chitosan-polyethylene glycol (PEG) hydrogel.	Mechanical properties/stability/biocompatibility/antibacterial performance: Ensured the stability of silver nanoparticles; Significantly enhanced the mechanical properties of the hydrogel; Robust antibacterial performance; Improved tissue compatibility.	[90,91,95,97–101,148]
	Au	Chitosan hydrogel; Poly(N-isopropylacrylamide) (PNIPAm) hydrogel; Soy protein hydrogel.	Mechanical properties/conductivity/environmental responsiveness/antibacterial performance: Amplified the antibacterial performance of the hydrogel; Enhanced the mechanical strength of the hydrogel; Elevated the hydrogel's conductivity, facilitating intercellular signal transmission; Augmented NANOG/CD34 expression, promoting wound healing; Imparted photothermal therapy (PTT) antibacterial effect to the hydrogel.	[74,109–115]
	Pt	PEG hydrogel; PVP hydrogel; OHA-CMCS hydrogel; Polyaniline hydrogel.	Conductivity/environmental responsiveness/antibacterial performance: Enhanced the photothermal therapy (PTT) effect of the hydrogel, leading to microbial eradication; Provided catalase activity to improve wound oxygenation; Offered conductivity, serving as a biosensor.	[93,149–151]

Metal Nano Types		Hydrogel Types	Functions	Refs.
Metal oxides	Pd	Agarose-chitosan hydrogel; 4arm-PEG-thiol hydrogel.	Stability/environmental responsiveness/antibacterial performance: Nanomaterials utilized as crosslinking agents to enhance the stability of hydrogels; Augmented PTT/PDT effects for bacterial and tumor cell eradication; Precisely controlled drug release.	[152,153]
	Iron oxide	PNIPAM hydrogel; paeonol-aldehyde (PA) and quaternized chitosan (QCS) hydrogel; PANI-P (AAm-co-AA) hydrogel.	Mechanical properties/conductivity/environmental responsiveness/antibacterial performance: Impart magnetic responsiveness to hydrogels, enabling effective penetration through wound biofilms; enhance photothermal therapy (PTT) effect for controlled drug release; create dual dynamic bond crosslinks to bolster mechanical properties of hydrogels; provide conductivity for use as a biosensor; mediate hydroxyl radical generation through catalytic degradation of hydrogen peroxide (CDT), leading to tumor cell destruction.	[117,121,135,154–156]
	Zinc oxide	Chitosan hydrogel; Alginate hydrogel.	Mechanical properties/biocompatibility/antibacterial performance: Enhance the antimicrobial efficacy, bioreactivity, and mechanical properties of composite materials; promote tissue regeneration.	[120,121,157,158]

Metal Nano Types		Hydrogel Types	Functions	Refs.
polymetallic	Copper oxide	Polyvinyl alcohol (PVA) hydrogel; Carboxymethyl cellulose hydrogel; Starch hydrogel; Gelatin modified with methyl acrylate (Gel-MA) hydrogel; CPAP/PDA hydrogel.	Self-healing properties/environmental responsiveness/antibacterial performance: Improve the self-healing capability of hydrogels; boost photothermal therapy (PTT) performance of hydrogels; stimulate fibroblast proliferation; enhance hydrogel's antibacterial potential, effectively targeting fungi.	[118,122–125,127,128,159,160]
	Manganese oxide	PEGMA-co-GMA-co-AAm (PPGA) hydrogel; HA-ADH hydrogel; Starch hydrogel; Pluronic F127 hydrogel; Silk fibroin (SF)/Carboxymethyl cellulose (CMC) hydrogel; Polydopamine (DSAMP) hydrogel.	Environmental responsiveness/lipase-like activity/antibacterial performance: Clear ROS, generate oxygen, modulate wound microenvironment, alleviate inflammation; reinforce hydrogel's antibacterial and antifungal properties; endow hydrogel with photocatalytic capabilities (PTT); confer peroxidase activity to hydrogel.	[136,161–164]
	Ag+Au	Chitosan hydrogel; iota carrageenan (CA)- poloxamer 407 (F127) hydrogel.	Mechanical properties/environmental responsiveness/biocompatibility/antibacterial performance: Enhance hydrogel mechanical properties; improve silver ion release, reduce cytotoxicity of silver nanoparticles; exhibit excellent biocompatibility and near-infrared (NIR) photothermal responsiveness.	[139,141,165–167]

Metal Nano Types	Hydrogel Types	Functions	Refs.
		Stability/environmental	
Au/Ag+ZnO	Carboxymethyl cellulose (CMC) hydrogel; polyethylene glycol (PEG) hydrogel.	responsiveness/biocompatibility/antibacterial performance: Enhance the antimicrobial capability of hydrogels; reduce the cytotoxicity of gold/silver nanoparticles; maintain the stability of metal nanoparticles and PDT performance.	[140,145,165,168–170]
Au+Pt	Oxidized hyaluronic acid (OHA)/carboxymethyl chitosan (CMCS) hydrogel; hyaluronic acid hydrogel; polydopamine (PDA) hydrogel.	Environmental responsiveness/lipase-like activity: Provide glucose oxidase and catalase activity to improve the diabetic wound microenvironment; enhance photothermal conversion efficiency (PCE) up to 81.78%; eliminate the ROS generated as byproducts during the PTT process.	[138,171–173]
Ag+ Fe <sub>3</sub> O <sub>4</sub>	Starch-based hydrogel.	Environmental responsiveness/antibacterial performance: Hybrid hydrogels exhibit magnetic responsiveness, facilitating the penetration of silver nanoparticles through biofilms and enhancing antibacterial efficacy.	[144,171,174,175]
Pt+Pd	PEG hydrogel; HA hydrogel.	Environmental responsiveness/lipase-like activity: Imparting catalase (CAT)-like and peroxidase (POD)-like activities, as well as photothermal therapy (PTT) capability, to the hydrogel.	[176,177]

## **5. The application of metal nanoparticle-hybrid hydrogels in wound healing.**

An ideal wound dressing aims to fulfill the following functions: maintaining moisture, allowing gas exchange, preventing microbial growth, providing insulation, ensuring biocompatibility, offering mechanical strength, ensuring sterility, being easy to remove, and cost-effectiveness. Apart from these fundamental considerations, modern dressings should also possess attributes such as absorbing exudate, aiding cell adhesion and proliferation, and loading and releasing antimicrobial agents or growth factors as therapeutic agents. Loaded metal nanoparticle hydrogel materials exhibit excellent mechanical properties, potent antimicrobial capabilities, environmental responsiveness, the ability to regulate cell differentiation and proliferation, and remarkable tissue compatibility. These characteristics make them ideal materials for creating antimicrobial wound dressings and tissue-engineered skin. As depicted in Table 3, these composite materials have been widely employed in the treatment and management of chronic wounds and burn injuries.



664 Table 3. Application of metal nanoparticle hybrid hydrogels in the field of wound healing.

Application	Hydrogel Types	Therapeutic Effects	Refs.
Chronic Wounds	Chitosan-PEG-Silver Nitrate-Based Hydrogel	The hydrogel ensures a continuous and stable release of silver ions, effectively combating bacterial infections. The silver nanoparticle-infused hydrogel exhibits higher porosity, increased swelling capacity, and elevated water vapor transmission rate (WVTR). Furthermore, it enhances antioxidant properties and promotes the healing of diabetic rabbit wounds.	[56]
	QCT-Ag NPs-Carbopol 934 hydrogel	Enhanced effectiveness against <i>Staphylococcus aureus</i> and <i>Escherichia coli</i> ; Increased percentage of epithelialization in diabetic wound healing.	[178]
	Au-Pt-OHC hydrogel	Metal nanoparticles in synergy with carboxymethyl chitosan (CMCS) exhibit antibacterial properties, protecting the wound site; Metal nanoparticles possess similar activities to glucose oxidase (GOD) and catalase (CAT), which can lower blood sugar, reduce oxidative damage, provide oxygen, improve the pathological microenvironment of diabetic wounds, and facilitate wound healing; The dynamic cross-linking through Schiff base reaction imparts excellent self-healing properties to the OHCN hydrogel dressings.	[138]
	PB@PDA@Ag hydrogel	The hydrogel demonstrates excellent photothermal therapy (PTT) performance, capable of disrupting cell integrity under laser irradiation, generating reactive oxygen species (ROS), and reducing ATP and oxidized GSH to synergistically combat MRSA. Simultaneously, the hydrogel mitigates local inflammatory responses and upregulates wound VEGF expression, effectively accelerating the healing of diabetic wounds infected with MRSA.	[97]

Application	Hydrogel Types	Therapeutic Effects	Refs.
Acute Wounds	MnO <sub>2</sub> -silk fibroin (SF)-carboxymethyl cellulose (CMC) hydrogel	The hydrogel exhibits injectability, suitable for irregular wounds in diabetes; encapsulated MnO <sub>2</sub> nanoparticles can catalyze excessive ROS, alleviate wound oxidative stress, promote angiogenesis, and reduce inflammation levels; the hydrogel can counteract the overexpression of matrix metalloproteinases (MMPs) in diabetic wounds (over 80%) and facilitate extracellular matrix remodeling; the nanocomposite hydrogel accelerates diabetes wound healing, with wound healing rates >76% in 7 days and 100% in 14 days.	[161]
	(HA-DA) -PDA-Ti <sub>3</sub> C <sub>2</sub> MXene hydrogel	The HA-DA molecules regulate macrophage polarization from M1 to M2 to achieve anti-inflammatory effects; the hydrogel exhibits mild PTT capabilities and controlled oxygen release; it clears excessive ROS from wounds, maintaining intracellular redox homeostasis and alleviating oxidative stress; possessing multifunctionality such as tissue adhesion, self-healing, injectability, and hemostasis, combined with gentle photothermal stimulation, greatly promotes proliferation and migration of human umbilical vein endothelial cells, facilitating the healing of infected diabetic wounds.	[179]
	Collagen (GT)-Ag NPs hydrogel	The GT/Ag freeze-dried hydrogel exhibits a swelling ratio of up to 4000%, effectively absorbing exudate from burn wounds and allowing gas exchange. It demonstrates excellent bactericidal effects against methicillin-resistant <i>Staphylococcus aureus</i> (MRSA) and <i>Pseudomonas aeruginosa</i> (PA), effectively removing biofilms. The hydrogel also possesses remarkable hemostatic capability. It promotes contraction of infected burn wounds, deposition of collagen protein, and angiogenesis while reducing inflammation. The hydrogel maintains stability in wound environment and degrades	[180]

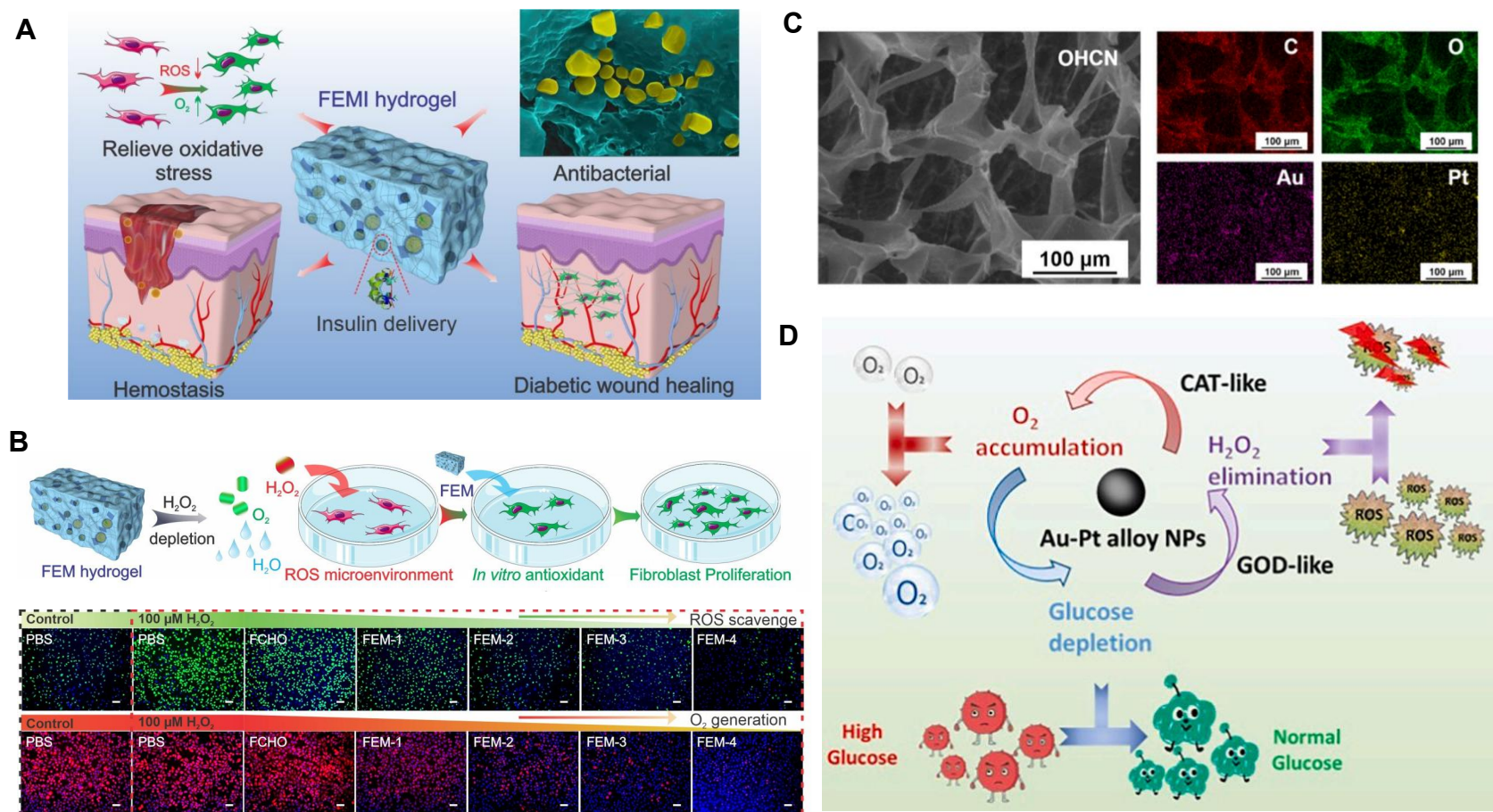
Application	Hydrogel Types	Therapeutic Effects	Refs.
		at a moderate rate (4 weeks), minimizing the discomfort of frequent dressing changes.	
	Human amniotic membrane (HAM)- Ag NPs- carbopol 934 hydrogel	The hydrogel exhibits antibacterial activity against both gram-positive and gram-negative bacteria. It possesses anti-inflammatory properties, stimulates angiogenesis, and promotes fibroblast migration. It significantly accelerates burn wound healing, as evidenced by a wound contraction percentage of $96.1 \pm 0.27\%$ after 20 days ( $p < 0.0001$ ) and an epithelialization period of $23.67 \pm 2.05$ days ( $p < 0.01$ ).	[181]
	Silver nanoparticle-thermosensitive methylcellulose (MC) hydrogel	Exhibiting excellent antibacterial activity against a variety of bacteria by 99.9%, effectively promoting collagen regeneration in burn wound surfaces, and accelerating the healing process.	[182]
Implants	Dex-G5-Ag hydrogel	The hydrogel exhibits pH-responsive release of antibacterial agents, displaying effective antibacterial activity against both gram-negative bacteria ( <i>Escherichia coli</i> and <i>Pseudomonas aeruginosa</i> ) and gram-positive bacteria ( <i>Staphylococcus epidermidis</i> and <i>Staphylococcus aureus</i> ); no significant hemolytic toxicity, cytotoxicity, tissue, or biochemical toxicity is observed upon cell incubation or implantation.	[183]
	A poly (hydroxyethyl methacrylate)–Ag nanoparticle porous	The hybrid hydrogel exhibits robust antibacterial efficacy against both gram-positive bacteria ( <i>Staphylococcus aureus</i> ) and gram-negative bacteria ( <i>Escherichia coli</i> ). Additionally, it demonstrates diminished immune response, showcasing in vivo resistance to foreign body reaction	[184]

Application	Hydrogel Types	Therapeutic Effects	Refs.
Tissue Engineering	hydrogel	(FBR), effectively preventing the formation of collagenous capsules.	
	Ag-starPEG-heparin hydrogel	The hydrogel maintains a prolonged antibacterial effect against strains of <i>Escherichia coli</i> and <i>Staphylococcus epidermidis</i> . Simultaneously, it demonstrates excellent hemocompatibility, with no evident hemolytic effects observed.	[185]
	Gold nanorod/GelMA/alginate hydrogel	Hydrogels can mimic the extracellular matrix (ECM) in vitro, providing cells with an ideal 3D culture environment. The presence of gold nanorods enhances cell adhesion and intercellular communication, promoting cell attachment, proliferation, and differentiation.	[58,73]
	Hydroxyethyl cellulose (HEC) combined with silver nanoparticles (Ag NPs)	The composite material combines the characteristics of low toxicity, antibacterial, anti-inflammatory, and tissue regeneration promotion, making it highly suitable for applications in skin tissue engineering.	[186]
	Chitosan-gelatin/ZnO nanocomposite hydrogel scaffold (CS-GEL/nZnO)	The hydrogel exhibits a high porosity (pore size ranging from 50–400µm) with well-distributed ZnO. It demonstrates enhanced swelling, biodegradability, and antibacterial properties. It can effectively control drug release and shows good compatibility with normal human skin fibroblasts. In situ synthesis of ZnO enhances its antibacterial efficacy and reduces cytotoxicity, making it an ideal material for skin tissue engineering.	[187]

## 5.1 Chronic Wounds

Chronic wounds, such as diabetic foot ulcers and pressure sores, often result in complications due to slow healing and an increased risk of infection. In such cases, microbial invasion further delays healing, creating a vicious cycle. Bacteria that colonize within the wound can rapidly develop into biofilms. The presence of biofilms varies significantly on the foundation of skin damage. These biofilms hinder wound healing through pathways such as inhibiting epithelialization, inducing prolonged chronic inflammation in the local environment, promoting cell apoptosis, and generating reactive oxygen species (ROS) [188–190]. Therefore, treating chronic wounds necessitates not only promoting recovery but also prioritizing pathogen inhibition. Wound dressings should possess enhanced antibacterial properties to address these challenges [5].

Metal nanoparticle hybrid hydrogels, with silver nanoparticles (Ag NPs) as a representative, perfectly align with the therapeutic demands of chronic wounds by effectively restraining biofilm growth and creating a microenvironment conducive to wound healing (Figure 5). Silver nanoparticle hydrogels exhibit notable antibacterial effects against common wound pathogens such as *Staphylococcus aureus* and *Pseudomonas aeruginosa*, especially showing remarkable antibacterial efficacy against various drug-resistant strains [33]. For instance, Reena *et al.* developed a quercetin (QCT)-Ag NP composite hydrogel for the synergistic treatment of chronic diabetic wounds [178]. Compared to plain hydrogels, the QCT-Ag NP hydrogel exhibited enhanced therapeutic effects against *Staphylococcus aureus* and *Escherichia coli*, significantly accelerating wound healing in diabetic wound models and improving re-epithelialization [178]. Apart from silver nanoparticle composites, gold nanoparticle hydrogel composites have also been shown to accelerate wound healing in diabetic wounds. Multiple studies highlight that composites combining gold nanoparticles with naturally derived materials such as cellulose, chitosan, alginate, and dextran can stimulate fibroblast migration and granulation while reducing wound inflammation [35,55,93,111]. A multifunctional self-healing hydrogel dressing containing Au-Pt alloy nanoparticles was reported to regulate the complex wound microenvironment, accelerating diabetic wound repair [93]. This material demonstrated excellent antibacterial and self-healing properties, along with functions such as blood glucose reduction and oxidative damage mitigation, significantly enhancing the pathological microenvironment and expediting the healing process of diabetic wounds [93]. Therefore, metal nanoparticle hybrid hydrogels are effective in maintaining a moist, sterile wound environment, suppressing drug-resistant bacterial colonization, modulating cell proliferation and differentiation, and promoting wound healing. These hybrid hydrogels offer a promising solution for the treatment of chronic wounds such as diabetic foot ulcers.



**Figure 5.** The application of metal nanoparticles hybrid hydrogels in the treatment of chronic wounds. (A) The FEMI hydrogel constructed an instructive microenvironment to ameliorate inflammation, accelerate cell proliferation, promote angiogenesis, enhance granulation tissue formation and re-epithelialization, and

702 stimulate MDR bacteria-infected diabetic wound healing in vivo. (B) Oxygen generation catalyzed by the MnO<sub>2</sub> nanosheets in the FEM hydrogel alleviated  
703 oxidative stress in L929 cells. Reproduced with permission from [162]. Copyright 2020, American Chemical Society.

704 (C) Representative SEM and EDS mapping images of the Au-Pt alloy NPs@OHC hydrogel. (D) The mutually reinforcing mechanism of GOD-like and CAT-like  
705 activities of Au-Pt alloy NPs, through which they effectively enhanced glucose depletion, ROS elimination and O<sub>2</sub> generation. Reproduced with permission from  
706 [138]. Copyright 2022, Elsevier.

## 5.2 Burns

The causes of death from extensive burns are often the result of bacteria infiltrating the body through the wound, leading to sepsis [191]. Hydrogels are potent candidate materials for burn wound dressings due to their natural biocompatibility and biodegradability, promoting collagen deposition and wound contraction to aid healing. However, many hydrogels lack the mechanical strength and antibacterial efficiency required to create a sterile environment conducive to wound healing [15,16]. Silver sulfadiazine is a standard antibacterial agent for burn wounds, but its topical use may cause various side effects, such as leukopenia, silver dermatitis, and kidney and liver toxicity, making it unsuitable for prolonged use [33].

Compared to traditional treatments, silver nanoparticle hydrogels demonstrate enhanced mechanical properties and excellent antibacterial and healing performances while avoiding the multiple side effects associated with conventional silver sulfadiazine. Silver nanoparticle hydrogels exhibit better antibacterial effects against multidrug-resistant bacteria. Research has incorporated Ag nanoparticles into thermosensitive methylcellulose (MC) hydrogels for treating burn wounds [182]. In comparison to silver sulfadiazine cream, the composite inhibits bacterial cell proliferation, disrupts biofilm matrix stability, and displays stronger antibacterial efficacy with lower toxicity, thereby promoting burn wound healing[182]. Further studies have developed a gel based on gelatin (GT) and silver nanoparticles (Ag NPs), which showcases high water absorption, along with effective antibacterial and antibiofilm activities to promote burn wound healing[180]. The composite swelling rate is as high as 4000%, effectively absorbing wound exudates and allowing gas exchange. It exhibits excellent antimicrobial effects against methicillin-resistant *Staphylococcus aureus* (MRSA) and *Pseudomonas aeruginosa* (PA), common pathogens in burn wounds, effectively removing mature biofilms. This gel demonstrates superior hemostatic ability compared to commercial gelatin sponges and alleviates pain when dressings are removed from the wound [180].

Beyond infection control and promoting wound healing, composite materials can also provide real-time monitoring of burn wound infections through their environmental responsiveness. Recent studies have built gold nanoparticle hybrid hydrogels based on label-free surface-enhanced resonance Raman scattering (SERRS) for detecting infections by *Pseudomonas aeruginosa* in burn wounds [192]. By uniformly embedding Au nanorods, Au nanospheres, and Au nanorods in a superlattice within the hydrogel, the composite creates various sensitivities and spatial resolutions to quantify pyocyanin, allowing for imaging of its spatial distribution within the biofilm [41]. This holds significance for monitoring burn wound infections in patients and providing timely treatment.

Metal nanoparticle hybrid hydrogels combine the benefits of hydrogels and metal nanoparticles, demonstrating superior antibacterial effects and low cytotoxicity compared to traditional wound antibacterial agents. Moreover, these composites possess various environmental



responsiveness traits, holding potential for creating multifunctional burn wound dressings with wound monitoring, intelligent drug release, and composite antibacterial properties.

### 5.3 Implants

Patients with extensive burns or chronic wounds often require long-term placement of catheters for corresponding treatments, and catheter-related infections are a common cause of sepsis in these patients [191].

Silver coatings effectively reduce the incidence of catheter-related infections, but silver-loaded and silver nanoparticle systems often exhibit hemolytic properties that hinder their long-term use [193]. Silver nanoparticle hydrogels can mitigate hemolysis and enhance the biocompatibility of catheter coatings, maintaining the antimicrobial activity of silver nanoparticles while partially mitigating foreign body reactions. Studies have shown that incorporating Ag nanoparticles into a multilayer hydrogel system composed of PEG and heparin reduces its hemolytic activity [185].

Stimuli-responsive hydrogels provide another potential approach to mitigate silver toxicity. Research has designed a pH-responsive nanocomposite hydrogel by connecting oxidized polysaccharides with silver nanoparticles encapsulated in cationic dendritic polymers, which serve as a coating for implantable medical devices and exhibit antibacterial activity against both gram-positive and gram-negative bacteria [183]. This composite can respond to pH reduction induced by bacterial infection and release antibacterial agents, displaying excellent antibacterial activity with minimal cytotoxicity [183].

The implantation of biomedical materials not only presents challenges in maintaining a sterile environment but also triggers the formation of collagen capsules through foreign body reactions. These reactions lead to permanent isolation of implants from surrounding tissues, hindering functionality. Research has found that PHEMA (poly(2-hydroxyethyl methacrylate)) and Ag-nanoparticle hydrogel implants exhibit good antibacterial performance against both gram-positive (*Staphylococcus aureus*) and gram-negative (*Escherichia coli*) bacteria, and by reducing immune reactions, they exhibit in vivo resistance to FBRs, completely preventing the formation of collagen capsules. This makes them an ideal material for next-generation implantable biomedical devices and tissue engineering scaffolds [184].

Metal nanoparticle hydrogels offer good biocompatibility, strong antimicrobial efficiency, and low cytotoxicity, making them ideal materials for producing medical implants such as catheters. They can effectively reduce catheter-related infections and have the potential to decrease the incidence of sepsis and mortality in patients with chronic wounds and extensive burns during perioperative periods.

### 5.4 Tissue Engineering

While a range of mature tissue-engineered skin products have been utilized in clinical settings and various types of artificial skin have been developed, most of these products only exhibit structural similarity to human skin and possess the skin's barrier function. Due to the

absence of skin appendages, they do not fully replicate the complete functions of natural skin, thus falling short of achieving true skin reconstruction. For instance, commonly used dermal substitutes in clinical applications often offer only limited coverage and are associated with high costs. MNHHs, with properties such as multifunctionality, environmental responsiveness, and antimicrobial properties, may present new ideas and directions in this area [74,194,195].

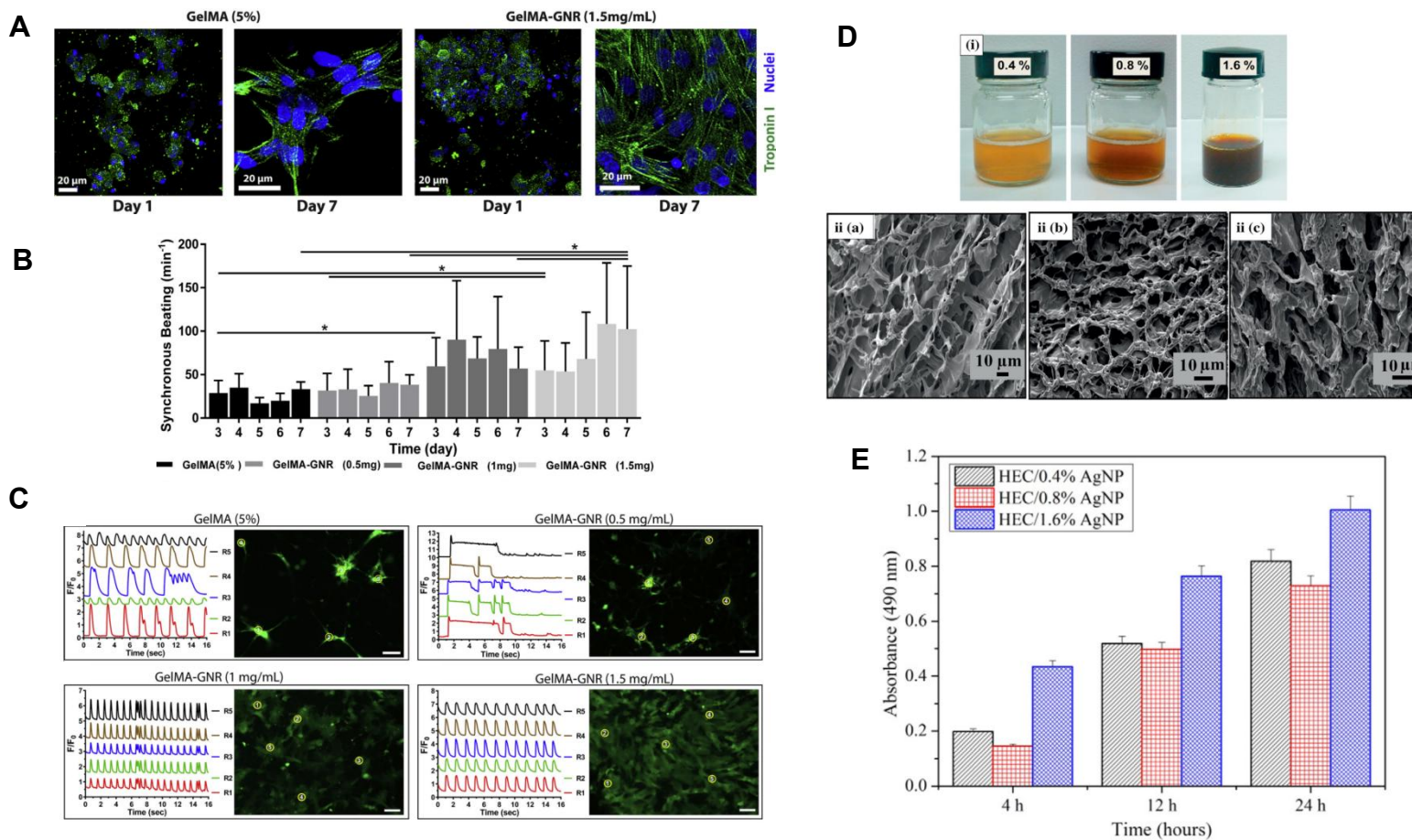
Natural hydrogels made from materials such as gelatin, collagen, and chitosan closely resemble the extracellular matrix (ECM) and serve as scaffolds in tissue engineering, playing various roles [22,74,194,195]. However, their limited mechanical strength and electrical properties have restricted their applications [196]. Cellular vitality in multicellular systems relies on close intercellular electrochemical signaling. The addition of metal nanoparticles enhances the mechanical and electrical properties of hydrogels, making these composite hydrogels ideal for tissue engineering.

The porosity of metal nanoparticle-hybrid hydrogels ensures stable exchange of water, oxygen, and metabolites at wound sites. Additionally, they can simulate the ECM in vitro, promoting cell attachment, proliferation, and differentiation. The Au nanoparticle rod/gelMA/alginate hydrogel provides an ideal 3D cultivation environment for cardiac muscle cells, improving cell adhesion and intercellular communication. As depicted in Figure 6, cardiac muscle cells cultured on the Au nanoparticle rod/gelMA/alginate hydrogel develop increased maturity and corresponding phenotypic structures after 7 days [58]. Compared to pure GelMA, these cardiac muscle cells in the Au nanoparticle rod/GelMA/alginate hydrogel exhibit rhythmic contractions [58]. Research has also shown that introducing gold nanoparticles into hydrogels can enhance the proliferation, vitality, and osteogenic differentiation of adipose-derived stem cells (ADSCs) and localize these effects over an extended period [197]. Metal nanoparticles can also enhance the regenerative properties of hydrogels. For example, the incorporation of copper nano-based metal-organic framework nanoenzymes into hydrogels has been found to effectively improve oxidative stress and inflammation, providing a suitable microenvironment for the regeneration of osteochondral defects [198]. In another study, magnetic Fe<sub>3</sub>O<sub>4</sub> nanoparticles were loaded into chitosan/PEG hydrogel, resulting in higher viability and osteogenic differentiation ability of mesenchymal stem cells [199].

In addition to simulating the ECM and promoting cell migration and proliferation, an ideal artificial skin should possess excellent antibacterial and anti-inflammatory properties. This aligns well with the strengths of metal nanoparticle-hybrid hydrogel composites. Zulkifli *et al.* reported the fabrication of a low-toxicity hydroxyethyl cellulose/silver nanoparticle (HEC/Ag-nanoparticle) nanocomposite hydrogel scaffold that combines antibacterial, anti-inflammatory, and tissue regeneration properties, making it suitable for skin tissue engineering applications (Figure 6) [186]. Rakhshaei *et al.* synthesized a chitosan-gelatin/ZnO nanoparticle composite hydrogel scaffold (CS-GEL/nZnO) in situ. This material exhibited good compatibility with normal human dermal

fibroblasts, showing higher antibacterial efficacy and lower cytotoxicity [187], making it an ideal material for skin tissue engineering.

In conclusion, metal nanoparticle-hybrid hydrogels enhance the conductivity and mechanical strength of hydrogels, maintain a sterile environment, promote the in vitro expression of cellular phenotypes and increase maturity. They hold significant research prospects in the field of tissue-engineered skin construction. However, further research is needed to determine the fate of metal nanoparticles after hydrogel degradation.



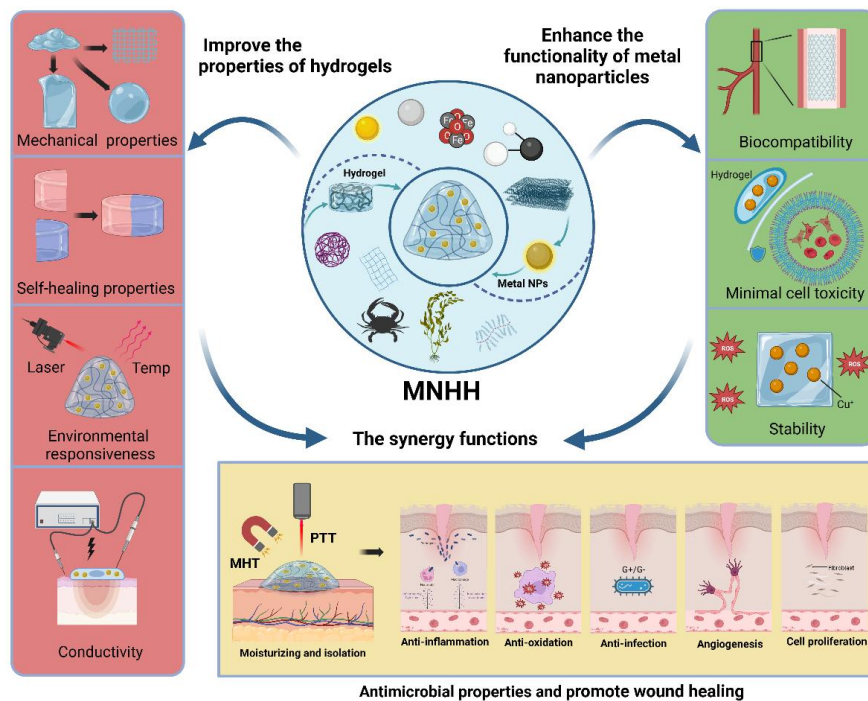
**Figure 6.** The application of metal nanoparticle hybrid hydrogels in tissue engineering. (A) Immunostained images of troponin I (green) on days 1 and 7 of culture for GelMA and 1.5 mg/mL GelMA-GNR hybrid hydrogels. (B) Synchronous beating frequency (beats per minute (BPM)) of cardiomyocytes from day 3 to day 7 of culture depicting robust and stable beating behavior in GelMA-GNR hybrids. A significantly higher number of beating frequencies was observed between highly

830 GNR-concentrated hybrids compared to 0.5 mg/mL GelMA-GNR and pure GelMA hydrogels (\* $p < 0.05$ ). (C) Calcium transient and extracted related frequency  
831 signals of intracellular changes in the concentration of  $\text{Ca}^{2+}$  within cultured cardiomyocytes for pure GelMA (5%), GelMA-GNRs (0.5 mg/mL), GelMA-GNRs (1  
832 mg/mL), and GelMA-GNRs (1.5 mg/mL). R1 to R5 represent regions 1–5, and scale bars depict 100  $\mu\text{m}$ . Reproduced with permission from [58]. Copyright 2016 ,  
833 Elsevier.

834 (D) (i) Photograph of the HEC/Ag nanoparticle solutions obtained at different concentrations of  $\text{AgNO}_3$  and (ii) SEM micrographs of the HEC/Ag nanoparticle  
835 scaffolds at different concentrations of  $\text{AgNO}_3$  (a) 0.4%, (b) 0.8%, (c) 1.6%. (E). Graph showing human fibroblast viability after 4, 12 and 24 h of incubation ( $1 \times$   
836  $10^6$  cells/well in complete MEM) of the HEC/Ag nanoparticle scaffolds at different  $\text{AgNO}_3$  concentrations. Reproduced with permission from [186]. Copyright 2017,  
837 Elsevier.

## 6. Summary and Prospects

Metal nanoparticle hybrid hydrogels epitomize a multifunctional wound care adjunct characterized by commendable mechanical attributes and environmental responsiveness. This amalgamation enables precision and intelligent therapy and monitoring of wounds. This review encapsulates the structural variants, design strategies, and therapeutic applications of metallic nanostructured composite hydrogel materials in the treatment of acute and chronic wounds. It deliberates on how these materials engender novel or refined functionalities and elucidates how contemporary wound management harnesses these attributes. Furthermore, within the ambit of this evolving realm, it underscores the latent potential of metallic nanostructured composite hydrogel materials in revolutionizing wound care [7,22,32,71,81,200].



**Figure 7.** Illustration of MNHH combining the properties of metal nanocarriers with hydrogels. Metal nanoparticles can effectively improve the mechanical properties, self-healing properties, and electrical conductivity of hydrogels. Metal nanonanomaterials can also endow hydrogels with new environmental responsiveness. Hydrogels can stabilize metal nanoparticles and reduce their cytotoxicity. The combination of hydrogels and metal nanoparticles not only compensates for each other's deficiencies but also generates a powerful synergistic effect, such as synergistic antibacterial and wound healing properties. (Created with BioRender.com).

The amalgamation of metallic nanoparticles with hydrogels amalgamates their respective characteristics, blending strengths and mitigating weaknesses (Figure 7). This convergence not

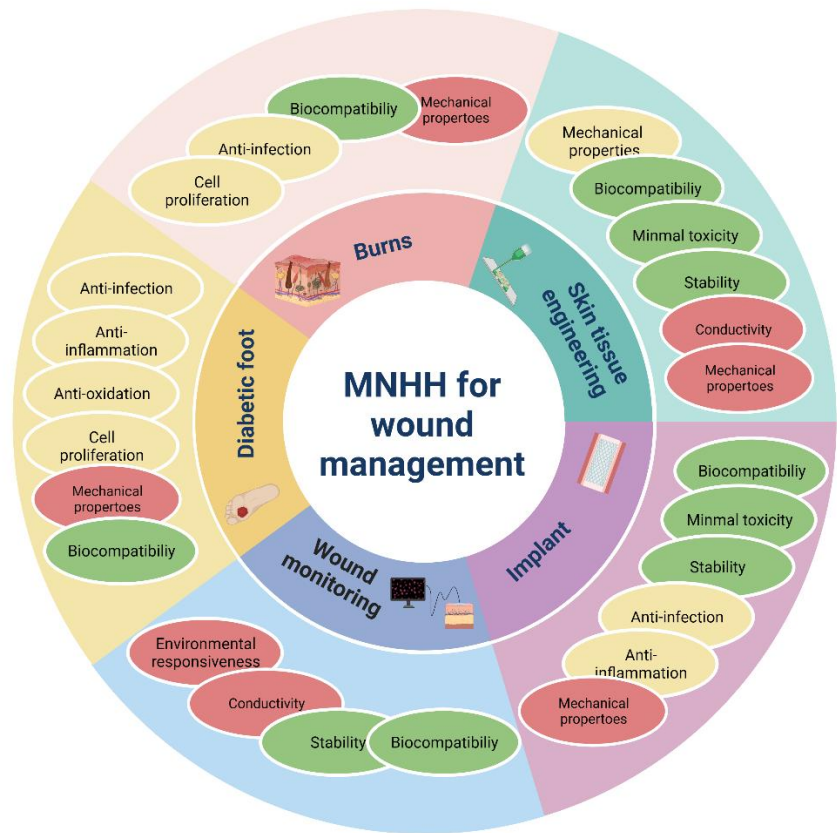
only augments the inherent attributes of metallic nanoparticles and hydrogels but also rectifies their intrinsic deficiencies, thus bestowing novel functional aspects upon both. Initially, the traits of metallic nanoparticles are incorporated within the hydrogel matrix, rendering the composite material selectively responsive to stimuli such as acoustic, optical, and electromagnetic cues, thereby effectuating precise wound treatment and monitoring [44]. Second, alterations in the environmentally sensitive structure of the hydrogel modify the optical, chemical, or electronic properties of embedded metallic nanoparticles, achieving both stable nanoparticles and intelligent drug release, along with environmental dynamic sensing and monitoring [32,87]. Third, the precise spatial arrangement of metallic nanoparticles within the hydrogel matrix passively amplifies their properties, engendering enhanced attributes suitable for biomedical applications such as tissue engineering and wound healing [32]. The integration of metallic nanoparticles effectively enhances the structure of hydrogels, elevating mechanical and self-healing properties and enhancing their processability and pliability, thus broadening the scope of hydrogel dressings in wound care. Additionally, composite materials enhance hydrogel drug delivery systems, achieving stable, tunable, and controlled drug release systems, providing more precise and intelligent drug therapy for wounds [14,15,22]. Metallic nanoparticles introduce novel functional traits to hydrogels. These composites can respond not only to local environmental changes but also to external stimuli such as light, heat, and magnetism, enabling the construction of multifunctional composite hydrogels capable of autonomous sensing, real-time monitoring, and controlled intervention. Conversely, hydrogels offer a means to address these shortcomings of metal nanoparticles. First, hydrogels can alleviate the potential toxicity associated with metal nanoparticles. Furthermore, hydrogels can reduce hemolytic activity and minimize damage to normal tissues. Additionally, hydrogels can enhance the long-term stability of metal nanoparticles. These features endow MNHH with a wide array of captivating capabilities. They can be employed to construct multifunctional materials for wound management and develop intelligent wound dressing systems integrating real-time monitoring and on-demand therapy, thereby surpassing the limitations of traditional wound care. These materials can serve as scaffolds for cell differentiation, manipulation, and proliferation, as well as engendering antibacterial biomaterials capable of eradicating drug-resistant pathogens. With these new attributes, composite hydrogels transcend the realm of being mere dressings for combating infection and promoting wound healing. They metamorphose into intelligent and adjustable wound management interfaces, ushering in new perspectives for precise wound treatment. These composite materials effectively mitigate the historical limitations of metallic nanoparticles in wound therapy while harnessing their advantages to optimize wound healing.

Metal nanoparticle hybrid hydrogels represent an ideal material for wound management (Figure 8). Through structural modifications, composite materials enhance the mechanical properties and stability of hydrogels, endowing them with improved malleability and a broader scope of applications. Additionally, these composites amplify the resistance of hydrogels to

infections and their capacity to expedite wound healing. In the context of acute wounds, metal nanoparticle hybrid hydrogels effectively absorb exudates from burn wounds while facilitating gas exchange. They exhibit exceptional bactericidal effects against various drug-resistant bacteria, effectively eradicating biofilms. Furthermore, these composites display significant hemostatic abilities, promoting wound contraction, collagen deposition, and blood vessel formation and reducing inflammation in infected burn wounds. They also mitigate the discomfort of frequent dressing changes. These hydrogels have anti-inflammatory and proangiogenic properties, promoting fibroblast migration and contributing to the regeneration of burn wound collagen, thereby expediting healing. For chronic wounds, composite hydrogels amalgamate the inherent antibacterial activity of metallic nanoparticles with photothermal and magneto-thermal effects, providing comprehensive, sustained, and precise antibacterial therapy for chronic infected wounds. They also effectively inhibit chronic wound biofilms. Moreover, composite hydrogels eliminate excessive ROS in wounds, maintain intracellular redox homeostasis, alleviate oxidative stress, and provide oxygen to improve the pathological microenvironment of diabetic wounds. Combined with attributes such as tissue adhesion, self-healing, injectability, and hemostasis, they stimulate cell proliferation and migration, along with the remodeling of the extracellular matrix, accelerating the healing of chronic wounds. In the realm of medical implants, metal nanoparticle hybrid hydrogels exhibit responsive release of antibacterial agents, ensuring long-term stable antibacterial effects while maintaining good tissue compatibility. They demonstrate no significant hemolytic or cytotoxic effects, reducing immune reactions and preventing the formation of collagen capsules. In the domain of tissue engineering, metal nanoparticle hybrid hydrogels can replicate the extracellular matrix (ECM) in vitro, offering an optimal 3D cultivation environment for cells. The presence of metallic nanoparticles enhances cell adhesion and communication, facilitating cell attachment, proliferation, and differentiation. With augmented swelling, biodegradation, and antibacterial abilities, they are relatively compatible with human dermal fibroblasts, encompassing characteristics such as low toxicity, antibacterial and anti-inflammatory properties, and the promotion of tissue regeneration. This provides novel pathways for the preparation of engineered skin tissues [194]. Furthermore, these composite materials can undergo structural or color changes under specific environmental stimuli, responding to external triggers and sensing biological molecules or environmental shifts [192]. This capability holds the potential to establish real-time monitoring of wound infections and enable on-demand drug administration in clinical settings [192]. It also offers a robust reference for formulating wound treatment strategies that involve selective drug release [192]. By embedding various forms of metallic nanoparticles within hydrogels, composite materials not only enhance the existing wound healing functions of both components but also generate unique attributes that a single material cannot provide. This innovation allows for real-time wound monitoring, precise drug administration, and intelligent responsiveness. This signifies that metal nanoparticle hybrid hydrogels are no longer merely



wound healing dressings but have the potential to evolve into multifunctional tools for comprehensive wound management.



**Figure 8.** Mechanisms of MNHH for Wound Management. Metal nanoparticle hybrid hydrogels have excellent mechanical properties, plasticity, antibacterial, anti-inflammatory, environmental responsiveness, conductivity and stability, etc. These features can be used in various aspects of wound management, including treating acute wounds, treating chronic wounds, skin tissue engineering, medical implants, real-time monitoring of wounds, etc. (Created with BioRender.com).

Hydrogels can be incorporated with various types of metal nanoparticles, such as monometallic nanoparticles, metal oxide nanoparticles, and alloys, each imparting distinct properties to the hydrogels, such as antimicrobial effects, environmental responsiveness, and improved mechanical properties. It is important to note that while the use of hydrogels can reduce the accumulation and toxicity of metallic nanoparticles in tissues, there is still a risk of these nanoparticles accumulating in organs such as the skin, liver, and kidneys over extended periods, potentially leading to various known or unknown toxic effects [95]. Additionally, the preparation, application, and handling of metal nanoparticle hybrid hydrogels unavoidably release these nanoparticles into the environment, where they can accumulate in soil, water ecosystems, and living organisms, posing risks to ecological environments and human health. Further experiments

and research are necessary to comprehensively investigate the long-term effects of metal nanoparticle hybrid hydrogels on both the human body and the environment.

By combining the biocompatibility of hydrogels with the conductivity of metallic nanoparticles, they can regulate cellular proliferation and migration, mimicking the extracellular matrix (ECM), thereby introducing novel avenues for engineering artificial skin tissues [194]. Through the incorporation of diverse forms of metallic nanoparticles within hydrogels, a unique set of characteristics emerges, enhancing their existing wound-healing capabilities. This amalgamation allows for real-time monitoring, precision drug delivery, and intelligent responses to wound conditions. Capitalizing on comprehensive properties encompassing mechanics, chemistry, environmental responsiveness, and electrical performance, metal nanoparticle hybrid hydrogels bridge the gap between human tissues and conventional electronic devices, potentially revolutionizing the field of bioelectronics. In the visible future, tissue-engineered skin, versatile wound dressings, and intelligent wound management devices founded on such materials hold promising prospects for robust development.

## Abbreviations

ADSCs: adipose-derived stem cells; Ag NPs: silver nanoparticles; Cu NPs: copper nanoparticles; CMCS: carboxymethyl chitosan; DFUs: diabetic foot ulcers; DOX: doxorubicin; DMAEMA: dimethyl aminoethyl methacrylate; ECM: extracellular matrix; GT: gelatin; HCG: human chorionic gonadotropin; HEMA: hydroxyethyl methacrylate; LSPR: local surface plasmon resonance; MNHH: metal nanoparticle hybrid hydrogels; MRSA: methicillin-resistant *Staphylococcus aureus*; MSCs: mesenchymal stem cells; MC: methylcellulose; NCs: nanocomposites; OHA: oxidized hyaluronic acid; PDA: polydopamine; PVA: polyvinyl alcohol; PEG: polyethylene glycol; PA: *Pseudomonas aeruginosa*; ROS: reactive oxygen species; SERRS: surface-enhanced resonance Raman scattering; SPIONs: superparamagnetic iron oxide nanoparticles.

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## Author contributions

Conceptualization, Yuxiang Wang, Mengya Zhang, Zhenzhen Yan; writing-original draft preparation, Yuxiang Wang, Zhenzhen Yan; review and editing, Jie Gao, Mengya Zhang; supervision, Jie Gao, Shichu Xiao, Shizhao Ji; funding acquisition, Jie Gao, Shichu Xiao. All authors have read and agreed to the published version of the manuscript.

988     **Declaration of competing interest**

989             The authors do not have any conflicts of interest to declare.

990 **References**

- 991 1. Sun BK, Siprashvili Z, Khavari PA. Advances in skin grafting and treatment of  
992 cutaneous wounds. *Science*. 2014; 346: 941–5.
- 993 2. Smolle C, Cambiaso-Daniel J, Forbes AA, et al. Recent trends in burn epidemiology  
994 worldwide: A systematic review. *Burns*. 2017; 43: 249–57.
- 995 3. Greenhalgh DG. Management of Burns. *N Engl J Med*. 2019; 380: 2349–59.
- 996 4. Home, Resources, diabetes L with, et al. IDF Diabetes Atlas 2022 Reports | IDF  
997 Diabetes Atlas [Internet]. [cited 3 February 2023]. Available at:  
998 <https://diabetesatlas.org/2022-reports/>
- 999 5. Everett E, Mathioudakis N. Update on management of diabetic foot ulcers. *Ann N Y*  
1000 *Acad Sci*. 2018; 1411: 153–65.
- 1001 6. Zeng Q, Qi X, Shi G, Zhang M, Haick H. Wound Dressing: From Nanomaterials to  
1002 Diagnostic Dressings and Healing Evaluations. *ACS Nano*. 2022; 16: 1708–33.
- 1003 7. Clasky AJ, Watchorn JD, Chen PZ, Gu FX. From prevention to diagnosis and treatment:  
1004 Biomedical applications of metal nanoparticle-hydrogel composites. *Acta Biomater*.  
1005 2021; 122: 1–25.
- 1006 8. Sun BK, Siprashvili Z, Khavari PA. Advances in skin grafting and treatment of  
1007 cutaneous wounds. *Science*. 2014; 346: 941–5.
- 1008 9. Nuutila K, Eriksson E. Moist Wound Healing with Commonly Available Dressings. *Adv*  
1009 *Wound Care*. 2021; 10: 685–98.
- 1010 10. Chen J, He J, Yang Y, et al. Antibacterial adhesive self-healing hydrogels to promote  
1011 diabetic wound healing. *Acta Biomater*. 2022; 146: 119–30.
- 1012 11. Guo B, Liang Y, Dong R. Physical dynamic double-network hydrogels as dressings to  
1013 facilitate tissue repair. *Nat Protoc*. 2023; 18: 3322–54.
- 1014 12. Huang Y, Mu L, Zhao X, Han Y, Guo B. Bacterial Growth-Induced Tobramycin Smart  
1015 Release Self-Healing Hydrogel for *Pseudomonas aeruginosa*-Infected Burn Wound  
1016 Healing. *ACS Nano*. 2022; 16: 13022–36.
- 1017 13. He J, Li Z, Wang J, et al. Photothermal antibacterial antioxidant conductive  
1018 self-healing hydrogel with nitric oxide release accelerates diabetic wound healing.  
1019 *Compos Part B Eng*. 2023; 266: 110985.
- 1020 14. Liang Y, He J, Guo B. Functional Hydrogels as Wound Dressing to Enhance Wound  
1021 Healing. *ACS Nano*. 2021; 15: 12687–722.
- 1022 15. Yang K, Han Q, Chen B, et al. Antimicrobial hydrogels: promising materials for medical  
1023 application. *Int J Nanomedicine*. 2018; Volume 13: 2217–63.
- 1024 16. Cao Z, Luo Y, Li Z, et al. Antibacterial Hybrid Hydrogels. *Macromol Biosci*. 2021; 21:

1025 2000252.

1026 17. Shen Z, Zhu X, Majidi C, Gu G. Cutaneous Ionogel Mechanoreceptors for Soft  
1027 Machines, Physiological Sensing, and Amputee Prostheses. *Adv Mater* Deerfield  
1028 Beach Fla. 2021; 33: e2102069.

1029 18. Liang Y, Zhao X, Hu T, et al. Adhesive Hemostatic Conducting Injectable Composite  
1030 Hydrogels with Sustained Drug Release and Photothermal Antibacterial Activity to  
1031 Promote Full-Thickness Skin Regeneration During Wound Healing. *Small* Wein  
1032 Bergstr Ger. 2019; 15: e1900046.

1033 19. Qu J, Zhao X, Liang Y, Zhang T, Ma PX, Guo B. Antibacterial adhesive injectable  
1034 hydrogels with rapid self-healing, extensibility and compressibility as wound dressing  
1035 for joints skin wound healing. *Biomaterials*. 2018; 183: 185–99.

1036 20. Zhao X, Wu H, Guo B, Dong R, Qiu Y, Ma PX. Antibacterial anti-oxidant electroactive  
1037 injectable hydrogel as self-healing wound dressing with hemostasis and adhesiveness  
1038 for cutaneous wound healing. *Biomaterials*. 2017; 122: 34–47.

1039 21. Bruggeman KF, Williams RJ, Nisbet DR. Dynamic and Responsive Growth Factor  
1040 Delivery from Electrospun and Hydrogel Tissue Engineering Materials. *Adv Healthc*  
1041 *Mater*. 2018; 7.

1042 22. Gradinaru V, Treweek J, Overton K, Deisseroth K. Hydrogel-Tissue Chemistry:  
1043 Principles and Applications. *Annu Rev Biophys*. 2018; 47: 355–76.

1044 23. Cao J, Wang P, Liu Y, Zhu C, Fan D. Double crosslinked HLC-CCS hydrogel tissue  
1045 engineering scaffold for skin wound healing. *Int J Biol Macromol*. 2020; 155: 625–35.

1046 24. Broussard KC, Powers JG. Wound dressings: selecting the most appropriate type. *Am J*  
1047 *Clin Dermatol*. 2013; 14: 449–59.

1048 25. Yang Y, Zhu Y, Wang K, et al. Activation of autophagy by in situ Zn<sup>2+</sup> chelation  
1049 reaction for enhanced tumor chemoimmunotherapy. *Bioact Mater*. 2023; 29: 116–31.

1050 26. Zhang S, Xie F, Li K, et al. Gold nanoparticle-directed autophagy intervention for  
1051 antitumor immunotherapy via inhibiting tumor-associated macrophage M2  
1052 polarization. *Acta Pharm Sin B*. 2022; 12: 3124–38.

1053 27. Wu Y, Su M, Zhang S, et al. A mesenchymal stem cell-derived  
1054 nanovesicle-biopotentiated bovine serum albumin-bridged gelatin hydrogel for  
1055 enhanced diabetic wound therapy. *Mater Des*. 2023; 230: 111960.

1056 28. Li Y, Wang L, Zhong G, et al. Size-transformable nanoparticles with sequentially  
1057 triggered drug release and enhanced penetration for anticancer therapy. *Nano Res*.  
1058 2023; 16: 11186–96.

1059 29. Li W, Bei Y, Pan X, et al. Selenide-linked polydopamine-reinforced hybrid hydrogels  
1060 with on-demand degradation and light-triggered nanzyme release for diabetic  
1061 wound healing. *Biomater Res*. 2023; 27: 49.

- 1062 30. Pang L, Jin H, Lu Z, et al. Treatment with Mesenchymal Stem Cell-Derived  
1063 Nanovesicle-Containing Gelatin Methacryloyl Hydrogels Alleviates Osteoarthritis by  
1064 Modulating Chondrogenesis and Macrophage Polarization. *Adv Healthc Mater.* 2023;  
1065 12: 2300315.
- 1066 31. Xia Y, Xiong Y, Lim B, Skrabalak SE. Shape-controlled synthesis of metal nanocrystals:  
1067 simple chemistry meets complex physics? *Angew Chem Int Ed Engl.* 2009; 48: 60–103.
- 1068 32. Dzulkharnien NSF, Rohani R. A Review on Current Designation of Metallic  
1069 Nanocomposite Hydrogel in Biomedical Applications. *Nanomaterials.* 2022; 12: 1629.
- 1070 33. Kalantari K, Mostafavi E, Afifi AM, et al. Wound dressings functionalized with silver  
1071 nanoparticles: promises and pitfalls. *Nanoscale.* 2020; 12: 2268–91.
- 1072 34. Liao C, Li Y, Tjong SC. Bactericidal and Cytotoxic Properties of Silver Nanoparticles. *Int*  
1073 *J Mol Sci.* 2019; 20: 449.
- 1074 35. Boisselier E, Astruc D. Gold nanoparticles in nanomedicine: preparations, imaging,  
1075 diagnostics, therapies and toxicity. *Chem Soc Rev.* 2009; 38: 1759–82.
- 1076 36. Liu C, Ling J, Yang L-Y, Ouyang X-K, Wang N. Chitosan-based carbon  
1077 nitride-polydopamine - silver composite dressing with antibacterial properties for  
1078 wound healing. *Carbohydr Polym.* 2023; 303: 120436.
- 1079 37. Wang P, Sun J, Lou Z, et al. Assembly-Induced Thermogenesis of Gold Nanoparticles  
1080 in the Presence of Alternating Magnetic Field for Controllable Drug Release of  
1081 Hydrogel. *Adv Mater.* 2016; 28: 10801–8.
- 1082 38. Mallick S, Nag M, Lahiri D, et al. Engineered Nanotechnology: An Effective Therapeutic  
1083 Platform for the Chronic Cutaneous Wound. *Nanomaterials.* 2022; 12: 778.
- 1084 39. Ma Y, Mao Y, Huang D, et al. Portable visual quantitative detection of aflatoxin B1  
1085 using a target-responsive hydrogel and a distance-readout microfluidic chip. *Lab*  
1086 *Chip.* 2016; 16: 3097–104.
- 1087 40. Shen Y, Liang L, Zhang S, et al. Organelle-targeting surface-enhanced Raman  
1088 scattering (SERS) nanosensors for subcellular pH sensing. *Nanoscale.* 2018; 10:  
1089 1622–30.
- 1090 41. Bodelón G, Montes-García V, López-Puente V, et al. Detection and imaging of  
1091 quorum sensing in *Pseudomonas aeruginosa* biofilm communities by  
1092 surface-enhanced resonance Raman scattering. *Nat Mater.* 2016; 15: 1203–11.
- 1093 42. Zhou Y, Sharma N, Deshmukh P, Lakhman RK, Jain M, Kasi RM. Hierarchically  
1094 structured free-standing hydrogels with liquid crystalline domains and magnetic  
1095 nanoparticles as dual physical cross-linkers. *J Am Chem Soc.* 2012; 134: 1630–41.
- 1096 43. Guo H, Liu Y, Yang Y, et al. A shape-shifting composite hydrogel sheet with spatially  
1097 patterned plasmonic nanoparticles. *J Mater Chem B.* 2019; 7: 1679–83.
- 1098 44. Jiang B, Hom WL, Chen X, et al. Magnetic Hydrogels from Alkyne/Cobalt

1099 Carbonyl-Functionalized ABA Triblock Copolymers. *J Am Chem Soc.* 2016; 138:  
1100 4616–25.

1101 45. Sutton A, Shirman T, Timonen JVI, et al. Photothermally triggered actuation of hybrid  
1102 materials as a new platform for in vitro cell manipulation. *Nat Commun.* 2017; 8:  
1103 14700.

1104 46. Zhang J, Mou L, Jiang X. Hydrogels Incorporating Au@Polydopamine Nanoparticles:  
1105 Robust Performance for Optical Sensing. *Anal Chem.* 2018; 90: 11423–30.

1106 47. Gao W, Vecchio D, Li J, et al. Hydrogel containing nanoparticle-stabilized liposomes  
1107 for topical antimicrobial delivery. *ACS Nano.* 2014; 8: 2900–7.

1108 48. Zhao X, Qi T, Kong C, et al. Photothermal exposure of polydopamine-coated  
1109 branched Au-Ag nanoparticles induces cell cycle arrest, apoptosis, and autophagy in  
1110 human bladder cancer cells. *Int J Nanomedicine.* 2018; 13: 6413–28.

1111 49. García-Astrain C, Chen C, Burón M, et al. Biocompatible hydrogel nanocomposite  
1112 with covalently embedded silver nanoparticles. *Biomacromolecules.* 2015; 16:  
1113 1301–10.

1114 50. Hu M, Gu X, Hu Y, Deng Y, Wang C. PVA/Carbon Dot Nanocomposite Hydrogels for  
1115 Simple Introduction of Ag Nanoparticles with Enhanced Antibacterial Activity.  
1116 *Macromol Mater Eng.* 2016; 301: 1352–62.

1117 51. Pakiari AH, Jamshidi Z. Nature and Strength of M–S Bonds (M = Au, Ag, and Cu) in  
1118 Binary Alloy Gold Clusters. *J Phys Chem A.* 2010; 114: 9212–21.

1119 52. Woehrle GH, Brown LO, Hutchison JE. Thiol-Functionalized, 1.5-nm Gold  
1120 Nanoparticles through Ligand Exchange Reactions: Scope and Mechanism of Ligand  
1121 Exchange. *J Am Chem Soc.* 2005; 127: 2172–83.

1122 53. Xue Y, Li X, Li H, Zhang W. Quantifying thiol–gold interactions towards the efficient  
1123 strength control. *Nat Commun.* 2014; 5: 4348.

1124 54. GhavamiNejad A, Park CH, Kim CS. In Situ Synthesis of Antimicrobial Silver  
1125 Nanoparticles within Antifouling Zwitterionic Hydrogels by Catecholic Redox  
1126 Chemistry for Wound Healing Application. *Biomacromolecules.* 2016; 17: 1213–23.

1127 55. Batool Z, Muhammad G, Iqbal MM, et al. Hydrogel assisted synthesis of gold  
1128 nanoparticles with enhanced microbicidal and in vivo wound healing potential. *Sci*  
1129 *Rep.* 2022; 12: 6575.

1130 56. Masood N, Ahmed R, Tariq M, et al. Silver nanoparticle impregnated chitosan-PEG  
1131 hydrogel enhances wound healing in diabetes induced rabbits. *Int J Pharm.* 2019; 559:  
1132 23–36.

1133 57. Zhu K, Shin SR, van Kempen T, et al. Gold Nanocomposite Bioink for Printing 3D  
1134 Cardiac Constructs. *Adv Funct Mater.* 2017; 27: 1605352.

- 1135 58. Navaei A, Saini H, Christenson W, Sullivan RT, Ros R, Nikkhah M. Gold  
1136 nanorod-incorporated gelatin-based conductive hydrogels for engineering cardiac  
1137 tissue constructs. *Acta Biomater.* 2016; 41: 133–46.
- 1138 59. Oleyaei SA, Razavi SMA, Mikkonen KS. Physicochemical and rheo-mechanical  
1139 properties of titanium dioxide reinforced sage seed gum nanohybrid hydrogel. *Int J*  
1140 *Biol Macromol.* 2018; 118: 661–70.
- 1141 60. Ye H, Cheng J, Yu K. In situ reduction of silver nanoparticles by gelatin to obtain  
1142 porous silver nanoparticle/chitosan composites with enhanced antimicrobial and  
1143 wound-healing activity. *Int J Biol Macromol.* 2019; 121: 633–42.
- 1144 61. Fuhrer R, Athanassiou EK, Luechinger NA, Stark WJ. Crosslinking metal nanoparticles  
1145 into the polymer backbone of hydrogels enables preparation of soft, magnetic  
1146 field-driven actuators with muscle-like flexibility. *Small Weinb Bergstr Ger.* 2009; 5:  
1147 383–8.
- 1148 62. Yu AC, Chen H, Chan D, et al. Scalable manufacturing of biomimetic moldable  
1149 hydrogels for industrial applications. *Proc Natl Acad Sci U S A.* 2016; 113: 14255–60.
- 1150 63. Klajn R, Bishop KJM, Grzybowski BA. Light-controlled self-assembly of reversible and  
1151 irreversible nanoparticle suprastructures. *Proc Natl Acad Sci U S A.* 2007; 104:  
1152 10305–9.
- 1153 64. Fu X, Hosta-Rigau L, Chandrawati R, Cui J. Multi-Stimuli-Responsive Polymer Particles,  
1154 Films, and Hydrogels for Drug Delivery. *Chem.* 2018; 4: 2084–107.
- 1155 65. Zhang H, Sun X, Wang J, et al. Multifunctional Injectable Hydrogel Dressings for  
1156 Effectively Accelerating Wound Healing: Enhancing Biomineralization Strategy. *Adv*  
1157 *Funct Mater.* 2021; 31: 2100093.
- 1158 66. Bardajee GR, Hooshyar Z, Rezanezhad H. A novel and green biomaterial based silver  
1159 nanocomposite hydrogel: synthesis, characterization and antibacterial effect. *J Inorg*  
1160 *Biochem.* 2012; 117: 367–73.
- 1161 67. Hauser AW, Evans AA, Na J-H, Hayward RC. Photothermally reprogrammable  
1162 buckling of nanocomposite gel sheets. *Angew Chem Int Ed Engl.* 2015; 54: 5434–7.
- 1163 68. Wu Y, Wang H, Gao F, Xu Z, Dai F, Liu W. An Injectable Supramolecular Polymer  
1164 Nanocomposite Hydrogel for Prevention of Breast Cancer Recurrence with  
1165 Theranostic and Mammoplastic Functions. *Adv Funct Mater.* 2018; 28: 1801000.
- 1166 69. Yan X, Sun T, Song Y, et al. In situ Thermal-Responsive Magnetic Hydrogel for  
1167 Multidisciplinary Therapy of Hepatocellular Carcinoma. *Nano Lett.* 2022; 22: 2251–60.
- 1168 70. Moorcroft SCT, Jayne DG, Evans SD, Ong ZY. Stimuli-Responsive Release of  
1169 Antimicrobials Using Hybrid Inorganic Nanoparticle-Associated Drug-Delivery  
1170 Systems. *Macromol Biosci.* 2018; 18: 1800207.
- 1171 71. Gao W, Vecchio D, Li J, et al. Hydrogel Containing Nanoparticle-Stabilized Liposomes  
1172 for Topical Antimicrobial Delivery. *ACS Nano.* 2014; 8: 2900–7.



- 1173 72. Wang P, Sun J, Lou Z, et al. Assembly-Induced Thermogenesis of Gold Nanoparticles  
1174 in the Presence of Alternating Magnetic Field for Controllable Drug Release of  
1175 Hydrogel. *Adv Mater.* 2016; 28: 10801–8.
- 1176 73. Baei P, Jalili-Firoozinezhad S, Rajabi-Zeleti S, Tafazzoli-Shadpour M, Baharvand H,  
1177 Aghdami N. Electrically conductive gold nanoparticle-chitosan thermosensitive  
1178 hydrogels for cardiac tissue engineering. *Mater Sci Eng C.* 2016; 63: 131–41.
- 1179 74. You J-O, Rafat M, Ye GJC, Auguste DT. Nanoengineering the Heart: Conductive  
1180 Scaffolds Enhance Connexin 43 Expression. *Nano Lett.* 2011; 11: 3643–8.
- 1181 75. Raghavan K, Porterfield JE, Kottam ATG, et al. Electrical Conductivity and Permittivity  
1182 of Murine Myocardium. *IEEE Trans Biomed Eng.* 2009; 56: 2044–53.
- 1183 76. Zhang A, Guo W, Ke H, et al. Sandwich-format ECL immunosensor based on Au  
1184 star@BSA-Luminol nanocomposites for determination of human chorionic  
1185 gonadotropin. *Biosens Bioelectron.* 2018; 101: 219–26.
- 1186 77. Darvishi S, Souissi M, Kharaziha M, Karimzadeh F, Sahara R, Ahadian S. Gelatin  
1187 methacryloyl hydrogel for glucose biosensing using Ni nanoparticles-reduced  
1188 graphene oxide: An experimental and modeling study. *Electrochimica Acta.* 2018; 261:  
1189 275–83.
- 1190 78. Zhai D, Liu B, Shi Y, et al. Highly sensitive glucose sensor based on pt  
1191 nanoparticle/polyaniline hydrogel heterostructures. *ACS Nano.* 2013; 7: 3540–6.
- 1192 79. Wu J, Yin L. Platinum nanoparticle modified polyaniline-functionalized boron nitride  
1193 nanotubes for amperometric glucose enzyme biosensor. *ACS Appl Mater Interfaces.*  
1194 2011; 3: 4354–62.
- 1195 80. Yan W, Feng X, Chen X, Hou W, Zhu J-J. A super highly sensitive glucose biosensor  
1196 based on Au nanoparticles-AgCl@polyaniline hybrid material. *Biosens Bioelectron.*  
1197 2008; 23: 925–31.
- 1198 81. You J-O, Auguste DT. Conductive, Physiologically Responsive Hydrogels. *Langmuir.*  
1199 2010; 26: 4607–12.
- 1200 82. Dai T, Wang C, Wang Y, Xu W, Hu J, Cheng Y. A Nanocomposite Hydrogel with Potent  
1201 and Broad-Spectrum Antibacterial Activity. *ACS Appl Mater Interfaces.* 2018; 10:  
1202 15163–73.
- 1203 83. Huang H, Lai W, Cui M, et al. An Evaluation of Blood Compatibility of Silver  
1204 Nanoparticles. *Sci Rep.* 2016; 6: 25518.
- 1205 84. Villanueva ME, Diez AM del R, González JA, et al. Antimicrobial Activity of Starch  
1206 Hydrogel Incorporated with Copper Nanoparticles. *ACS Appl Mater Interfaces.* 2016;  
1207 8: 16280–8.
- 1208 85. Li Q, Lu F, Zhou G, et al. Silver Inlaid with Gold Nanoparticle/Chitosan Wound  
1209 Dressing Enhances Antibacterial Activity and Porosity, and Promotes Wound Healing.  
1210 *Biomacromolecules.* 2017; 18: 3766–75.

- 1211 86. Alavi M, Nokhodchi A. An overview on antimicrobial and wound healing properties of  
1212 ZnO nanobiofilms, hydrogels, and bionanocomposites based on cellulose, chitosan,  
1213 and alginate polymers. *Carbohydr Polym.* 2020; 227: 115349.
- 1214 87. Franco D, Calabrese G, Guglielmino SPP, Conoci S. Metal-Based Nanoparticles:  
1215 Antibacterial Mechanisms and Biomedical Application. *Microorganisms.* 2022; 10:  
1216 1778.
- 1217 88. Hussain SM, Hess KL, Gearhart JM, Geiss KT, Schlager JJ. In vitro toxicity of  
1218 nanoparticles in BRL 3A rat liver cells. *Toxicol In Vitro.* 2005; 19: 975–83.
- 1219 89. Shin S-H, Ye M-K, Kim H-S, Kang H-S. The effects of nano-silver on the proliferation  
1220 and cytokine expression by peripheral blood mononuclear cells. *Int*  
1221 *Immunopharmacol.* 2007; 7: 1813–8.
- 1222 90. Huang M, Ye K, Hu T, et al. Silver Nanoparticles Attenuate the Antimicrobial Activity of  
1223 the Innate Immune System by Inhibiting Neutrophil-Mediated Phagocytosis and  
1224 Reactive Oxygen Species Production. *Int J Nanomedicine.* 2021; 16: 1345–60.
- 1225 91. Qi X, Huang Y, You S, et al. Engineering Robust Ag-Decorated Polydopamine  
1226 Nano-Photothermal Platforms to Combat Bacterial Infection and Prompt Wound  
1227 Healing. *Adv Sci.* 2022; 9: 2106015.
- 1228 92. Kalirajan C, Palanisamy T. Bioengineered Hybrid Collagen Scaffold Tethered with  
1229 Silver-Catechin Nanocomposite Modulates Angiogenesis and TGF-  $\beta$  Toward Scarless  
1230 Healing in Chronic Deep Second Degree Infected Burns. *Adv Healthc Mater.* 2020; 9:  
1231 2000247.
- 1232 93. Zhang B, Lv Y, Yu C, et al. Au-Pt nanozyme-based multifunctional hydrogel dressing  
1233 for diabetic wound healing. *Biomater Adv.* 2022; 137: 212869.
- 1234 94. Li Z, You S, Mao R, et al. Architecting polyelectrolyte hydrogels with Cu-assisted  
1235 polydopamine nanoparticles for photothermal antibacterial therapy. *Mater Today Bio.*  
1236 2022; 15: 100264.
- 1237 95. Xu L, Wang Y-Y, Huang J, Chen C-Y, Wang Z-X, Xie H. Silver nanoparticles: Synthesis,  
1238 medical applications and biosafety. *Theranostics.* 2020; 10: 8996–9031.
- 1239 96. Baukum J, Pranjan J, Kaolaor A, Chuysinuan P, Suwantong O, Supaphol P. The  
1240 potential use of cross-linked alginate/gelatin hydrogels containing silver  
1241 nanoparticles for wound dressing applications. *Polym Bull.* 2020; 77: 2679–95.
- 1242 97. Tong C, Zhong X, Yang Y, et al. PB@PDA@Ag nanosystem for synergistically  
1243 eradicating MRSA and accelerating diabetic wound healing assisted with laser  
1244 irradiation. *Biomaterials.* 2020; 243: 119936.
- 1245 98. Masood N, Ahmed R, Tariq M, et al. Silver nanoparticle impregnated chitosan-PEG  
1246 hydrogel enhances wound healing in diabetes induced rabbits. *Int J Pharm.* 2019; 559:  
1247 23–36.
- 1248 99. Obradovic B, Stojkovska J, Jovanovic Z, Miskovic-Stankovic V. Novel alginate based

1249 nanocomposite hydrogels with incorporated silver nanoparticles. *J Mater Sci Mater*  
1250 *Med.* 2012; 23: 99–107.

1251 100. Neibert K, Gopishetty V, Grigoryev A, et al. Wound-healing with mechanically robust  
1252 and biodegradable hydrogel fibers loaded with silver nanoparticles. *Adv Healthc*  
1253 *Mater.* 2012; 1: 621–30.

1254 101. Fan Z, Liu B, Wang J, et al. A Novel Wound Dressing Based on Ag/Graphene Polymer  
1255 Hydrogel: Effectively Kill Bacteria and Accelerate Wound Healing. *Adv Funct Mater.*  
1256 2014; 24: 3933–43.

1257 102. Wechsler ME, Jocelyn Dang HKH, Simmonds SP, et al. Electrostatic and Covalent  
1258 Assemblies of Anionic Hydrogel-Coated Gold Nanoshells for Detection of Dry Eye  
1259 Biomarkers in Human Tears. *Nano Lett.* 2021; 21: 8734–40.

1260 103. Chen X, Tao J, Zhang M, et al. Iota carrageenan gold-silver NPs photothermal  
1261 hydrogel for tumor postsurgical anti-recurrence and wound healing. *Carbohydr*  
1262 *Polym.* 2022; 298: 120123.

1263 104. Liu M, Zhang J, Liu S, Li B. A label-free visual aptasensor for zearalenone detection  
1264 based on target-responsive aptamer-cross-linked hydrogel and color change of gold  
1265 nanoparticles. *Food Chem.* 2022; 389: 133078.

1266 105. Oliveira MJ, Cunha I, de Almeida MP, et al. Reusable and highly sensitive SERS  
1267 immunoassay utilizing gold nanostars and a cellulose hydrogel-based platform. *J*  
1268 *Mater Chem B.* 2021; 9: 7516–29.

1269 106. Batool Z, Muhammad G, Iqbal MM, et al. Hydrogel assisted synthesis of gold  
1270 nanoparticles with enhanced microbicidal and in vivo wound healing potential. *Sci*  
1271 *Rep.* 2022; 12: 6575.

1272 107. Abdollahiyan P, Baradaran B, de la Guardia M, Oroojalian F, Mokhtarzadeh A.  
1273 Cutting-edge progress and challenges in stimuli responsive hydrogel  
1274 microenvironment for success in tissue engineering today. *J Control Release Off J*  
1275 *Control Release Soc.* 2020; 328: 514–31.

1276 108. You J-O, Rafat M, Ye GJC, Auguste DT. Nanoengineering the heart: conductive  
1277 scaffolds enhance connexin 43 expression. *Nano Lett.* 2011; 11: 3643–8.

1278 109. Peña B, Maldonado M, Bonham AJ, et al. Gold Nanoparticle-Functionalized Reverse  
1279 Thermal Gel for Tissue Engineering Applications. *ACS Appl Mater Interfaces.* 2019; 11:  
1280 18671–80.

1281 110. Cui Y, Zhao Y, Tian Y, Zhang W, Lü X, Jiang X. The molecular mechanism of action of  
1282 bactericidal gold nanoparticles on *Escherichia coli*. *Biomaterials.* 2012; 33: 2327–33.

1283 111. Zheng K, Setyawati MI, Leong DT, Xie J. Antimicrobial Gold Nanoclusters. *ACS Nano.*  
1284 2017; 11: 6904–10.

1285 112. Linklater DP, Baulin VA, Le Guével X, et al. Antibacterial Action of Nanoparticles by  
1286 Lethal Stretching of Bacterial Cell Membranes. *Adv Mater Deerfield Beach Fla.* 2020;

1287 32: e2005679.

1288 113. Al-Bakri AG, Mahmoud NN. Photothermal-Induced Antibacterial Activity of Gold  
1289 Nanorods Loaded into Polymeric Hydrogel against *Pseudomonas aeruginosa* Biofilm.  
1290 *Molecules*. 2019; 24: 2661.

1291 114. Liu J, Li Z, Lin Q, et al. A Robust, Resilient, and Multi-Functional Soy Protein-Based  
1292 Hydrogel. *ACS Sustain Chem Eng*. 2018; 6: 13730–8.

1293 115. Hu B, Berkey C, Feliciano T, et al. Thermal-Disrupting Interface Mitigates Intercellular  
1294 Cohesion Loss for Accurate Topical Antibacterial Therapy. *Adv Mater Deerfield Beach  
1295 Fla*. 2020; 32: e1907030.

1296 116. Zhang H, Sun X, Wang J, et al. Multifunctional Injectable Hydrogel Dressings for  
1297 Effectively Accelerating Wound Healing: Enhancing Biomineralization Strategy. *Adv  
1298 Funct Mater*. 2021; 31: 2100093.

1299 117. Alavi M, Karimi N. Ultrasound assisted-phytofabricated Fe<sub>3</sub>O<sub>4</sub> NPs with antioxidant  
1300 properties and antibacterial effects on growth, biofilm formation, and spreading  
1301 ability of multidrug resistant bacteria. *Artif Cells Nanomedicine Biotechnol*. 2019; 47:  
1302 2405–23.

1303 118. Hassabo AG, El-Naggar ME, Mohamed AL, Hebeish AA. Development of  
1304 multifunctional modified cotton fabric with tri-component nanoparticles of silver,  
1305 copper and zinc oxide. *Carbohydr Polym*. 2019; 210: 144–56.

1306 119. Alsaaed FAT, El-Lateef HMA, Khalaf MM, Mohamed IMA, Al-Omair MA, Gouda M.  
1307 Drug Delivery System Based on Carboxymethyl Cellulose Containing Metal-Organic  
1308 Framework and Its Evaluation for Antibacterial Activity. *Polymers*. 2022; 14: 3815.

1309 120. Zamani D, Moztaezadeh F, Bizari D. Alginate-bioactive glass containing Zn and Mg  
1310 composite scaffolds for bone tissue engineering. *Int J Biol Macromol*. 2019; 137:  
1311 1256–67.

1312 121. He J, Fang J, Wei P, et al. Cancellous bone-like porous Fe@Zn scaffolds with  
1313 core-shell-structured skeletons for biodegradable bone implants. *Acta Biomater*.  
1314 2021; 121: 665–81.

1315 122. Zhong T, Oporto GS, Jacyński J, Jiang C. Nanofibrillated Cellulose and Copper  
1316 Nanoparticles Embedded in Polyvinyl Alcohol Films for Antimicrobial Applications.  
1317 *BioMed Res Int*. 2015; 2015: 456834.

1318 123. Zangeneh MM, Ghaneialvar H, Akbaribazm M, et al. Novel synthesis of *Falcaria*  
1319 *vulgaris* leaf extract conjugated copper nanoparticles with potent cytotoxicity,  
1320 antioxidant, antifungal, antibacterial, and cutaneous wound healing activities under in  
1321 vitro and in vivo condition. *J Photochem Photobiol B*. 2019; 197: 111556.

1322 124. Kruk T, Szczepanowicz K, Stefańska J, Socha RP, Warszyński P. Synthesis and  
1323 antimicrobial activity of monodisperse copper nanoparticles. *Colloids Surf B  
1324 Biointerfaces*. 2015; 128: 17–22.

- 1325 125. Rajasekaran P, Santra S. Hydrothermally Treated Chitosan Hydrogel Loaded with  
1326 Copper and Zinc Particles as a Potential Micronutrient-Based Antimicrobial Feed  
1327 Additive. *Front Vet Sci.* 2015; 2: 62.
- 1328 126. Yadollahi M, Gholamali I, Namazi H, Aghazadeh M. Synthesis and characterization of  
1329 antibacterial carboxymethylcellulose/CuO bio-nanocomposite hydrogels. *Int J Biol*  
1330 *Macromol.* 2015; 73: 109–14.
- 1331 127. Ruparelia JP, Chatterjee AK, Duttagupta SP, Mukherji S. Strain specificity in  
1332 antimicrobial activity of silver and copper nanoparticles. *Acta Biomater.* 2008; 4:  
1333 707–16.
- 1334 128. Villanueva ME, Diez AMDR, González JA, et al. Antimicrobial Activity of Starch  
1335 Hydrogel Incorporated with Copper Nanoparticles. *ACS Appl Mater Interfaces.* 2016;  
1336 8: 16280–8.
- 1337 129. Chen S, Tang F, Tang L, Li L. Synthesis of Cu-Nanoparticle Hydrogel with Self-Healing  
1338 and Photothermal Properties. *ACS Appl Mater Interfaces.* 2017; 9: 20895–903.
- 1339 130. Ramanujam K, Sundrarajan M. Antibacterial effects of biosynthesized MgO  
1340 nanoparticles using ethanolic fruit extract of *Emblca officinalis*. *J Photochem*  
1341 *Photobiol B.* 2014; 141: 296–300.
- 1342 131. Leung YH, Ng AMC, Xu X, et al. Mechanisms of antibacterial activity of MgO:  
1343 non-ROS mediated toxicity of MgO nanoparticles towards *Escherichia coli*. *Small*  
1344 *Weinh Bergstr Ger.* 2014; 10: 1171–83.
- 1345 132. He Y, Ingudam S, Reed S, Gehring A, Strobaugh TP, Irwin P. Study on the mechanism  
1346 of antibacterial action of magnesium oxide nanoparticles against foodborne  
1347 pathogens. *J Nanobiotechnology.* 2016; 14: 54.
- 1348 133. Hezaveh H, Muhamad II. Impact of metal oxide nanoparticles on oral release  
1349 properties of pH-sensitive hydrogel nanocomposites. *Int J Biol Macromol.* 2012; 50:  
1350 1334–40.
- 1351 134. Harris M, Ahmed H, Barr B, et al. Magnetic stimuli-responsive chitosan-based drug  
1352 delivery biocomposite for multiple triggered release. *Int J Biol Macromol.* 2017; 104:  
1353 1407–14.
- 1354 135. Cao Y, Cheng Y, Zhao G. Near-Infrared Light-, Magneto-, and pH-Responsive  
1355 GO-Fe<sub>3</sub>O<sub>4</sub>/Poly(N-isopropylacrylamide)/alginate Nanocomposite Hydrogel  
1356 Microcapsules for Controlled Drug Release. *Langmuir ACS J Surf Colloids.* 2021; 37:  
1357 5522–30.
- 1358 136. Li L, Xiao B, Mu J, et al. A MnO<sub>2</sub> Nanoparticle-Dotted Hydrogel Promotes Spinal Cord  
1359 Repair via Regulating Reactive Oxygen Species Microenvironment and Synergizing  
1360 with Mesenchymal Stem Cells. *ACS Nano.* 2019; 13: 14283–93.
- 1361 137. Bi X, Bai Q, Liang M, et al. Silver Peroxide Nanoparticles for Combined Antibacterial  
1362 Sonodynamic and Photothermal Therapy. *Small.* 2022; 18: 2104160.

- 1363 138. Zhang B, Lv Y, Yu C, et al. Au–Pt nanozyme-based multifunctional hydrogel dressing  
1364 for diabetic wound healing. *Biomater Adv.* 2022; 137: 212869.
- 1365 139. Li Q, Lu F, Zhou G, et al. Silver Inlaid with Gold Nanoparticle/Chitosan Wound  
1366 Dressing Enhances Antibacterial Activity and Porosity, and Promotes Wound Healing.  
1367 *Biomacromolecules.* 2017; 18: 3766–75.
- 1368 140. Khan MdI, Behera SK, Paul P, et al. Biogenic Au@ZnO core–shell nanocomposites kill  
1369 *Staphylococcus aureus* without provoking nuclear damage and cytotoxicity in mouse  
1370 fibroblasts cells under hyperglycemic condition with enhanced wound healing  
1371 proficiency. *Med Microbiol Immunol (Berl).* 2019; 208: 609–29.
- 1372 141. Singh C, Mehata AK, Priya V, et al. Bimetallic Au–Ag Nanoparticles: Advanced  
1373 Nanotechnology for Tackling Antimicrobial Resistance. *Molecules.* 2022; 27: 7059.
- 1374 142. Nieto-Argüello A, Medina-Cruz D, Pérez-Ramírez YS, et al. Composition-Dependent  
1375 Cytotoxic and Antibacterial Activity of Biopolymer-Capped Ag/Au Bimetallic  
1376 Nanoparticles against Melanoma and Multidrug-Resistant Pathogens. *Nanomaterials.*  
1377 2022; 12: 779.
- 1378 143. Khan MI, Mazumdar A, Pathak S, et al. Biogenic Ag/CaO nanocomposites kill  
1379 *Staphylococcus aureus* with reduced toxicity towards mammalian cells. *Colloids Surf B*  
1380 *Biointerfaces.* 2020; 189: 110846.
- 1381 144. Ghaseminezhad SM, Shojaosadati SA, Meyer RL. Ag/Fe<sub>3</sub>O<sub>4</sub> nanocomposites  
1382 penetrate and eradicate *S. aureus* biofilm in an in vitro chronic wound model. *Colloids*  
1383 *Surf B Biointerfaces.* 2018; 163: 192–200.
- 1384 145. Panchal P, Paul DR, Sharma A, Choudhary P, Meena P, Nehra SP. Biogenic mediated  
1385 Ag/ZnO nanocomposites for photocatalytic and antibacterial activities towards  
1386 disinfection of water. *J Colloid Interface Sci.* 2020; 563: 370–80.
- 1387 146. Panchal P, Paul DR, Gautam S, et al. Photocatalytic and antibacterial activities of green  
1388 synthesized Ag doped MgO nanocomposites towards environmental sustainability.  
1389 *Chemosphere.* 2022; 297: 134182.
- 1390 147. Mao C, Xiang Y, Liu X, et al. Photo-Inspired Antibacterial Activity and Wound Healing  
1391 Acceleration by Hydrogel Embedded with Ag/Ag@AgCl/ZnO Nanostructures. *ACS*  
1392 *Nano.* 2017; 11: 9010–21.
- 1393 148. Varaprasad K, Mohan YM, Ravindra S, et al. Hydrogel-silver nanoparticle composites:  
1394 A new generation of antimicrobials. *J Appl Polym Sci.* 2010; 115: 1199–207.
- 1395 149. Zhai D, Liu B, Shi Y, et al. Highly sensitive glucose sensor based on pt  
1396 nanoparticle/polyaniline hydrogel heterostructures. *ACS Nano.* 2013; 7: 3540–6.
- 1397 150. Ramkumar VS, Pugazhendhi A, Prakash S, et al. Synthesis of platinum nanoparticles  
1398 using seaweed *Padina gymnospora* and their catalytic activity as PVP/PtNPs  
1399 nanocomposite towards biological applications. *Biomed Pharmacother.* 2017; 92:  
1400 479–90.

- 1401 151. Song C, Phuengkham H, Kim YS, et al. Syringeable immunotherapeutic nanogel  
1402 reshapes tumor microenvironment and prevents tumor metastasis and recurrence.  
1403 Nat Commun. 2019; 10: 3745.
- 1404 152. Jiang Y-W, Gao G, Hu P, et al. Palladium nanosheet-knotted injectable hydrogels  
1405 formed via palladium-sulfur bonding for synergistic chemo-photothermal therapy.  
1406 Nanoscale. 2020; 12: 210–9.
- 1407 153. Yin X, Fan T, Zheng N, et al. Palladium nanoparticle based smart hydrogels for NIR  
1408 light-triggered photothermal/photodynamic therapy and drug release with wound  
1409 healing capability. Nanoscale Adv. 2023; 5: 1729–39.
- 1410 154. Liang Y, Li Z, Huang Y, Yu R, Guo B. Dual-Dynamic-Bond Cross-Linked Antibacterial  
1411 Adhesive Hydrogel Sealants with On-Demand Removability for Post-Wound-Closure  
1412 and Infected Wound Healing. ACS Nano. 2021; 15: 7078–93.
- 1413 155. Ding M, Fan Y, Lv Y, et al. A prodrug hydrogel with tumor microenvironment and  
1414 near-infrared light dual-responsive action for synergistic cancer immunotherapy.  
1415 Acta Biomater. 2022; 149: 334–46.
- 1416 156. Sun X, Wang H, Ding Y, Yao Y, Liu Y, Tang J. Fe<sup>3+</sup>-Coordination mediated synergistic  
1417 dual-network conductive hydrogel as a sensitive and highly-stretchable strain sensor  
1418 with adjustable mechanical properties. J Mater Chem B. 2022; 10: 1442–52.
- 1419 157. Alsaaed FAT, El-Lateef HMA, Khalaf MM, Mohamed IMA, Al-Omair MA, Gouda M.  
1420 Drug Delivery System Based on Carboxymethyl Cellulose Containing Metal-Organic  
1421 Framework and Its Evaluation for Antibacterial Activity. Polymers. 2022; 14: 3815.
- 1422 158. He J, Fang J, Wei P, et al. Cancellous bone-like porous Fe@Zn scaffolds with  
1423 core-shell-structured skeletons for biodegradable bone implants. Acta Biomater.  
1424 2021; 121: 665–81.
- 1425 159. Li Z, You S, Mao R, et al. Architecting polyelectrolyte hydrogels with Cu-assisted  
1426 polydopamine nanoparticles for photothermal antibacterial therapy. Mater Today Bio.  
1427 2022; 15: 100264.
- 1428 160. Tao B, Lin C, Deng Y, et al. Copper-nanoparticle-embedded hydrogel for killing  
1429 bacteria and promoting wound healing with photothermal therapy. J Mater Chem B.  
1430 2019; 7: 2534–48.
- 1431 161. Pu Y, Wang P, Yang R, et al. Bio-fabricated nanocomposite hydrogel with ROS  
1432 scavenging and local oxygenation accelerates diabetic wound healing. J Mater Chem  
1433 B. 2022; 10: 4083–95.
- 1434 162. Wang S, Zheng H, Zhou L, et al. Nanoenzyme-Reinforced Injectable Hydrogel for  
1435 Healing Diabetic Wounds Infected with Multidrug Resistant Bacteria. Nano Lett. 2020;  
1436 20: 5149–58.
- 1437 163. Saraf P, Abdollahi Movaghar M, Montazer M, Mahmoudi Rad M. Bio and photoactive  
1438 starch/MnO<sub>2</sub> and starch/MnO<sub>2</sub>/cotton hydrogel nanocomposite. Int J Biol Macromol.

1439 2021; 193: 681–92.

1440 164. Tu C, Lu H, Zhou T, et al. Promoting the healing of infected diabetic wound by an  
1441 anti-bacterial and nano-enzyme-containing hydrogel with inflammation-suppressing,  
1442 ROS-scavenging, oxygen and nitric oxide-generating properties. *Biomaterials*. 2022;  
1443 286: 121597.

1444 165. Anjum S, Nawaz K, Ahmad B, Hano C, Abbasi BH. Green synthesis of biocompatible  
1445 core-shell (Au–Ag) and hybrid (Au–ZnO and Ag–ZnO) bimetallic nanoparticles and  
1446 evaluation of their potential antibacterial, antidiabetic, antiglycation and anticancer  
1447 activities. *RSC Adv*. 12: 23845–59.

1448 166. Singh C, Mehata AK, Priya V, et al. Bimetallic Au-Ag Nanoparticles: Advanced  
1449 Nanotechnology for Tackling Antimicrobial Resistance. *Mol Basel Switz*. 2022; 27:  
1450 7059.

1451 167. Chen X, Tao J, Zhang M, et al. Iota carrageenan gold-silver NPs photothermal  
1452 hydrogel for tumor postsurgical anti-recurrence and wound healing. *Carbohydr*  
1453 *Polym*. 2022; 298: 120123.

1454 168. Hong EJ, Sivakumar P, Ravichandran V, Choi DG, Kim Y-S, Shim MS. Pro-Oxidant  
1455 Drug-Loaded Au/ZnO Hybrid Nanoparticles for Cancer-Specific  
1456 Chemo-Photodynamic Combination Therapy. *ACS Biomater Sci Eng*. 2019; 5:  
1457 5209–17.

1458 169. Mao C, Xiang Y, Liu X, et al. Photo-Inspired Antibacterial Activity and Wound Healing  
1459 Acceleration by Hydrogel Embedded with Ag/Ag@AgCl/ZnO Nanostructures. *ACS*  
1460 *Nano*. 2017; 11: 9010–21.

1461 170. Majhi RK, Mohanty S, Khan MI, Mishra A, Brauner A. Ag@ZnO Nanoparticles Induce  
1462 Antimicrobial Peptides and Promote Migration and Antibacterial Activity of  
1463 Keratinocytes. *ACS Infect Dis*. 2021; 7: 2068–72.

1464 171. Aioub M, Panikkanvalappil SR, El-Sayed MA. Platinum-Coated Gold Nanorods:  
1465 Efficient Reactive Oxygen Scavengers That Prevent Oxidative Damage toward Healthy,  
1466 Untreated Cells during Plasmonic Photothermal Therapy. *ACS Nano*. 2017; 11:  
1467 579–86.

1468 172. Han HH, Kim S-J, Kim J, et al. Bimetallic Hyaluronate-Modified Au@Pt Nanoparticles  
1469 for Noninvasive Photoacoustic Imaging and Photothermal Therapy of Skin Cancer.  
1470 *ACS Appl Mater Interfaces*. 2023; 15: 11609–20.

1471 173. Duan Q, Wang J, Zhang B, et al. Polydopamine coated Au-Pt nanorods: Enhanced  
1472 photothermal properties and efficient reactive oxygen scavengers. *Colloids Surf B*  
1473 *Biointerfaces*. 2022; 210: 112247.

1474 174. Eghbalifam N, Shojaosadati SA, Hashemi-Najafabadi S. Role of bioactive magnetic  
1475 nanoparticles in the prevention of wound pathogenic biofilm formation using smart  
1476 nanocomposites. *J Nanobiotechnology*. 2023; 21: 161.



- 1477 175. Xu J, Ma S, Zhang W, et al. In vitro magnetosome remineralization for  
1478 silver-magnetite hybrid magnetosome biosynthesis and used for healing of the  
1479 infected wound. *J Nanobiotechnology*. 2022; 20: 364.
- 1480 176. Ming J, Zhu T, Yang W, et al. Pd@Pt-GOx/HA as a Novel Enzymatic Cascade  
1481 Nanoreactor for High-Efficiency Starving-Enhanced Chemodynamic Cancer Therapy.  
1482 *ACS Appl Mater Interfaces*. 2020; 12: 51249–62.
- 1483 177. Wei J, Li J, Sun D, et al. A Novel Theranostic Nanoplatform Based on Pd@Pt-PEG-Ce6  
1484 for Enhanced Photodynamic Therapy by Modulating Tumor Hypoxia  
1485 Microenvironment. *Adv Funct Mater*. 2018; 28: 1706310.
- 1486 178. Badhwar R, Mangla B, Neupane YR, Khanna K, Popli H. Quercetin loaded silver  
1487 nanoparticles in hydrogel matrices for diabetic wound healing. *Nanotechnology*. 2021;  
1488 32.
- 1489 179. Li Y, Fu R, Duan Z, Zhu C, Fan D. Artificial Nonenzymatic Antioxidant MXene  
1490 Nanosheet-Anchored Injectable Hydrogel as a Mild Photothermal-Controlled  
1491 Oxygen Release Platform for Diabetic Wound Healing. *ACS Nano*. 2022; 16:  
1492 7486–502.
- 1493 180. Huang Y, Bai L, Yang Y, Yin Z, Guo B. Biodegradable gelatin/silver nanoparticle  
1494 composite cryogel with excellent antibacterial and antibiofilm activity and hemostasis  
1495 for *Pseudomonas aeruginosa*-infected burn wound healing. *J Colloid Interface Sci*.  
1496 2022; 608: 2278–89.
- 1497 181. Jhumi IJ, Arafat T-A-, Karmakar PC, et al. Silver Nanoparticle Incorporated Human  
1498 Amniotic Membrane Gel Accelerates Second-Degree Burn Wound Healing in Wister  
1499 Rat. *Evid-Based Complement Altern Med ECAM*. 2023; 2023: 9808556.
- 1500 182. Kim MH, Park H, Nam HC, Park SR, Jung J-Y, Park WH. Injectable methylcellulose  
1501 hydrogel containing silver oxide nanoparticles for burn wound healing. *Carbohydr*  
1502 *Polym*. 2018; 181: 579–86.
- 1503 183. Dai T, Wang C, Wang Y, Xu W, Hu J, Cheng Y. A Nanocomposite Hydrogel with Potent  
1504 and Broad-Spectrum Antibacterial Activity. *ACS Appl Mater Interfaces*. 2018; 10:  
1505 15163–73.
- 1506 184. Xu T, Zhang J, Zhu Y, et al. A poly(hydroxyethyl methacrylate)–Ag nanoparticle porous  
1507 hydrogel for simultaneous *in vivo* prevention of the foreign-body reaction and  
1508 bacterial infection. *Nanotechnology*. 2018; 29: 395101.
- 1509 185. Fischer M, Vahdatzadeh M, Konradi R, et al. Multilayer hydrogel coatings to combine  
1510 hemocompatibility and antimicrobial activity. *Biomaterials*. 2015; 56: 198–205.
- 1511 186. Zulkifli FH, Hussain FSJ, Zeyohannes SS, Rasad MSBA, Yusuff MM. A facile synthesis  
1512 method of hydroxyethyl cellulose-silver nanoparticle scaffolds for skin tissue  
1513 engineering applications. *Mater Sci Eng C Mater Biol Appl*. 2017; 79: 151–60.
- 1514 187. Rakhshaei R, Namazi H, Hamishehkar H, Kafil HS, Salehi R. In situ synthesized

1515 chitosan–gelatin/ZnO nanocomposite scaffold with drug delivery properties: Higher  
1516 antibacterial and lower cytotoxicity effects. *J Appl Polym Sci.* 2019; 136: 47590.

1517 188. Pastar I, Stojadinovic O, Yin NC, et al. Epithelialization in Wound Healing: A  
1518 Comprehensive Review. *Adv Wound Care.* 2014; 3: 445–64.

1519 189. Kirker KR, Secor PR, James GA, Fleckman P, Olerud JE, Stewart PS. Loss of viability and  
1520 induction of apoptosis in human keratinocytes exposed to *Staphylococcus aureus*  
1521 biofilms in vitro. *Wound Repair Regen Off Publ Wound Heal Soc Eur Tissue Repair Soc.*  
1522 2009; 17: 690–9.

1523 190. Leung KP, D'Arpa P, Seth AK, et al. Dermal wound transcriptomic responses to  
1524 Infection with *Pseudomonas aeruginosa* versus *Klebsiella pneumoniae* in a rabbit ear  
1525 wound model. *BMC Clin Pathol.* 2014; 14: 20.

1526 191. Greenhalgh DG. Management of Burns. *N Engl J Med.* 2019; 380: 2349–59.

1527 192. Bodelón G, Montes-García V, López-Puente V, et al. Detection and imaging of  
1528 quorum sensing in *Pseudomonas aeruginosa* biofilm communities by  
1529 surface-enhanced resonance Raman scattering. *Nat Mater.* 2016; 15: 1203–11.

1530 193. Xu L, Li X, Takemura T, Hanagata N, Wu G, Chou L. Genotoxicity and molecular  
1531 response of silver nanoparticle (NP)-based hydrogel. *J Nanobiotechnology.* 2012; 10:  
1532 16.

1533 194. Guimarães CF, Ahmed R, Marques AP, Reis RL, Demirci U. Engineering  
1534 Hydrogel-Based Biomedical Photonics: Design, Fabrication, and Applications. *Adv*  
1535 *Mater Deerfield Beach Fla.* 2021; 33: e2006582.

1536 195. Abdollahiyan P, Baradaran B, de la Guardia M, Oroojalian F, Mokhtarzadeh A.  
1537 Cutting-edge progress and challenges in stimuli responsive hydrogel  
1538 microenvironment for success in tissue engineering today. *J Control Release Off J*  
1539 *Control Release Soc.* 2020; 328: 514–31.

1540 196. Chyzy A, Plonska-Brzezinska ME. Hydrogel Properties and Their Impact on  
1541 Regenerative Medicine and Tissue Engineering. *Mol Basel Switz.* 2020; 25: 5795.

1542 197. Heo DN, Ko W-K, Bae MS, et al. Enhanced bone regeneration with a gold  
1543 nanoparticle–hydrogel complex. *J Mater Chem B.* 2014; 2: 1584–93.

1544 198. Cao Z, Wang H, Chen J, et al. Silk-based hydrogel incorporated with metal-organic  
1545 framework nanozymes for enhanced osteochondral regeneration. *Bioact Mater.* 2022;  
1546 20: 221–42.

1547 199. Cao Z, Wang D, Li Y, et al. Effect of nanoheat stimulation mediated by magnetic  
1548 nanocomposite hydrogel on the osteogenic differentiation of mesenchymal stem cells.  
1549 *Sci China Life Sci.* 2018; 61: 448–56.

1550 200. Zhao Y, Lo C-Y, Ruan L, et al. Somatosensory actuator based on stretchable  
1551 conductive photothermally responsive hydrogel. *Sci Robot.* 2021; 6: eabd5483.

