

Review

Nanotheranostics - Application and Further Development of Nanomedicine Strategies for Advanced Theranostics

Madaswamy S. Muthu^{1,2}, David Tai Leong¹, Lin Mei³✉ and Si-Shen Feng¹✉

1. Department of Chemical & Biomolecular Engineering, National University of Singapore, Blk 5 #02-09, 4 Engineering Drive 4, Singapore 117585, Singapore.
2. Department of Pharmacology, Institute of Medical Sciences, Banaras Hindu University, Varanasi 221005, India.
3. Division of Life and Health Sciences, Graduate School at Shenzhen, Tsinghua University, Shenzhen 518055, China.

✉ Corresponding author: Division of Life and Health Sciences, Graduate School at Shenzhen, Tsinghua University, Shenzhen 518055, China. Tel./fax: + 86 - 75526036736; E-mail: mei.lin@sz.tsinghua.edu.cn (L. Mei). Or Department of Chemical & Biomolecular Engineering, National University of Singapore, Blk 5 #02-09, 4 Engineering Drive 4, Singapore 117585, Singapore. Tel.: + 65 - 6874 3835; Fax: + 65 - 6779 1936; E-mail: chefss@nus.edu.sg (Si-Shen Feng).

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Abstract

Nanotheranostics is to apply and further develop nanomedicine strategies for advanced theranostics. This review summarizes the various nanocarriers developed so far in the literature for nanotheranostics, which include polymer conjugations, dendrimers, micelles, liposomes, metal and inorganic nanoparticles, carbon nanotubes, and nanoparticles of biodegradable polymers for sustained, controlled and targeted co-delivery of diagnostic and therapeutic agents for better theranostic effects with fewer side effects. The theranostic nanomedicine can achieve systemic circulation, evade host defenses and deliver the drug and diagnostic agents at the targeted site to diagnose and treat the disease at cellular and molecular level. The therapeutic and diagnostic agents are formulated in nanomedicine as a single theranostic platform, which can then be further conjugated to biological ligand for targeting. Nanotheranostics can also promote stimuli-responsive release, synergetic and combinatory therapy, siRNA co-delivery, multimodality therapies, oral delivery, delivery across the blood-brain barrier as well as escape from intracellular autophagy. The fruition of nanotheranostics will be able to provide personalized therapy with bright prognosis, which makes even the fatal diseases curable or at least treatable at the earliest stage.

Key words: Cancer nanotechnology; Drug targeting; Molecular biomaterials; Molecular imaging; Oral chemotherapy; Pharmaceutical nanotechnology.

1. Introduction

The word “theranostics” refers to the simultaneous integration of diagnosis and therapy [1]. Nanotheranostics is to apply and further develop nanomedicine strategies for advanced theranostics, *i.e.* to apply and further develop the various nanocarriers such as polymer conjugations, dendrimers, micelles, liposomes, metal and inorganic nanoparticles, carbon

nanotubes, nanoparticles of biodegradable polymers for sustained, controlled and targeted co-delivery of diagnostic and therapeutic agents for better theranostic effects and fewer side effects. The purpose is to diagnose and treat the diseases at their earliest stage, when the diseases are most likely curable or at least treatable. Nanotheranostics can be promising

even for the fatal diseases such as cancer, cardiovascular diseases and AIDS, which creates the chance to make treatment much less troublesome and prognosis bright, thus saving resources and enhancing the quality of life for the patients. Nanomedicine, defined as application of nanotechnology to diagnose, treat and prevent diseases at cellular and molecular level, can also be efficient for development of theranostic candidate to combine diagnosis and therapy simultaneously [1-3]. Advanced theranostic nanomedicine is multifunctional in nature, capable of diagnosis and delivery of therapy to the diseased cells with the help of targeting ligand and biomarkers [3-6].

Mainly for medical purposes: Theranostic nanomedicine means colloidal nanoparticles ranging in sizes from 10 to 1000 nm (1 μm). They consist of macromolecular materials/polymers in which the diagnostic and therapeutic agents are adsorbed, conjugated, entrapped, encapsulated for diagnosis and treatment simultaneously at cellular and molecular level [7-9].

Theranostic nanomedicine can work better than other theranostics since they have advanced capabilities in an all-in-one single platform, which include sustained/controlled release, targeted delivery, higher transport efficiency by endocytosis [9], stimulus responsive agent release (*i.e.*, smart delivery) [9,10], synergetic performance (e.g., combination therapy, siRNA co-delivery) [11], multimodality diagnosis and/or therapies and quality performances (e.g., oral delivery, escape from multi drug resistance (MDR) protein, autophagy inhibition etc) [12-17]. The encapsulation of single diagnostic or therapeutic agent in nanomedicine may not have high efficacy/specificity/sensitivity for the applications. There-

fore, multimodality nanotheranostics can be developed to make use of the advantages, which may be achieved by co-encapsulation of multiple diagnostic modes and therapeutic modes in targeting nanomedicine platforms [18]. Interestingly, siRNA can also be included in theranostic nanomedicine as inhibitor of theranostic resistance. The siRNA based theranostic nanomedicine has shown to have greatly improved the diagnosis and therapy as multimodality therapy [11]. As a novel approach, nanomedicine has also been developed for oral chemotherapy. We have reported D- α -tocopheryl polyethylene glycol 1000 succinate (TPGS) based nanomedicine for oral delivery of chemotherapeutic agents (e.g., docetaxel and paclitaxel) with enhanced oral bioavailability (**Figure 1**) [12,19,20]. Oral delivery of theranostic nanomedicine (*i.e.*, oral theranostics) will be a task for future research, which will radically promote the practice of cancer theranostics and improve the quality of life for cancer patients, realizing the patients' dream of "chemotherapy at home" [12]. Autophagy or autophagocytosis is a catabolic process in which intracellular degradation of dysfunctional cellular components or foreign invaders occurs in lysosomes. Also, autophagy affects nanomedicine after endocytosis and its therapeutic effect by changing intracellular pharmacokinetics of nanomedicine (*i.e.*, absorption, distribution, excretion and metabolism of nanomedicine). Therefore, autophagy inhibitors loaded in the theranostic nanomedicine can enhance the delivery of diagnostic and therapeutic agents [13]. Thus, advanced nanotheranostics has been under progress for concurrent diagnosis and therapy of diseases in high efficiency at the cellular and molecular level [16, 17].

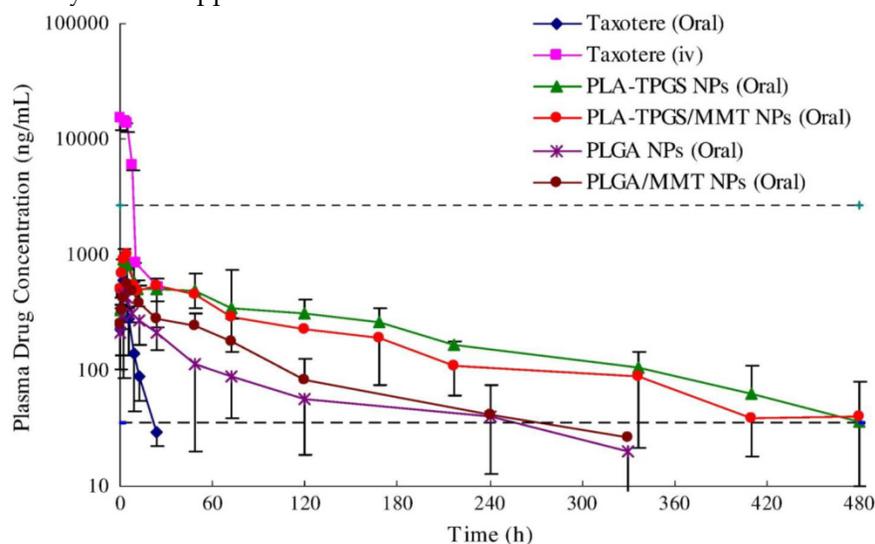


Figure 1. Plasma concentration–time profiles of docetaxel after oral administration to Sprague-Dawley rats at 10 mg/kg dose formulated in the PLGA nanoparticles, PLA–TPGS nanoparticles (NPs), PLGA/montmorillonite NPs, PLA–TPGS/montmorillonite NPs or Taxotere®, compared with the *i.v.* administration of Taxotere® ($n = 5$). The therapeutic window is defined as the drug concentration in plasma between the maximum tolerated level (2700 ng/ml) and the minimum effective level (35 ng/ml). Reproduced with permission from Figure 4 of ref. [12] Elsevier Ltd, © (2013).

The therapeutic agents in theranostic nanomedicine also include hydrophobic organic drugs, proteins, peptides and genetic materials. In addition to therapeutic agent, diagnostic agents commonly used in theranostic nanomedicine include those for optical imaging (using fluorescent dyes or quantum dots), magnetic resonance imaging (MRI) (using superparamagnetic metals *i.e.*, iron oxides), nuclear imaging (using radionuclides) and computed tomography (using heavy elements *e.g.*, iodine) [3, 5, 6]. Quantum dots are semiconductor crystals that emit signal when stimulated by external energy sources. The quantum dots are popular nanomaterial among the diagnostic agents used within theranostic nanomedicine as they have significant advantages over organic dyes. Furthermore, quantum dots emit highly intense signals, larger absorption coefficients, high level of brightness and they are photostable [21, 22].

Any disease would be curable or at least treatable if it can be diagnosed at its earliest stage [8]. Hence, advanced theranostic platforms were made for sensitive diagnosis, accurate targeting, effective and controlled delivery of materials [16, 23]. Here, this review was carried out with a view to summarize the recent works on advanced theranostic nanomedicine platforms such as drug-polymer conjugates, polymeric/magnetic nanoparticles, solid lipid nanoparticles, dendrimers, liposomes, micelles, gold nanoparticles and carbon nanomaterials. The advantages of theranostic nanomedicine for the future generations include: 1) intracellular diagnosis and *in vivo* biodistribution 2) advanced therapy 3) therapeutic monitoring following the treatment [24, 25].

2. Theranostic nanomedicine

Theranostic nanomedicine may be defined as nanomedicine that combines diagnostics with thera-

peutics [3]. The variety of nanomedicine platforms are exploited for the purposes, which are summarized in **Table 1**. Indeed, some nanomedicines *e.g.*, gold nanoparticles, magnetic nanoparticles or carbon nanotubes have intrinsic diagnostic/therapeutic properties. They act as self theranostic nanomedicines or platforms. The advanced theranostic nanomedicines conjugated with targeting moiety can recognize specific target, bind and be internalized via specific mechanism *e.g.*, receptor mediated endocytosis [26]. The nanomedicine of appropriate size and surface coating can have prolonged half-life in the circulation after intravenous (*i.v.*) administration [27]. It was observed that nanomedicines in the size range of 100-200 nm with hydrophilic surface modifications such as polyethylene glycol (PEG) and vitamin E TPGS are commonly used with best effects for theranostic applications [19, 27-30]. For example, we have reported docetaxel loaded poly-lactic acid-D- α -tocopheryl polyethylene glycol 1000 succinate (PLA-TPGS) nanoparticles having hydrophilic surface modification which can achieve a 360 h effective chemotherapy in comparison with only 22 h for Taxotere® after *i.v.* administration (**Figure 2**) [31]. In recent work, we investigated the effects of the PEG chain length of the TPGS on the cellular uptake efficiency and found that shortest PEG tethering chain length, *i.e.* PEG 1000, could have the highest cellular uptake of the nanoparticles due to their highest surface energy to overcome the bending energy needed for the detached piece of cell membrane bilayer to rap the nanomedicine into the biological cells by the mechanism of endocytosis [32]. The interesting preliminary work done by our group suggested the potential use of TPGS 1000 for the development of TPGS based theranostic nanomedicines to achieve desired effects.

Table 1. Some advanced theranostic nanomedicine platforms under progress for simultaneous integration of diagnosis and therapy.

Type of theranostic nanomedicine	Material (s)	Therapeutic agent	Diagnostic agent	Size	Targeting agent	Advancement	Reference
Drug-polymer conjugates	HPMA	64Cu	64Cu	N.A.	RGD	Cancer imaging and radiochemo-therapy	[39]
Polymeric nanoparticles	PLA-TPGS	Docetaxel	Quantum dots	~ 250nm	Folic acid	Co-delivery of docetaxel and quantum dots	[59]
Solid lipid nanoparticles	Low-density lipoprotein, Cholesterol	Paclitaxel/siRNA	Quantum dots	~ 130nm	cRGD	Multimodal therapy	[66]
Dendrimers	Polypropyleneimine	Phthalocyanines	Phthalocyanines	~ 62nm	LHRH	Delivery of single theranostic agent	[75]
Liposomes	TPGS, Phospholipids, Cholesterol	Docetaxel	Quantum dots	~ 210nm	Folic acid	Co-delivery of docetaxel and quantum dots	[88]
Micelles	TPGS	Iron oxide nanoparticles	Iron oxide nanoparticles	~ 178nm	Passive	Delivery of single theranostic agent	[108]
Gold nanoparticles	Gold nanoparticles	DOX	Gold nanoparticles	~ 55nm	CPLGLAG G peptide	Stimulus responsive drug release	[120]
Carbon nanomaterials	SWCNTs	Intrinsic property	Intrinsic property	Length of ~ 140nm	Passive	Self photoluminescent and photothermal property	[131]

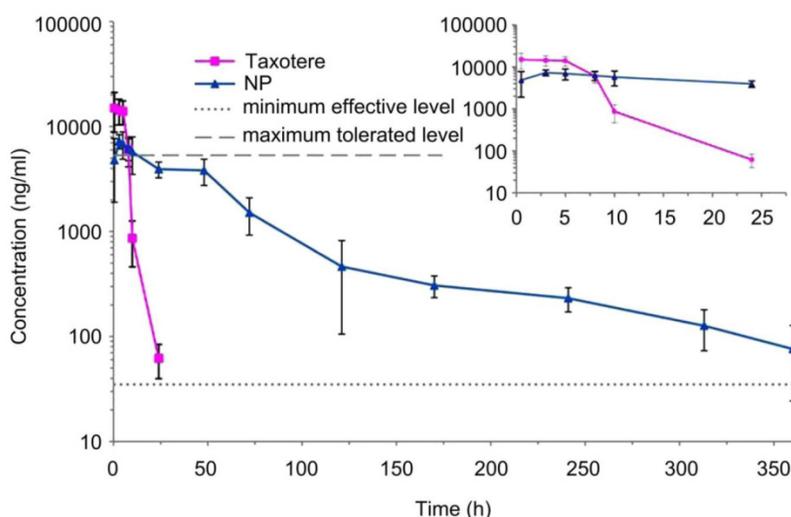


Figure 2. *In vivo* pharmacokinetics profiles of docetaxel plasma concentration vs. time after *i.v.* administration of Taxotere® and the TPGS-emulsified PLA-TPGS NPs formulation using Sprague-Dawley rats at the same docetaxel dose of 10 mg/kg ($n = 5$). Reproduced with permission from Figure 5 of ref. [31] Bentham Science Publishers Ltd, © (2010).

2.1. Drug-polymer conjugates

Drug-polymer conjugates are prepared by covalent interactions using different chemical pathways that mainly depend on the functional groups of drug and polymeric carrier involved in the chemical conjugations. The two major types of conjugates include protein conjugates and drug conjugates with appropriate polymers [33]. The most successful polymer for theranostic drug-polymer conjugate is N-(2-hydroxypropyl) methacrylamide (HPMA) [33]. The common methods for functionalization of HPMA copolymers with diagnostic and therapeutic agents are chemical conjugation and copolymerization [33, 34]. HPMA based conjugates are used for theranostics since they are stable, non-toxic and biocompatible for *in vivo* applications [33, 35, 36]. There are many studies showing the applications of HPMA polymer in combination with diagnostic agents. For example, a passive targeted HPMA-doxorubicin (DOX) conjugate labeled with I-131 has been studied in Phase I clinical trial [37]. In another study, targeted HPMA drug-conjugate was prepared as theranostic nanomedicine. HPMA with Gadolinium was prepared by copolymerization method, attached with Arg-Gly-Asp (RGD) and labeled with In-111as diagnostic agent [38]. Most recently, Yuan et al. [39] synthesized poly(HPMA) based theranostic copolymers loaded with Cu-64 (*i.e.*, intrinsic theranostic agent) and RGD was used as targeting ligand for targeting tumor angiogenesis (**Figure 3A**). The tumor localization of the drug-polymer conjugate was evaluated in mice bearing human prostate cancer xenografts by positron emission tomography (PET). PET quantitative analysis demonstrated that tumor Cu-64 radioactivity in tumor-bearing mice 3h following *i.v.* injection

of the drug-polymer conjugate was significantly higher than the tumor Cu-64 radioactivity in tumor-bearing mice injected with the non-targeted drug-polymer conjugate. The drug-polymer conjugate showed 1 fold improvement in the pharmacokinetics of Cu-64 in tumor [39].

2.2. Polymeric/magnetic nanoparticles

Polymeric nanoparticles from biodegradable polymers have been extensively studied for various therapies [9,40,41]. The polymeric blocks were used to prolong the circulation half-life due to lower phagocytic uptake [42-44]. Polymeric nanoparticles are now used in theranostic applications for the targeted co-delivery of diagnostic and therapeutic agent owing to their biocompatibility, storage stability, protection of loaded drug/diagnostic agent and controlled/sustained release [43]. Biodegradable polymers are used for nanoparticles preparation to provide biological compatibility with less cytotoxicity. The biodegradable polymeric nanoparticles showed their advantage over micelles and liposomes by their excellent storage stability [42]. Poly(D,L-lactide-co-glycolide) (PLGA), PLA-TPGS and poly(D,L-lactide-co-glycolide)-polyethylene glycol (PLGA-PEG) are the mostly reported biodegradable polymers for the fabrication of theranostic polymeric nanoparticles [45,46]. PLA and PLGA will be easily hydrolyzed into their monomers (*i.e.*, lactic acid or glycolic acid) and eliminated from human systems via metabolic pathways. The polymeric nanoparticles were prepared by either polymerization of monomers (*e.g.*, emulsion method) or dispersion of polymers (*e.g.*, nanoprecipitation, salting out, and solvent evaporation methods) [45-49].

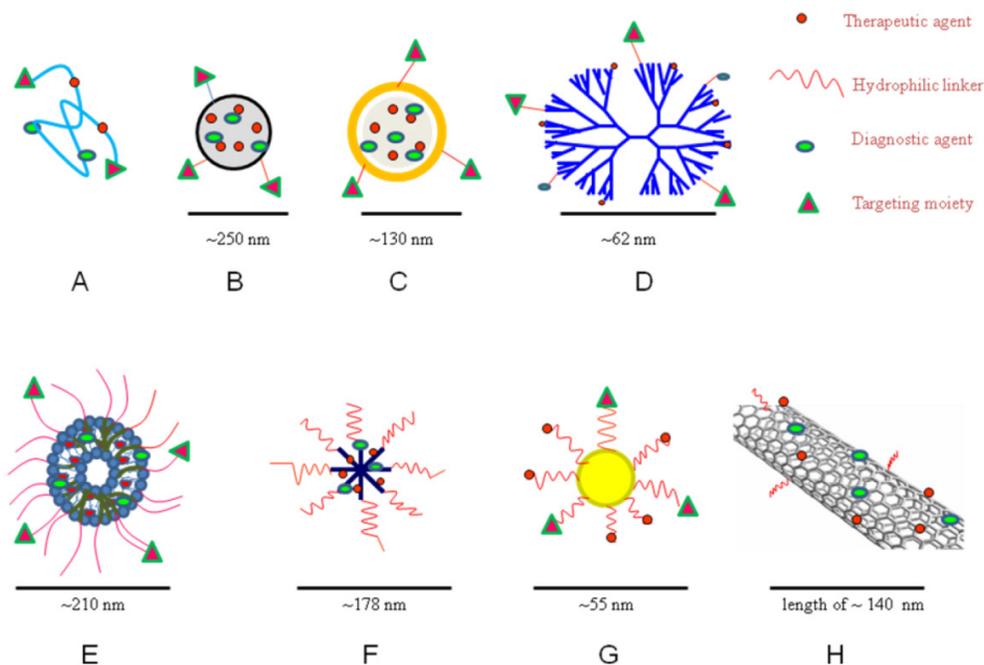


Figure 3. Schematic diagram of theranostic A) polymer-drug conjugate; B) polymeric nanoparticle; C) solid lipid nanoparticle; D) dendrimer; E) liposome; F) micelle; G) gold nanoparticle; and H) carbon nanotube

The magnetic nanoparticles are iron oxide nanoparticles made from magnetite or hematite [50]. Iron oxide nanoparticles were highly used owing to their superparamagnetic effects and acceptable biocompatibility. Co-precipitation and thermal decomposition methods are the facile and convenient methods to synthesize iron oxide nanoparticles. They mainly act as theranostic in cancer treatment alone or loaded into other nanopatforms like polymeric nanoparticles, liposomes etc [50-54]. In addition to intrinsic theranostic property, magnetic nanoparticles have prominent transverse relaxation time (T₂) among diagnostic agents for MRI and play role in cancer therapy as hyperthermia agent and immunotherapeutic platform for autoimmune diseases [54,55]. The surface coating of iron oxide nanoparticles using dextran, PEG, oleic acid or surfactant improves the stability and water dispersibility of the nanoparticles [56, 57].

In one study, Zhang et al. [58] prepared cholic acid conjugated PLGA nanoparticles with co-administration of autophagy inhibitors such as 3-methyladenine and chloroquine. The IC₅₀ values of the docetaxel formulated in PLGA nanoparticles in combination with 10 mM 3-methyladenine or 30 mM chloroquine are found 5.7 or 8.0 fold more effective for the nanoparticle drug delivery after 24 h treatment. The xenograft tumor volume of the severe combined immunodeficiency (SCID) mice after 20 day treatment with the PLGA nanoparticles formulation combined with 3-methyladenine or chloroquine are

found to be only about a half in comparison with the PLGA nanoparticles formulation only [58]. Thus, the incorporation of autophagy inhibitor in future theranostic platform, can improve the co-delivery of diagnostic and therapeutic agent. In addition, they found a new mechanism of cancer cells to have polymeric nanoparticles captured and degraded by auto-lysosomes, which is thought to be autophagy pathway [58]. Previous studies reported that polymeric nanoparticles are internalized into the cells through endocytosis, and then can be transported into lysosomes for degradation only by endosome pathway (Figure 4) [13, 58].

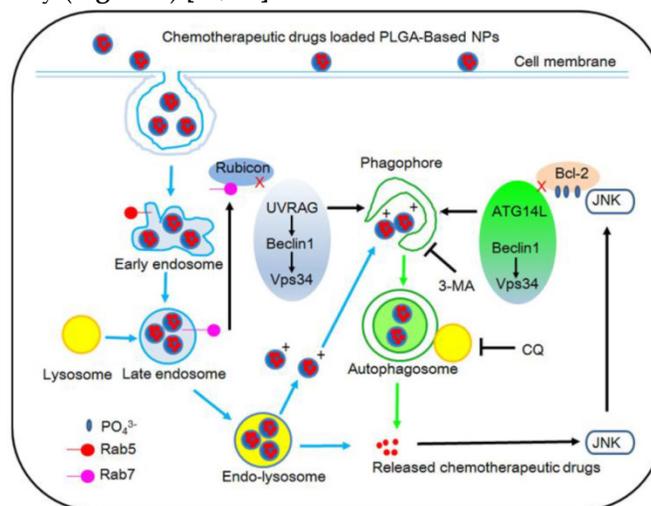


Figure 4. Schematic representation of the degradation pathway of PLGA-based nanoparticles in cancer cell. Reproduced with permission from Figure 8 of ref. [58] Elsevier Ltd, © (2014).

In our group, we demonstrated PLA-TPGS based theranostic platforms [59]. A good example of PLA-TPGS based theranostic is PLA-TPGS and acid functionalized D- α -tocopheryl polyethylene glycol 1000 succinate (TPGS-COOH) copolymer blend nanoparticles prepared with folate targeting (**Figure 3B**). The nanoparticles were loaded with both docetaxel and quantum dots. The targeting effect of quantum dots loaded PLA-TPGS/TPGS-COOH nanoparticles was studied in both MCF-7 breast cancer cells which overexpresses folate receptors and NIH-3T3 fibroblast cells which are expressing low quantity of folate receptors. The studies showed higher internalization/cytotoxicity of folate-decorated quantum dots loaded PLA-TPGS/TPGS-COOH nanoparticles by MCF-7 breast cancer cells than by the NIH 3T3 fibroblast cells [59]. Therefore, copolymers of TPGS conjugated with targeting ligands will be a promising theranostic tool for targeted diagnosis and therapy. Later, we developed a multimodal imaging system by co-encapsulating superparamagnetic iron oxide nanoparticles for MRI and quantum dots for fluorescence imaging [18]. The nanoparticles of PLA-TPGS were fabricated to combine their advantages and to promote a sustained and controlled imaging with passive targeting to the cancer cells. This novel strategy reduced the toxicity of the individual contrast agents and improved their biocompatibility and cellular uptake. The xenograft model was also conducted for biodistribution of the quantum dots and iron oxides loaded PLA-TPGS nanoparticle among the various organs, which showed greatly enhanced tumor imaging. The *ex vivo* fluorescent images analysis showed the significant percentage fluorescent intensity increase of 67.1% in liver, 51.5% in kidney and 152.8% in tumor. The surface adsorption of nanoparticles in blood-brain barrier showed more fluorescent signal for brain samples than other organs. Also, percentage fluorescent intensity increase in brain was observed less for treated group owing to poor improvement in biodistribution of the quantum dots and iron oxides loaded PLA-TPGS nanoparticle across the blood-brain barrier (**Figure 5**). The multimodal imaging system shows great advantages of both contrast agents making the resultant probe highly sensitive with good depth penetration for longer duration up to 6 h, which confirms the diagnosis obtained from each individual imaging [18]. Further, therapeutics encapsulation and ligand conjugation with this multimodal system was suggested to develop an advanced multimodal theranostic nanomedicine. As a multimodal approach, Medarova et al. [60] developed iron oxide nanoparticles for simultaneous *in vivo* imaging and siRNA delivery into tumors by high resolution MRI and near infrared (NIR) *in vivo* optical imaging.

The siRNA was coupled with aminated dextran particles using N-succinimidyl-3-(2-pyridyldithio) propionate as a bridge compound. Further, myristoylated polyarginine peptide, a membrane translocation peptide, and the NIR dye Cy5.5 were conjugated to iron oxide nanoparticles surface. By tracking these probes *in vivo* by MRI and NIR fluorescence optical imaging, the delivery of siRNA and its silencing efficiency was monitored for 48 h by dextran coated iron oxide nanoparticles (**Figure 6**) [60].

2.3. Solid lipid nanoparticles

Solid lipid nanoparticles are a safe and effective alternative colloidal matrix carrier to conventional emulsions, liposomes, and polymeric nanoparticles for intravascular delivery [9]. They are made up of solid hydrophobic core containing dissolved or dispersed drug. Solid lipid nanoparticles are nanomedicine made from biocompatible lipids (e.g., triglycerides) which are solid at room temperature. The commonly used methods of preparation are hot and cold homogenization. Solid lipid nanoparticles gain access to the blood compartment easily because of their small size and lipophilic surface. The size range of less than 100 nm allows solid lipid nanoparticles to cross tight-endothelial cells of blood-brain barrier for brain targeting. The high drug loading efficiency renders the drug stable in solid lipid matrix, and provides controlled release up to several weeks [61-63]. Similar to other nanomedicines, solid lipid nanoparticles are used for targeted co-delivery of diagnostic and therapeutic agent as theranostic platform [63, 64]. Recently, lymphatic delivery of solid lipid nanoparticles emerged as a technology to provide better transport into the lymphatics resulting in enhanced oral bioavailability of therapeutic agents [65]. For example, Shuhendler et al. [66] reported a novel targeted NIR light-emitting solid lipid nanoparticles by conjugating $\alpha(v)$ $\beta(3)$ integrin-specific ligand *i.e.*, cyclic Arg-Gly-Asp (cRGD) and loaded NIR quantum dots for live animal imaging [66]. They were injected intravenously to nude mice bearing xenograft breast tumors. Tumor micropharmacokinetics and whole animal biodistribution by optical imaging of the formulations were studied. The active tumor targeting with cRGD showed significantly greater distribution in the liver, spleen, and kidneys than the non-targeted solid lipid nanoparticles. The enhanced specificity and retention of RGD-solid lipid nanoparticles in tumor neovasculature for 120 h suggested the potential use of the solid lipid nanoparticles for theranostic application of neovascular-specific therapies and imaging.

In another work, Bae et al. [67] reported quantum dots loaded solid lipid nanoparticles for anti-

cancer theranostics with synergistic/multimodal therapeutic effects of paclitaxel and siRNA (Figure 3C). The low density lipoprotein (LDL)-mimetic solid lipid nanoparticles were prepared with stable core/shell nanostructure incorporating quantum dots and paclitaxel within the lipid shell while anionic siRNA molecules are electrostatically complexed with the outer surface of solid lipid nanoparticles. The prepared solid lipid nanoparticles/siRNA complexes efficiently delivered both paclitaxel and Bcl-2 target-

ing siRNA into human lung carcinoma cells and exhibited synergistic anticancer activities by triggering caspase-mediated apoptosis. The strong fluorescence intensity of quantum dots within solid lipid nanoparticles enables in situ visualization and intracellular translocation of solid lipid nanoparticles in cancer cells. The experiment showed that LDL-mimetic solid lipid nanoparticles as a multifunctional/multimodal and optically traceable nanocarrier for efficient anti-cancer theranostics [67].

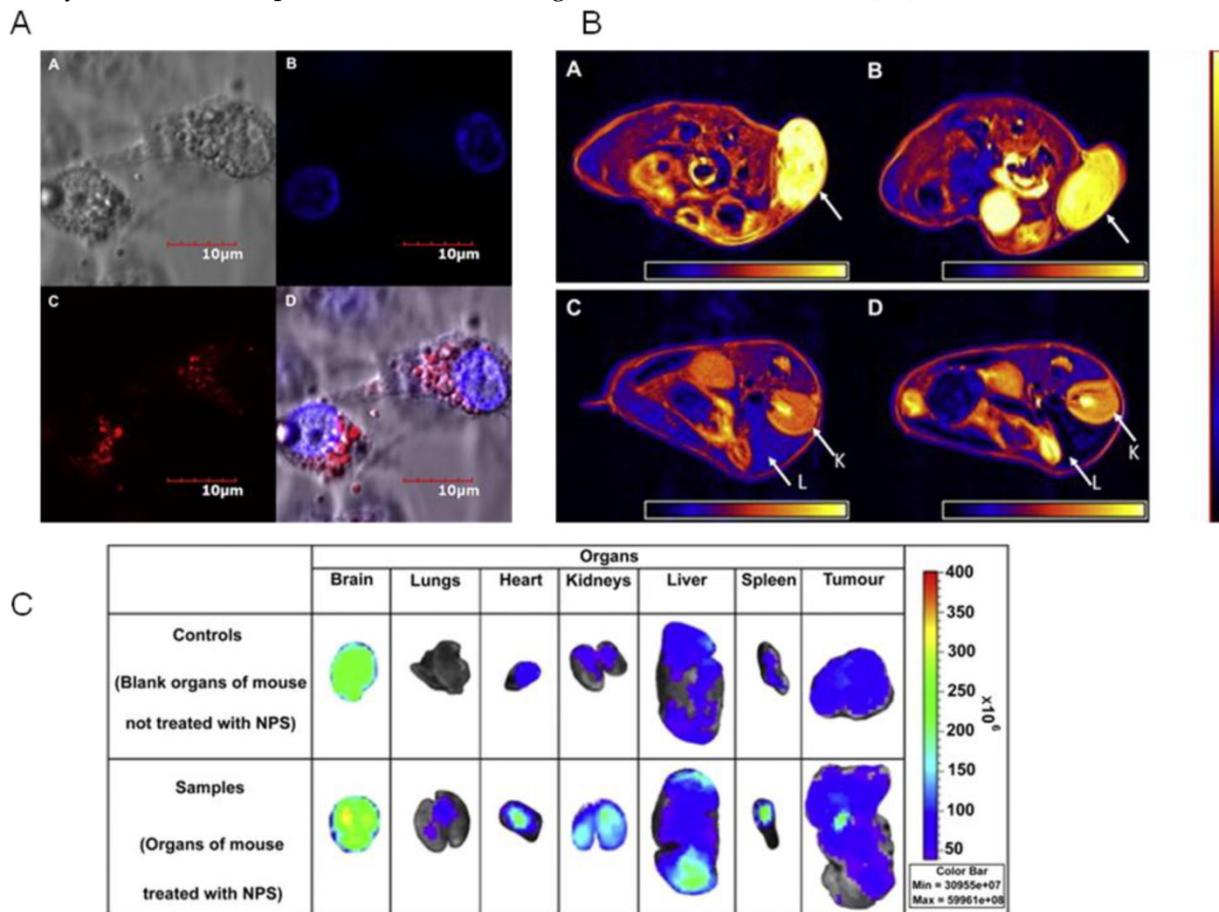


Figure 5. Multimodal imaging of polymeric nanoparticles A) Confocal images of MCF-7 cells treated with the quantum dots and iron oxides loaded PLA-TPGS nanoparticle *in vitro* (scale bar = 10 μm). A: Bright field image of cells. B: Blue coded stained nuclei. C: Red coded quantum dots from nanoparticles in cytoplasm. D: Complete overlapped image. B) Axial MRI image sections of the MCF-7 grafted tumor bearing mice. Images A and B show the part of the tumor (shown by the arrow) before and after 6 h of administration of the quantum dots and iron oxides-loaded PLA-TPGS nanoparticle into the mice. Images C and D show the kidney (K) and liver (L) part of the mice before and 6 h after the administration of the PLA-TPGS nanoparticle formulation of quantum dots and iron oxides (dosage: 1.5 mg of Cd/kg of body weight or equivalent of 6.0 mg of Fe/kg body weight). The decrease in intensity in the regions of the tumor and liver can be noticed in comparison with the color scale aside. C) Fluorescent images of the various organs. Upper row: control. Lower row: Organs of the mouse treated with the quantum dots and iron oxides-loaded PLA-TPGS nanoparticle (dosage: 1.5 mg of Cd/kg of body weight or equivalent of 6.0 mg of Fe/kg body weight). Reproduced with permission from Figure 2, 5, 6 of ref. [18] Elsevier Ltd, © (2011).

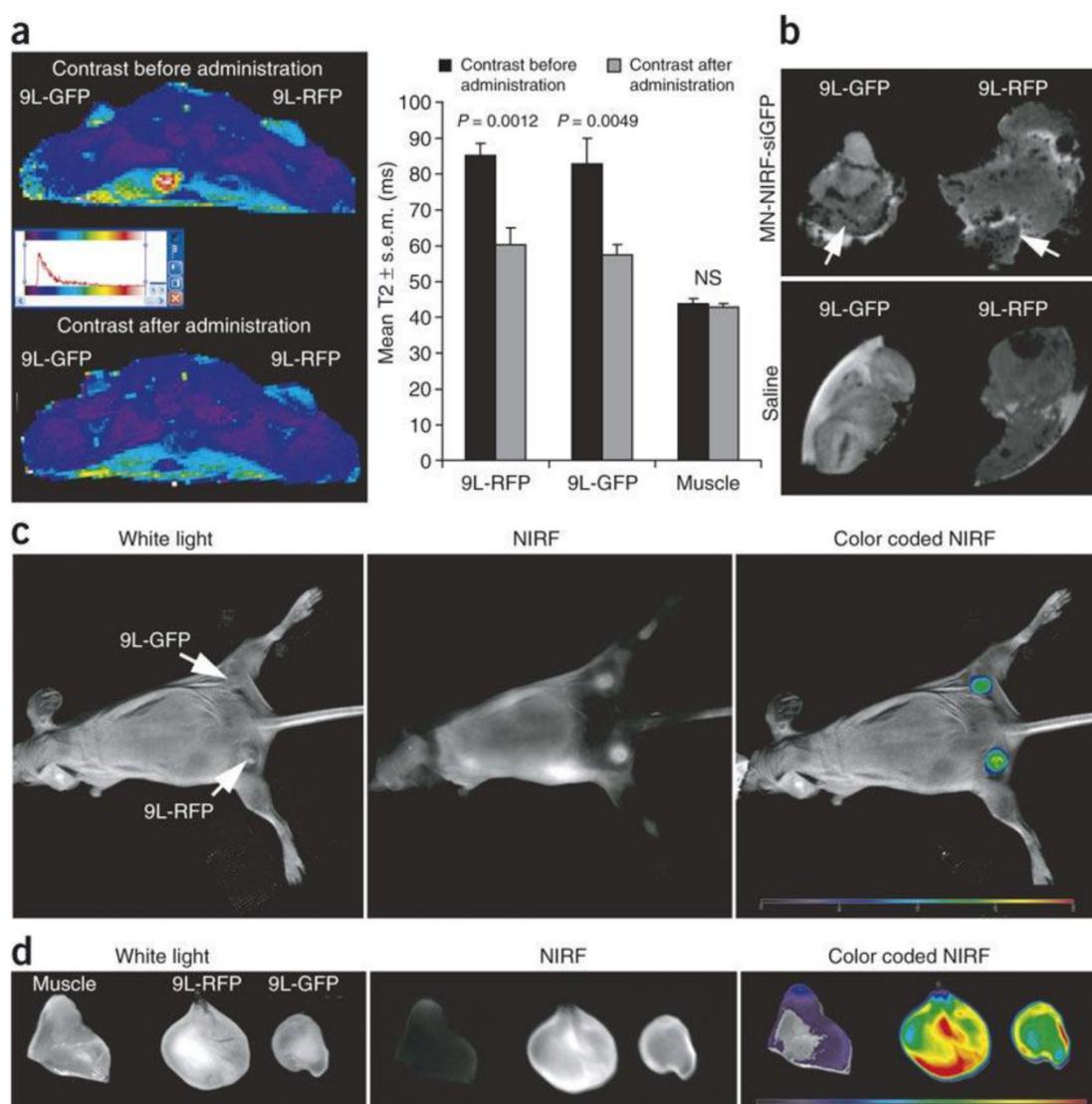


Figure 6. Theranostic approach using dextran coated iron oxide nanoparticles (a) *In vivo* MRI was performed on mice bearing bilateral green fluorescent protein (9L-GFP) and red fluorescent protein (9L-RFP) tumors before and 24 h after nanoparticles administration. After injection of the probe, there was a significant drop in T2 relaxation times associated with the tumors. Note that T2 relaxation times of muscle tissue remained unchanged. (b) *Ex vivo* high-resolution MRIs of excised tumors (78 μ m isotropic). Distinct foci of signal loss (arrows), reflecting probe accumulation, were easily identifiable in tumors derived from mice injected with the probe but not from saline-injected controls. (c) *In vivo* NIR optical imaging of the same mice as in a produced a high-intensity NIR signal associated with the tumors. This confirmed the delivery of the nanoparticles probe to these tissues. (d) *Ex vivo* NIR optical imaging demonstrated a significantly higher fluorescence in tumors than in muscle tissue ($P = 0.0058$). Reproduced with permission from Figure 3 of ref. [60], Macmillan Publishers Ltd: Nature Medicine, © (2007).

2.4. Dendrimers

Dendrimers are synthetic nanomedicine that comprises a highly branched spherical polymer. Dendrimers used in nanotheranostics are usually 10 to 100nm [68]. Dendrimers can be synthesized starting from the central core toward the periphery (divergent synthesis) or in a top-down approach starting from the periphery (convergent synthesis). They are synthesized by the repetitive addition of branching units to an amine core (ethylene diamine or ammonia). The basic structure of dendrimers is a repeated branching around the core resulting in an early-perfect three-dimensional (3D) geometrical pattern. Dendrimers showed toxicity by disrupting cell mem-

branes due to their positive surface charge. In some cases, dendrimers encapsulated drug for targeted drug delivery tends to release rapidly, before they reach a targeted site [69, 70]. By controlling the degree of polymerization, dendrimers can be synthesized in various sizes, molecular weights and chemical compositions [71, 72]. The higher generation dendrimers resemble spherical shape, having a number of cavities and branches to hold both therapeutic and diagnostic agents for theranostic application. The fifth generation dendrimers (G5) having more hydrophobicity are generally preferred owing to enhanced drug stability in dendrimers [69-72]. In one study, a replication-deficient adenovirus serotype 5 carrying the so-

dium-iodide symporter (hNIS) gene was coated with poly(amidoamine) dendrimers generation 5 (PAMAM-G5) and investigated for transduction efficacy by I-123 scintigraphy in a liver cancer xenograft mouse model. After dendrimer coating, replication-deficient adenovirus serotype 5/hNIS demonstrated partial protection from neutralizing antibodies and enhanced transduction efficacy in coxsackie-adenovirus receptor-negative cells *in vitro*. *In vivo* I-123 scintigraphy of nude mice revealed significantly reduced hepatic transgene expression after *i.v.* injection of dendrimer-coated replication-deficient adenovirus serotype 5/hNIS [73]. Further, Saad et al. [74] designed, characterized, and evaluated a theranostic dendrimer for *in vitro* and *in vivo*. These nanocarriers delivered the paclitaxel and diagnostic agent (Cy5.5). A synthetic analog of luteinizing hormone-releasing hormone (LHRH) peptide targeted to receptors overexpressed on the membrane of cancer cells was attached to the dendrimer as a tumor targeting moiety. Significant differences were found between various studied non-targeted carriers in their cellular internalization, cytotoxicity, tumor and organ distribution and anticancer efficacy. High cellular uptake of tumor targeted theranostic dendrimer was accompanied by targeted accumulation of paclitaxel which reduced the adverse effect on healthy organs and increased the specificity and sensitivity of cancer imaging using fluorescent probes. It shows the theranostic nature of LHRH receptor targeted dendrimer [74].

In another study, Taratula et al. [75] developed a novel dendrimer-based theranostic platform for tumor-targeted delivery of phthalocyanines (Pc) (**Figure 3D**). The preparation procedure involved the modification of the Pc molecule with a hydrophobic linker, which significantly enhances physical encapsulation of the hydrophobic drug into a generation 4 polypropylenimine (PPIG4) dendrimer. To improve biocompatibility and tumor-targeted delivery, the surface of the Pc-PPIG4 complexes was additionally modified with PEG and LHRH peptide, respectively. The synthesized phthalocyanine derivative entrapped in the dendrimer-based nanocarrier exhibits a distinct NIR absorption (700 nm) and fluorescence emission (710 and 815 nm), required for an efficient photodynamic therapy and fluorescence imaging. It was demonstrated that subcellular localization *in vitro* and organ distribution *in vivo* of the developed nanocarrier can be determined based on the intrinsic fluorescence properties of encapsulated phthalocyanine. The prepared formulation showed high cytotoxicity and significant photodynamic therapy up to 24 h. The *in vitro* and *in vivo* imaging experiments revealed that the LHRH targeted theranostic dendrimer is capable of an efficient internalization into cancer cells as well

as tumor accumulation. The study revealed the significant potential of dendrimers as an efficient NIR theranostic agent [75]. Likewise, dendrimers have been under development for recent years and proven to be successful theranostic carriers in number of pre-clinical studies.

2.5. Liposomes

Liposomes are small bilayer vesicles enclosing aqueous compartment that can be produced using amphiphilic phospholipids and cholesterol [76]. Liposomes are spherical, vary in size most are 400 nm or less. Liposomes are effective platforms for drug/diagnostic delivery owing to their size, hydrophobic and hydrophilic character, biocompatibility, biodegradability, low toxicity and immunogenicity. Commonly, liposomes with smaller diameter (80-200 nm) with neutral or negative charge are used for theranostic purpose [77-79]. The major three types of liposome preparation methods are mechanical dispersion, solvent dispersion and detergent removal. However, the potential drawbacks of liposomes are low drug loading efficiency, batch-to-batch variation in manufacturing, and poor stability [77-79]. The nanosized diagnostic agents such as iron oxide nanoparticles, quantum dots and gold nanoparticles can be entrapped within the theranostic liposomes and the therapeutic agent can be either encapsulated in the core or embedded in the lipophilic bilayer shell [80-85]. The advanced theranostic liposomes are conjugated with molecular biomarkers for targeting effect. To overcome opsonization by the immune system and fast elimination from blood circulation, stealth liposomes *i.e.*, PEG-coated liposomes, were formulated with stability and longer half-life in blood [84, 86]. Recently, our group prepared liposomes surface-coated with TPGS and loaded docetaxel and evaluated for possibility against brain tumor by *in vitro* cell line studies with PEGylated liposomes, conventional nude liposomes (without TPGS coating) and TPGS coated liposomes. The TPGS-coated liposomes showed higher efficacy than PEGylated liposomes [87]. Muthu et al. [88] prepared TPGS coated theranostic liposomes containing docetaxel and quantum dots with and without targeting moieties (**Figure 3E**). Folic acid was used as targeting probe to target folate receptor overexpressing MCF-7 breast cancer cell lines. The higher cellular uptake and cytotoxicity of targeted theranostic liposomes was observed in comparison to non-targeted liposomes (**Figure 7**). Along similar lines, Wen et al. [89] have developed quantum dots and apomorphine incorporated theranostic liposomes to eliminate uptake by the liver and to enhance brain targeting. The formulation was evaluated for *in vitro* brain endothelial cell uptake

and *in vivo* bioimaging. *In vitro* cellular uptake study confirmed the delivery of liposomes through receptor mediated endocytosis routes. A significant distribution was observed for theranostic liposomes compared to free quantum dots. The brain uptake was increased 2.4 fold after the quantum dots were incorporated into liposomes. Quantum dots uptake was decreased in heart and liver by liposomes delivery. The fluorescence in the brain observed up to 1 h for the liposome treated group. However, free quantum dots was rapidly eliminated from the brain and retained more in liver up to 35 min. The suggested mechanisms for the cellular uptake were clathrin- and caveola-mediated endocytosis [89]. In most recent work, Wen et al. [90] prepared theranostic liposomes loaded with quantum dots camptothecin and iri-

notecan for simultaneous bioimaging and drug delivery. The different formulations, including cationic, PEGylated and deformable liposomes, were compared for their theranostic efficiency. The cytotoxicity and cell migration assay demonstrated superior activity of cationic liposomes compared with other carriers. Based on the results, cationic liposomes had higher efficiency to accumulate in solid tumors for exhibiting fluorescent signals compared to other controls. The cationic liposomes showed the brightest fluorescence in tumors than control liposomes. This signal could last for up to 24 h for cationic nanosystems. The versatile and tunable properties of the liposomes made them efficient theranostic delivery for extended duration.

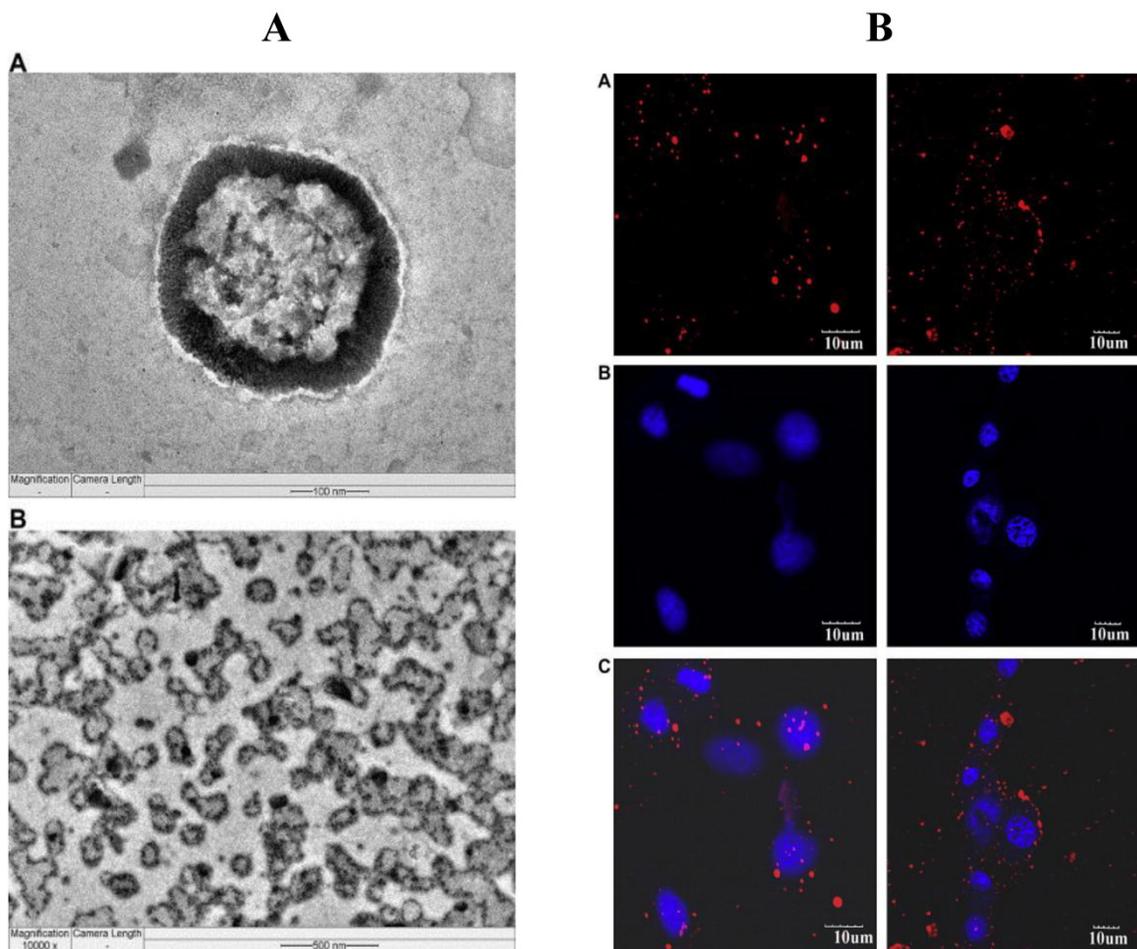


Figure 7. *In vitro* theranostic delivery using TPGS liposomes A) Field-emission transmission electron microscopy image of (A) an individual quantum dots loaded-TPGS coated liposome in 100 nm scale, and (B) multiple quantum dots-loaded TPGS coated liposomes after the storage in 500 nm scale. B) Confocal laser scanning microscopy images using MCF-7 cells after 2 h incubation with the non-targeted TPGS based multi-functional liposomes (left column) and targeted TPGS based multi-functional liposomes (right column). Row (A): Quantum dots showing the red fluorescence from liposomes distributed in cytoplasm, (B): Channels showing the blue fluorescence from dye stained nuclei, and (C): Merged channels of quantum dots and blue dye. Scale bar = 10 μ m. Reproduced with permission from Figure 3, 6 of ref. [88] Elsevier Ltd, © (2012).

2.6. Micelles

Micelles are self-assembling colloidal structure with a hydrophobic core and hydrophilic shell. They have narrow size distribution and less than 100 nm in size [91]. The micelles are another safer alternative for parenteral administration of poorly water-soluble materials [92, 93]. The stability of the micelles depends on strong cohesive force between drug and polymer core as well as cross linking of the shell or core. They are generally prepared by direct dissolution method and organic solvent method [94]. Therapeutic/diagnostic agents can be loaded into hydrophobic core of micelles and the outer hydrophilic layer with targeting agent, which can then be administered intravenously [95-98]. In some cases, targeted drug delivery by micelles are hindered by premature drug release from the micellar nanomedicine before they reaches the molecular targets. The theranostic micelles of particle size less than 50 nm in diameter avoid renal exclusion, reticulo endothelial system and provide them with enhanced endothelial cell permeability in solid tumors [99, 100]. Micelles are efficient platform for cancer drug delivery e.g., Genexol-PM™ which is a paclitaxel loaded micellar formulation by using poly(ethylene glycol)-block-poly(D,L-lactide) [101]. Some clinical trials were already performed that evaluated the safety and efficacy of Genexol-PM™ [102-104].

TPGS is an alternative material for the preparation of drug/diagnostic material loaded targeted/non-targeted micelles [105-107]. We prepared theranostic TPGS micelles containing superparamagnetic iron oxides for diagnosis and therapy of cancer (Figure 3F). It had improved thermal and magnetic properties, in-vitro cellular uptake, cytotoxicity and in-vivo imaging effects in comparison to commercial Resovist® and Pluronic F127 micelles. The prepared TPGS micelles were found to be highly monodisperse, suitable size range and stable. The cellular uptake and cytotoxicity were investigated *in vitro* with a MCF-7 breast cancer cell line for 24 h. Cell viability was decreased after hyperthermia treatment using micelles (Figure 8). Also, T2-mapped images of xenograft grown on SCID mice showed that iron oxide loaded TPGS micelle had ~ 1.7 times and ~ 1.05 times T2 decrease at the tumor site compared to Resovist and Pluronic F127 micelle formulation, respectively (Figure 9) [108]. In another work, Kim et al prepared hyaluronic acid-DOX conjugate by the amide bond formation between amine groups of DOX and carboxylic groups of hyaluronic acid [109]. Hyaluronic acid-DOX conjugates self-assembled to micelle-like nanoparticles. The cytotoxicity study on

cancer cells confirmed the anticancer effect of hyaluronic acid-DOX conjugate micelles. Further, micelles were coated with a gold half-shell by the thermal vapor deposition method, which might contribute to prolonging the residence time using gold surface. The gold half-shell-coated hyaluronic acid-DOX conjugate micelles are successful platform, may be exploited for future cancer theranostic applications [109]. Owing to stability, ease of preparation, hydrophobic encapsulation and success in preclinical and clinical studies, micelles are emerging platforms as theranostic delivery systems.

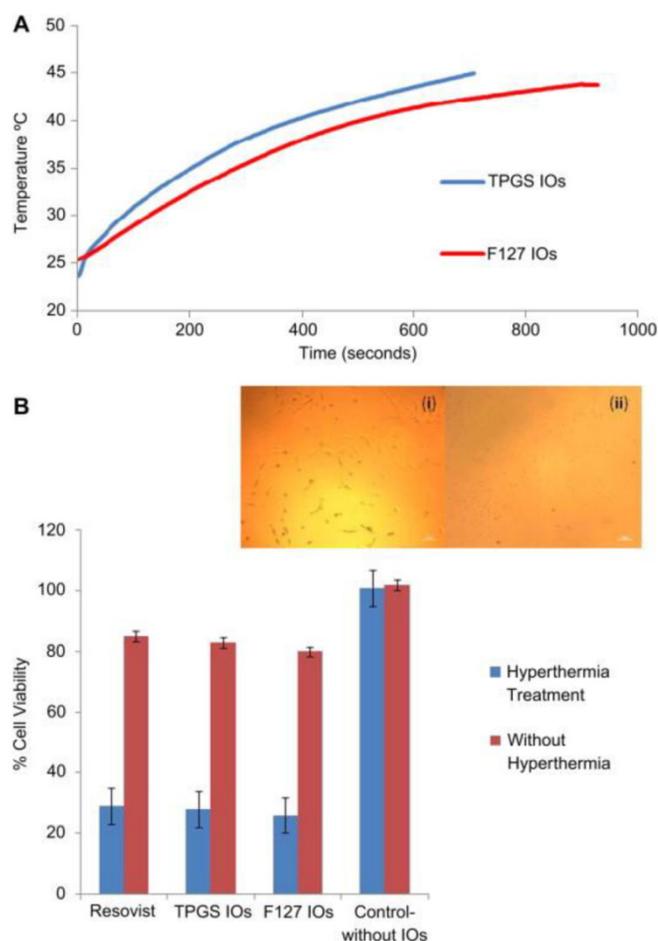


Figure 8. *In vitro* effect of theranostic micelles loaded with iron oxide nanoparticles (A) Hyperthermia study shows that the time-dependent temperature rise of 1 mg/ml of the iron oxide nanoparticles (IOs)-loaded TPGS and F127 micelles on exposure to 89 kA/m alternating current field at 240 kHz frequency. The specific absorption rate value for the IOs-loaded TPGS and F127 micelles was found to be 51.4 and 25.5 Watt/g. (B) The cytotoxic assay performed after hyperthermia treatment of MCF-7 cancer cells incubated with the IOs-loaded TPGS and F127 micelle and Resovist®. Hyperthermia treatment in all cases leads to significant cell death. Inset image (i) shows the cells incubated with the IOs-loaded TPGS micelles but no AC field applied and inset image (ii) shows the cells incubated with the IOs-loaded TPGS micelles and hyperthermia treatment using AC field. From (ii), it can be seen that after hyperthermia treatment, the cell loses viability and do not attach. Reproduced with permission from Figure 6 of ref. [108] Elsevier Ltd, © (2011).

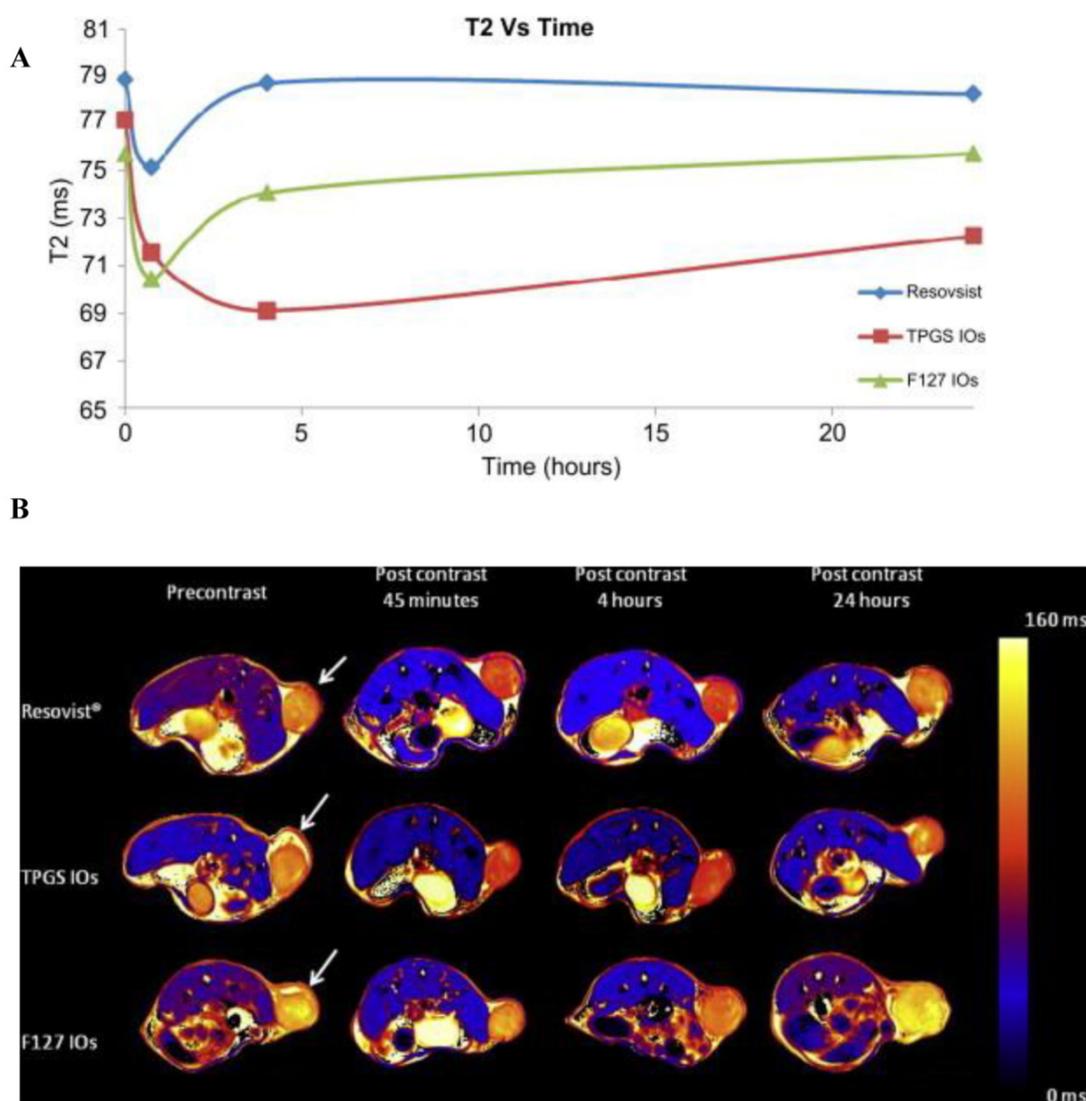


Figure 9. *In vivo* imaging of theranostic micelles loaded with iron oxide nanoparticles A) Graph showing the change of T2 values measured from MCF-7 xenograft tumor at the time point before and 45 min, 4 h and 24 h after injection of the iron oxide nanoparticles (IOs)-loaded TPGS and F127 micelle and Resovist®, respectively at a concentration of 5 mg of Fe/Kg of animal weight. It can be found that the T2 value decreases due to accumulation of IOs at tumor by ~4.3%, 7.3% and 6.9% for Resovist®, the IOs-loaded TPGS and F127 micelles respectively at 45 min after injection. B) T2 mapped images showing the MCF-7 xenograft tumor at the designated time point before and 45 min, 4 h and 24 h after injection of Resovists®, the IOs-loaded TPGS and F127 micelles respectively at a concentration of 5 mg of Fe/Kg of animal weight. The change in T2 in the tumor (marked by the arrow) can be noticed in comparison with the T2 color scale aside. Reprinted with permission from Figure 9, 10 of ref. [108] Elsevier Ltd, © (2011).

2.7. Gold nanoparticles

Gold nanoparticles based on gold cores are another versatile platform that provides desirable values for theranostic systems [110-113]. They are prepared with core size from 1.5 to 10 nm, providing large area for efficient drug and ligand conjugations [114]. Gold nanoparticles are commonly synthesized by chemical treatment of hydrogen tetrachloroaurate. Gold nanoparticles can be conjugated with drug and targeting ligand as advanced theranostics that specifically recognizes the target receptor for active targeting [115, 116]. The therapeutic loading are achieved by either non covalent interaction (e.g. via electrostatic interaction) or covalent chemical conjugation of (*i.e.*, organic

drug). The inherent features of gold nanoparticles include diagnostic property, tunable core size, monodispersity, low toxicity, large surface to volume ratio, surface plasmon absorption, ability to bind to biomolecules via Au-S bonds, light-scattering properties and ease of fabrication [115-117]. Recently, gold nanoparticles showed the possibility of treating MDR tumors by targeted photothermal treatment in combination with a chemotherapeutic agent [118]. Heo et al. [119] described gold nanoparticles surface-functionalized with PEG, biotin, paclitaxel and rhodamine B linked beta-cyclodextrin (beta-CD) as theranostic platform. Paclitaxel formed inclusion complex with beta-CD which was then conjugated with gold nanoparticles. *In vitro* studies suggest that

gold nanoparticles have higher affinity towards cancer cells such as HeLa, A549 and MG63 in comparison to NIH3T3 cells. Furthermore, gold nanoparticles displayed significant cytotoxic effect against HeLa cancer cells. The preliminary work indicates that the gold nanoparticles are feasible for use as theranostic nanomedicine.

In another work, smart theranostic gold nanoparticles were developed *i.e.*, DOX was conjugated to gold nanoparticles via Au-S bond by using a peptide substrate, Cys-Pro-Leu-Gly-Leu-Ala-Gly-Gly (CPLGLAGG), which is specifically cleaved by the protease (**Figure 3G**). The animal studies showed that after injection of the functionalized gold nanoparticles to the tumor-bearing mice, the over-expressed protease in tumor tissue and intracellular glutathione have led to the rapid release of DOX from the functionalized gold nanoparticles. Here, enhanced efficacy on tumor growth inhibition and fluorescent imaging was realized simultaneously. The gold nanoparticles with stimulus responsive drug release property showed a promising smart theranostic application for concurrent cancer diagnosis and therapy [120].

2.8. Carbon nanomaterials

The carbon nanomaterials or nano-carbons have been studied for theranostic purpose owing to their unique physical and chemical properties [121]. Nano-carbons are classified into sp^2 -carbon nanomaterials such as zero dimensional (0D) fullerene, one dimensional (1D) carbon nanotubes (CNTs), two dimensional (2D) graphene and carbon dots (*i.e.*, nano-clusters having size < 10 nm) [121, 122]. The large surface area, ability to encapsulate therapeutic/diagnostic agent and suitability for surface modifications of CNTs made them suitable for theranostic applications [123-125]. The CNTs have cylindrical structure, based on their number of layer of graphene sheets CNTs are classified into single-walled carbon nanotubes (SWCNTs) or multi-walled carbon nanotubes (MWCNTs). CNTs are commonly synthesized by the discharge method, laser method, ball milling method and chemical vapor deposition method [125-130]. Recent years various synthetic approaches of CNTs functionalization have brought multifunctional-CNTs based platforms for theranostic applications. Robinson et al. [131] demonstrated an intrinsic theranostic application of intravenously injected SWCNTs (average length ~140 nm) as photo luminescent agents for *in vivo* tumor imaging in the 1.0-1.4 μ m emission region and as NIR absorbers and heaters at 808 nm for photothermal tumor elimination at lower doses (**Figure 3H**). An *ex vivo* resonance Raman imaging revealed the SWCNT distribution within tumors at a high spatial resolution. Fluorescence im-

aging of SWCNTs shows confirmation of SWCNTs uptake by the tumors. The 100% tumor destruction was achieved for large numbers of photothermally treated mice without any toxic side effects after 6 months post-treatment. Highly effective tumor elimination with SWCNTs was achieved at 10 times lower injected doses and lower irradiation powers than other control preparation. These studies suggest that significant benefits of utilizing the intrinsic properties of biocompatible SWCNTs for theranostic applications [131].

In another study Das et al. [132] designed a theranostic MWCNTs by including acid-oxidised MWCNTs with four varieties of functional moieties: a fluorochrome (Alexa-fluor, AF488/647), targeting agent (*i.e.*, folic acid), radionuclide (Technetium-99m), and methotrexate. The cellular uptake studies showed the selective internalization of theranostic MWCNTs by folate receptor positive human lung (A549) and breast (MCF 7) cancer cells through folate receptor mediated endocytosis. The tumor specific accumulation of targeted theranostic MWCNTs in xenografted mice after 24 h was 19.14 and 8.62 times higher in comparison to free and non-targeted theranostic MWCNTs. This study shows the controlled delivery of methotrexate from theranostic MWCNTs, receptor mediated delivery, optical detectability of fluorochromes, and radio-traceability of ^{99m}Tc . In summary, MWCNTs could be a promising multimodal theranostic platform for cancer diagnosis and therapy. In one study, graphene oxide (GO)-based theranostic nanohybrid is designed for tumor diagnosis and therapy [133]. The DOX is chemically conjugated to the poly(ethylenimine)-co-poly(ethylene glycol) (PEI-PEG) grafted GO via a matrix metalloproteinase-2 (MMP2)-cleavable peptide linkage. The intrinsic fluorescence property of DOX was quenched by GO under normal condition. During MMP2 enzyme over-expression in tumor, peptide was cleaved and released DOX for tumor therapy and concurrent fluorescence signal of DOX was used for *in situ* tumor cell imaging. Here, positively charged theranostic GO showed an efficient transfection for nanotherapeutics. This study opens a window for tumor treatment by theranostic approach with a combination of diagnosis and pathology responsive therapy [133]. Here, CNTs have demonstrated the efficacy during therapeutic and diagnostic delivery in preclinical level for future use.

3. Conclusions and perspectives

In this review, the recent developments of the various theranostic nanomedicines and their pre-clinical success were discussed. We noticed that in most cases, the interesting results of theranostic na-

nanomedicines in the literature are available only for *in vitro* studies. There are more challenges to be faced for their *in vivo* applications to pre-clinical and clinical level. A search on PubMed® shows that around 645 articles have been published in last 5 years within this research interest. However, almost all of them are focused on preparation, physico-chemical characterization and *in vitro* cell culture work of nanotheranostics with little *in vivo* evaluation. The *in vivo* data available are either therapeutic or diagnostic but not in combination of both. In fact, it is until recently that only a handful of investigations have revealed some *in vivo* facts of real theranostic nanomedicine which are summarized in **Table 2**. The advanced nanotheranostic thus becomes an approach of future generation; with the variety of features in nanomedicine includes stimulus-responsive drug release (e.g., pH, temperature, magnetism, and ultrasound), synergistic performance (e.g., siRNA delivery, combination therapy), multi-modal approach and quality performances (e.g., oral delivery, autophagy inhibition etc). Further, research efforts are needed to explore these concepts on available clinical platform of nanomedicines, towards the development of versatile and smart theranostic applications [134-136]. Quantum dots, gold nanoparticles and iron oxide nanoparticles loaded theranostic nanomedicines could be potential carrier to address some of these issues in near future. The iron oxide nanoparticles show excellent biosafety as they degrade and metabolize into the serum Fe pool to form hemoglobin or enter into metabolic pathway [137]. However, use of heavy metal

based quantum dots as theranostic probes for human use is a major concern at present. It is a challenge to study the *in vivo* biodistribution and toxicology of quantum dots in animal systems that could potentially mimic its toxicity in human use. In future, fabrication of biocompatible, non-immunogenic, ultra-small size (<5.0 nm) quantum dots for nanomedicine loading that would be excreted through a renal clearance mechanism is highly awaited [21, 138, 139]. Carbon nanotubes exert potential to cause toxicities *in vivo* and *in vivo*. They produce oxidative stress (free radical formation) by causing lipid peroxidation which leads to inflammation and cell damage in major organs such as lungs and liver [140-144]. Also, oxidative stress induced cytotoxicity was reported for gold nanoparticles [145] but this cytotoxicity appears to be a common effect amongst other nanoparticles [146-151]. Therefore, theranostic carbon nanotubes and gold nanoparticles have raised a concern of safety for clinical use. Clearly, there are many options available for a nanotheranostic approach towards killing cancer cells but other non-cytotoxic nanoparticulate effects like induction of endothelial leakiness and crippling of cell migration during wound healing should not be neglected [152, 153]. Finally, multi-modal theranostic nanomedicines (*i.e.*, combination of multi diagnostics and drugs) could be advantageous for theranostic purposes. Theranostic approach using nanomedicine (*i.e.*, nanotheranostics) which target molecular biomarkers with advanced designs is likely to contribute to increased precision for cancer therapy.

Table 2. *In vivo* efficacy analysis of theranostic nanomedicines.

Type of theranostic nanomedicine	Targeting/Therapeutic/Diagnostic agent	Site of administration	Duration of diagnosis	Duration of therapy	Fold of efficacy enhancement	Reference
Drug-polymer conjugates	RGD/64Cu	i.v.	3 h	3 h	~ 1 fold in tumor	[39]
Polymeric nanoparticles	Passive/Quantum dots/Iron oxide nanoparticles	i.v.	6 h	--	~ 1.5 folds in tumor	[18]
Magnetic nanoparticles	Cy 5.5/siRNA/ Iron oxide nanoparticles	i.v.	48 h	48 h	<i>In vivo</i> silencing in tumor was observed	[60]
Solid lipid nanoparticles	RGD/Lead selenide	i.v.	120 h	--	~ 1 fold in tumor vasculature	[66]
Dendrimers	LHRH/ Phthalocyanines	i.v.	10 h	24 h	Significant fluorescent was observed in tumor with cytotoxicity	[75]
Liposomes	Passive/Camptothecin/Irinotecan/Cholesterol	Intratumoral	24 h	24 h	~ 6 folds longer duration of detection/more drug concentration at tumor site	[90]
Micelles	Passive/Iron oxide nanoparticles	i.v.	24 h	24 h	~ 1fold T2 value decreases with significant cell death	[108]
Carbon nanomaterials	Folic acid/MWCNTs/Technitium-99m	i.v.	24 h	1-15 days (2 doses per week)	~ 8.5 folds higher than non-targeted MWCNTs after 24 h of diagnosis with at least ~ 2 folds higher tumor inhibition	[132]

Abbreviations

MDR, multi drug resistance; MRI, magnetic resonance imaging; PEG, polyethylene glycol; TPGS, D- α -tocopheryl polyethylene glycol 1000 succinate; HPMA, N-(2-hydroxypropyl) methacrylamide; DOX, doxorubicin; RGD, Arg-Gly-Asp; PET, positron emission tomography; PLGA, Poly (D,L-lactide-co-glycolide); PLA-TPGS, poly-lactic acid-D- α -tocopheryl polyethylene glycol 1000 succinate; PLGA-PEG, poly(D,L-lactide-co-glycolide)-polyethylene glycol; SCID, severe combined immunodeficiency; T2, transverse relaxation time; TPGS-COOH, acid functionalized D- α -tocopheryl polyethylene glycol 1000 succinate; cRGD, cyclic Arg-Gly-Asp; NIR, near infrared; LDL, low density lipoprotein; 3D, three-dimensional; hNIS, sodium-iodide symporter; PAMAM-G5, poly(amidoamine) dendrimers generation 5; LHRH, luteinizing hormone-releasing hormone; Pc, phthalocyanines; PPIG4, generation 4 polypropylenimine; beta-CD, beta-cyclodextrin; CPLGLAGG, Cys-Pro-Leu-Gly-Leu-Ala-Gly-Gly; CNTs, carbon nanotubes; SWCNTs, single-walled carbon nanotubes; MWCNTs, multi-walled carbon nanotubes; GO, graphene oxide; IOs, iron oxide nanoparticles; NPs, nanoparticles; AIDS, acquired immunodeficiency syndrome; i.v., intravenous; 0D, zero dimensional; 1D, one dimensional; 2D, two dimensional; PEI-PEG, poly(ethylenimine)-co-poly(ethylene glycol); MMP2, matrix metalloproteinase-2.

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Competing Interests

The authors have declared that no competing interest exists.

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Author Biography



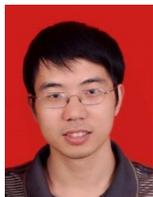
Dr Madaswamy S. Muthu earned Bachelor degree in Pharmacy, Master's in Pharmaceutical Technology from India and Ph.D. degree in Pharmaceutics from IIT, Varanasi, India in 2009. He did his

postdoctoral training in Department of Chemical Engineering at National University of Singapore as a recipient of BOYSCAST Fellowship and CREST Award from India. Muthu's research interest is to develop nanomedicine as multi-functional platform for diagnosis and therapy. He has authored over 35 peer-reviewed publications with a cumulative impact factor of >110 and h-Index of 12.



Dr David Tai Leong's research focuses on understanding nanomaterials interactions with biological systems, translating this understanding to useful biomaterials and using bio-derived materials in interesting

non-biological applications. His work has been published in top journals like Nature Communications, Nano Letters, NPG Asia Materials and Biomaterials. He graduated from National University of Singapore with a Bachelor of Chemical Engineering and a PhD in Biology. He did his postdoctoral training at the Howard Hughes Medical Institute at University of Pennsylvania.



Dr Lin Mei is an Associate Professor at Tsinghua University Shenzhen Graduate School in biomaterials, drug delivery and nanomedicine. He got his bachelor's degree from Fudan University, and PhD from Peking Union Medical College, Tsinghua University. He has co-authored over 40 SCI articles that resulted in 15 citations per article and h-Index 13.



Dr Si-Shen Feng is a Professor in biomaterials and nanomedicine. He got his 6-year diploma from Peking University, MEng from Tsinghua University and PhD from Columbia University.

He has co-authored over 140 WOS articles that resulted in 35 citations per article and h-Index 39. Currently he is an Associate Editor of *Biomaterials* (2012 JIF=7.604) and *Nanomedicine* (2012 JIF=5.260). His research interest includes 1) Molecular biomaterials, 2) nanomedicine for drug targeting. 3) nanomedicine for multimodality cancer therapy, 4) si-RNA based nanomedicine; 6) nanoimmunotherapy

and 7) nanomedicine for treatment of cancer stem cells etc.