

EphA2-targeted alpha particle theranostics for enhancing PDAC treatment

Ajay Kumar Sharma^{1±}, *Kuldeep Gupta*^{1±}, *Akhilesh Mishra*¹, *Gabriela Lofland*¹, *Sophia Y. Chen*², *Ian Marsh*¹, *Peyton T Fair*², *Robert F. Hobbs*¹, *Todd M. Armstrong*², *Elizabeth M. Jaffee*², *Edward Gabrielson*³, *Lei Zheng*², and *Sridhar Nimmagadda*^{1, 2, 4, 5, *}

Author affiliations:

¹The Russell H. Morgan Department of Radiology and Radiological Science

²Department of Oncology, The Sidney Kimmel Comprehensive Cancer Center and the Bloomberg–Kimmel Institute for Cancer Immunotherapy

³Department of Pathology and Oncology

⁴Department of Pharmacology and Molecular Sciences

⁵Division of Clinical Pharmacology, Department of Medicine

Johns Hopkins University School of Medicine,

Baltimore, MD, 21287, USA.

±authors contributed equally

*Correspondence to: Sridhar Nimmagadda, Ph.D.
Johns Hopkins Medical Institutions
1550 Orleans Street, CRB II, #492
Baltimore, MD 21287
Phone: 410-502-6244
Fax: 410-614-3147
Email: snimmag1@jhmi.edu

Keywords: Pancreatic cancer, PET, Imaging, Radiotherapy, Peptide radiopharmaceuticals, Gallium-68, Alpha-particle therapy

ABSTRACT

Background: Pancreatic ductal adenocarcinoma (PDAC) presents a formidable challenge in oncology due to its aggressive nature and resistance to therapy. Current treatments, including surgery, chemotherapy, and radiotherapy, have limited success in improving patient outcomes. This study addresses the urgent need for novel radiotheranostic strategies for PDAC by investigating EphA2 as a potential target.

Methods and Results: Analysis of genomic data from the Cancer Cell Line Encyclopedia (CCLE) and The Cancer Genome Atlas (TCGA) revealed elevated EphA2 expression in PDAC, confirmed by immunohistochemical staining of tumor tissue microarrays (TMAs). Further analysis showed variable EphA2 expression across PDAC cell lines, with surface receptor density not always correlating with mRNA levels. A low molecular weight peptide was developed and labeled with gallium-68 for PET imaging. *In vitro* studies demonstrated specific binding to EphA2-expressing PDAC cells with rapid internalization. *In vivo* PET imaging in subcutaneous and orthotopic PDAC models confirmed high tumor uptake and minimal off-target binding, confirming EphA2 as a valid imaging target. For molecular radiotherapy, a DOTA-conjugated peptide was labeled with the alpha-particle emitter, actinium-225. *In vitro* studies revealed dose-dependent cytotoxicity in PDAC cells, with an IC₅₀ of 0.32 µCi/mL. In a tumor model, treatment with Ac-225 labeled peptide significantly inhibited tumor growth compared to controls, with mild adverse effects.

Conclusion: These results establish EphA2 as a promising radiotheranostic target in PDAC, with potential for both non-invasive imaging and targeted radiotherapy. Given the potential, further optimization of EphA2-targeted agents are warranted to advance personalized treatment strategies for PDAC patients.

Introduction

Pancreatic ductal adenocarcinoma (PDAC) is a recalcitrant disease with a mortality rate nearly equivalent to its incidence rate [1, 2]. Most PDAC patients present with distant metastasis at diagnosis and only about 12% are predicted to survive beyond 5 years [1]. This dismal outlook stems from the disease's elusive nature, marked by an inability to detect it early coupled with high therapeutic resistance attributed to the dense desmoplastic stroma and immune suppressive microenvironment characteristic of PDAC [3].

Current clinical management of PDAC involves a triad of approaches including surgery, systemic chemotherapy, and radiotherapy [1]. However, while these modalities have shown efficacy in certain contexts, they often fall short in significantly improving patient outcomes. Despite the groundbreaking successes witnessed with checkpoint immunotherapies and molecular radiotherapy in other solid malignancies, their translation to PDAC has been met with limited success [3, 4]. The promise of molecular radiotherapy, which is transforming the landscape of advanced cancer management, particularly evident in prostate and neuroendocrine cancers [5], remains largely unfulfilled in PDAC due to the scarcity of suitable radiotheranostic targets and agents tailored to this aggressive disease.

Radiopharmaceutical therapy (RPT) has emerged as a promising treatment approach for multifocal disease, delivering targeted radiation to cancer cells across disseminated disease sites while sparing healthy tissues [6, 7]. Among RPT strategies, targeted alpha-emitter therapy (TAT) stands out, as it induces largely irreparable double-strand DNA breaks, leading to highly selective cytotoxicity in cancer cells [8, 9]. Actinium-225 (^{225}Ac) is a potent alpha emitting radionuclide used in TAT due to its high linear energy transfer (LET), leading to potent cancer cell killing, and its short path length (around 100 μm), minimizing off-target toxicity [10, 11]. Preliminary data suggest that alpha-emitting radionuclides have a significantly lower impact on kidney function compared to beta-emitting radionuclides [12], although, additional studies are required to assess long-term renal toxicity. The clinical use of ^{225}Ac could also be impacted by restricted availability, high production costs, and the complex management of its radioactive decay products, which can cause unintended radiation exposure. Despite these challenges, ^{225}Ac -based therapies, such as [^{225}Ac]Ac-PSMA-617 for metastatic prostate cancer and [^{225}Ac]Ac-DOTATATE for neuroendocrine tumors, are demonstrating significant promise, especially for patients resistant to beta-emitting therapies or with radioresistant tumors [13, 14]. These approaches, which are in various stages of clinical and preclinical evaluation, underscore the potential for developing similar therapeutic options for PDAC.

Given these advancements, there is a pressing need for the development of novel radiotheranostic approaches specifically tailored to address the challenges of PDAC. Low molecular weight peptide-based imaging agents, such as those targeting somatostatin receptor 2 (SSTR2) and fibroblast activation protein (FAP), have shown some utility in PDAC [6, 7]. Nonetheless, the repertoire of such agents remains limited for PDAC, particularly in the realm of effective radiotherapeutics. One promising target is EphA2 (Ephrin receptor A2), which is highly expressed in PDAC and implicated in cancer progression through its roles in cell adhesion, migration, proliferation, and the maintenance of the tumor's immune suppressive microenvironment [15]. Although antibody-based agents have been developed for EphA2 [16], low molecular weight agents offer better pharmacokinetics and improved tumor penetration, opening new avenues for targeted molecular radiotherapy in PDAC [17, 18].

Previous efforts to target EphA2 have focused on developing antibody constructs for imaging. Examples include [^{64}Cu]DOTA-1C1 mAb, which binds both human and mouse EphA2 and has been used for noninvasive PET imaging of EphA2 in colorectal, melanoma, glioblastoma, and ovarian cancers [19]. Radiolabeled analogs of other anti-EphA2 antibodies, such as DS-8895a and 4B3, have similarly shown promise in detecting EphA2 expression non-invasively [20, 21]. Despite these successes, antibody-based agents have limitations, such as suboptimal pharmacokinetics and high production costs. Low molecular weight agents exhibit tractable pharmacokinetics, improved tumor penetration, reduced immunogenicity, and lower production costs. Peptide-based agents like [^{18}F]AFP-SWL, [$^{99\text{m}}\text{Tc}$]HYNIC-SWL, and [^{68}Ga]DOTA-SD01 have shown specificity for EphA2 in melanoma, non-small cell lung, and breast cancers, but issues with plasma degradation and low tumor uptake have limited their use [22-24]. Recently developed high-affinity bicyclic peptides, including [^{18}F]AIF-ETN and [^{68}Ga]Ga-BCY18469, demonstrate *in vivo* stability and enhanced imaging contrast in prostate and fibrosarcoma models [25, 26], further highlighting the potential of EphA2 as a radiotheranostic target.

In this study, we report the validation of EphA2 as a radiotheranostic target in PDAC. Leveraging genomic data sets and immunohistochemical (IHC) analyses of human tumor samples, we demonstrate the potential of EphA2 as a molecular radiotherapy target in PDAC. We detail the development of gallium-68 (^{68}Ga) labeled peptide-based radiotracers for PET imaging, evaluating their pharmacokinetics, biodistribution, and EphA2 specificity both *in vitro* and *in vivo* across a spectrum of PDAC models. Additionally, we introduce an Actinium-225 (^{225}Ac) radiotherapeutic analog and assess its efficacy in controlling tumor growth in PDAC models, thereby paving the way for targeted therapeutic interventions in this recalcitrant disease.

Results

Analysis of EphA2 expression in CCLE and TCGA human genomic database.

EphA2 plays a crucial role in cancer tumorigenesis and has been considered a potential therapeutic target [15]. However, to fully harness its potential as an imaging and therapeutic target, a detailed and comparative understanding of EphA2 expression in both cancerous and healthy tissues is necessary.

An analysis of genomic data from the Cancer Cell Line Encyclopedia (CCLE) revealed variable expression of the EphA2 gene across different human cancer cell lines, with pancreatic cancer cells showing higher expression levels compared to others (**Figure 1A**). To validate the cell line data and characterize EphA2 expression in human cancers, we analyzed genomic data from The Cancer Genome Atlas (TCGA). This analysis showed variable expression of EphA2 across different human cancer types, with notably high expression in pancreatic, bladder, and colorectal cancers, and low expression in lung, breast, prostate, and lymphoma. The median expression of the EphA2 gene was particularly high in pancreatic cancer compared to other cancer types (**Figure 1B**). Furthermore, EphA2 expression was consistently higher in tumors compared to their corresponding normal tissues, with the most significant difference observed between PDAC and normal pancreas tissue (**Figure 1C**). To confirm the database mining results, we further analyzed PDAC samples in a TMA by IHC analysis and found that more than 95% of tumor samples stained for membranous EphA2 expression (**Figure S1**).

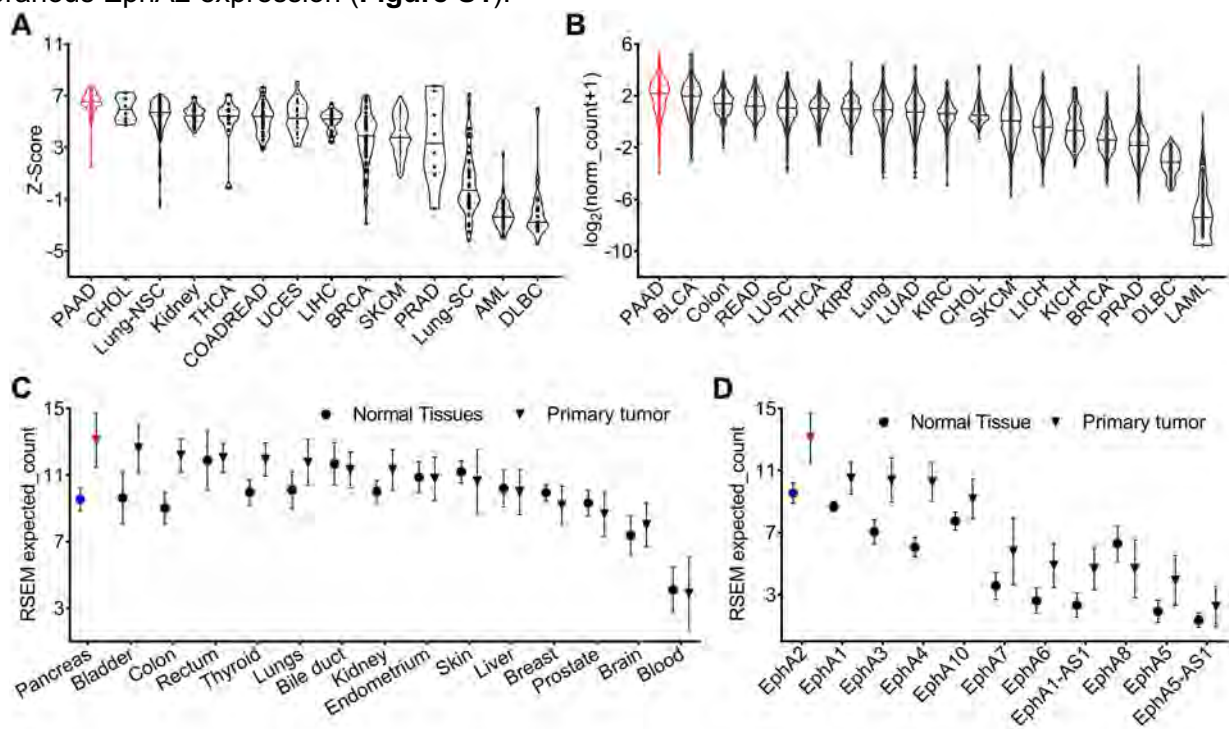


Figure 1. CCLE and TCGA database of mRNA expression of EphA2. **A)** EphA2 expression in cell lines in CCLE. **B)** EphA2 mRNA expression in different types of tumors in TCGA. **C)** Comparison of mRNA expression of EphA2 in different normal tissues and corresponding tumors. **D)** Expression of different EPH receptors in pancreatic tumors. PAAD = pancreatic cancer; BLCA = Bladder cancer; READ = Rectal cancer; LUSC = Lung squamous cell carcinoma; THCA = Thyroid cancer; KIRP = Kidney papillary cell carcinoma; LUAD = Lung adenocarcinoma; KIRC = Kidney clear cell carcinoma; CHOL = Bile duct cancer; SKCM = melanoma; LIHC = Liver cancer; KICH = Kidney chromophobe; BRCA = Breast cancer; PRAD = Prostate cancer; DLBC = Large-B-cell lymphoma; LAML = Acute myeloid leukemia.

Within the Ephrin receptor family, nine different functional receptors (EphA1-EphA9) are known in the mouse and human genomes. To understand the expression of different Ephrin receptors in PDAC, we analyzed the TCGA dataset and compared the expression of different Ephrin receptors in PDAC and healthy pancreas tissue. Our analysis revealed greater expression of EphA2 in PDAC compared to other Eph receptors (**Figure 1D**). Collectively, these genomic analyses highlight the high expression pattern of EphA2 in PDAC, which may provide a robust platform for the development of radiotheranostic agents.

Structure and evaluation of AJ201 for EphA2 receptor binding.

Recently, low molecular weight peptides that bind EphA2 have been reported. Here, we introduce AJ201, a 15-amino acid bicyclic peptide derived from BCY6099, comprising six hydrophilic and nine hydrophobic amino acids [17, 18]. To enhance its hydrophilicity, we incorporated a linker with a bis-ethylene glycol moiety and three sarcosine amino acid chain, whereas BCY6099 utilizes a linker composed of 10 sarcosine units. Since peptides often undergo renal clearance, we have further modified AJ201 by incorporating an arginine and a glycine motif, a known brush border membrane cleavable linker, with the goal of reducing renal retention of radioactivity. To facilitate radiotracer generation, the modified 24-amino acid peptide was then conjugated with bifunctional chelators, NOTA (1,4,7-Triazacyclononane-1,4,7-triacetic acid) (**Figure 2A**) and DOTA (2,2',2'',2'''-(1,4,7,10-tetraazacyclododecane-1,4,7,10-tetrayl)tetraacetic acid) and characterized by mass spectrometry (**Figure S2**). NOTA is extensively used to form a highly stable complex with the radiometal [⁶⁸Ga], while DOTA serves as a chelator for both [⁶⁸Ga] and [¹⁷⁷Lu] the latter being part of an FDA-approved radiotheranostic pair [27].

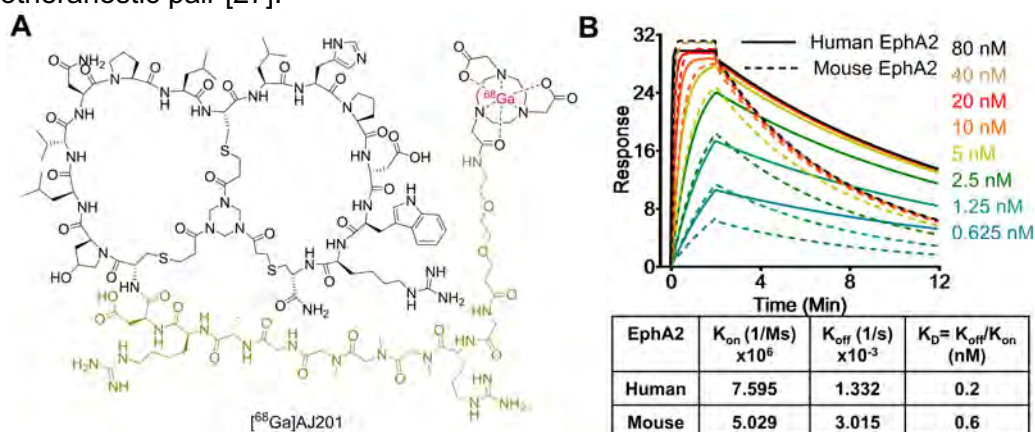


Figure 2. Structure and *in vitro* characterization of AJ201. **A**) Structure of bicyclic peptide AJ201 having NOTA as bifunctional chelator for ⁶⁸Ga-labeling. In the structure, black color represents binding moiety, parakeet color represents the linker and red color represents the radiometal **B**) Surface plasmon resonance (SPR) analysis showing affinity of AJ201 for EphA2 using recombinant human (solid) and mouse (dashed) EphA2 proteins.

To assess the affinity of AJ201 for EphA2, we conducted surface plasmon resonance (SPR) assays (**Table S1**). The results showed that AJ201 binds to both human and mouse EphA2 with strong affinity, displaying dissociation constants (K_D) of 0.2 nM and 0.6 nM, respectively (**Figure 2B**). These findings suggest that AJ201 is a promising candidate for further development as a molecular imaging agent for tumor detection.

Evaluation of EphA2 receptor expression in PDAC cell lines by RT-PCR and flow cytometry.

To confirm the observations from the CCLE dataset, we selected seven human PDAC cell lines (CFPAC1, Panc1005, BxPC3, Hs766T, AsPC1, Su8686, and Panc1) and evaluated EphA2 expression using RT-PCR and flow cytometry. Jurkat cells, a human T lymphocyte cell line, served as a negative control. RT-PCR analysis revealed high and variable expression levels of EphA2 mRNA in all the PDAC cell lines tested, while Jurkat cells showed only basal expression (**Figure 3A**). These findings were corroborated by flow cytometry, which assessed cell surface EphA2 expression. High and variable levels of cell surface EphA2 were detected across all PDAC cell lines, with the highest expression in Panc1 cells and the lowest in Jurkat cells (**Figure 3B**).

Further analysis of receptor density in PDAC cells using PE-Quantibrite beads demonstrated significant variability. Panc1 cells exhibited the highest receptor density (2.7×10^5 receptors per cell), while CFPAC1 cells had the lowest (0.58×10^5 receptors per cell) (**Figure 3C**). Other PDAC cell lines showed the following receptor densities: Panc1005 (0.68×10^5), BxPC3 (0.85×10^5), HS766T (1.3×10^5), AsPC1 (1.55×10^5), and Su8686 (2.48×10^5).

Interestingly, we did not observe a clear positive relationship between mRNA abundance and receptor density in PDAC cells. This discrepancy underscores the importance of validating EphA2 expression through multiple methods to complement genomic data and better understand the activity of EphA2-targeted therapeutics.

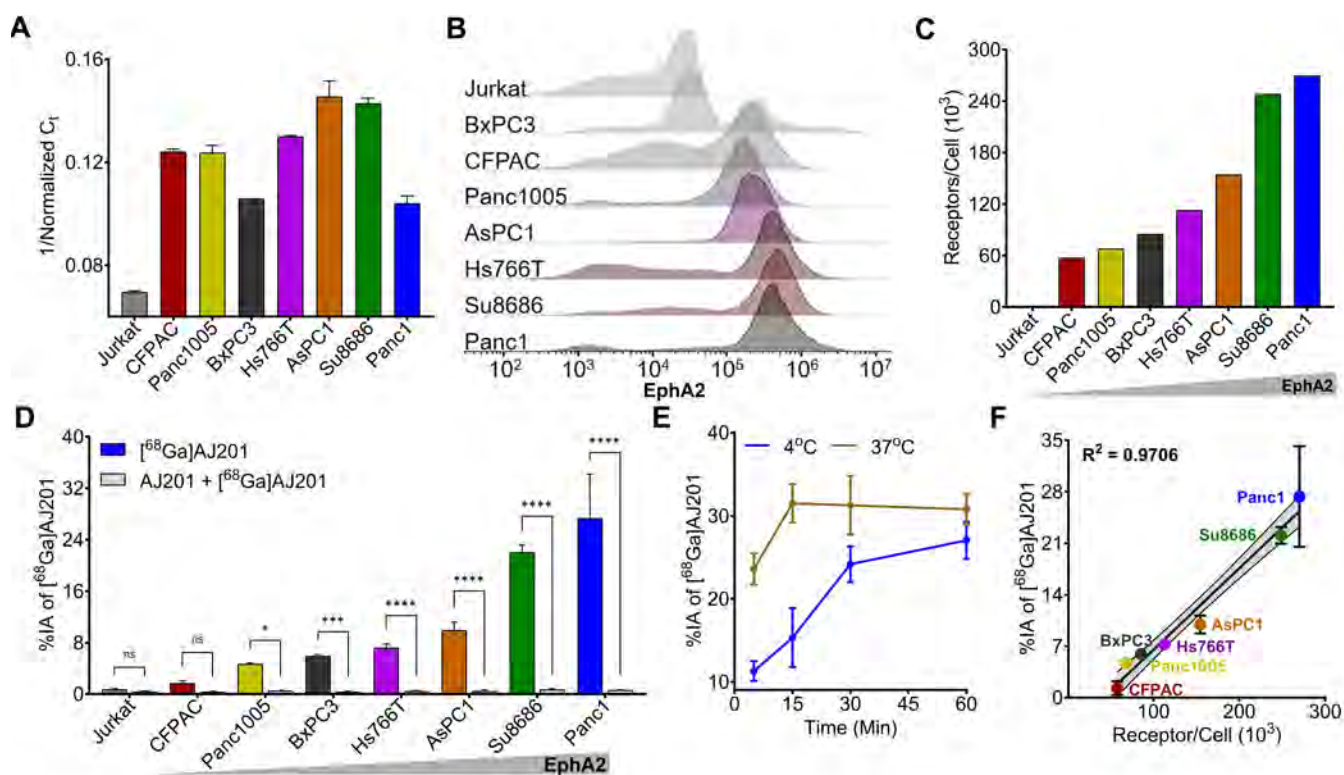


Figure 3. *In vitro* specificity of $[^{68}\text{Ga}]\text{AJ201}$ for EphA2 in human pancreatic cancer cells. A) Quantification of EphA2-mRNA using RT-PCR. **B)** Flow cytometry analysis of EphA2 receptor expression on cell surface. **C)** A representative plot of EphA2 receptor density in PDAC cells measured by quantibrite assay. **D)** $[^{68}\text{Ga}]\text{AJ201}$ binding (percent incubated activity, %IA) to different cells. Cells were incubated with $1\ \mu\text{Ci}$ $[^{68}\text{Ga}]\text{AJ201}$ at $4\ ^\circ\text{C}$ for 1 h. $[^{68}\text{Ga}]\text{AJ201}$ uptake is EphA2 expression dependent, and co-incubation with $2\ \mu\text{M}$ of non-radioactive AJ201 ($0.2\ \text{nmol}$, blocking dose) significantly reduced radiotracer uptake confirming EphA2 specificity. **E)** *In vitro* uptake of $[^{68}\text{Ga}]\text{AJ201}$ over 60 min in Panc1 cells at $4\ ^\circ\text{C}$ and $37\ ^\circ\text{C}$. **F)** Correlation of $[^{68}\text{Ga}]\text{AJ201}$ uptake with surface EphA2 receptor density. Data in panels **A**, **D**, **E** and **F** are presented as mean \pm SD ($n = 3-4$). Significance was calculated using multiple unpaired *t* test in **D**; ns, $P \geq 0.05$; *, $P \leq 0.05$; ***, $P \leq 0.001$; ****, $P \leq 0.0001$. Simple linear regression and Pearson coefficient were used in **F**. All *in vitro* experiments were performed three times and representatives are shown.

Radiolabeling and *in vitro* evaluation of $[^{68}\text{Ga}]\text{AJ201}$.

To develop a PET imaging agent, AJ201 was labeled with $[^{68}\text{Ga}]$, achieving high radiochemical yields ($66 \pm 25\%$, $n = 53$, decay-corrected), radiochemical purity ($>98\%$), moderate specific activity ($15-20\ \text{GBq}/\mu\text{mol}$) and co-eluted with $[^{\text{nat}}\text{Ga}]\text{AJ201}$, confirming its chemical identity (**Scheme S2**, **Figure S3**). $[^{68}\text{Ga}]\text{AJ201}$ demonstrated excellent stability at $37\ ^\circ\text{C}$ for at least 3 h in formulation buffer (10% EtOH/saline) and human serum (**Figure S4**).

We conducted cell binding assays to assess the *in vitro* specificity of $[^{68}\text{Ga}]\text{AJ201}$ for EphA2. Seven PDAC cell lines were incubated with $1\ \mu\text{Ci}$ $[^{68}\text{Ga}]\text{AJ201}$ for 60 min, followed by washing and measurement of cell-associated activity. All steps were done at $4\ ^\circ\text{C}$ to minimize internalization. We observed variable uptake of $[^{68}\text{Ga}]\text{AJ201}$, with the highest uptake in Panc1 cells (27.4 ± 6.8 percent incubated activity, %IA) and the lowest in CFPAC cells (1.7 ± 0.3 %IA). The uptake order was: Panc1 (27.4 ± 6.8 %IA) > Su8686 (22.0 ± 1.1 %IA) > AsPC1 (9.9 ± 1.2 %IA) > Hs766T (7.2 ± 0.6 %IA) > BxPC3 (5.9 ± 0.2 %IA) > Panc1005 (4.7 ± 0.1 %IA) > CFPAC (1.7 ± 0.3 %IA). The least radioactivity was bound to Jurkat cells (0.8 ± 0.1 %IA), which showed basal EphA2 expression (**Figure 3D**). These results indicate that $[^{68}\text{Ga}]\text{AJ201}$ binding to PDAC cells is dependent on EphA2 expression on the cell surface.

To understand binding kinetics, Panc1 cells were incubated with $[^{68}\text{Ga}]\text{AJ201}$ at $4\ ^\circ\text{C}$ and $37\ ^\circ\text{C}$ for different time intervals (**Figure 3E**). We observed rapid uptake of radioactivity by Panc1 cells, reaching a plateau within 60 min. At $37\ ^\circ\text{C}$, uptake was fast, reaching equilibrium by 15 min, with a slight decline between 15 and 60 min. In contrast, at $4\ ^\circ\text{C}$, uptake was slower, stabilizing around 30 min without a subsequent decrease. These differences likely reflect faster binding and internalization at $37\ ^\circ\text{C}$, with a greater overall magnitude, indicating that $[^{68}\text{Ga}]\text{AJ201}$ is rapidly internalized upon binding to EphA2. To confirm the specificity of $[^{68}\text{Ga}]\text{AJ201}$ binding to EphA2, we conducted additional experiments. Binding of $[^{68}\text{Ga}]\text{AJ201}$ to Panc1 cells was significantly reduced by more than 95% ($P < 0.0001$) in the presence of non-radioactive AJ201 ($2\ \mu\text{M}$), confirming that $[^{68}\text{Ga}]\text{AJ201}$ binding is specific to EphA2 (**Figure 3D**). Further validation involved correlating $[^{68}\text{Ga}]\text{AJ201}$ uptake with receptor density quantified using Quantibrite beads. The results showed a strong

correlation between radiotracer uptake and receptor density ($R^2 = 0.97$, $P < 0.0001$) (**Figure 3F**). These findings collectively demonstrate that the *in vitro* binding of [^{68}Ga]AJ201 to PDAC cells is directly dependent on surface expression of EphA2.

***In vivo* distribution of radiotracer in mice bearing human tumor xenografts.**

To evaluate the pharmacokinetics of [^{68}Ga]AJ201, we conducted whole-body dynamic PET scans on mice with Panc1 tumor xenografts. [^{68}Ga]AJ201 uptake was observed in Panc1 tumors within 5 min post-administration (**Figure 4A**). High accumulation of radioactivity in the Panc1 tumors and washout from healthy tissues resulted in high-contrast tumor-specific images by 60 min. However, high radioactivity accumulation was also observed in the kidneys. Region of Interest (ROI) analysis indicated continuous accumulation of radioactivity in tumors, peaking at 30 min and remaining constant until 90 min. In contrast, there was continuous washout of radioactivity from non-target tissues such as muscle (**Figure 4B**). Collectively, these data indicate that [^{68}Ga]AJ201 exhibits optimal pharmacokinetics and biodistribution, providing high-contrast images of PDAC within 60 min post-administration.

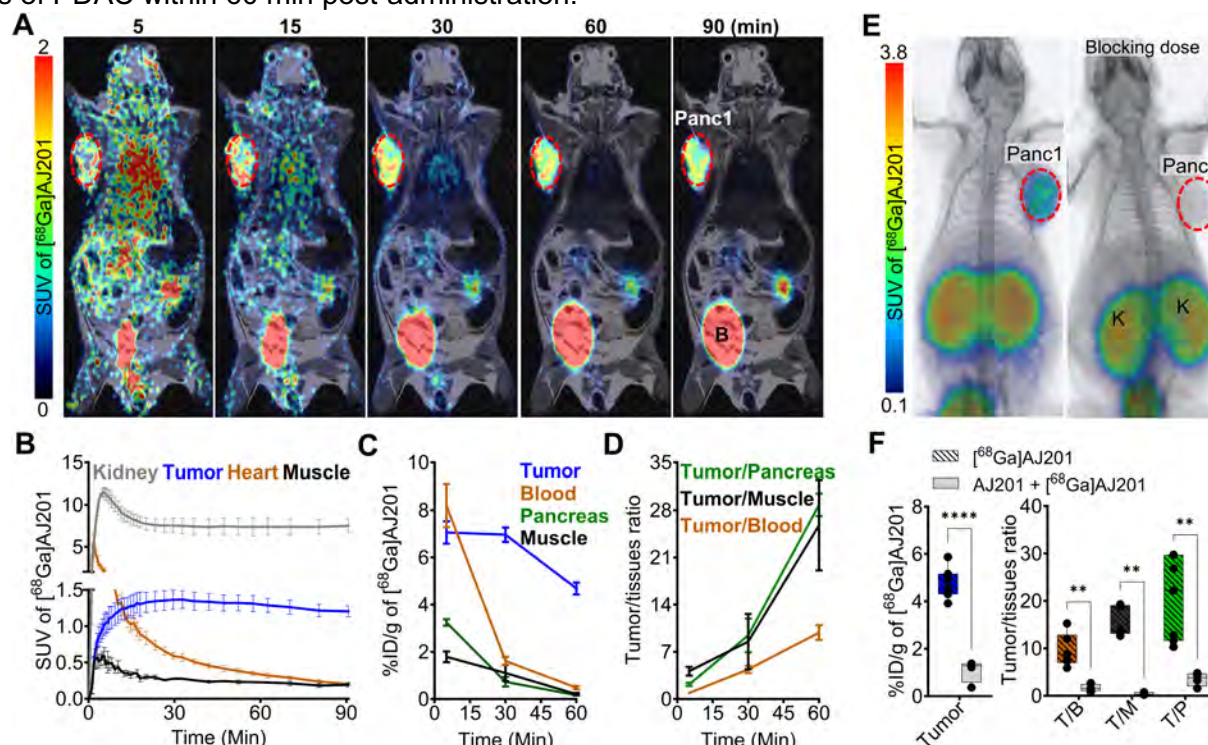


Figure 4. Pharmacokinetics of [^{68}Ga]AJ201 in NSG mice bearing Panc1 tumor xenografts. A) Coronal sections of the fused dynamic PET/MR images showing [^{68}Ga]AJ201 distribution. Primary tumor is indicated by red circle. Mice were intravenously injected with ~ 9.25 MBq (~ 250 μCi) [^{68}Ga]AJ201; B, Bladder. **B)** Time-activity curves of [^{68}Ga]AJ201 in the kidney, tumor, heart and muscle derived from PET data in A. **C)** Uptake of [^{68}Ga]AJ201 in tumor, blood, pancreas and muscle derived from *ex vivo* biodistribution study (percent incubated dose per gram, %ID/g). **D)** Tumor-to-muscle, tumor-to-blood and tumor-to-pancreas ratios derived from biodistribution data. **E)** Whole-body PET/CT images of Panc1 xenografts with [^{68}Ga]AJ201, without (left) and with (right) pre-administration of a blocking dose (50 μg of AJ201) (tumor denoted with dashed red line and K = Kidney). **F)** [^{68}Ga]AJ201 quantification in tumors by *ex vivo* biodistribution in mice treated with and without a blocking dose where T/B is tumor-to-blood; T/M is tumor-to-muscle and T/P is tumor-to-pancreas ratios; data in panels B represented as mean \pm SEM ($n = 3$); data in panels C and D are from mice intravenously injected with ~ 2.96 MBq (~ 80 μCi) [^{68}Ga]AJ201 and sacrificed at different time-points after injection, data represented as mean \pm SEM ($n = 3$ or 4); data in figure F is shown as box and whisker plots (median \pm IQR) showing all data points ($n = 4$). Statistics were calculated using multiple unpaired *t* test in F. ** $P \leq 0.01$; ****, $P \leq 0.0001$.

To validate the imaging data, radiotracer uptake in different tissues was measured at pre-determined time points by *ex vivo* biodistribution studies in mice with Panc1 tumors. These studies showed high radioactivity accumulation in tumors, kidneys, and bladder at all time points and radioactivity in the kidneys remained high until 120 min. Tumors exhibited high radioactivity accumulation (4.7-7.9 percent incubated dose per gram, %ID/g) between 5 and 120 min post-administration. In contrast, low radioactivity accumulation was observed in other tissues such as the heart (0.29 ± 0.08 %ID/g), lung (0.65 ± 0.04 %ID/g), liver (0.32 ± 0.02 %ID/g), intestines (0.49 ± 0.07 %ID/g), femur (0.28 ± 0.06 %ID/g), and brain (0.04 ± 0.01 %ID/g). Rapid clearance of the radiotracer from blood and muscle contributed to high tumor-to-blood (9.9 ± 1.1) and tumor-to-muscle (25.8 ± 6.7) ratios by 60 min. Minimal accumulation of radioactivity in the normal pancreas resulted in high tumor-to-pancreas ratios (28.8 ± 0.9) (**Figure 4C, 4D, Table 1**), demonstrating the potential of [^{68}Ga]AJ201 for visualizing PDAC. Next, to confirm the *in vivo* specificity of [^{68}Ga]AJ201 for EphA2, non-radioactive AJ201

(1 mg/kg) was injected subcutaneously 30 min prior to [⁶⁸Ga]AJ201 in mice with Panc1 tumors. PET/CT images and ex vivo biodistribution data showed a significant reduction in tumor radioactivity uptake, indicating that [⁶⁸Ga]AJ201 uptake in Panc1 tumors is EphA2-specific (**Figure 4E and 4F**). Collectively, these *in vivo* data indicate that [⁶⁸Ga]AJ201 exhibits suitable pharmacokinetics and image contrast for detecting PDAC.

Table 1. Kinetics and distribution of [⁶⁸Ga]AJ201 in mice bearing Panc1 tumor xenografts; data is presented as mean ± SEM (n = 4 or 5) (%ID/g for organs and dimensionless for ratios).

| Tissues | 5 min | 30 min | 60 min | 60 min with Blocking | 90 min | 120 min |
|-----------------------|---------------|---------------|---------------|----------------------|---------------|--------------|
| Blood | 8.20 ± 0.92 | 1.61 ± 0.18 | 0.49 ± 0.07 | 0.65 ± 0.11 | 1.18 ± 0.27 | 0.90 ± 0.29 |
| Muscle | 1.79 ± 0.24 | 1.11 ± 0.34 | 0.21 ± 0.05 | 0.26 ± 0.03 | 0.37 ± 0.11 | 0.26 ± 0.04 |
| Tumor | 7.06 ± 0.48 | 6.96 ± 0.31 | 4.68 ± 0.25 | 1.08 ± 0.24 | 6.04 ± 1.46 | 6.46 ± 0.39 |
| Thymus | 4.61 ± 0.51 | 2.35 ± 0.66 | NA | 2.28 ± 0.53 | 1.64 ± 0.42 | 1.21 ± 0.52 |
| Heart | 4.19 ± 1.06 | 0.97 ± 0.15 | 0.29 ± 0.08 | 0.31 ± 0.05 | 0.76 ± 0.13 | 0.68 ± 0.17 |
| Lung | 8.24 ± 0.93 | 2.29 ± 0.26 | 0.65 ± 0.04 | 0.80 ± 0.14 | 1.40 ± 0.27 | 1.15 ± 0.22 |
| Liver | 4.25 ± 0.99 | 1.15 ± 0.19 | 0.32 ± 0.02 | 0.48 ± 0.07 | 0.90 ± 0.17 | 0.84 ± 0.13 |
| Pancreas | 3.24 ± 0.08 | 0.74 ± 0.10 | 0.16 ± 0.01 | 0.30 ± 0.03 | 0.57 ± 0.15 | 0.36 ± 0.07 |
| Stomach with contents | 1.80 ± 0.39 | 0.77 ± 0.31 | 0.15 ± 0.03 | 0.19 ± 0.06 | 0.27 ± 0.06 | 0.30 ± 0.01 |
| Small intestine | 3.25 ± 0.30 | 1.16 ± 0.18 | 0.49 ± 0.07 | 0.51 ± 0.08 | 0.60 ± 0.15 | 0.45 ± 0.24 |
| Large Intestine | 3.67 ± 0.66 | 1.95 ± 0.98 | 0.15 ± 0.01 | 0.93 ± 0.40 | 1.46 ± 0.35 | 1.02 ± 0.30 |
| Spleen | 7.95 ± 1.66 | 3.87 ± 1.10 | 0.74 ± 0.17 | 0.70 ± 0.11 | 1.81 ± 0.78 | 1.55 ± 0.47 |
| Adrenals | 4.91 ± 1.83 | 2.44 ± 0.46 | NA | 2.36 ± 1.09 | 1.85 ± 0.46 | 2.69 ± 0.27 |
| Kidney | 37.50 ± 5.93 | 56.93 ± 1.26 | 45.45 ± 2.90 | 71.27 ± 14.16 | 61.75 ± 11.47 | 51.98 ± 7.46 |
| Bladder | 28.09 ± 12.12 | 53.77 ± 30.79 | 48.64 ± 15.54 | 14.41 ± 13.23 | 18.27 ± 6.35 | 19.03 ± 8.08 |
| Femur | 2.77 ± 0.13 | 1.36 ± 0.37 | 0.28 ± 0.06 | 0.38 ± 0.05 | 0.68 ± 0.11 | 0.83 ± 0.33 |
| Brain | 0.40 ± 0.08 | 0.09 ± 0.01 | 0.04 ± 0.01 | 0.04 ± 0.001 | 0.05 ± 0.01 | 0.05 ± 0.01 |
| Tumor/blood | 0.89 ± 0.14 | 3.31 ± 1.17 | 9.86 ± 1.10 | 1.66 ± 0.37 | 5.43 ± 1.32 | 8.36 ± 1.85 |
| Tumor/Muscle | 4.12 ± 0.66 | 6.40 ± 3.6 | 25.78 ± 6.71 | 4.40 ± 1.19 | 16.96 ± 2.11 | 24.94 ± 1.93 |
| Tumor/Pancreas | 2.18 ± 0.14 | 7.08 ± 2.57 | 28.78 ± 0.97 | 3.50 ± 0.70 | 10.66 ± 0.20 | 18.74 ± 2.39 |

To evaluate the potential of [⁶⁸Ga]AJ201 to detect variable EphA2 levels *in vivo*, PET/CT images were acquired in six additional pancreatic tumor xenografts (CFPAC, Panc1005, BxPC3, AsPC1, Hs766T, and Su8686) at 60 min post-administration. We observed high and variable uptake of [⁶⁸Ga]AJ201 in PDAC xenografts and minimal uptake in normal tissues across all models tested (**Figure 5A**). Ex vivo biodistribution studies in the same tumor models showed high uptake in Hs766T (8.0 ± 2.8 %ID/g) and Su8686 (7.7 ± 1.0 %ID/g) xenografts, moderate uptake in Panc1005 (5.3 ± 0.9 %ID/g) and AsPC1 (4.0 ± 0.5 %ID/g), and low uptake in CFPAC (2.4 ± 0.2 %ID/g) and BxPC3 (2.7 ± 0.4 %ID/g). These results support the imaging studies, showing minimal uptake in healthy tissues, except for kidneys, and high tumor-to-blood and tumor-to-muscle ratios in all xenograft models (**Figure 5B, Table S2**). Additionally, high tumor-to-pancreas ratios across all xenografts confirmed that [⁶⁸Ga]AJ201 detects variable EphA2 levels in PDAC *in vivo* (**Figure S5**). Furthermore, IHC analysis of the same tumors showed high immunoreactivity in Panc1, Hs766T and Su8686, moderate immunoreactivity in Panc1005 and AsPC1, and low immunoreactivity in CFPAC and BxPC3 xenografts (**Figure 5C**). This result supports the observation that [⁶⁸Ga]AJ201 uptake in imaging and biodistribution studies is indeed EphA2-specific. We generally observed that cell lines and tumors with high EphA2 expression exhibited higher [⁶⁸Ga]AJ201 uptake, underscoring the robustness of our imaging agent. However, exceptions such as the Panc1005, Hs7667 and Su8686 models, which showed greater variability, may be attributed to unique tumor microenvironmental features specific to each model. These factors, including tumor perfusion, receptor accessibility, or stromal density, may not be fully captured by IHC. Collectively, imaging and biodistribution data across seven PDAC xenografts establish the potential of [⁶⁸Ga]AJ201 to detect PDAC and variable EphA2 levels *in vivo*.

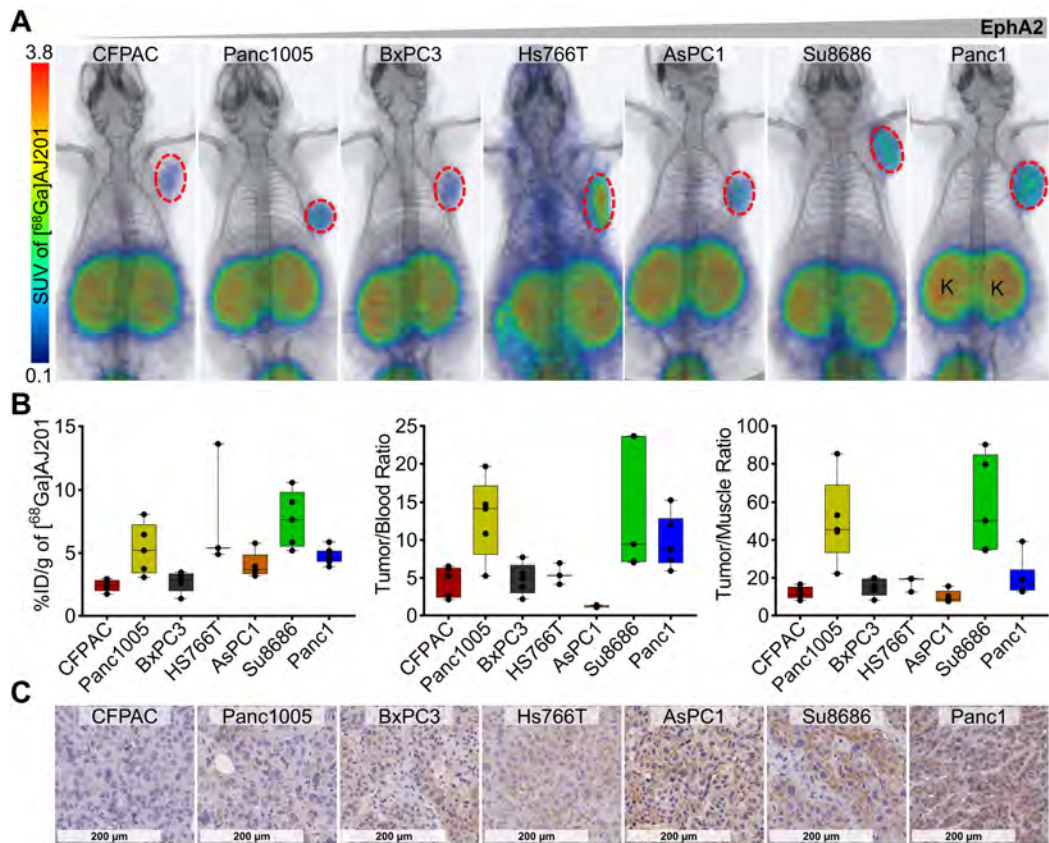


Figure 5. *In vivo* specificity of $[^{68}\text{Ga}]\text{AJ201}$ for EphA2 in NSG mice with PDAC tumor xenografts. A) Whole-body PET/CT images of different human PDAC xenografts at 60 min after the injection of radiotracer. Mice were injected with ~ 7.4 MBq (~ 200 μCi) $[^{68}\text{Ga}]\text{AJ201}$; K, kidney. Panc1 mouse image is reproduced from figure 4E. **B)** $[^{68}\text{Ga}]\text{AJ201}$ uptake quantification (%ID/g) in different PDAC tumors by *ex vivo* biodistribution at 60 min after injection. Left: %ID/g of different tumor xenografts, tumor-to-blood (middle) and tumor-to-muscle (right) ratios in each individual mice harboring respective xenografts. **C)** IHC staining for EphA2 expression in PDAC xenografts (digitally scanned at 40x); data in figure B is shown as box and whisker plots (median \pm IQR) showing all data points ($n = 4-5$).

To investigate the *in vitro* and *in vivo* specificity of $[^{68}\text{Ga}]\text{AJ201}$ for mouse EphA2, we conducted *in vitro* binding studies with the KPC, a mouse cell line, which exhibits high EphA2 expression, as confirmed by flow cytometry (Figure S6A). The *in vitro* binding study demonstrated EphA2-dependent uptake (Figure S6B). Further, $[^{68}\text{Ga}]\text{AJ201}$ -PET imaging and *ex vivo* biodistribution data confirmed the *in vivo* specificity of $[^{68}\text{Ga}]\text{AJ201}$ for EphA2-expressing tumors (Figure S6C-D, Table S3). These results collectively suggest that $[^{68}\text{Ga}]\text{AJ201}$ effectively targets EphA2-expressing cells in immunocompetent mice.

Human radiation dosimetry estimates.

Pharmacokinetic data obtained from biodistribution studies of Panc1 tumor-bearing mice were utilized to predict the time-integrated activity coefficients (TIACs, formerly known as residence times) of $[^{68}\text{Ga}]\text{AJ201}$ in humans, as previously described [28-30]. These TIAC estimates were then input into MIRDCalc to determine the absorbed dose coefficients for organs from ^{68}Ga using the ICRP adult female reference phantom (Table S4). The results indicated that the kidneys received the highest absorbed dose (0.38 rem/mCi), followed by the bladder (0.15 rem/mCi), adrenals (0.06 rem/mCi), and lungs (0.04 rem/mCi). Based on these results, a 13 mCi dose can be safely administered for PET imaging, with an estimated effective dose equivalent of less than 5 rem.

In vivo distribution of $[^{68}\text{Ga}]\text{AJ201}$ in orthotopic models of PDAC.

Leveraging the favorable pharmacokinetics and high tumor-to-pancreas ratios observed, we assessed the potential of $[^{68}\text{Ga}]\text{AJ201}$ -PET for visualizing orthotopic pancreatic tumors. In orthotopic Panc1 tumor model, PET/MR images acquired 60 min after injecting $[^{68}\text{Ga}]\text{AJ201}$ revealed a robust uptake of the tracer in the tumor, while minimal accumulation was observed in normal tissues (Figure 6A and 6B) with a high tumor-to-muscle ratios of 14.77 ± 4.46 and tumor-to-pancreas ratios of 10.35 ± 2.24 (Figure 6C). To further corroborate the imaging data, we conducted immunohistochemistry (IHC) analysis for EphA2 receptor expression on tumor sections (Figure 6D). The IHC results aligned with the imaging findings, providing

additional validation. This successful demonstration of detecting small-sized orthotopic pancreatic tumors underscores the potential utility of [⁶⁸Ga]AJ201-PET or its analogs for PDAC visualization.

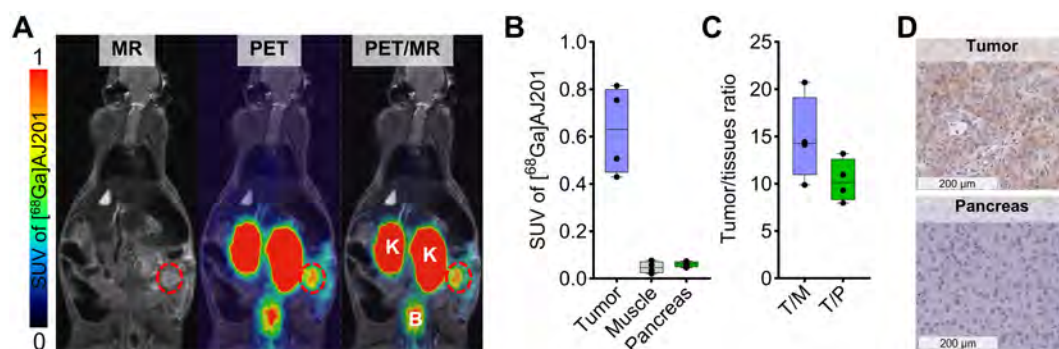


Figure 6. *In vivo* distribution of [⁶⁸Ga]AJ201 in Panc1-orthotopic tumor model. **A)** Coronal sections of the fused PET/MR images showing [⁶⁸Ga]AJ201 distribution. Primary tumor is indicated by red circle; K = Kidney, B = Bladder. **B)** Quantification of accumulated activity in tumor, muscle and pancreas of images shown in panel A (n = 4-5) **C)** tumor-to-muscle (T/M) and tumor-to-pancreas (T/P) ratios from the images shown in panel A (n = 4) **D)** EphA2 IHC of orthotopic Panc1 tumor and normal pancreas to validate the EphA2 expression. Panc1 orthotopic tumor model was generated by surgically implanting a 3-5 mm³ section of Panc1 tumor xenograft directly onto the pancreas. The implanted tumors were allowed to grow for 10 days, after which they were ready for imaging. At this stage, MRI measurements indicated that tumor sizes ranged from 10-50 mm³. data in figure **B** and **C** is shown as box and whisker plots (median ± IQR) showing all data points (n = 3-5).

EphA2 targeted radiotherapeutic [²²⁵Ac]AJ210 controls tumor growth in syngeneic KPC tumor model.

Next, we hypothesized that the consistently high expression of EphA2 observed in PDAC could be leveraged for targeted molecular radiotherapy. We chose the alpha-particle emitter [²²⁵Ac] for radiation delivery due to its ability to induce largely irreparable double-strand breaks, leading to selective cytotoxicity in cancer cells. This approach is increasingly recognized as a safe and effective treatment option [11, 31].

To test this hypothesis, we first developed a DOTA-conjugated derivative of AJ201, named AJ210, to facilitate the chelation of [²²⁵Ac]. The DOTA analog, AJ210, labeled with Ga-68 (**Scheme S3**), demonstrated *in vitro* affinity and specificity, high *in vitro* stability as well as favorable pharmacokinetics, tumor uptake, and retention properties similar to AJ201 in Panc1 and KPC tumor models (**Figure S7-S11, Table S5**). We then substituted [²²⁵Ac] for Ga-68 to study therapeutic effects in KPC tumor model (**Figure S12**). KPC models is a well-established tumor model that closely recapitulates the aggressive, treatment-resistant nature and desmoplastic stroma of human PDAC, making it invaluable for studying disease progression and testing novel therapeutic approaches.

To evaluate the effect of [²²⁵Ac]AJ210 on cell viability, KPC cells were incubated with various dosages of [²²⁵Ac]AJ210 for 72 h, followed by a viability assessment. The results showed that [²²⁵Ac]AJ210 induced dose-dependent cell killing, with an IC₅₀ of 0.32 μCi/mL (**Figure 7A**). Next, we investigated whether targeting EphA2 in tumors would control tumor growth in a preclinical model of PDAC. Mice with established subcutaneous KPC tumors, which replicate the treatment-resistant nature of human PDAC [32], received a total dose of 1 μCi of [²²⁵Ac]AJ210 and were monitored for tumor growth. H&E staining of lung, liver and kidney sections revealed no visible histological abnormalities in [²²⁵Ac]AJ210 treated animals compared to the saline treated controls, suggesting minimal acute renal toxicity (**Figure S13-S15**). However, we acknowledge that some weight loss was observed in treated animals (**Figure S16**), and while the underlying cause remains unclear, the possibility of treatment-related toxicity cannot be ruled out. Next, hematological parameters were evaluated to assess systemic toxicity. Mild changes were observed at 3 and 7 days, though these deviations were significant in some parameters at 28 days, suggesting a potential late-stage systemic effect of [²²⁵Ac]AJ210 (**Figure S17**). Tumor growth curves demonstrated significantly improved tumor response (**Figure 7B**, p < 0.001) and survival with [²²⁵Ac]AJ210 treatment compared to saline controls (**Figure 7C**, p = 0.0029). Differences in tumor growth became evident as early as 7 days and persisted throughout the study period. These proof-of-principle therapy studies highlight the potential of targeting EphA2 for molecular radiotherapy in PDAC.

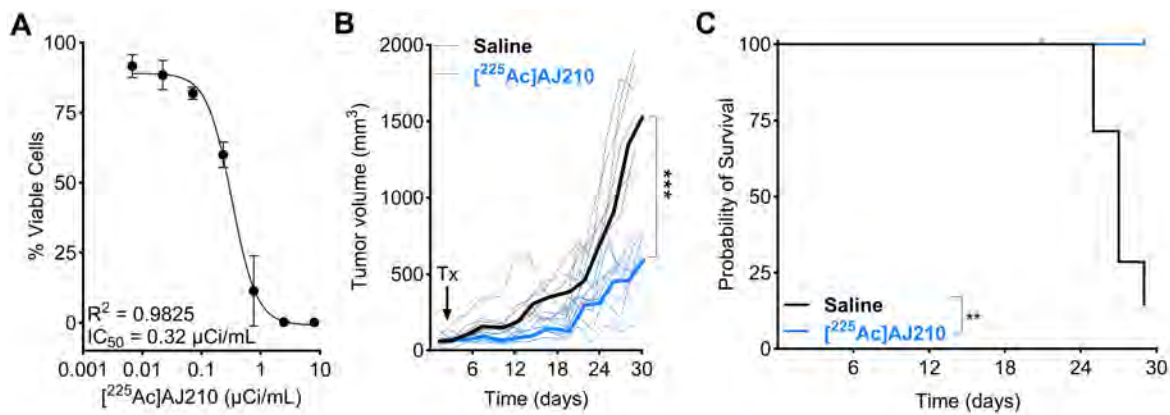


Figure 7. *In vitro* and *in vivo* therapeutic efficacy of [²²⁵Ac]AJ210 **A**) *In vitro* cell growth inhibition by [²²⁵Ac]AJ210 after 72 h incubation with KPC cells (data; mean ± SD, n = 4) at 37 °C. **B**) Effect of [²²⁵Ac]AJ210 (n = 7) on the KPC tumor growth (data; median bold line and individual replicates) after administration of total 37 kBq via tail-vein injection; each line represents one animal, arrow indicates [²²⁵Ac]AJ210 treatment (Tx) **C**) Kaplan–Meier plot of survival for the group treated with saline and [²²⁵Ac]AJ210. Median survival of saline treated group is 27 days and [²²⁵Ac]AJ210-treated group did not reach 50% and mice were sacrificed after reaching 1000 mm³ tumor volume.

Discussion

In this study, by integrating large-scale genomic analyses from CCLE and TCGA with immunohistochemical validation using PDAC tissue microarrays, we confirm that EphA2 is highly expressed in PDAC, establishing its suitability as a radiotheranostic target. To capitalize on this expression for non-invasive detection and targeted therapy, we developed EphA2-specific binders amenable to radiolabeling with both imaging and radiotherapeutic isotopes. Our results demonstrate that gallium-68–labeled radiotracers bind to EphA2 with high affinity *in vitro* across all tested PDAC cell lines and enable expression-dependent tumor detection *in vivo* within 60 min of radiotracer injection. Additionally, we extend beyond imaging by developing and evaluating the first EphA2-targeted alpha-particle therapy using [²²⁵Ac]-labeled peptides. Given the dense stromal barriers and resistance to conventional treatments seen in PDAC, alpha-particle therapy is particularly promising due to its high LET and short path length, which enable highly localized cytotoxicity while minimizing off-target damage. Our findings demonstrate potent dose-dependent cytotoxicity in PDAC cells and significant tumor growth inhibition *in vivo*, supporting EphA2-targeted alpha therapy as a novel and effective strategy. To our knowledge, this study is the first to comprehensively establish EphA2 as a radiotheranostic target in PDAC by integrating genomic validation, targeted imaging, and therapeutic efficacy.

Radiological assessment remains the gold standard for PDAC detection, and the lack of efficient diagnostic methods contribute to poor survival rates [1]. Accurate diagnosis is crucial for determining surgical candidacy and planning treatment for PDAC. Advances in computed tomography (CT) and magnetic resonance imaging (MRI) techniques, along with increased utilization of cross-sectional imaging, have led to improved diagnosis of pancreatic neoplasms [33]. However, [¹⁸F]-fluorodeoxyglucose (FDG) PET/CT, while useful for identifying local progression, metastatic spread, and evaluating treatment response, suffers from low sensitivity [34, 35]. Thus, there is significant interest in developing novel imaging agents for PDAC. In this regard, several targets including MUC5AC, MUC16, CA19.9 and alpha(v)beta(6) targeted antibodies and peptides have been pursued and showed promising results [36–39]. Previous efforts to target EphA2, have focused on developing antibody constructs as imaging agents. For instance, [⁶⁴Cu]DOTA-1C1 mAb, which binds both human and mouse orthologs, was used for noninvasive PET imaging of EphA2 levels in various tumor types, including colorectal cancer, melanoma, glioblastoma, and ovarian cancer [19]. Similarly, radiolabeled analogs of other anti-EphA2 antibodies, such as DS-8895a and 4B3, have been used to detect EphA2 expression non-invasively in tumors [20, 21]. Despite their potential, these antibody-based agents face limitations such as suboptimal pharmacokinetics and higher production costs. To overcome these challenges, low molecular weight analogs have been pursued due to their favorable pharmacokinetics. Peptides like [¹⁸F]AFP-SWL, [^{99m}Tc]-HYNIC-SWL and [⁶⁸Ga]DOTA-SD01 [24] have shown specificity for detecting EphA2 expression in melanoma, non-small cell lung and breast cancers but suffered from degradation in plasma and low tumor uptake limiting their application [22, 23]. However, none of these agents focused on PDAC.

Recent reports have highlighted high-affinity bicyclic peptides that are stable *in vivo* [17]. Derivatives of these bicyclic peptides [¹⁸F]AIF-ETN and [⁶⁸Ga]Ga-BCY18469 exhibited good image contrast and EphA2 detection in prostate and fibrosarcoma cancer models [25, 26], providing suitable constructs for further development and evaluation. [⁶⁸Ga]AJ201 demonstrates several key advantages over previously studied EphA2-targeting

radiotracers, including higher tumor uptake and improved tumor selectivity. PET imaging and biodistribution studies indicate that [⁶⁸Ga]AJ201 exhibits a tumor accumulation profile comparable to [⁶⁸Ga]BCY18469, with slight differences attributed to variations in EphA2 expression across models. However, compared to [¹⁸F]AIF-ETN, [⁶⁸Ga]Ga-ETN, and [⁶⁸Ga]Ga-BCY6164, [⁶⁸Ga]AJ201 shows significantly higher tumor uptake (SUV 1.31 ± 0.11 vs. 0.9, 0.4, and 0.2, respectively) and lower off-target accumulation in the liver and spleen, supporting its potential as a superior imaging agent. Additionally, [⁶⁸Ga]AJ201 successfully detected small orthotopic tumors (<10 mm³), underscoring its potential for early PDAC diagnosis.

Building on the imaging capabilities of these radiotracers, we further developed an alpha-particle-emitting therapeutic analog, [²²⁵Ac]AJ210. Alpha-particle therapy offers several advantages over beta-emitting radionuclides, particularly for PDAC, which is characterized by a dense stromal microenvironment that limits drug penetration. Unlike beta particles, alpha particles have a short path length (~100 μm) and high linear energy transfer (LET), enabling highly localized tumor cell destruction while sparing surrounding healthy tissues. These properties make alpha therapy particularly well-suited for targeting PDAC, which is resistant to conventional treatments. This study represents a proof-of-principle investigation demonstrating the feasibility of EphA2-targeted alpha-particle therapy. Our results demonstrate that [²²⁵Ac]AJ210 exerts potent, dose-dependent cytotoxic effects on PDAC cells and significantly inhibits tumor growth in vivo. The therapeutic effects of developed [²²⁵Ac]AJ210 are likely mediated through three key mechanisms. First, [²²⁵Ac]AJ210 selectively binds to EphA2-expressing pancreatic tumors, delivering alpha-particle radiation with high LET. Second, EphA2 receptor engagement promotes internalization and degradation, potentially impairing oncogenic signaling and reducing tumor cell invasiveness [40]. Further studies are needed to determine whether [²²⁵Ac]AJ210 modulates EphA2 receptor turnover. Third, EphA2 is known to be expressed on tumor-associated vasculature, where it plays a role in angiogenesis and vascular remodeling [41]. By targeting EphA2 on endothelial cells, [²²⁵Ac]AJ210 could disrupt tumor vasculature, impairing blood supply to the tumor. Additionally, direct alpha-particle irradiation of tumor endothelium could further compromise vascular integrity, contributing to tumor control. Together, these mechanisms highlight [²²⁵Ac]AJ210 as a dual-action therapeutic agent with both direct tumoricidal and anti-angiogenic properties.

While our results support the potential of [²²⁵Ac]AJ210 as an effective targeted alpha therapy, kidney retention remains a common concern for peptide-based radiopharmaceuticals due to renal clearance pathways. Our studies revealed elevated kidney uptake of [⁶⁸Ga]AJ201 and [⁶⁸Ga]AJ210, likely due to their hydrophilic residues, a behavior observed in other bicyclic peptides such as BCY18469 and ETN. To address this, we introduced a cleavable amino acid linker designed for enzymatic processing by brush border membrane enzymes in the kidneys [42]. However, no significant reduction in kidney uptake was observed within the tested 60-120 min timeframe, suggesting that additional modifications are needed. The cyclic nature of the peptide may hinder linker accessibility, or alternative renal clearance mechanisms may contribute to prolonged retention. Given that previous reports have only demonstrated effective enzymatic cleavage in linear peptides [43-45], future studies will focus on refining linker design and exploring alternative strategies for reducing renal accumulation.

Although preliminary research suggests that α-emitting RPT has a lower impact on kidney function compared to β-emitting RPT [12], further studies are required to assess long-term renal toxicity. Established nephroprotective strategies, such as administering D-lysine, could help mitigate non-specific renal uptake and absorbed dose [46-48]. Given that radiotracer uptake does not always directly correlate with toxicity, future studies will incorporate renal function markers and long-term toxicity analyses to better elucidate the implications of renal retention. Systemic exposure to alpha-emitters also poses risks of off-target toxicity in normal organs particularly in the liver, spleen, and bone marrow, necessitating careful dose optimization and monitoring [49, 50]. Regarding the observed weight loss, since it was not present in control animals, tumor burden alone is unlikely to be the primary cause. Instead, this may reflect a combination of systemic effects from radiation therapy, mild treatment-related toxicity, or metabolic stress induced by alpha-particle irradiation. Additional investigations, including metabolic and inflammatory markers, will help clarify these effects in future studies. While the therapeutic effects observed here are encouraging, further efforts are required to refine the pharmacokinetic profile of [²²⁵Ac]AJ210 and optimize its therapeutic window. This includes structural modifications to improve tumor-to-background ratios, dose adjustments to enhance efficacy while minimizing systemic toxicity, and combination strategies to maximize treatment responses.

Conclusions

In summary, this study establishes EphA2 as a promising radiotheranostic target in PDAC and demonstrates the effectiveness of LMW agents for both imaging and targeted alpha therapy. These agents exhibit high

affinity and specificity, leading to significant tumor accumulation and regression with mild toxicity. Our findings provide a strong foundation for EphA2-targeted radiotheranostics, warranting further optimization to enhance therapeutic efficacy and clinical translation.

Methods

CCLE and human genomic database mining for EphA2 expression

Data was collected from CCLE (cancer cell line encyclopedia on 11-05-2021: <https://depmap.org/portal/ccle/>) for EphA2 mRNA expression. These data points were sorted for each cancer types, 14 cohorts were selected and rearranged in the descending order of median EphA2 mRNA expression. Human genomic database (TCGA) was collected using UCSC Xena interface (collected on 05-19-2021 from <https://xenabrowser.net/>) for expression of EphA2 mRNA in 34 cancer types and 18 cohorts were chosen for analysis. Median of these 18 cohorts was calculated and arranged in descending order. Similarly, to compare expression of EphA2 gene in healthy and primary tumors, 15 cohorts were chosen and arranged in descending order. All data were plotted in GraphPad prism 9.0.

EphA2 Immunohistochemistry of TMA233

For immunohistochemistry, tissue slides were heated to 60 °C and washed with xylene and alcohol to remove paraffin. Antigen retrieval was carried out using citrate buffer (pH 6.0, 95-100 °C, 20 min) and the endogenous peroxidase and alkaline phosphatase activity was blocked using BioXALL. The primary anti-human EphA2 antibody was applied at a dilution of 1:250 and incubated overnight at 4 °C (Cell Signaling Cat# 6997S). After washing slides with PBS, the secondary antibody, Signalstain Boost IHC Detection Reagent (HRP), was applied and incubated for 30 min at room temperature. The slides were the washed again with PBS and the stain was developed using ImmPACT DAB substrate (Vector Lab #SK4105) according to manufacturer's instructions, counterstained with Mayer's Hematoxylin for 1 min, dehydrated using alcohol and xylene, and cover slipped. The scoring of EphA2 was determined by the intensity and distribution of staining in tumor cells. A score of 0 indicates no staining or weak staining in less than 10% of tumor cells, while a score of 1 reflects weak to moderate membranous or membranous and cytoplasmic staining in more than 10% of tumor cells. A score of 2 signifies moderate membranous or membranous and cytoplasmic staining in more than 50% of tumor cells, and a score of 3 represents strong membranous or membranous and cytoplasmic staining in more than 80% of tumor cells.

Chemicals

AJ200 and AJ201 were synthesized by CPC Scientific Inc. (Sunnyvale, CA) with >90% purity and further characterized by MALDI-TOF-MS. NOTA-NHS and DOTA-NHS esters were purchased from CheMatech and Macrocyclics, respectively.

Synthesis of AJ201

AJ201 is a bicyclic peptide, contains 24 amino acid chain and a conjugated with a 2,2',2''-(1,4,7-triazacyclononane-1,4,7-triyl)triacetic acid (NOTA) as a bifunctional chelator. The sequence of AJ201 peptide is NOTA-PEG₂-GR-[SAR₃]-GA-[hArg]-DC-[HyP]-LVNPLCLHP-[dD]-W-[hArg]-C-NH₂ with TATA-based cyclization. AJ201 was characterized by MALDI-TOF-MS (**Figure S2**). Theoretical chemical formula: C₁₄₃H₂₂₇N₄₅O₄₁S₃; Exact mass: 3326.62; Molecular weight: 3328.84; and the observed MALDI-TOF-MS mass [M + H]⁺ is 3329.0. This peptide sequence was derived from reported peptide [17, 18].

Synthesis of AJ210

To a stirred solution of AJ200 (3.2 mg, 1.2 μmol) in 400 μL of DMF in a reaction vial, DOTA-NHS ester (2.0 mg, 2.6 μmol) and DIPEA (5 μL, 25 μmol) were added and stirred at room temperature for 3 h (**Scheme S2**). DMF was evaporated using a rotary evaporator under reduced pressure and the residual product was purified on a RP-HPLC system using a semi-preparative C-18 Luna column (5 mm, 10 x 250 mm Phenomenex, Torrance, CA). The HPLC condition was gradient elution started with 5% acetonitrile: water (0.1% TFA) and reached at 95% acetonitrile: water (0.1% TFA) in 20 min at a flow rate of 5 mL/min. The product AJ210 was collected at RT ~10.3 min, lyophilized to form an off-white powder (72% yield) and characterized by MALDI-TOF-MS (**Figure S10**). Theoretical chemical formula: C₁₃₁H₂₀₃N₄₁O₃₉S₃; Exact mass: 3070.43; Molecular weight 3072.49; and the observed MALDI-TOF-MS mass [M + H]⁺ is 3072.6.

In vitro binding Affinity Study of AJ201 and AJ210 with Purified hEphA2 and mEphA2 by SPR

All experiments were conducted using a Biacore T200 instrument (GE Healthcare Life Sciences) with a CM5 chip at 25 °C. His-tagged human EphA2 (R&D systems, catalog # 3035-A2, 56.9 kDa, 4.46 μM stock concentration) and mouse EphA2 (SinoBiological, cat.# 50586-M08H, 58 kDa, 8.6 μM stock concentration) were immobilized onto the CM5 chip. AJ201 (3328.8 Da, 10 mM stock concentration) and AJ210 (3072.5 Da, 10 mM stock concentration) were used as analyte to flow over the ligand immobilized surface. Flow Cell

(FC) 1 was used as the reference for FC2, FC3 for FC4. Anti-his antibody (2 mg/ml stock concentration) was diluted (1:100 dilution, 0.02 mg/ml diluted concentration) in 10 mM sodium acetate buffer at pH 4.5 and immobilized on all FCs to a level of ~8000 to 11000 RU using the standard amine coupling chemistry. HBS-P (10 mM HEPES pH 7.4, 150 mM NaCl, 0.05% v/v surfactant P20) was used as the immobilization running buffer. Human EphA2 was diluted (1:5 dilution) in HBS-P captured onto FC2 to a level of ~750 RU. Mouse EphA2 was diluted (1:10 dilution) in HBS-P captured onto FC4 to a level of ~750 RU. HBS-P was used as the capture running buffer. Based on these captured response values, theoretical R_{max} values were calculated and are presented in **table S1**. The R_{max} values assume 1:1 interaction mechanism. Overnight kinetics were performed for all analytes in the presence of HBS-P+0.1% DMSO. The flow rate of all analyte solutions was maintained at 50 μ L/min. The contact and dissociation times used were 120s and 600s, respectively. Glycine solution (pH 1.5) was injected for 15 s for surface regeneration and fresh ligands were captured in the beginning of each injection cycle. Sensorgrams from the overnight kinetics was evaluated by using 1:1 kinetics model fitting.

Synthesis of [nat Ga]AJ201

In a reaction vial, to a stirred solution of AJ201 (0.6 mg, 0.18 μ mol) in 200 μ L of 1M sodium acetate buffer (NaOAc pH 5.0), 20 μ L of aqueous 0.1M nat GaCl₃ solution and 0.6 mL of 0.1 M HCl was added. The reaction mixture was incubated at 65 °C for 30 min and purified on a reversed phase high performance liquid chromatography (RP-HPLC) system using the same conditions as described in the synthesis of AJ210. The product [nat Ga]AJ201 was collected at RT 10.3 min, lyophilized to form an off-white powder (85% yield) and characterized by MALDI-TOF-MS (**Figure S2**). Theoretical chemical formula: C₁₄₃H₂₂₄GaN₄₅O₄₁S₃; Exact Mass: 3392.5; Molecular Weight: 3395.5; and the observed MALDI-TOF-MS mass [M + H]⁺ is 3395.7.

Synthesis of [68 Ga]AJ201

68 Ge/ 68 Ga generator was eluted manually using 6 mL 0.1M HCl (Ultrapure trace-metal-free) in four different fractions (2 mL, 1 mL, 1 mL and 2 mL). To the microcentrifuge vial (1.5 mL) containing 200 μ L of 1 M NaOAc buffer (pH 5) and 20 μ g (6 nmol) of AJ201, added 4-6 mCi of 68 GaCl₃ in 0.6 mL from second fraction. The reaction mixture was incubated for 10 min at 65 °C and purified on a RP-HPLC system using the same conditions as described in the synthesis of AJ210. The radiolabeled product [68 Ga]AJ201 was collected at RT 10.3 min, with decay corrected radiochemical yield of 66 \pm 25 % (n = 53). Desired radiolabeled fraction was concentrated, formulated in 10% EtOH in saline and used for *in vitro* and *in vivo* studies. The whole radiolabeling process was done in ~35 min and quality control, stability studies and chemical identity was performed using the RP-HPLC system.

Synthesis of [68 Ga]AJ210

To the glass vial containing 200 μ L of 1 M NaOAc buffer (pH 5) and 20 μ g (6 nmol) of AJ210, added 4-6 mCi of 68 GaCl₃. The reaction mixture was incubated for 10 min at 95 °C and purified on a RP-HPLC system using the same conditions as described in the synthesis of AJ210. The radiolabeled product [68 Ga]AJ210 was collected at RT 10.0 min. Desired fraction was concentrated, formulated in 10% EtOH in saline and used for *in vitro* and *in vivo* studies.

Synthesis of [225 Ac]AJ210

Ac-225 labeling was conducted using a reported method with modifications [51]. Briefly, 225 Ac(NO₃)₃ received as a solid and was dissolved in 20 μ L of 0.2 M HCl, further diluted with 100 μ L of 1 M sodium acetate buffer (NaOAc; pH = 5). To the microcentrifuge vial (1.5 mL) containing 50 μ L of 1 M sodium acetate buffer (NaOAc; pH = 5), 1.8 mg of ascorbic acid and 40 μ g (20 nmol) of AJ210, added 100 μ Ci of 225 Ac(OAc)₃ in 50 μ L of 1 M NaOAc (pH = 5). The reaction mixture was incubated for 40 min at 95 °C, diluted with 500 μ L of EtOH: saline (1:1) and purified on a reversed phase high performance liquid chromatography (RP-HPLC) system. The radiolabeled product [225 Ac]AJ210 was collected in saline containing 10 mg of ascorbic acid at RT 9.96 min with 40 % radiochemical yield. Desired radiolabeled fraction was concentrated, formulated in 10% EtOH in saline containing 10 mg of ascorbic acid and used for radiotherapy studies.

In vitro stability of radiotracers

The stability of the radiotracers was assessed in saline and human serum at 37 °C to mimic physiological conditions. Approximately 1.5 mCi of the radiotracer, prepared in 100–150 μ L of saline, was added to 0.5 mL of either saline or human serum in separate microcentrifuge tubes. The mixtures were gently vortexed and then incubated at 37 °C in an incubator. At predetermined time-points (1, 2, and 3 h), 100 μ L aliquots were collected from the incubation mixtures for analysis. For serum samples, proteins were removed by adding 100 μ L of saline and 50 μ L of ethanol, followed by ultrafiltration using 10 kDa centrifugal filters made of

regenerative cellulose membranes. The filtration process was performed by centrifugation at 14,000 rpm for 10 min and repeated once more to ensure complete protein removal. The filtrate was collected for analysis. The radiochemical integrity of the radiotracer in both saline and serum was evaluated using radio-high-performance liquid chromatography (radio-HPLC).

Cell culture

Cell lines were either bought from ATCC or gifted from the collaborator. All cells were cultured in the recommended media in an incubator at 37 °C in an atmosphere containing 5% CO₂ with humidity. Briefly, Panc1 and Hs766T were maintained in DMEM medium, CFPAC was maintained in IMDM media, AsPC1, BxPC3, Panc1005 and Su8686 in RPMI-1640. All cells were supplemented with 10% Fetal Bovine Serum and 1% P/S antibiotics.

RNA extraction, cDNA synthesis and Quantitative PCR

All cultured cell lines after removing the media, washed with cold PBS followed by snap-freezing in Liquid Nitrogen, stored at -80 °C till further use. Total RNA was isolated using the RNeasy Mini kit (Qiagen, Cat # 74104) following manufacturer's instructions. First-strand cDNA was synthesized from 1 µg of total RNA using the QuantiTect Reverse Transcription kit (Qiagen Cat.# 205311) following the standard protocol. The resulting cDNA was analyzed for the expression of EphA2 gene using SYBR green in Applied Biosystems PCR machine. β-Actin, a housekeeping gene was used as an internal loading control. Primer sequences (5'-3') for EphA2 Fwd-TGTGCCAGGCAGGCTACG, Rev-CTCCAAGCAGGGGCTCTCA; and β-Actin Fwd-CACGAACTACCTTCAACTCC Rev-CATACTCCTGCTTGCTGATCPCR. PCR cycle parameters involved an initial denaturation at 95 °C for 5 min, then 40 cycles of 10 s at 95 °C, 20 s at 58 °C. Fluorescence readings were taken at 75 °C after each cycle. The expression data was analyzed by normalize the Ct value with β-Actin and relative abundance was compared.

Detection of EphA2 expression by Flow cytometry

To evaluate EphA2 surface expression, human pancreatic cancer cells (1x10⁶) were stained with PE-labeled anti-human EphA2 monoclonal antibody (Clone SHM16, BioLegend Cat # 356804). Similarly mouse pancreatic cell lines were stained with FITC labeled anti-mouse EphA2 monoclonal antibody (SinoBiological Cat # 50586-R301-F). These samples were incubated in FACS buffer (0.5% FBS with 2 mM EDTA) for 30 min on ice. Samples were washed with 1X PBS and resuspended in 400 µL FACS buffer and analyzed on FACSCalibur flow cytometer. Data analysis was performed using FlowJo software for geometric mean fluorescence intensity (MFI) and histograms. Receptor density measurements were performed using Quantibrite Beads (BD Biosciences, cat #340495), which contain four levels of phycoerythrin (PE) per bead. Gates were drawn on Low, Medium Low, Medium High, and High PE binding beads, and the geometric mean (FL-2 A: PE-A) from these populations was correlated with the lot-specific PE molecule/bead on a logarithmic scale. This correlation was used to translate cell population geometric mean to receptor/cell for the respective cell type.

In vitro binding assays with Ga-68 labeled radiotracers

In vitro binding assays were performed to determine the binding of [⁶⁸Ga]AJ201 and [⁶⁸Ga]AJ210 to Jurkat and PDAC cell lines. Approximately 1 µCi of radiotracer was incubated with cells in 100 µL culture media for 60 min at 4 °C. After incubation, cells were washed three times with ice cold PBS and counted on an automated gamma counter (1282 Compugamma CS, Pharmacia/LKB Nuclear, Inc., Gaithersburg, MD). To demonstrate EphA2-specific binding of [⁶⁸Ga]AJ201, blocking was performed with 2 µM of AJ201 and for [⁶⁸Ga]AJ210, blocking was performed with 2 µM of AJ210. For kinetic study, 8x10⁶ Panc1 cells/vial were incubated with approximately 8 µCi/vial of [⁶⁸Ga]AJ201 in culture media in triplicates at 37 °C and 4 °C in separate tubes. 1x10⁶ cells were aliquoted at predetermined timepoints (5, 15, 30, 60 min). Excess radioactivity was removed by washing three times with PBS. Activity in cell pellets were measured on an automated gamma counter.

Tumor Models

Animal studies were performed under Johns Hopkins University Animal Care and Use Committee (ACUC)-approved protocol (Principal investigator: Sridhar Nimmagadda, Ph.D. and Protocol number M021M175). Male and Female NSG mice (5-6 weeks old) were purchased from JHU immunocompromised core and used to establish xenografts by administering cells subcutaneously (top right flank, unless otherwise noted) to form various tumor models within 3-4 weeks. Following cell numbers were used: Panc1, AsPC1, BxPC3 (1 M), Hs766T and SU8686 (2 M), CFPAC and Panc1005 (5 M). Imaging or biodistribution studies (n = 3-5) were conducted on mice with tumor volumes of 100-200 mm³. The Panc1 orthotopic tumor model was established

by surgically implanting a 3-5 mm³ section of Panc1 tumor xenograft directly onto the pancreas. The implanted tumors were allowed to grow and were ready for imaging after 10 days of implantation after which they were ready for imaging. At this stage, MRI measurements indicated that tumor sizes ranged from 10-50 mm³.

Evaluation of Pharmacokinetics of [⁶⁸Ga]AJ201

Dynamic PET images were acquired on a Simultaneous 7T Bruker PET-MR scanner to evaluate the pharmacokinetics of [⁶⁸Ga]AJ201. Mice bearing Panc1 tumor xenografts were anesthetized under 2.5% isoflurane and a catheter was fixed in the tail vein before being secured on the PET-MR bed. An activity of ~250 µCi (9.3 MBq; 0.5 to 0.8 nmol) of [⁶⁸Ga]AJ201 was administered intravenously and whole-body PET dynamic scans were performed. Dynamic PET scans were initiated one min before radiotracer injection and acquired at varying intervals to capture early and late-phase kinetics: every 30 s from -1 to 5 min, every min from 5 to 15 min, every 3 min from 15 to 30 min, every 5 min from 30 to 60 min, and every 10 min from 60 to 90 min. The acquired PET data were reconstructed and corrected for radioactive decay and dead time using ParaVision 360 V2 by Bruker. The percentage of injected dose per cc (%ID/cc) values were obtained by drawing ROI on the tumor, muscle, heart, liver and kidney using PMOD software, and image fusion and visualization were also performed using PMOD software.

Whole body PET-CT imaging of mouse xenografts

Mice bearing flank tumors were injected intravenously with ~250 µCi (9.3 MBq) of Ga-68 labeled radiotracer in 200 µL of 10% ethanol in saline. Mice were anesthetized under 2.5% isoflurane just before the PET imaging study and continued during the acquisition. PET images were acquired 60 min after injection of the radiotracer. Images were acquired in 2 bed positions for a total of 10 min using an ARGUS small-animal PET/CT scanner. Images were reconstructed using 2D-OSEM and corrected for radioactive decay and dead time. Image fusion, visualization, and 3D rendering were accomplished using Amira 2020.3.1 (FEI, Hillsboro, OR).

Ex vivo biodistribution

Mice with 100-200 mm³ tumor volume were used for *ex vivo* biodistribution studies. For radiotracer pharmacokinetics and dosimetry studies, mice with Panc1 tumor xenograft received ~80 µCi (2.96 MBq) [⁶⁸Ga]AJ201 and were sacrificed at pre-determined time points (5, 30, 60, 90 and 120 min). All other mice were injected with ~50 µCi (1.85 MBq; 0.2 to 0.5 nmol) Ga-68 labeled radiotracer and were sacrificed at 60 min. The selected tissues were collected, weighed, counted, and their %ID/g values calculated for biodistribution analysis. For pharmacokinetics and dosimetry studies, Selected tissues included blood, muscle, tumor, thymus, heart, lung, liver, pancreas, stomach. Small intestine, large intestine, spleen, adrenals, kidney, bladder, femur, brain and for other tumor xenografts, selected tissues were blood, muscle, tumor, heart, lung, liver, pancreas, small intestine, spleen, kidney.

PET-MR imaging of Panc1 orthotopic tumor model

Mice having orthotopic panc1 tumors were injected intravenously with [⁶⁸Ga]AJ201 and PET images were acquired at 60 min after radiotracer injection for 10 min in 1 bed positions (full body) and whole-body MRI using a Simultaneous 7T Bruker PET-MR. The PET data were acquired, reconstructed, and corrected for radioactive decay using ParaVision 360 V2 by Bruker. The %ID per cc values were obtained after drawing ROI (region of interest) in tumor and muscle using PMOD software. Image fusion, visualization, were also accomplished using PMOD software (Bruker).

Immunohistochemistry

To perform immunohistochemistry, the tissue slides were deparaffinized by baking at 60 °C and washing with xylene and alcohol. Antigen retrieval was carried out using citrate buffer (pH 6.0, 95-100 °C, 20 min) and the endogenous peroxidase and alkaline phosphatase activity was blocked using BioXALL. The primary anti-human EphA2 antibody was applied at a dilution of 1:250 and incubated overnight at 4 °C (Cell Signaling Cat# 6997S). After washing with PBS, the secondary antibody, Signalstain Boost IHC Detection Reagent (HRP), was applied and incubated for 30 min at room temperature. The slides were washed and developed using ImmPACT DAB substrate (Vector Lab #SK4105). After washing, the slides were counterstained with Mayer's Hematoxylin for 1 min, dehydrated using alcohol and xylene, and then cover slipped.

Therapeutic evaluation of [²²⁵Ac]AJ210

Male C57BL/6 mice (5-6 weeks old) were used to establish syngeneic tumor by administering KPC cells subcutaneously in top right flank. For this study, 0.5 million cells were inoculated subcutaneously into the

upper flank of each animal. Tumor growth was closely monitored, and once tumors became palpable, their volumes were measured using a vernier caliper. Animals were then randomized into groups to ensure balanced baseline tumor sizes, with median volumes of approximately 60 mm³ (PBS group median: 60 mm³; radiotherapeutic group median: 57 mm³). Following randomization, two subsequent doses of 0.5 µCi of [²²⁵Ac]AJ210 were administered intravenously with the interval of 24 h. Similarly, saline was administered in the control group. Measurements of tumor volume and body weight were conducted in alternative days until the end of study. Blood was collected retro-orbitally at 3-, 7- and 28-days post radiotherapy injection and hematological parameter were assessed using SCIL Vet ABC Plus instrument.

H&E staining

Tissue blocks and slides of liver, kidneys and lungs were prepared by JHU histology core and staining was also carried out by core. Briefly, tissue samples were fixed in formalin for 24 h and rinsed with PBS and stored in PBS. These tissue samples were dehydrated through graded ethanol series, cleared in xylene, and embedded in paraffin. Sections (4–5 µm thick) were cut using a microtome and mounted on glass slides. The slides were deparaffinized in xylene, rehydrated through graded ethanol to distilled water, and stained with hematoxylin for 5 min. After rinsing in running water, sections were differentiated in 1% acid alcohol, blued in ammonia water, and counterstained with eosin for 1–2 min. Slides were dehydrated, cleared in xylene, and mounted with a coverslip using a permanent mounting medium. Images were captured under a brightfield microscope to evaluate tissue structure and histopathological features.

Statistical analysis

All statistical analyses were performed using Prism 9.0 Software (GraphPad Software, La Jolla, CA). Unpaired Student's *t* test and one- or two-way ANOVA were utilized for column, multiple column, and grouped analyses, respectively. Statistical significance was set at ns, $P \geq 0.05$; *, $P \leq 0.05$; **, $P \leq 0.01$; ***, $P \leq 0.001$; ****, $P \leq 0.0001$. Correlation was performed using simple linear regression without keeping the term constant at zero.

Abbreviations

PDAC, Pancreatic ductal adenocarcinoma; CCLE, Cancer Cell Line Encyclopedia; TCGA, The Cancer Genome Atlas; TMA, Tissue microarrays; EphA2, Ephrin receptor A2; SSTR2, Somatostatin receptor 2, FAP, Fibroblast activation protein; PET, Positron emission tomography; CT, computed tomography; MRI, Magnetic resonance imaging; IHC, Immunohistochemistry, ⁶⁸Ga, Gallium-68; ²²⁵Ac, Actinium-225; ¹⁷⁷Lu, Lutetium-177; mRNA, messenger Ribonucleic acid, PAAD, pancreatic cancer; BLCA, Bladder cancer; READ, Rectal cancer; LUSC, Lung squamous cell carcinoma; THCA, Thyroid cancer; KIRP, Kidney papillary cell carcinoma; LUAD, Lung adenocarcinoma; KIRC, Kidney clear cell carcinoma; CHOL, Bile duct cancer; SKCM, melanoma; LIHC, Liver cancer; KICH, Kidney chromophobe; BRCA, Breast cancer; PRAD, Prostate cancer; DLBC, Large-B-cell lymphoma; LAML, Acute myeloid leukemia; DOTA, 2,2',2'',2'''-(1,4,7,10-tetraazacyclododecane-1,4,7,10-tetrayl)tetraacetic acid; NOTA, 1,4,7-Triazacyclononane-1,4,7-triacetic acid; FDA, Food and drug administration; ROI, Region of Interest; NSG, NOD scid gamma; SEM, standard error of mean; TIAC, Time-integrated activity coefficient; FDG, [¹⁸F]-fluorodeoxyglucose; GEP-NET, Gastroenteropancreatic neuroendocrine tumors; PRRT, Peptide receptor radionuclide therapy; LMW, Low molecular weight; NaOAc, sodium acetate; RP-HPLC, Reverse phase high performance liquid chromatography; mCi, millicurie; MALDI-TOF-MS, Matrix assisted laser desorption ionization time of flight mass spectrometry; EtOH, ethanol; ATCC, American type culture collection; cDNA, Complementary DNA

Supplementary Material

Acknowledgements

This study was funded by NIH R01CA236616 (S.N.), and the ⁶⁸Ge/⁶⁸Ga generator was supported by NIH R01CA269235 (S.N.). Core resources (histology and imaging) were supported by NIH P30CA006973. Synthesis and characterization were supported by OSB-1 award from the HERA Ovarian cancer foundation (AKS). We thank Ms. Xiaoju Yang and Mr. Desmond Jacob for conducting PET-CT and PET-MR studies in MRB molecular imaging service center and cancer functional imaging core. The authors also thank Drs. Aykut Üren and Purushottam Tiwari at Georgetown University for performing SPR experiments. The authors thank the JHU Mass Spectrometry and Proteomics Core for facilitating the characterization of peptides.

Authors' Contributions

A.K. Sharma: Conceptualization, methodology, data curation, formal analysis, writing—original draft, writing—review and editing. **K. Gupta:** Conceptualization, methodology, data curation, formal analysis, writing—original draft, writing—review and editing. **A. Mishra:** Methodology, data curation, writing—review and editing. **G. Lofland:** Data curation, writing—review and editing. **S.Y. Chen:** Data curation, writing—review and editing. **I. Marsh:** Data curation, writing—review and editing. **P.T. Fair:** Methodology, animal care. **R.F. Hobbs:** Formal analysis, writing—review and editing. **T.M. Armstrong:** Data curation, writing—review and editing. **E.M. Jaffee:** Formal analysis, writing—review and editing, animal models. **E. Gabrielson:** Methodology, data curation, writing—review and editing. **L. Zheng:** Formal analysis, writing—review and editing, animal models. **S. Nimmagadda:** Funding acquisition, conceptualization, methodology, data curation, formal analysis, writing—original draft, writing—review and editing.

Competing Interests

Authors report no competing interest related to the described work.

Data availability. All study data are included in the article and/or supporting information. Additional data are available upon request from the corresponding author.

References

1. Kleeff J, Korc M, Apte M, La Vecchia C, Johnson CD, Biankin AV, et al. Pancreatic cancer. *Nat Rev Dis Primers*. 2016; 2: 16022.
2. Halbrook CJ, Lyssiotis CA, Pasca di Magliano M, Maitra A. Pancreatic cancer: Advances and challenges. *Cell*. 2023; 186: 1729-54.
3. Ho WJ, Jaffee EM, Zheng L. The tumour microenvironment in pancreatic cancer - clinical challenges and opportunities. *Nat Rev Clin Oncol*. 2020; 17: 527-40.
4. Brabander T, van der Zwan WA, Teunissen JJM, Kam BLR, Feelders RA, de Herder WW, et al. Long-Term Efficacy, Survival, and Safety of [(177)Lu-DOTA(0),Tyr(3)]octreotate in Patients with Gastroenteropancreatic and Bronchial Neuroendocrine Tumors. *Clin Cancer Res*. 2017; 23: 4617-24.
5. Bodei L, Herrmann K, Schoder H, Scott AM, Lewis JS. Radiotheranostics in oncology: current challenges and emerging opportunities. *Nat Rev Clin Oncol*. 2022; 19: 534-50.
6. Kessler L, Hirnas N, Pabst KM, Hamacher R, Ferdinandus J, Schaarschmidt BM, et al. (68)Ga-Labeled Fibroblast Activation Protein Inhibitor ((68)Ga-FAPI) PET for Pancreatic Adenocarcinoma: Data from the (68)Ga-FAPI PET Observational Trial. *J Nucl Med*. 2023; 64: 1910-7.
7. Singh S, Halperin D, Myrehaug S, Herrmann K, Pavel M, Kunz PL, et al. [(177)Lu]Lu-DOTA-TATE plus long-acting octreotide versus high-dose long-acting octreotide for the treatment of newly diagnosed, advanced grade 2-3, well-differentiated, gastroenteropancreatic neuroendocrine tumours (NETTER-2): an open-label, randomised, phase 3 study. *Lancet*. 2024; 403: 2807-17.
8. Poty S, Francesconi LC, McDevitt MR, Morris MJ, Lewis JS. alpha-Emitters for Radiotherapy: From Basic Radiochemistry to Clinical Studies-Part 1. *J Nucl Med*. 2018; 59: 878-84.
9. Poty S, Francesconi LC, McDevitt MR, Morris MJ, Lewis JS. alpha-Emitters for Radiotherapy: From Basic Radiochemistry to Clinical Studies-Part 2. *J Nucl Med*. 2018; 59: 1020-7.
10. Jalloul W, Ghizdovat V, Stolniceanu CR, Ionescu T, Grierosu IC, Pavaleanu I, et al. Targeted Alpha Therapy: All We Need to Know about (225)Ac's Physical Characteristics and Production as a Potential Theranostic Radionuclide. *Pharmaceuticals (Basel)*. 2023; 16.
11. Scheinberg DA, McDevitt MR. Actinium-225 in targeted alpha-particle therapeutic applications. *Curr Radiopharm*. 2011; 4: 306-20.
12. Park EA, Graves SA, Menda Y. The Impact of Radiopharmaceutical Therapy on Renal Function. *Semin Nucl Med*. 2022; 52: 467-74.
13. Sathekge M, Bruchertseifer F, Vorster M, Lawal IO, Knoesen O, Mahapane J, et al. mCRPC Patients Receiving 225Ac-PSMA-617 Therapy in the Post-Androgen Deprivation Therapy Setting: Response to Treatment and Survival Analysis. *Journal of Nuclear Medicine*. 2022; 63: 1496-502.
14. Ulaner GA, VanderMolen LA, Li G, Ferreira D. Dotatate PET/CT and 225Ac-Dotatate Therapy for Somatostatin Receptor-expressing Metastatic Breast Cancer. *Radiology*. 2024; 312: e233408.
15. Xiao T, Xiao Y, Wang W, Tang YY, Xiao Z, Su M. Targeting EphA2 in cancer. *J Hematol Oncol*. 2020; 13: 114.
16. Shitara K, Satoh T, Iwasa S, Yamaguchi K, Muro K, Komatsu Y, et al. Safety, tolerability, pharmacokinetics, and pharmacodynamics of the afucosylated, humanized anti-EPHA2 antibody DS-8895a: a first-in-human phase I dose escalation and dose expansion study in patients with advanced solid tumors. *J Immunother Cancer*. 2019; 7: 219.
17. Bennett G, Brown A, Mudd G, Huxley P, Van Rietschoten K, Pavan S, et al. MMAE Delivery Using the Bicycle Toxin Conjugate BT5528. *Mol Cancer Ther*. 2020; 19: 1385-94.
18. Mudd GE, Brown A, Chen L, van Rietschoten K, Watcham S, Teufel DP, et al. Identification and Optimization of EphA2-Selective Bicycles for the Delivery of Cytotoxic Payloads. *J Med Chem*. 2020; 63: 4107-16.
19. Cai W, Ebrahimnejad A, Chen K, Cao Q, Li ZB, Tice DA, et al. Quantitative radioimmunoPET imaging of EphA2 in tumor-bearing mice. *Eur J Nucl Med Mol Imaging*. 2007; 34: 2024-36.
20. Gan HK, Parakh S, Lee FT, Tebbutt NC, Ameratunga M, Lee ST, et al. A phase 1 safety and bioimaging trial of antibody DS-8895a against EphA2 in patients with advanced or metastatic EphA2 positive cancers. *Invest New Drugs*. 2022; 40: 747-55.
21. Burvenich IJ, Parakh S, Gan HK, Lee FT, Guo N, Rigopoulos A, et al. Molecular Imaging and Quantitation of EphA2 Expression in Xenograft Models with 89Zr-DS-8895a. *J Nucl Med*. 2016; 57: 974-80.
22. Pretze M, Mosch B, Bergmann R, Steinbach J, Pietzsch J, Mamat C. Radiofluorination and first radiopharmacological characterization of a SWLAY peptide-based ligand targeting EphA2. *J Labelled Comp Radiopharm*. 2014; 57: 660-5.
23. Liu Y, Lan X, Wu T, Lang J, Jin X, Sun X, et al. (99m)Tc-labeled SWL specific peptide for targeting EphA2 receptor. *Nucl Med Biol*. 2014; 41: 450-6.

24. Qu B, Li X, Ma Y, Wang Y, Han Y, Hou G, et al. (68)Ga labeled EphA2-targeted cyclic peptide: a novel positron imaging tracer for triple-negative breast cancer? *Dalton Trans.* 2024; 53: 7946-52.
25. Gan Q, Cui K, Cao Q, Zhang N, Yang MF, Yang X. Development of a (18)F-Labeled Bicyclic Peptide Targeting EphA2 for Molecular Imaging of PSMA-Negative Prostate Cancer. *J Med Chem.* 2023; 66: 14623-32.
26. El Fakiri M, Regupathy AR, Uhlmann L, Ayada N, Geis NM, Domogalla LC, et al. Development and preclinical characterization of a novel radiotheranostic EphA2-targeting bicyclic peptide. *Theranostics.* 2024; 14: 4701-12.
27. Hofling AA, Fotenos AF, Niu G, Fallah J, Agrawal S, Wang SJ, et al. Prostate Cancer Theranostics: Concurrent Approvals by the Food and Drug Administration of the First Diagnostic Imaging Drug Indicated to Select Patients for a Paired Radioligand Therapeutic Drug. *J Nucl Med.* 2022; 63: 1642-3.
28. Knorr K, Oh SW, Kronke M, Wurzer A, D'Alessandria C, Herz M, et al. Preclinical biodistribution and dosimetry and human biodistribution comparing (18)F-rhPSMA-7 and single isomer (18)F-rhPSMA-7.3. *EJNMMI Res.* 2022; 12: 8.
29. Sharma AK, Gupta K, Mishra A, Lofland G, Marsh I, Kumar D, et al. CD38-Specific Gallium-68 Labeled Peptide Radiotracer Enables Pharmacodynamic Monitoring in Multiple Myeloma with PET. *Adv Sci (Weinh).* 2024; 11: e2308617.
30. Mishra A, Kumar D, Gupta K, Lofland G, Sharma AK, Banka DS, et al. Gallium-68-labeled Peptide PET Quantifies Tumor Exposure of PD-L1 Therapeutics. *Clin Cancer Res.* 2022.
31. Sgouros G, Bodei L, McDevitt MR, Nedrow JR. Radiopharmaceutical therapy in cancer: clinical advances and challenges. *Nat Rev Drug Discov.* 2020; 19: 589-608.
32. He M, Henderson M, Muth S, Murphy A, Zheng L. Preclinical mouse models for immunotherapeutic and non-immunotherapeutic drug development for pancreatic ductal adenocarcinoma. *Ann Pancreat Cancer.* 2020; 3.
33. Chu LC, Goggins MG, Fishman EK. Diagnosis and Detection of Pancreatic Cancer. *Cancer J.* 2017; 23: 333-42.
34. Li X, Lu N, Lin L, Chen Y, Yang S, Wang H, et al. (18)F-FAPI-04 Outperforms (18)F-FDG PET/CT in Clinical Assessments of Patients with Pancreatic Adenocarcinoma. *J Nucl Med.* 2024; 65: 206-12.
35. Kauhanen SP, Komar G, Seppanen MP, Dean KI, Minn HR, Kajander SA, et al. A prospective diagnostic accuracy study of 18F-fluorodeoxyglucose positron emission tomography/computed tomography, multidetector row computed tomography, and magnetic resonance imaging in primary diagnosis and staging of pancreatic cancer. *Ann Surg.* 2009; 250: 957-63.
36. Ganguly T, Bauer N, Davis RA, Foster CC, Harris RE, Hausner SH, et al. Preclinical Evaluation of (68)Ga- and (177)Lu-Labeled Integrin $\alpha(v)\beta(6)$ -Targeting Radiotheranostic Peptides. *J Nucl Med.* 2023; 64: 639-44.
37. Sharma SK, Mack KN, Piersigilli A, Pourat J, Edwards KJ, Keinanen O, et al. ImmunoPET of Ovarian and Pancreatic Cancer with AR9.6, a Novel MUC16-Targeted Therapeutic Antibody. *Clin Cancer Res.* 2022; 28: 948-59.
38. Henry KE, Shaffer TM, Mack KN, Ring J, Ogirala A, Klein-Scory S, et al. Exploiting the MUC5AC Antigen for Noninvasive Identification of Pancreatic Cancer. *J Nucl Med.* 2021; 62: 1384-90.
39. Hausner SH, Abbey CK, Bold RJ, Gagnon MK, Marik J, Marshall JF, et al. Targeted in vivo imaging of integrin $\alpha v\beta 6$ with an improved radiotracer and its relevance in a pancreatic tumor model. *Cancer Res.* 2009; 69: 5843-50.
40. Miao H, Li DQ, Mukherjee A, Guo H, Petty A, Cutter J, et al. EphA2 mediates ligand-dependent inhibition and ligand-independent promotion of cell migration and invasion via a reciprocal regulatory loop with Akt. *Cancer Cell.* 2009; 16: 9-20.
41. Dobrzanski P, Hunter K, Jones-Bolin S, Chang H, Robinson C, Pritchard S, et al. Antiangiogenic and antitumor efficacy of EphA2 receptor antagonist. *Cancer Res.* 2004; 64: 910-9.
42. Arano Y. Renal brush border strategy: A developing procedure to reduce renal radioactivity levels of radiolabeled polypeptides. *Nucl Med Biol.* 2021; 92: 149-55.
43. Trachsel B, Valpreda G, Lutz A, Schibli R, Mu L, Béhé M. Reducing kidney uptake of radiolabelled exendin-4 using variants of the renally cleavable linker MVK. *EJNMMI Radiopharm Chem.* 2023; 8: 21.
44. Vaidyanathan G, Kang CM, McDougald D, Minn I, Brummet M, Pomper MG, et al. Brush border enzyme-cleavable linkers: Evaluation for reducing renal uptake of radiolabeled prostate-specific membrane antigen inhibitors. *Nucl Med Biol.* 2018; 62-63: 18-30.
45. Zhang M, Jacobson O, Kiesewetter DO, Ma Y, Wang Z, Lang L, et al. Improving the Theranostic Potential of Exendin 4 by Reducing the Renal Radioactivity through Brush Border Membrane Enzyme-Mediated Degradation. *Bioconjug Chem.* 2019; 30: 1745-53.

46. Vegt E, Melis M, Eek A, de Visser M, Brom M, Oyen WJ, et al. Renal uptake of different radiolabelled peptides is mediated by megalin: SPECT and biodistribution studies in megalin-deficient mice. *Eur J Nucl Med Mol Imaging*. 2011; 38: 623-32.
47. Verwijnen SM, Krenning EP, Valkema R, Huijmans JG, de Jong M. Oral versus intravenous administration of lysine: equal effectiveness in reduction of renal uptake of [¹¹¹In-DTPA]octreotide. *J Nucl Med*. 2005; 46: 2057-60.
48. Silbernagl S. The renal handling of amino acids and oligopeptides. *Physiol Rev*. 1988; 68: 911-1007.
49. Nakamae H, Wilbur DS, Hamlin DK, Thakar MS, Santos EB, Fisher DR, et al. Biodistributions, myelosuppression, and toxicities in mice treated with an anti-CD45 antibody labeled with the alpha-emitting radionuclides bismuth-213 or astatine-211. *Cancer Res*. 2009; 69: 2408-15.
50. Parihar AS, Chopra S, Prasad V. Nephrotoxicity after radionuclide therapies. *Transl Oncol*. 2022; 15: 101295.
51. Banerjee SR, Lisok A, Minn I, Josefsson A, Kumar V, Brummet M, et al. Preclinical Evaluation of (²¹³Bi)- and (²²⁵Ac)-Labeled Low-Molecular-Weight Compounds for Radiopharmaceutical Therapy of Prostate Cancer. *J Nucl Med*. 2021; 62: 980-8.

Supplementary Information
For
EphA2-targeted alpha particle theranostics for enhancing PDAC treatment

*Ajay Kumar Sharma^{1±}, Kuldeep Gupta^{1±}, Akhilesh Mishra¹, Gabriela Lofland¹, Sophia Y. Chen², Ian Marsh¹, Peyton T Fair², Robert F. Hobbs¹, Todd M. Armstrong², Elizabeth M. Jaffee², Edward Gabrielson³, Lei Zheng², and Sridhar Nimmagadda^{1, 2, 4, 5, *}*

Author affiliations:

¹The Russell H. Morgan Department of Radiology and Radiological Science

²Department of Oncology, The Sidney Kimmel Comprehensive Cancer Center and the Bloomberg–Kimmel Institute for Cancer Immunotherapy

³Department of Pathology and Oncology

⁴Department of Pharmacology and Molecular Sciences

⁵Division of Clinical Pharmacology, Department of Medicine

Johns Hopkins University School of Medicine,

Baltimore, MD, 21287, USA.

[±]authors contributed equally

*Correspondence to: Sridhar Nimmagadda, Ph.D.
Johns Hopkins Medical Institutions
1550 Orleans Street, CRB II, #492
Baltimore, MD 21287
Phone: 410-502-6244
Fax: 410-614-3147
Email: snimmag1@jhmi.edu

Keywords: Pancreatic cancer, PET, Imaging, Radiotherapy, Peptide radiopharmaceuticals, Gallium-68, Alpha-particle therapy

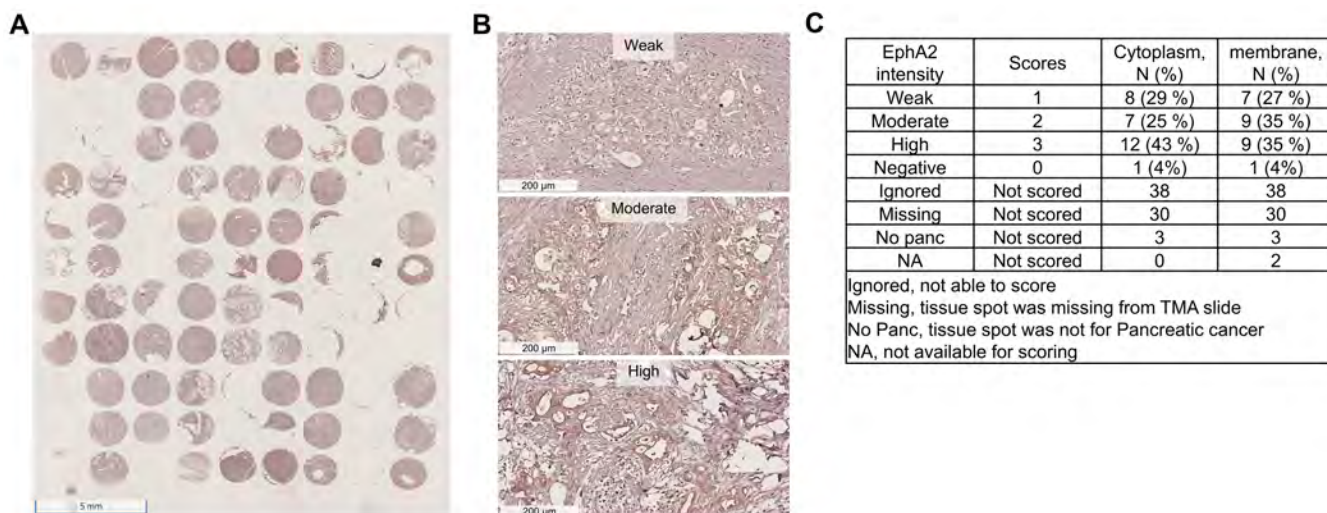
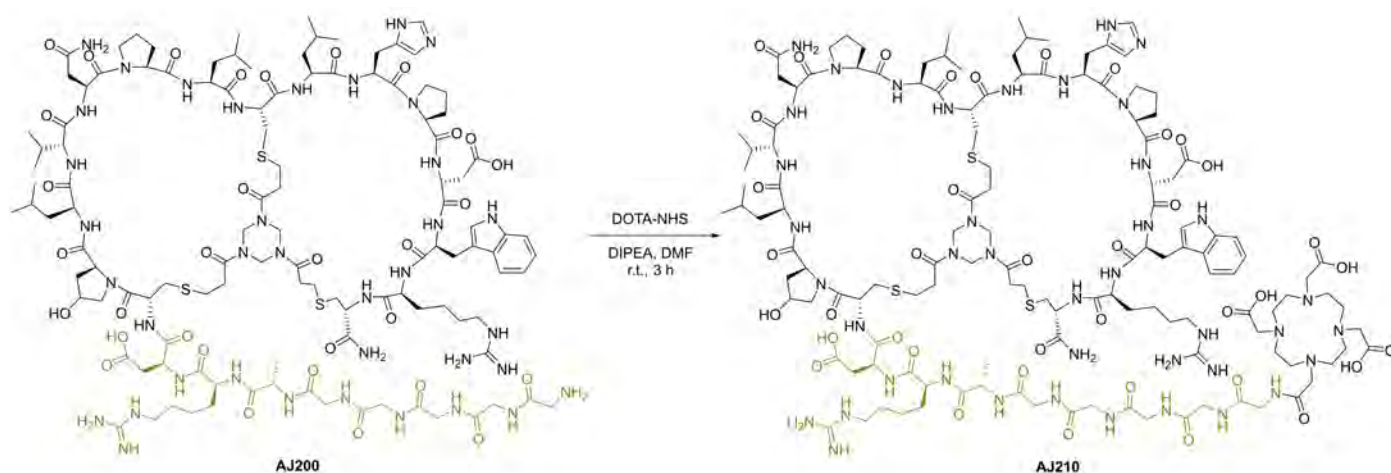


Figure S1. Immunohistochemistry analysis of EphA2 expression in a Tissue Microarray (TMA) of PDACs. **A)** A full TMA slide showcasing IHC staining for EphA2 across multiple PDAC samples demonstrating the variability in EphA2 expression among the tumor samples. **B)** Representative images from the TMA slide displaying tumor sections with varying levels of EphA2 expression highlighting the differences in staining intensity, ranging from low to high expression of EphA2. **C)** Quantitative analysis of the PDAC samples based on IHC staining intensity for membranous EphA2 expression. A scoring system was employed to categorize the samples, revealing that 95% of the PDAC samples exhibited positive staining for membranous EphA2. The scoring of EphA2 was determined by the intensity and distribution of staining in tumor cells. A score of 0 indicates no staining or weak staining in less than 10% of tumor cells, while a score of 1 reflects weak to moderate membranous or membranous and cytoplasmic staining in more than 10% of tumor cells. A score of 2 signifies moderate membranous or membranous and cytoplasmic staining in more than 50% of tumor cells, and a score of 3 represents strong membranous or membranous and cytoplasmic staining in more than 80% of tumor cells.



Scheme S1. Synthesis of AJ210 using a DOTA Chelator. The DOTA chelator was conjugated to AJ200 through a reaction mediated by N,N-Diisopropylethylamine (DIPEA), resulting in the formation of AJ210. The synthesized AJ210, featuring the DOTA chelator, was designed to facilitate the radiolabeling with Ga-68 and Ac-225, for imaging and therapeutic applications, respectively. In the structures, black color represents binding moiety and parakeet color represents the linker.

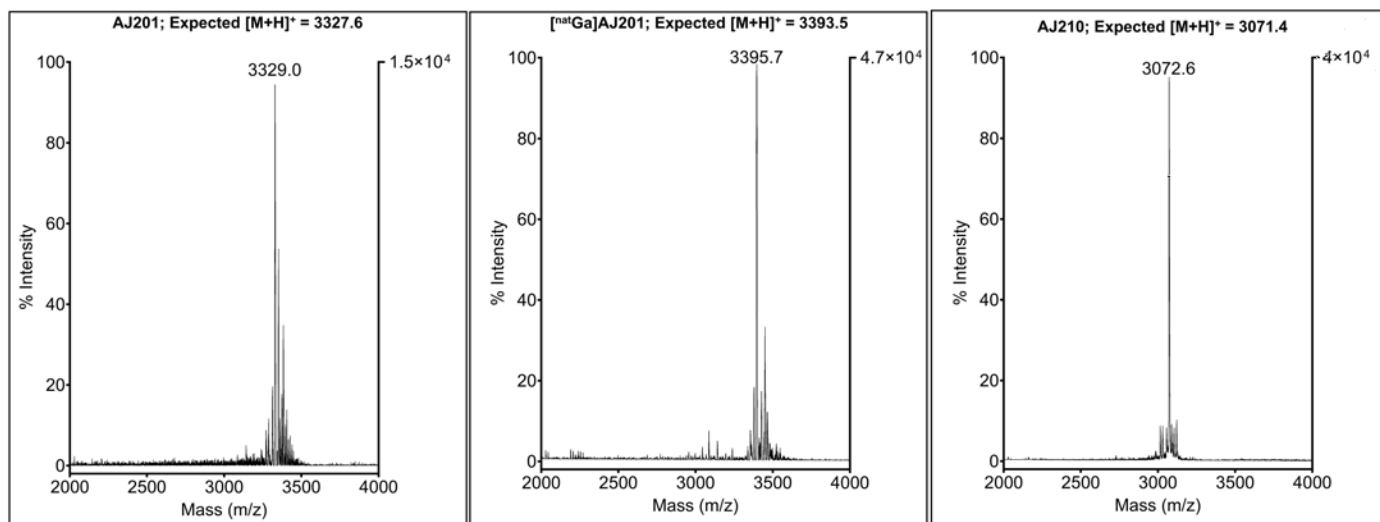
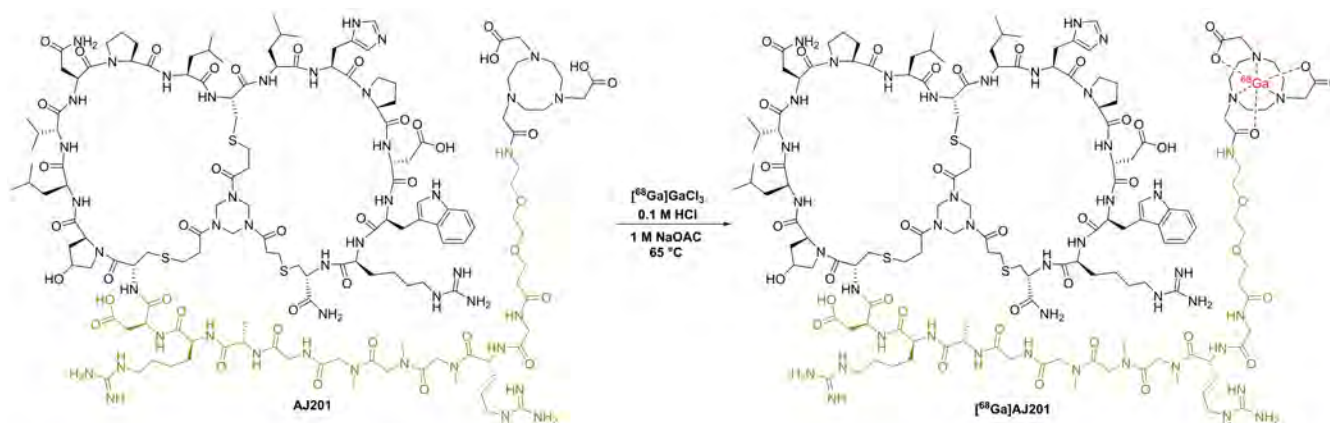


Figure S2. Characterization of AJ201, [^{nat}Ga]AJ201 and AJ201 peptides using MALDI-TOF Mass spectrometry.

Table S1. Parameters for SPR study

| Ligand (L) | FC | Analyte (A) | Ligand Binding | MW _L (Da) | MW _A (Da) | Stoichiometric Ratio | R _{max} |
|-------------|----|-------------|----------------|----------------------|----------------------|----------------------|------------------|
| Human EphA2 | 2 | AJ201 | 750 | 56900 | 3328.8 | 1:1 | 43.9 |
| Mouse EphA2 | 4 | AJ201 | 750 | 58000 | 3328.8 | 1:1 | 43.9 |
| Human EphA2 | 2 | AJ201 | 850 | 56900 | 3072.5 | 1:1 | 40.1 |



Scheme S2. Synthesis scheme of [⁶⁸Ga]AJ201. The labeling of AJ201 with ⁶⁸Ga was conducted with heating at 65 °C for 10 min. This ensured efficient incorporation of the radioactive isotope. For comparison, the labeling process using natural Gallium (^{nat}Ga) was performed under similar conditions but extended to 30 min at 65 °C. This step verifies the robustness of the labeling procedure and provides a reference for the efficiency of radiolabeling with ⁶⁸Ga. In the structures, black color represents binding moiety, parakeet color represents the linker and red color represents the radiometal.

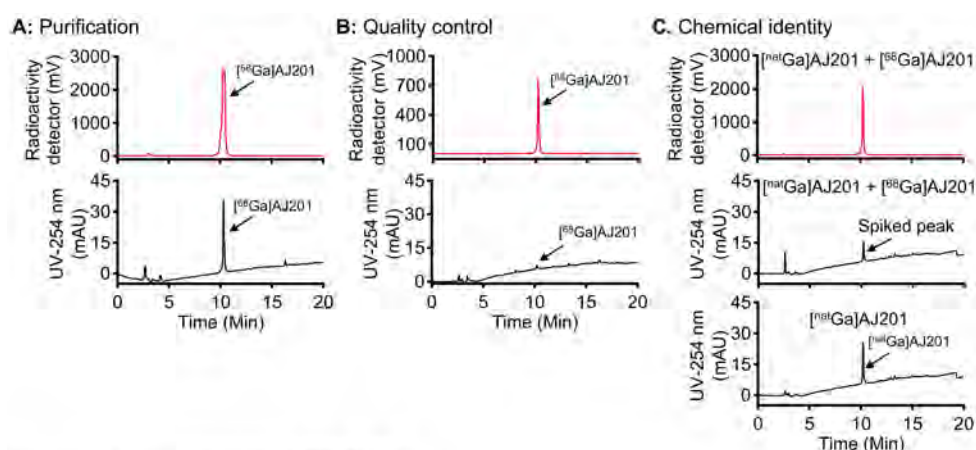


Figure S3. Radiolabeling and characterization of [⁶⁸Ga]AJ201. **A)** HPLC chromatograms for the purification process of [⁶⁸Ga]AJ201, showing the separation of the radiolabeled product from small impurities and unreacted ⁶⁸Ga. **B)** HPLC chromatogram of the purified [⁶⁸Ga]AJ201 after formulation, confirming the >99% radiochemical purity of the radiolabeled product. **C)** HPLC chromatograms confirming the chemical identity of [⁶⁸Ga]AJ201 by comparing it with [^{nat}Ga]AJ201. The matching retention times and peak profiles between [⁶⁸Ga]AJ201 and [^{nat}Ga]AJ201 confirm the successful and specific incorporation of ⁶⁸Ga into the AJ201 peptide, validating the radiolabeling process.

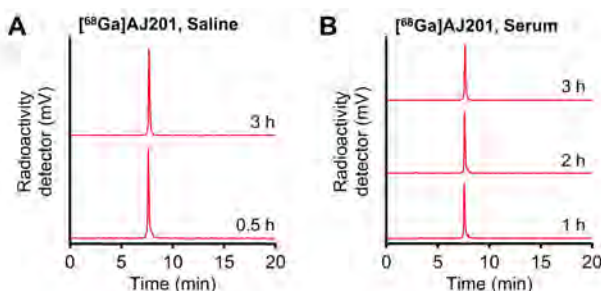


Figure S4. Stability study of [⁶⁸Ga]AJ201. **A)** HPLC chromatograms demonstrating the stability of [⁶⁸Ga]AJ201 in saline at 0.5 and 3 h at 37 °C, shows single peak and consistent retention time, indicating that [⁶⁸Ga]AJ201 remains stable without noticeable degradation or impurity formation. **B)** HPLC chromatograms of [⁶⁸Ga]AJ201 after the incubation in human serum at 1, 2 and 3 h at 37 °C, shows single peak and consistent retention time, indicating that [⁶⁸Ga]AJ201 remains stable without noticeable degradation or impurity formation.

Table S2. Biodistribution of [⁶⁸Ga]AJ201 in mice bearing pancreatic tumor xenografts at 60 min post-injection; data is presented as mean ± SEM (n = 4 or 5) of %ID/g.

| Tissues | CFPAC | Panc1005 | BxPC3 | Hs766T | AsPC1 | Su8686 |
|-----------------|--------------|---------------|--------------|--------------|--------------|---------------|
| Blood | 0.69 ± 0.21 | 0.44 ± 0.05 | 0.58 ± 0.04 | 1.39 ± 0.30 | 3.32 ± 0.24 | 0.71 ± 0.18 |
| Muscle | 0.21 ± 0.04 | 0.11 ± 0.01 | 0.18 ± 0.01 | 0.46 ± 0.13 | 0.41 ± 0.03 | 0.16 ± 0.04 |
| Tumor | 2.4 ± 0.21 | 5.31 ± 0.90 | 2.72 ± 0.37 | 7.97 ± 2.83 | 4.01 ± 0.46 | 7.66 ± 1.00 |
| Heart | 0.34 ± 0.08 | 0.20 ± 0.02 | 0.29 ± 0.01 | 0.90 ± 0.25 | 1.25 ± 0.10 | 0.25 ± 0.06 |
| Lung | 0.89 ± 0.20 | 0.54 ± 0.05 | 0.70 ± 0.04 | 1.71 ± 0.55 | 2.78 ± 0.13 | 0.76 ± 0.16 |
| Liver | 0.43 ± 0.09 | 0.29 ± 0.03 | 0.42 ± 0.02 | 0.89 ± 0.21 | 1.59 ± 0.07 | 0.34 ± 0.06 |
| Pancreas | 0.32 ± 0.07 | 0.21 ± 0.03 | 0.25 ± 0.02 | 0.61 ± 0.22 | 0.65 ± 0.04 | 0.22 ± 0.05 |
| Small intestine | 0.51 ± 0.10 | 0.25 ± 0.03 | 0.32 ± 0.02 | 0.62 ± 0.02 | 1.12 ± 0.08 | 0.29 ± 0.05 |
| Spleen | 0.87 ± 0.15 | 0.52 ± 0.05 | 0.64 ± 0.05 | 2.75 ± 0.65 | 1.61 ± 0.11 | 0.60 ± 0.16 |
| Kidney | 69.08 ± 4.56 | 67.05 ± 6.90 | 59.03 ± 7.17 | 52.63 ± 4.07 | 59.57 ± 2.86 | 37.69 ± 2.64 |
| Tumor/blood | 4.53 ± 0.90 | 12.93 ± 2.38 | 4.86 ± 0.92 | 5.47 ± 0.81 | 1.20 ± 0.06 | 14.2 ± 3.89 |
| Tumor/Muscle | 12.1 ± 1.45 | 50.09 ± 10.21 | 15.24 ± 2.14 | 17.17 ± 2.33 | 9.95 ± 1.49 | 57.99 ± 11.48 |
| Tumor/Pancreas | 8.68 ± 1.24 | 26.90 ± 5.62 | 11.01 ± 1.71 | 13.76 ± 2.30 | 6.23 ± 0.65 | 39.77 ± 7.21 |

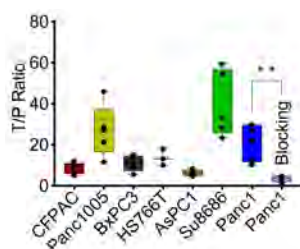


Figure S5. Ex vivo biodistribution study at 60 min post-injection, highlighting the tumor-to-pancreas ratio of [⁶⁸Ga]AJ201 in various pancreatic tumor xenograft models at 60 min post-injection. This provides insight into the specificity and uptake of [⁶⁸Ga]AJ201 in tumor tissues compared to normal pancreatic tissue across different models. data is shown as box and whisker plots (median ± IQR) showing all data points (n = 4-5). **, P<0.01 by unpaired student's t-test.

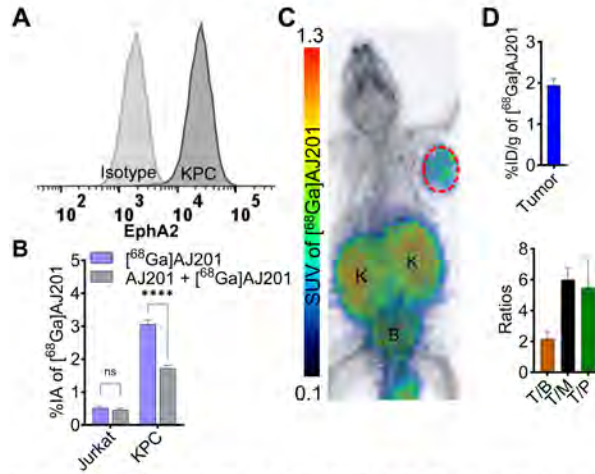


Figure S6. *In vitro* and *in vivo* evaluation of [⁶⁸Ga]AJ201 in KPC syngeneic tumor model. A) Validation of EphA2 expression in KPC cells by flow cytometry. **B)** *In vitro* tracer uptake assay of [⁶⁸Ga]AJ201 in KPC cells, with and without peptide blocking, demonstrating the specific binding of [⁶⁸Ga]AJ201 to EphA2, as indicated by reduced tracer uptake in the presence of an excess of unlabeled peptide. **C)** Whole-body static PET imaging of a KPC syngeneic tumor-bearing mouse at 60 min post-injection of the radiotracer [⁶⁸Ga]AJ201, showing the accumulation of the radiotracer in the tumor area. **D)** Ex vivo biodistribution study of [⁶⁸Ga]AJ201 at 60 min post-injection in the KPC syngeneic tumor model, providing a quantitative analysis of radiotracer accumulation in tumor (top), demonstrating the preferential uptake of [⁶⁸Ga]AJ201 in the tumor compared to other organs (bottom). T/B is tumor-to-blood; T/M is tumor-to-muscle and T/P is tumor-to-pancreas ratios.

Table S3. Biodistribution of [⁶⁸Ga]AJ201 in KPC syngeneic tumor at 60 min post-injection; data is presented as mean ± SEM (n = 5) of %ID/g.

| Tissues | KPC |
|------------------------|---------------|
| Blood | 0.75 ± 0.15 |
| Muscle | 0.28 ± 0.08 |
| Tumor | 1.51 ± 0.28 |
| Heart | 0.30 ± 0.06 |
| Lung | 0.78 ± 0.13 |
| Liver | 2.46 ± 0.77 |
| Pancreas | 0.22 ± 0.04 |
| Stomach | 0.95 ± 0.26 |
| Small intestine | 0.62 ± 0.25 |
| Large Intestine | 0.61 ± 0.28 |
| Spleen | 0.71 ± 0.30 |
| Kidney | 50.29 ± 9.75 |
| Bladder | 74.89 ± 15.33 |
| Femur | 0.71 ± 0.22 |
| Brain | 0.04 ± 0.01 |
| Tumor/blood | 2.17 ± 0.46 |
| Tumor/Muscle | 6.00 ± 0.77 |
| Tumor/Pancreas | 6.67 ± 2.18 |

Table S4. Predicted time-integrated activity coefficients (TIACs) and absorbed dose coefficients of [⁶⁸Ga]AJ201 in human organs

| Tissues | Residence time (h) | Organ dose (rem/mCi) |
|------------------------------|---------------------------|-----------------------------|
| Blood | 0.05152 | n/a |
| Muscle | 0.07064 | 0.00962 |
| Tumor | n/a | n/a |
| Thymus | 0.0002384 | 0.020165 |
| Heart | 0.001764 | 0.032745 |
| Lung | 0.01099 | 0.04292 |
| Liver | 0.01723 | 0.023976 |
| Pancreas | 0.0006321 | 0.027084 |
| Stomach with contents | 0.0004823 | 0.015799 |
| Small intestine | 0.003647 | 0.016391 |
| Large Intestine | 0.001341 | 0.018389 |
| Spleen | 0.002451 | 0.036445 |
| Adrenals | 0.0002761 | 0.06253 |
| Kidney | 0.08395 | 0.3885 |
| Bladder | 0.006394 | 0.15133 |
| Femur | 0.005607 | 0.014208 |
| Brain | 0.0008446 | 0.0032153 |

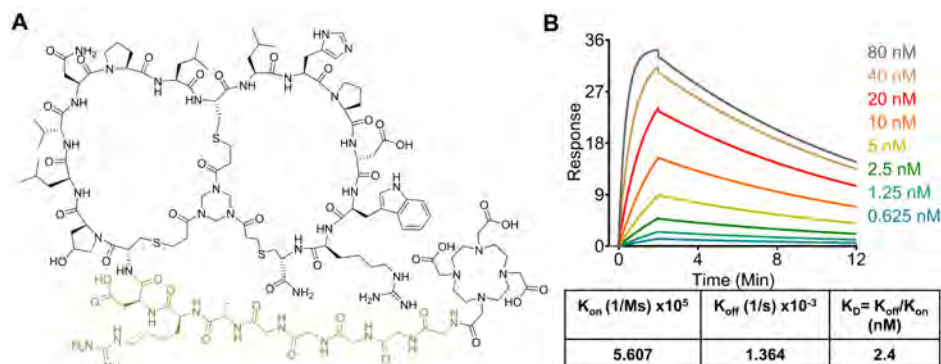
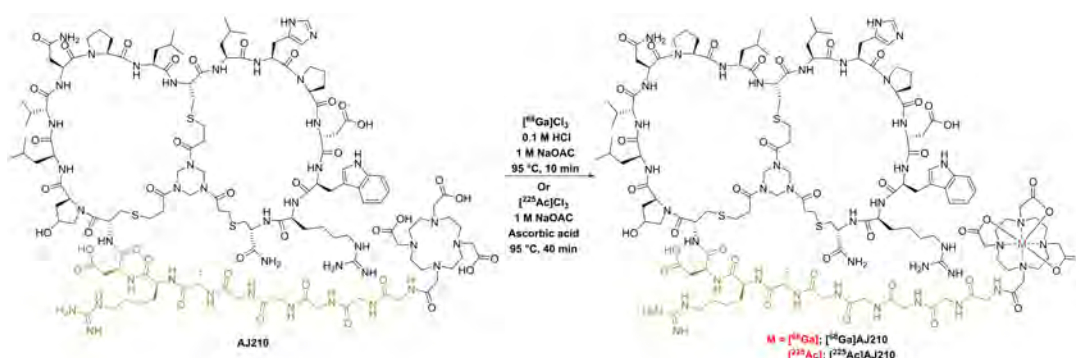


Figure S7. Structure and *in vitro* characterization of AJ210. **A)** Structure of the bicyclic peptide AJ210, which contains the DOTA as a bifunctional chelator as a for radiolabeling with ^{68}Ga and ^{225}Ac . In the structure, black color represents binding moiety and parakeet color represents the linker. **B)** Surface Plasmon Resonance (SPR) analysis demonstrating the binding affinity of AJ210 for EphA2 using recombinant human EphA2 protein. The SPR sensorgrams show the interaction kinetics between AJ210 and EphA2, providing data on the association and dissociation rates, which reflect the affinity of AJ210 for the EphA2 receptor.



Scheme S3. Synthesis scheme of radiometalation reaction to form ^{68}Ga AJ210 and ^{225}Ac AJ210. The synthesis of ^{68}Ga AJ210 involves radiolabeling AJ210 with ^{68}Ga . The labeling reaction is performed by heating at 95 °C for 10 min, resulting in the formation of ^{68}Ga AJ210. The synthesis of ^{225}Ac AJ210 involves radiolabeling AJ210 with ^{225}Ac . This reaction is conducted by heating at 95 °C for 40 min, yielding ^{225}Ac AJ210. The radiolabeled compounds ^{68}Ga AJ210 and ^{225}Ac AJ210 are prepared for different applications. ^{68}Ga AJ210 is utilized for PET imaging and ^{225}Ac AJ210 is employed as a radiotherapeutic agent. In the structures, black color represents binding moiety, parakeet color represents the linker and red color represents the radiometal.

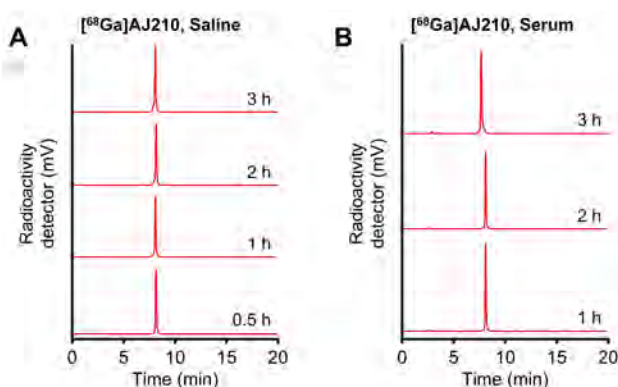


Figure S8. Stability analysis of ^{68}Ga AJ210. **A)** HPLC chromatograms of ^{68}Ga AJ210 in saline at 37 °C over 0.5, 1, 2 and 3 h exhibit a single peak with consistent retention time, confirming its stability without detectable degradation or impurity formation. **B)** HPLC chromatograms of ^{68}Ga AJ210 following incubation in human serum at 37 °C for 1, 2 and 3 h, shows a single peak with unchanged retention time, indicating that ^{68}Ga AJ210 remains stable without significant degradation or impurity formation.

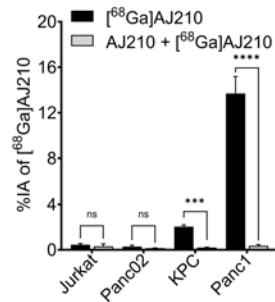


Figure S9. Binding of [⁶⁸Ga]AJ210 to various human and mouse cell lines expressed as the percent of incubated activity (%IA). Cells were incubated with 1 μCi of [⁶⁸Ga]AJ210 at 4 °C for 1 h. The data demonstrate the binding efficiency of [⁶⁸Ga]AJ210 across different cell types. Co-incubation with 2 μM of non-radioactive AJ210 (blocking dose) significantly reduces the radiotracer uptake in EphA2-expressing cells, confirming the specificity of [⁶⁸Ga]AJ210 for EphA2. Statistics were calculated using two-way ANOVA,; ns, $P \geq 0.05$; ***, $P \leq 0.001$; ****, $P \leq 0.0001$.

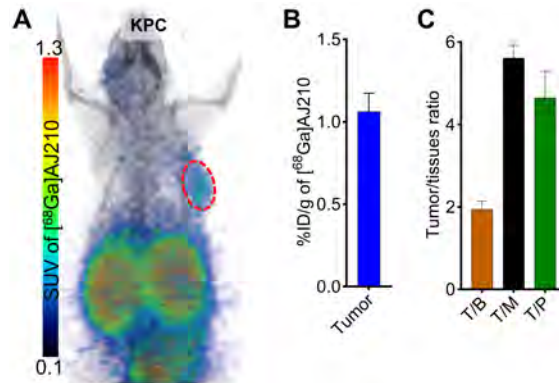


Figure S10. *In vivo* evaluation of [⁶⁸Ga]AJ210 in KPC syngeneic tumor model. A) Whole-body static PET image obtained 60 min after injection of [⁶⁸Ga]AJ210 into a KPC syngeneic tumor-bearing mouse. The PET image shows the distribution of the radiotracer throughout the body and providing a visual representation of the tracer's localization in the tumor and other tissues. **B)** Tumor uptake from an ex vivo biodistribution study performed 60 min post-injection of [⁶⁸Ga]AJ210. **C)** tumor-to-tissues ratios from an ex vivo biodistribution study performed 60 min post-injection of [⁶⁸Ga]AJ210. T/B is tumor-to-blood; T/M is tumor-to-muscle and T/P is tumor-to-pancreas ratios.

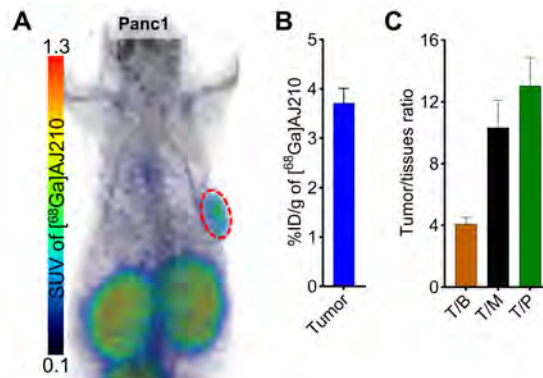


Figure S11. *In vivo* evaluation of [⁶⁸Ga]AJ210 in Panc1 tumor model. A) Whole-body static PET image obtained 60 min after injection of [⁶⁸Ga]AJ210 into a Panc1 bearing tumor xenograft model. The PET image shows the distribution of the radiotracer throughout the body and providing a visual representation of the tracer's localization in the tumor and other tissues. **B)** Tumor uptake from an ex vivo biodistribution study performed 60 min post-injection of [⁶⁸Ga]AJ210. **C)** tumor-to-tissues ratios from an ex vivo biodistribution study performed 60 min post-injection of [⁶⁸Ga]AJ210. T/B is tumor-to-blood; T/M is tumor-to-muscle and T/P is tumor-to-pancreas ratios.

Table S5. Biodistribution of [⁶⁸Ga]AJ210 in mice bearing pancreatic tumor xenografts at 60 min post-injection; data is presented as mean ± SD (n = 5) of %ID/g.

| Tissues | KPC | Panc1 |
|---------|-------------|-------------|
| Blood | 0.56 ± 0.14 | 0.96 ± 0.33 |
| Muscle | 0.19 ± 0.04 | 0.40 ± 0.16 |
| Femur | 0.29 ± 0.07 | 0.38 ± 0.08 |
| Tumor | 1.06 ± 0.25 | 3.72 ± 0.66 |

| | | |
|-----------------|--------------|--------------|
| Lung | 0.57 ± 0.13 | 0.39 ± 0.08 |
| Heart | 0.24 ± 0.05 | 0.84 ± 0.14 |
| Liver | 0.26 ± 0.05 | 0.34 ± 0.06 |
| Small intestine | 0.64 ± 0.47 | 0.62 ± 0.22 |
| Stomach | 0.17 ± 0.07 | 0.09 ± 0.03 |
| Spleen | 0.35 ± 0.07 | 0.74 ± 0.22 |
| Pancreas | 0.24 ± 0.06 | 0.30 ± 0.08 |
| Kidney | 59.9 ± 16.35 | 24.40 ± 9.98 |
| Tumor/blood | 1.94 ± 0.44 | 4.09 ± 0.97 |
| Tumor/Muscle | 5.61 ± 0.69 | 10.33 ± 4.01 |
| Tumor/Pancreas | 4.65 ± 1.46 | 13.05 ± 4.11 |

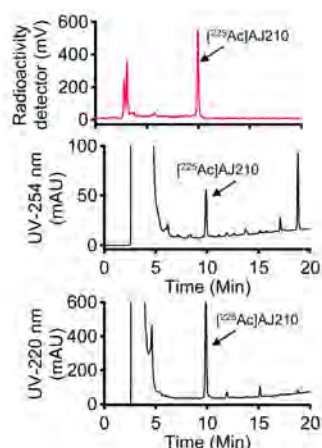


Figure S12. Radiosynthesis of $[^{225}\text{Ac}]\text{AJ210}$. HPLC chromatograms for the purification process of $[^{225}\text{Ac}]\text{AJ210}$, showing the separation of the radiolabeled product from small impurities and unreacted ^{225}Ac .

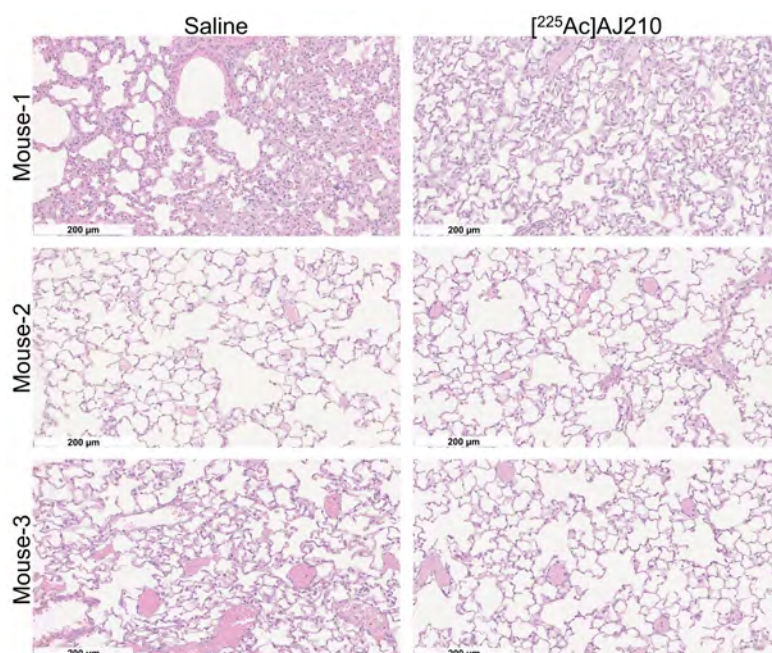


Figure S13. H&E-stained histological sections of lungs from mice treated with saline as a control and $[^{225}\text{Ac}]\text{AJ210}$. The slides show normal lung tissue morphology with no significant pathological changes in saline and $[^{225}\text{Ac}]\text{AJ210}$ treated animals (n = 3).

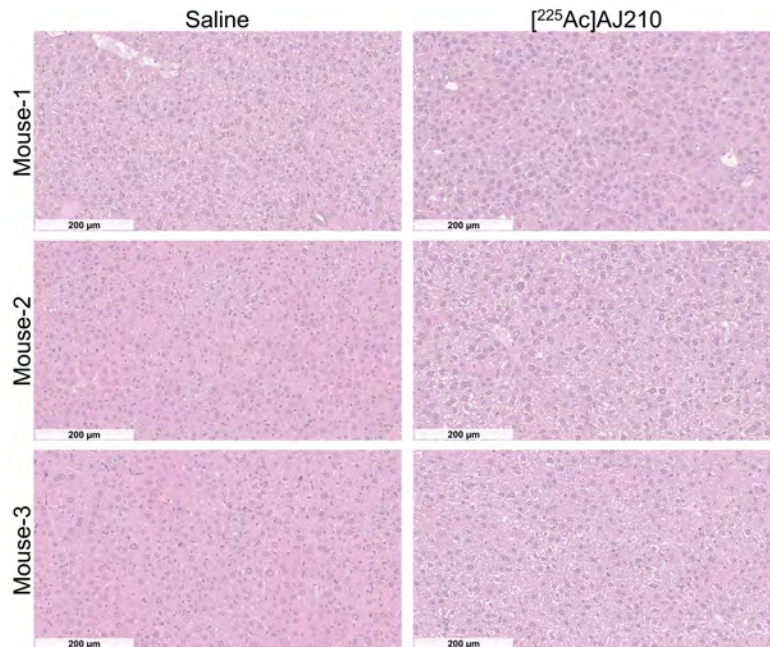


Figure S14. H&E-stained histological sections of liver from mice treated with saline as a control and $[^{225}\text{Ac}]\text{AJ210}$. The slides show normal liver tissue morphology with no significant pathological changes in saline and $[^{225}\text{Ac}]\text{AJ210}$ treated animals (n = 3).

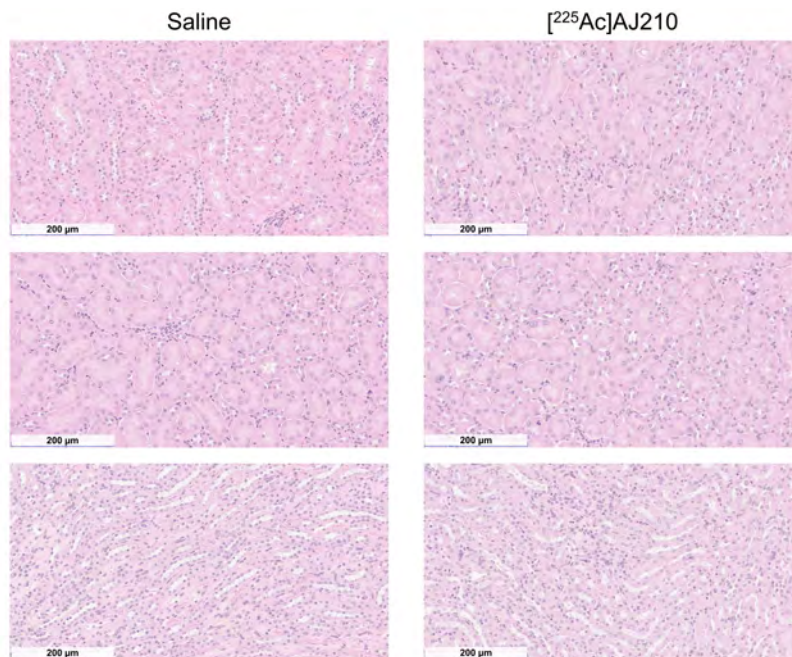


Figure S15. H&E-stained histological sections of kidney from mice treated with saline as a control and $[^{225}\text{Ac}]\text{AJ210}$. The slides show normal kidney tissue morphology with no significant pathological changes in saline and $[^{225}\text{Ac}]\text{AJ210}$ treated animals (n = 3).

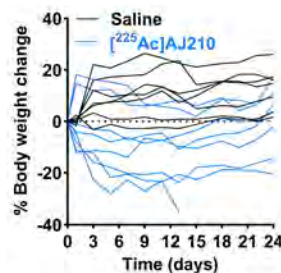


Figure S16. Percentage body weight change during the radiotherapeutic evaluation of $[^{225}\text{Ac}]\text{AJ210}$ in KPC bearing mice; The figure displays the percentage change in body weight for individual KPC-bearing mice during the radiotherapeutic evaluation of $[^{225}\text{Ac}]\text{AJ210}$. Each line represents data from a single animal over the course of the study. One mouse experienced more than 20% weight loss and was sacrificed on day 13 due to health concerns.

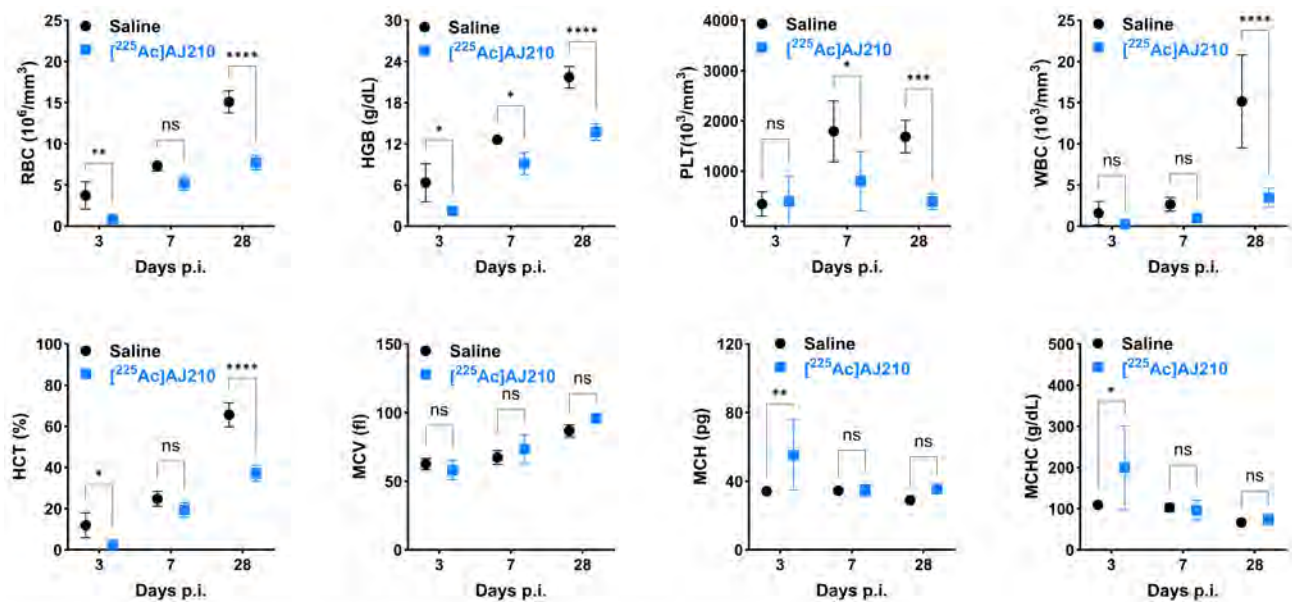


Figure S17. Hematological parameters of mice treated with saline (control) and [²²⁵Ac]AJ210. Parameters analyzed include red blood cell count (RBC), hemoglobin concentration (HGB), platelet count (PLT), white blood cell count (WBC), hematocrit (HCT), mean corpuscular volume (MCV), mean corpuscular hemoglobin (MCH), and mean corpuscular hemoglobin concentration (MCHC). Data indicate changes in the parameter, suggesting marginal hematological impact of [²²⁵Ac]AJ210 treatment. Data represented as mean ± SD (n = 3 or 4); Statistics were calculated using two-way ANOVA,; ns, $P \geq 0.05$; *, $P \leq 0.05$; **, $P \leq 0.01$; ***, $P \leq 0.001$; ****, $P \leq 0.0001$.