

## Review

# Tailoring noble metal nanoparticle designs to enable sensitive lateral flow immunoassay

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## Abstract

Lateral flow immunoassay (LFIA) with gold nanoparticles (AuNPs) as signal reporters is a popular point-of-care diagnostic technique. However, given the weak absorbance of traditional 20–40 nm spherical AuNPs, their sensitivity is low, which greatly limits the wide application of AuNP-based LFIA. With the rapid advances in materials science and nanotechnology, the synthesis of noble metal nanoparticles (NMNPs) has enhanced physicochemical properties such as optical, plasmonic, catalytic, and multifunctional activity by simply engineering their physical parameters, including the size, shape, composition, and external structure. Using these engineered NMNPs as an alternative to traditional AuNPs, the sensitivity of LFIA has been significantly improved, thereby greatly expanding the working range and application scenarios of LFIA, particularly in trace analysis. Therefore, in this review, we will focus on the design of engineered NMNPs and their demonstration in improving LFIA. We highlight the strategies available for tailoring NMNP designs, the effect of NMNP engineering on their performance, and the working principle of each engineering design for enhancing LFIA. Finally, current challenges and future improvements in this field are briefly discussed.

Key words: lateral flow immunoassay; noble metal nanoparticles; nanoparticle design; engineering

## 1. Introduction

Lateral flow immunoassay (LFIA) is a popular point-of-care testing technique because it meets the ASSURED criteria of the WHO [1]. It provides a wide range of applications in food safety, environmental monitoring, and clinical diagnosis [2, 3]. For example, LFIA has played a crucial role in the response and management of coronavirus disease 2019 [4], particularly in resource-limited areas with low access to the real-time reverse transcriptase quantitative polymerase chain reaction testing [5]. In a typical LFIA test, effective detection of the analyte depends on the specific immunological recognition of analytes and detection-antibody-conjugated nanoparticle labels and the accumulation of nanoparticle labels at

the test and control zones by the capillary force, thereby achieving effective signal transduction [6]. In sandwich LFIA testing, the label capture is positively related to the analyte concentration; as a result, the higher the concentration of the analyte, the stronger the signal on the test line. On the contrary, for competitive LFIA testing, the signal strength of the nanoparticle label is negatively correlated with the analyte concentration. Over the past few decades, spherical gold nanoparticles (AuNPs) have become a major component of nanoparticle labels in LFIA because of their visual readout without any instruments, good colloidal stability, and easy functionalization [7]. However, traditional LFIA,

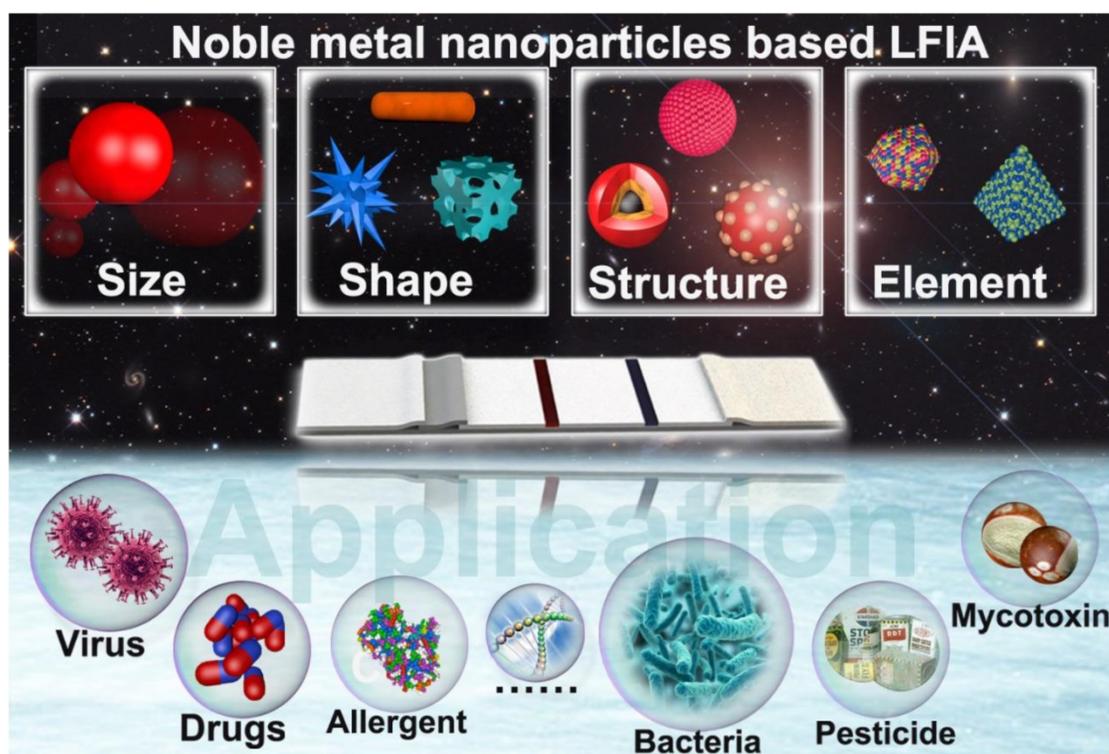
which uses 20–40 nm AuNPs as signal labels, has suboptimal sensitivity compared with other immunoassay methods, thereby greatly limiting its wide applications in the detection of trace analytes. Therefore, developing strategies to improve the sensitivity and extend the application range of the LFIA is necessary [8].

In recent years, a myriad of approaches has been enabled to enhance the LFIA sensitivity. These strategies primarily involve the introduction of sample treatments to preconcentrate the analyte, the screening of high-affinity recognition elements [9], the development of novel nanoparticle labels and signal transduction techniques with increased sensitivity [8], and the combination of various signal amplification methods [6]. With these improvements, the detection performance of LFIA in sensitivity has been significantly enhanced. Recently, several pivotal review papers have discussed the progress and achievements in reducing the limit of detection (LOD) and improving the sensitivity of LFIA. Nevertheless, these improvements could result in increased cost and complexity and compromised portability, which is contrary to the main technical strength of LFIA. Consequently, traditional colorimetric signal transduction with AuNPs as labels still dominates the LFIA because of its superiorities over other alternative labels and signal readout patterns.

As mentioned earlier, the generation of detectable colorimetric signals relies on the adequate accumulation of AuNP labels in the detected region. Therefore, the low sensitivity of traditional colorimetric LFIA can be effectively solved by enhancing the signal strength of the label [6]. Noble metal nanoparticles (NMNPs), including AuNPs, are a new functional nanomaterial, which have received considerable attention in the field of bioanalysis because of their unique physical and chemical properties, including optical [10, 11], plasmonic [12], and catalytic activities [13]. NMNPs not only serve as traditional colorimetric labels, but also achieve other signal transduction principles and functions, such as surface-enhanced Raman scattering (SERS) [14], fluorescence [15–19], and enzyme mimicking [20, 21], thereby contributing to highly sensitive detection in LFIA [22–25]. Furthermore, the great success in large-scale synthesis of high-quality NMNPs has promoted their applications for the revolution of LFIA technologies. In particular, the physicochemical properties of NMNPs are reported to be closely associated with their size, shape, elemental composition, external structure, interparticle distance, and dielectric constant, thereby allowing us to tailor

the properties of NMNPs through controlling these physical parameters [20, 26, 27]. For example, localized surface plasmon resonance (LSPR), a representative optical feature of NMNPs, can be selectively tuned by simply engineering the nanoparticle size [28], shape [29], composition [30], and construction [31]. In general, the LSPR absorption of NMNPs gradually increases with the increase of nanoparticle size, thereby enabling more sensitive colorimetric signal output when larger-sized NMNPs are used as LFIA labels [32, 33]. Moreover, compared with spherical nanoparticles of similar size, anisotropic NMNPs with more complex structures display stronger optical signal sensitivity, which is favorable for enhanced detection sensitivity in LFIA [34, 35]. The enzyme-mimicking activities of NMNPs (*e.g.*, AuNPs or AgNPs) can be significantly enhanced by incorporating with platinum-group metals, which can endow them excellent peroxidase-like activities for amplifying the colorimetric signal intensity generated from the label by additional enzymatic deposition step, thereby improving LFIA sensitivity [36]. In addition, NMNPs can be equipped with new functions by compositing other functional materials, thereby facilitating their multifunctional uses in LFIA [37–39]. Collectively, manipulating the properties of NMNPs by controlling one of the parameters or a combination of them is an effective strategy to achieve the best performance of NMNPs in LFIA.

With this design concept in mind, numerous excellent studies on the fine tuning of the physical parameters of NMNPs and their uses in enhancing the performance of LFIA have been reported [40–42]. The past few decades have witnessed great progress and achievements in tailoring NMNP designs to improve LFIA. Although several publications have been conducted on the principles, labels, sensitivities, multiplexing abilities, and applications of LFIA [43–48], to our knowledge, no systematic and comprehensive review has been conducted on the design of engineered NMNPs and their role in enhancing the LFIA performance. Herein, in this contribution, we focus on exploiting NMNPs by engineering their physical parameters, including size, shape, composition, and external structures, to improve LFIA (**Scheme 1**). We highlight the available strategies to tailor the NMNP designs, the impacts of NMNP engineering on their properties, and the underlying enhancement mechanisms of each nanoparticle engineering design in LFIA applications. This review will conclude with a discussion of existing challenges and further improvements.



**Scheme 1.** Schematic illustration of engineered noble-metal nanoparticles and their application in LFIA.

## 2. Nanoparticle size

The optical properties of NMNPs are closely related to their sizes. The relationship between them has been extensively studied [49]. In general, large NMNPs have strong optical signal transduction relative to small ones because the molar extinction coefficients of NMNPs increase with the increase of the nanoparticle size [50, 51]. For instance, 80 nm AuNPs show about two orders of magnitude increase in the molar extinction coefficient compared with 15 nm AuNPs [52]. Therefore, large NMNPs with high optical intensity contribute to the sensitivity of LFIA theoretically. However, some studies have indicated that the use of oversized nanoparticles as LFIA labels can reduce the sensitivity [33, 53]. Thus, investigating the role of the size of NMNPs on their performance in LFIA is of great significance. The nanoparticle size not only affects the signal transduction but also impacts the interaction behavior of the nanoparticles with biomolecules or other components involved in LFIA. In addition, metal *in situ* growth (MISG), as a commonly used signal amplification strategy, has been widely proposed to enhance the sensitivity of AuNP-LFIA by increasing the size of AuNP and the optical signal strength [54, 55]. In this content, gold [56–58], silver [59, 60], and copper [61, 62] growth strategies are currently the potential approaches for

amplifying the optical signal intensity of AuNPs by reducing metal ions into metallic elements to deposit on the surface of AuNPs, followed by a significant increase in the nanoparticle size. With these engineering designs of nanoparticle size, the optical signal transduction of nanoparticle labels is remarkably enhanced, thereby improving the LFIA sensitivity and attracting enormous interests for applications in bioanalysis, particularly in trace analysis. Herein, we will focus on the currently available strategies to precisely control the size of NMNPs and the latest advancement of applying size-dependent nanoparticle reporters to enhance the LFIA performance (**Table 1**). Moreover, the MISG-based signal amplification technologies and their uses in enhancing the LFIA sensitivity are discussed (**Table 2**).

**Table 1.** A summary of some representative LFIAs by size-controlled noble metal nanoparticles.

Size range of AuNPs	Optimal size	Analyte	LOD	Ref.
20–39 nm	39 nm	Progesterone	No given	[85]
40–150 nm	80 nm	DNA	50 fmol	[177]
10–40 nm	20 nm	Prostate acid phosphatase	0.25 ng mL <sup>-1</sup>	[84]
6.4–52 nm	33.4 nm	Potato virus X	3 ng mL <sup>-1</sup>	[86]
14–38 nm	38 nm	Hepatitis B surface antigen	No given	[178]
34–137.8 nm	42.7 nm	Hepatitis B surface antigen	10 ng mL <sup>-1</sup>	[179]
20–180 nm	100 nm	Ochratoxin A	0.27 ng mL <sup>-1</sup> (IC <sub>50</sub> )	[53]
30–100 nm	100 nm	C-reactive Protein	1.6 pM	[33]
16–115 nm	115 nm	Cardiac troponin I	0.03 ng mL <sup>-1</sup>	[32]

**Table 2.** A summary of some representative LFIA based on the metal *in-situ* growth strategy.

Noble metal growth	Analyte	Dynamic range	LOD	Ref.
Gold growth	Atrazine	No given	1 ng mL <sup>-1</sup>	[54]
	HCG	No given	0.3 mIU mL <sup>-1</sup>	[55]
	DNA of <i>E. coli</i> O157:H7	0.39-3.13 nM	0.4 nM	[56]
	<i>E. coli</i> O157:H7	5×10 <sup>3</sup> -1.6×10 <sup>8</sup> CFU mL <sup>-1</sup>	5×10 <sup>3</sup> CFU mL <sup>-1</sup>	[87]
	<i>S. enteritidis</i>	10 <sup>3</sup> -10 <sup>8</sup> CFU mL <sup>-1</sup>	10 <sup>4</sup> CFU mL <sup>-1</sup>	[58]
	<i>E. coli</i> O157:H7	1.25×10 <sup>2</sup> -2.5×10 <sup>8</sup> CFU mL <sup>-1</sup>	12.5 CFU mL <sup>-1</sup>	[57]
Silver growth	Cardiac troponin I	No given	0.016 ng mL <sup>-1</sup>	[59]
	Abrin-a	0.1-100 ng mL <sup>-1</sup>	0.1 ng mL <sup>-1</sup>	[60]
	H5N5	0.5-250 ng mL <sup>-1</sup>	0.5 ng mL <sup>-1</sup>	[88]
	Avian influenza virus	2 <sup>-2</sup> -2 <sup>-9</sup> dilution	2 <sup>-12</sup> dilution	[89]
	Newcastle disease virus	No given	2 <sup>-10</sup> dilution	
	Fumonisin B <sub>1</sub>	No given	2 ng mL <sup>-1</sup>	[91]
	<i>Ralstonia solanacearum</i>	2×10 <sup>3</sup> -2×10 <sup>6</sup> CFU mL <sup>-1</sup>	2×10 <sup>2</sup> CFU mL <sup>-1</sup>	[92]
	Prostate specific antigen	No given	0.1 ng mL <sup>-1</sup>	[93]
	Potato leafroll virus	No given	0.2 ng mL <sup>-1</sup>	[94]
	Troponin I	No given	0.24 ng mL <sup>-1</sup>	[95]
	Copper growth	HCG	1 pg mL <sup>-1</sup> -100 ng mL <sup>-1</sup>	1 pg mL <sup>-1</sup>
p24 antigen		50 fg mL <sup>-1</sup> -1 ng mL <sup>-1</sup>	50 fg mL <sup>-1</sup>	[62]
<i>E. coli</i> O157:H7		No given	6 CFU mL <sup>-1</sup>	

## 2.1. Strategies for nanoparticle size regulation

The synthesis of NMNPs with a variety of sizes can be achieved in the solid or liquid state by using two classical approaches, namely, “top-down” and “bottom-up” (Figure 1A) [20, 63]. The top-down method begins with a macroscopic bulk metal material entity and achieves structural dimensions in the nanoscale by using the physical and lithographic technologies, such as micropatterning [64], mechanical grinding [65], pyrolysis [66], mechanical alloying [67], and laser ablation [68, 69]. However, obtaining high-quality NMNPs with controlled size and nanocrystal using these technologies is difficult. By contrast, the bottom-up approach usually uses ionic, atomic, or molecular units to assemble and form the nano-sized structures through diverse processes [70]. From the generation of the components to their growth and assembly into nanoentities, the bottom-up method is primarily regulated on the basis of the chemical synthesis mechanism [71]. Compared with the top-down method, the bottom-up approach provides more possibilities for the design and synthesis of nanoparticles with desired size and morphology. Moreover, this method allows the investigation of the structural formation dynamics and structure–property relationship at the atomic or molecular level [72]. To date, the currently available bottom-up methods involve the Turkevich, Brust–Schiffrin, microemulsion, electrochemical, photochemical, microwave, green synthesis, and biosynthesis methods [73]. Although these methods have gained huge success in synthesizing various size-tunable NMNPs, the size range of NMNPs larger than 100 nm via such methods remains a challenge. The seed-mediated growth method based on the nucleation and growth processes has attracted great interest and has become the potential and versatile

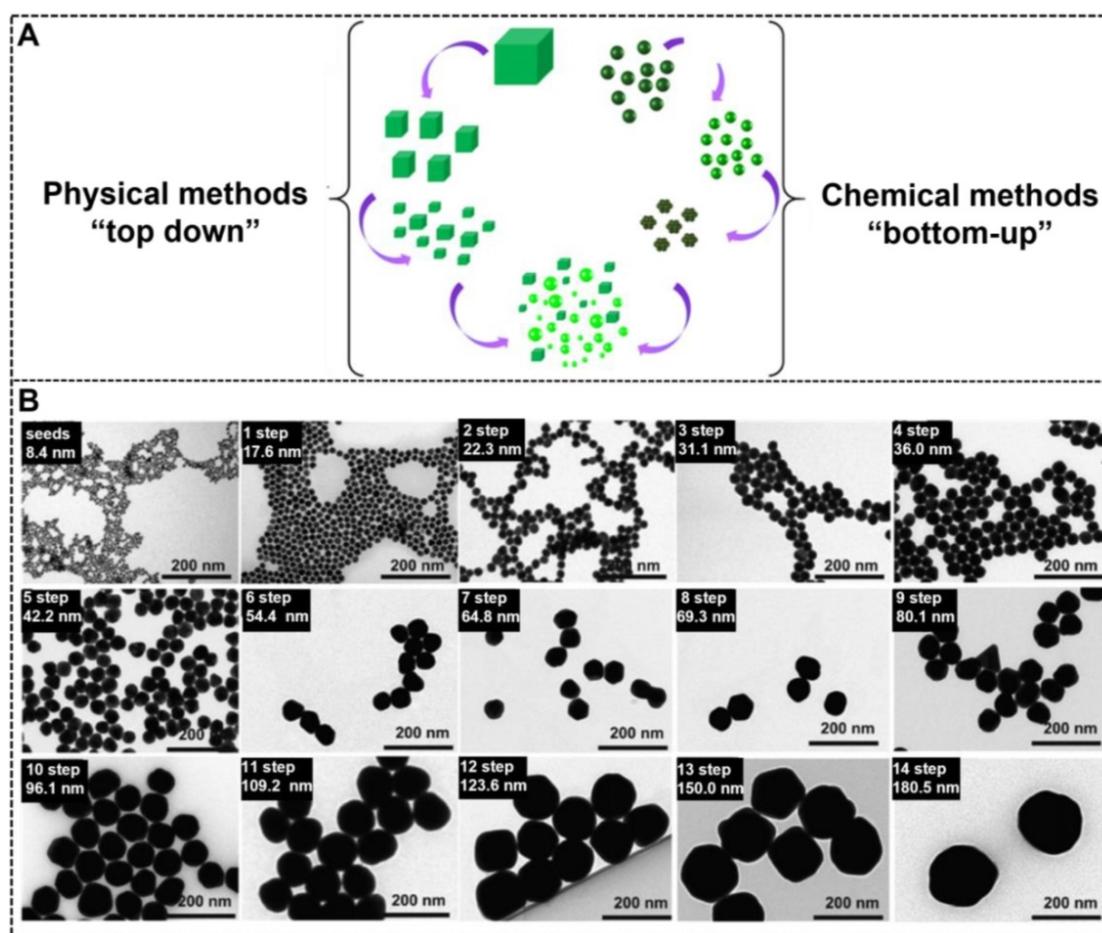
method to control the size of NMNPs [74, 75]. In general, the classic seed-mediated growth process involves two steps: the synthesis of seed nanoparticles and their subsequent growth in a growth solution consisting of metal precursors, reducing agents, and structure-directing agents (SDA). Unlike the above-mentioned methods, the seed-mediated growth method exhibits more advantages because it can allow the structural design by the selection of seed nanoparticles and the manipulation of crystal growth conditions. In this case, the seed crystals are step-wise enlarged by adding the metal atoms; thus, the size of nanoparticles can be readily controlled by varying the synthetic conditions, including the seeds, physical parameters (e.g., pH and temperature), metal precursors, reducing agents, or additives and impurities [76-78]. Taking the synthesis of AuNPs as an example, Natan et al. pioneered the seed-mediated growth method to prepare AuNPs of up to 100 nm with improved monodispersity [79]. Subsequently, Murphy et al. and Liz-Marzán et al. further improved the seed-mediated growth process to ensure the controlled synthesis of nanoparticles [70]. Inspired by these works, a series of kinetically controlled seed-mediated growth strategies was recently reported for synthesizing monodisperse AuNPs with sizes of more than 100 nm by adjusting the reaction conditions. Using this principle, Bastús et al. reported the synthesis of monodisperse citrate-stabilized quasi-spherical AuNPs with the size of up to ~200 nm by regulating the synthetic conditions, including the gold precursor to seed nanoparticle concentration, reaction temperature, pH value, and reducing agents, to enable the dynamic control of growth processes [78]. Figure 1B shows that the size of AuNPs increases with the increase of the growth step number, and AuNPs of up to ~180.5 ± 10.7 nm in size with a narrow distribution are synthesized after the 14-step growth.

Similarly, Xia's group explored a controlled synthesis system for controllable preparation of spherical AuNPs with a size range of 5-150 nm and silver nanocubes with a size range of 30-200 nm by using a successive, seed-mediated growth strategy [76-77].

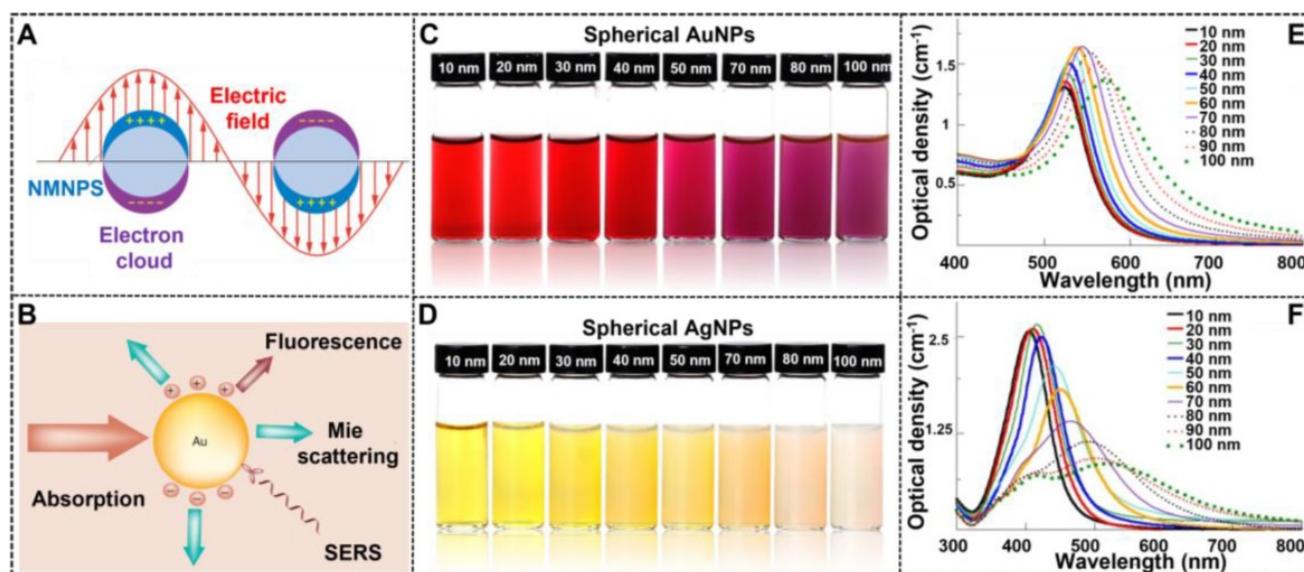
## 2.2. Effect of nanoparticle size on optical properties

NMNPs have obtained a wide range of applications in various fields because of their unique optical properties, which primarily derive from the LSPR. As shown in **Figure 2A**, LSPR is the coherent oscillation of the free electron away from the equilibrium position when NMNPs are excited by the incident light [80]. As a result of the LSPR phenomenon, NMNPs can absorb and/or scatter light at specific wavelengths (**Figure 2B**) [81], thereby giving their solution a certain color. In addition, the LSPR peak position of NMNPs and their solution color can be easily tuned over a wide range of wavelengths and colors through manipulating the size of NMNPs. Using the theoretical calculations and experimental observations, a large number of studies

have demonstrated the enhanced optical features of NMNPs with the increase of the size of nanoparticles [49, 52], such as the finely tunable extinction spectra from the ultraviolet regions to the visible regions and even to the near-infrared regions, and the increased extinction cross-section with the molar extinction coefficient ranging from  $10^8$  to  $10^{11}$   $M^{-1} cm^{-1}$  [82]. For example, the spherical AuNPs with sizes of 30 nm exhibit the maximal LSPR peak at  $\sim 525$  nm, thereby giving their solution a typical wine-red color. When the size of spherical AuNPs increases up to 100 nm, the maximal LSPR peak is red-shifted to  $\sim 560$  nm with a brick-red color (**Figures 2C and E**) [104]. In addition, spherical AgNPs also display size-dependent variations in the LSPR and color. For example, when the size of silver nanospheres is 50 nm, their major LSPR peak is located at  $\sim 420$  nm with a distinctive yellow color solution, whereas the LSPR and color of spherical AgNPs will shift to  $\sim 485$  nm with a characteristic Khaki grey color solution as the size of nanospheres increases up to 100 nm (**Figures 2D and F**) [104]. The unique superiority of NMNPs with size-dependent variations in the optical properties



**Figure 1.** (A) Schematic illustration of synthesizing metal nanoparticles with different sizes by physical and chemical methods. Adapted with permission from [20]. Copyright 2019 Springer Nature. (B) Transmission electron microscopy images of AuNPs with the size increases from  $8.4 \pm 1.0$  to  $180.5 \pm 10.7$  nm obtained by seeded growth. Adapted with permission from [78]. Copyright 2011 American Chemical Society.



**Figure 2.** (A) Depiction of LSPR of spherical NMNPs. Adapted with permission from [80]. Copyright 2009 Annual Reviews. (B) Important optical performance caused by the interaction of light with AuNPs, including light absorption, Mie scattering, surface-enhanced luminescence and surface-enhanced Raman scattering from absorbed molecules. Adapted with permission from [81]. Copyright 2007 Future Medicine Ltd ISSN. The photographs of AuNPs (C) and AgNPs (D). UV-vis spectra of AuNPs (E) and AgNPs (F). Adapted with permission from [104]. Copyright Fortis Life Sciences Company.

allows the customized design and preparation of various high-performance colorimetric signal probes based on the requirements for various applications. Furthermore, these properties provide the potential opportunities for elucidating the relationship between the nanoparticle size and its performances in LFIA.

Noble metal nanoclusters (NMNCs) are the transition between single metal atoms and metal nanoparticles. When the size of metal nanoparticles is down to below 2 nm, consisting of several to dozens of atoms, they exhibit unique photoluminescent properties, thus providing great potential as fluorescence labels for applications in diverse fields [23]. However, compared with quantum dots and organic fluorophores, NMNCs show obvious drawbacks for low quantum yield, thus limiting its application in high-sensitivity detection. In recent years, attempts have been devoted to exploring strategies for improving the NMNC brightness. Many promising approaches, such as the modification of fluorescence behaviors (*e.g.*, aggregation induced emission or confined fluorescence enhancement), the optimization of synthesis process (*e.g.*, microwave assisted-homogeneous heating), and the improvement of environmental conditions (*e.g.*, temperature, pressure, and pH), have been developed for preparing highly luminescent nanoclusters. By virtue of these improvements, the synthesis of highly fluorescent NMNCs with the advantages over other fluorescent materials has been successfully achieved.

### 2.3. Size engineering in LFIA

The size of nanoparticles is an important factor

to determine their performance in LFIA. Large nanoparticles usually possess stronger optical signal intensities than the small ones, thereby contributing to the improvement of the sensitivity of traditional LFIA theoretically. Therefore, we will describe the latest advancement in size engineering of nanoparticles and their applications in improving LFIA sensitivity.

#### Size effect

The size of nanoparticles plays a decisive role in fabricating high-performance LFIA because the size affects not only signal transduction, but also immunoreaction efficiency between the nanoparticle probe and other components in LFIA. Thanks to the large advances in the synthesis of highly luminescent nanoclusters, NMNCs have been proposed as promising fluorescent labels for improving the LFIA. Jiang et al. first described the successful preparation of highly luminescent green emitting Au nanoclusters (AuNCs) and demonstrated their applications in improving the multiplexed LFIA detection [23]. By combining a two-line design and a portable fluorescent reader, the developed multiplex LFIA can allow the simultaneous and quantitative detection of clenbuterol and ractopamine with LODs of 0.003 and 0.023  $\mu\text{g L}^{-1}$ , respectively. Nevertheless, the application of NMNCs in LFIA is still limited. When the nanoparticle size exceeds 5 nm, noble metal nanomaterials can effectively generate colorimetric signals by absorbing or scattering incident light and produce thermal contrast signals by the photothermal effect [83]. In addition, the intensities of colorimetric or thermal signal linearly increases with the increase

of the nanoparticle size, which suggest that the use of large NMNPs as LFIA labels is suitable for highly sensitive LFIA detection. However, the excessive size of nanoparticle labels will have a negative impact on their interaction with biomolecules involved in LFIA, thereby resulting in reduced sensitivity. Therefore, illuminating the effects of the label size and signal intensity on the LFIA performance is desired. In this regard, considerable literature has studied the relationship between the nanoparticle size and LFIA sensitivity [32, 84]. For example, Laitinen et al. explored the impact of size of spherical AuNPs in the range of 20 nm to 39 nm on the sensitivity of competitive LFIA [85]. Safenkova and coworkers used five kinds of spherical AuNPs with the size ranging from 6.4 nm to 52 nm to investigate the impact of size on the sandwich LFIA platform [86]. All these studies confirm that large AuNPs could increase the LFIA sensitivity compared with small AuNPs. However, given the synthetic limitations of large AuNPs, the size range of AuNPs used in these studies is quite narrow, making it difficult to accurately describe the effect of size on LFIA sensitivity. Given the breakthrough of the synthesis of large AuNPs, our group synthesized four kinds of spherical AuNPs with sizes of 20, 60, 100, and 180 nm by a kinetically controlled seed-mediated growth strategy and then applied them as signal reporters in a competitive LFIA to explore the impact of spherical AuNP on the detection sensitivity [53]. Using ochratoxin A as a model analyte, the results revealed that spherical AuNPs with an appropriate size of 100 nm could remarkably enhance the signal transduction of LFIA to increase sensitivity because of their increased molar extinction coefficient and binding affinity to target analytes. Under the circumstance, increasing the AuNP size can improve the sensitivity of competitive LFIA. Notably, with the further increase of the AuNP size to 180 nm, the gravity of nanoparticles will dominate their move in the pores of the strip. The reduced Brownian motion of probes at the strip will increase the nonspecific binding of the probe and result in an increase in background signal, thereby reducing the LFIA sensitivity despite the exceptional molar extinction coefficient of 180 nm AuNPs. In addition, when the size of AuNPs exceeds 80 nm, light scattering of spherical AuNPs increases sharply, which disapprove the absorption-dominated signal transduction in LFIA [82]. Recently, a similar observation was reported by Zhan et al., who investigated such impacts in sandwich LFIA from the theoretical and experimental perspective [33]. Prior to experimental study, COMSOL computational modeling was developed to extend scaling analysis and predict LFIA performance. This model can be

used to understand the greater impact of the reaction and convection on AuNP capture than diffusion and to confirm the key parameters that determine the LFIA performance, including AuNP size and concentration, reaction rate constant, and flow rate. With C-reactive protein (CRP) as the model analyte, the modeling results of a sandwich LFIA for CRP are depicted in **Figure 3**, which agree well with the theoretical simulation-assisted experimental results. In their work, 100 nm AuNPs display the largest enhancement in sensitivity in comparison with conventional 30 nm AuNPs. The modeling results demonstrate that large AuNPs (i.e., 400 nm) would reduce the LFIA sensitivity and increase the background because of their settlement on the membrane and slow diffusion rate. This finding is consistent with our results. Thus, we believe that appropriate nanoparticle labeling design contributes to the LFIA performance with higher sensitivity and negligible background.

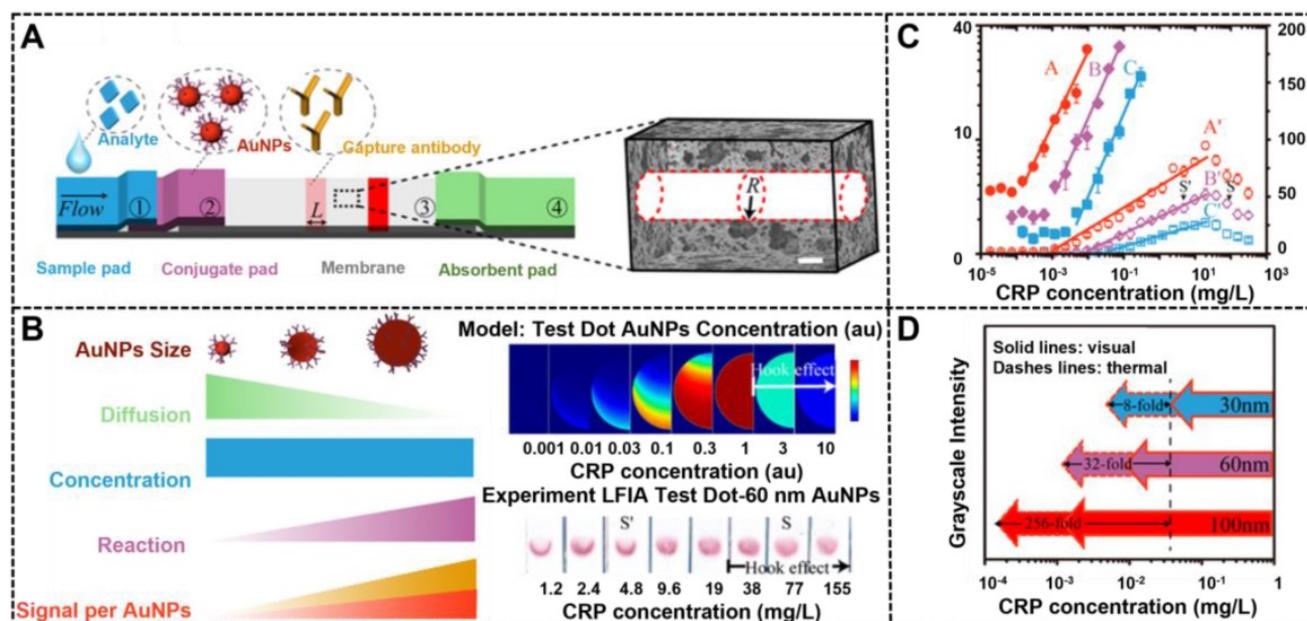
#### Growth-mediated size increase

The use of large AuNPs with enhanced signal intensity can improve the LFIA sensitivity. However, the increase in sensitivity is relatively limited by the inherent contradictions of size-dependent signal intensity and immunoreaction efficiency. Thus, signal amplification techniques are integrated with conventional AuNP-based LFIA to retain the capture and diffusion of AuNPs on the membrane. This combination does not change the travel of AuNPs on the membrane, and it maximizes their capture. MISG-mediated signal amplification technologies have obtained extensive application in LFIA because of their ultrahigh signal amplification efficiency. Metal growth intensification depends on the reduction of metal ions into metal element to deposit onto the surface of AuNPs, thereby increasing the AuNP size to enhance its colorimetric signal strength and improve the sensitivity of LFIA (**Figure 4A**). Using this amplification strategy, the LOD of LFIA can be reduced by at least one to two orders of magnitude. For example, the first success of enhancing the sensitivity of AuNP-LFIA by using gold growth was achieved by Kaur and co-workers, in which a gold enhancer solution containing  $\text{HAuCl}_4$  and  $\text{NH}_2\text{OH}\cdot\text{HCl}$  was designed and prepared for AuNP enlargement [54]. Subsequently, the gold growth enhancement for LFIA has also been demonstrated in detecting other target analytes, including proteins, nucleic acids, and microorganisms [55, 56, 87]. Compared with gold growth, silver growth exhibits stronger signal amplification capacity because of its apparent black color after the deposition of metallic Ag onto the AuNP surface, which enables

more intensive contrast against the white background of the nitrocellulose membrane [59, 60, 88, 89]. Thus, silver growth strategy has been regarded as an effective method to develop highly sensitive LFIA. Horton et al. pioneered the successful use of silver enhancement to improve LFIA detection with a 1000-fold increase in sensitivity [90]. Encouraged by this achievement, many improved LFIA methods by silver amplification have been reported for the sensitive determination of multifarious target analytes, such as proteins, pathogens, small molecules, and metal ions [91-95]. Copper growth is another common MISG signal amplification approach that could increase the sensitivity of AuNP-LFIA relative to gold or silver growth. Recently, Li et al. explored the use of a copper growth-assisted strategy to enhance AuNP-LFIA for the sensitive detection of human chorionic gonadotropin with the detection sensitivity of  $1 \text{ pg mL}^{-1}$ , which increased about two to three orders of magnitude than conventional AuNP-LFIA without signal amplification [61].

Although traditional MISG technologies have obtained a significant progress in improving LFIA detection, their wide applications are still compromised by several limitations. First, the signal amplification ability of the conventional MISG method is limited because it can only conduct one-step growth enhancement. Hence, our group first reported a two-step cascade signal amplification strategy on the conventional AuNP-LFIA platform to achieve ultrasensitive detection of *Escherichia coli* O157:H7 (Figure 4B). In this work, a cascade signal

amplification strategy consists of gold *in situ* growth and nanozyme-mediated catalytic deposition, which benefits from the ultrahigh peroxidase-mimicking activity of enlarged AuNPs after gold growth. After executing this cascade signal amplification strategy, the enhanced method can detect ultralow concentrations of *E. coli* O157:H7 with a LOD of  $1.25 \times 10^1 \text{ CFU mL}^{-1}$ , which is about 10-fold lower than that of gold growth-amplified strip [58]. Second, the traditional MISG strategy primarily relies on a layer-by-layer growth pattern in which the metal shell is deposited directly onto the AuNP surface, thereby resulting in strong background signal and low growth reproducibility caused by the strong nonspecific binding between metal ions and proteins and/or nitrocellulose membrane, self-nucleation of metal ions under excessive reducing agents, and uncontrollable metal growth. Our group has recently developed a polymer-type SDA-assisted controlled copper *in situ* growth strategy to amplify the detection signal of traditional AuNP-LFIA and minimize the background signal caused by nonspecific binding, self-nucleation, and uncontrolled growth (Figure 4C). In this design, the controllable signal amplification is achieved by using polyethyleneimine as a SDA to regulate the thermodynamics of anisotropic copper growth on the AuNP surface and restrict free nucleation and reduction of copper ions through stabilizing the chemical potential of the reduction agent and decreasing the free ion concentration. Consequently, the sensitivities of this amplification for p24 antigen and *E. coli* O157:H7 are as low as  $50 \text{ fg mL}^{-1}$  for p24



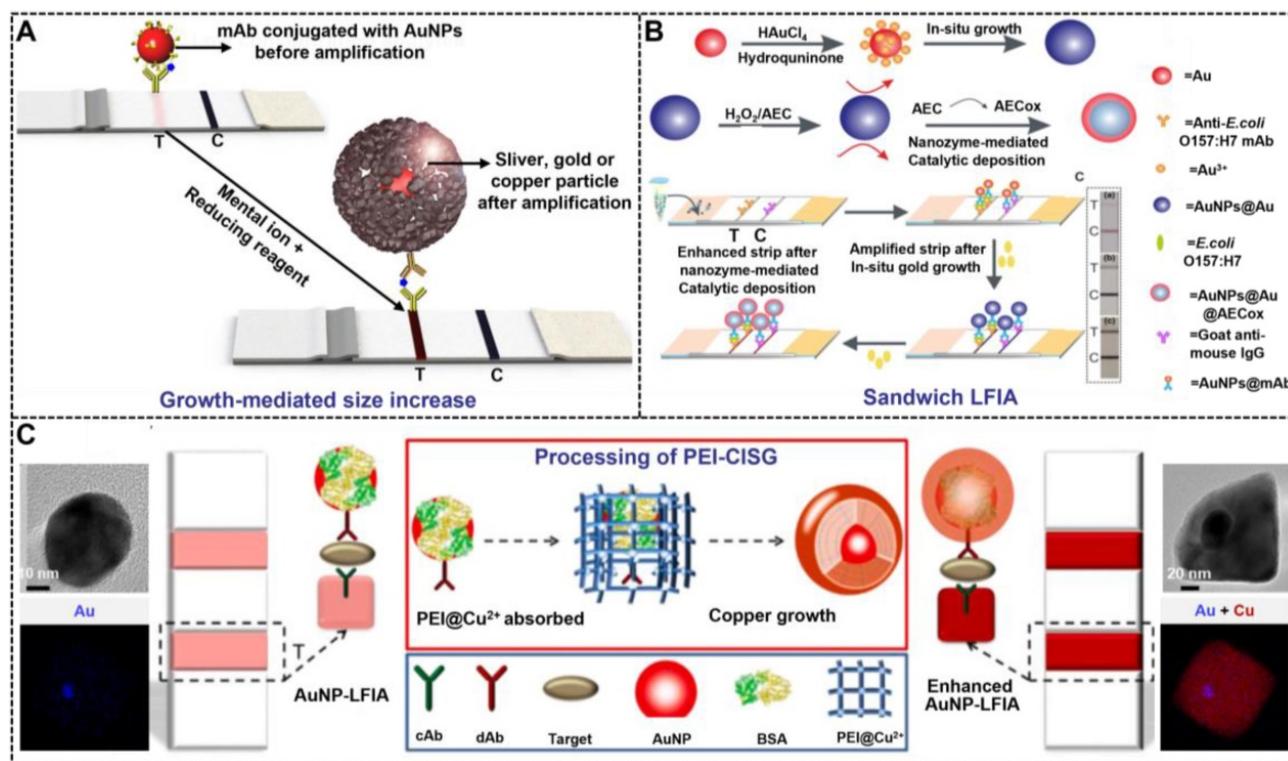
**Figure 3.** Scaling analysis of the effect of AuNPs size on LFIA. **(A)** Architecture of LFIA, the nitrocellulose membrane is conceptually simplified as bundles of cylindrical pores with radius  $R$ . **(B)** Comparison of different sized AuNPs, indicates 100 nm AuNPs can improve LFIA sensitivity due to higher reaction rate and signal per AuNPs. **(C)** COMSOL modeling result of 100 nm AuNP and experimental result of 60 nm AuNPs in the test zone of sandwich LFIA of CRP. **(D)** Experimental thermal (solid symbols) and visual (hollow symbols) signals of CRP LFIA. Adapted with permission from [33]. Copyright 2017 American Chemical Society.

antigen and 6 CFU mL<sup>-1</sup> for *E. coli* O157:H7, respectively [62]. Third, the traditional MISG strategy usually needs additional steps of washing and preparing growth solution. Increasing endeavors have been devoted to constructing various modified MISG-based LFIA strips to simplify growth and amplification. For example, a commercially available silver-enhanced LFIA test device (Figure 5), namely, Fujifilm SILVAMP TB LAM (FujiLAM), is recently developed by Fujifilm Healthcare for monitoring the presence of lipoarabinomannan in urine to assist the sensitive and accurate diagnosis of tuberculosis. Different from the conventional test strip, this modified device contains two additional buttons located at both ends, which are used to store the silver ion reagent and reducing agent. Consequently, silver growth amplification can be easily achieved by completely pushing the two buttons to release the corresponding growth solution. Compared with the AlereLAM assay for the diagnosis of tuberculosis in people with HIV as recommended by the WHO, FujiLAM displays superior diagnostic sensitivity without compromising specificity and simplicity, although an additional signal amplification step is required [96].

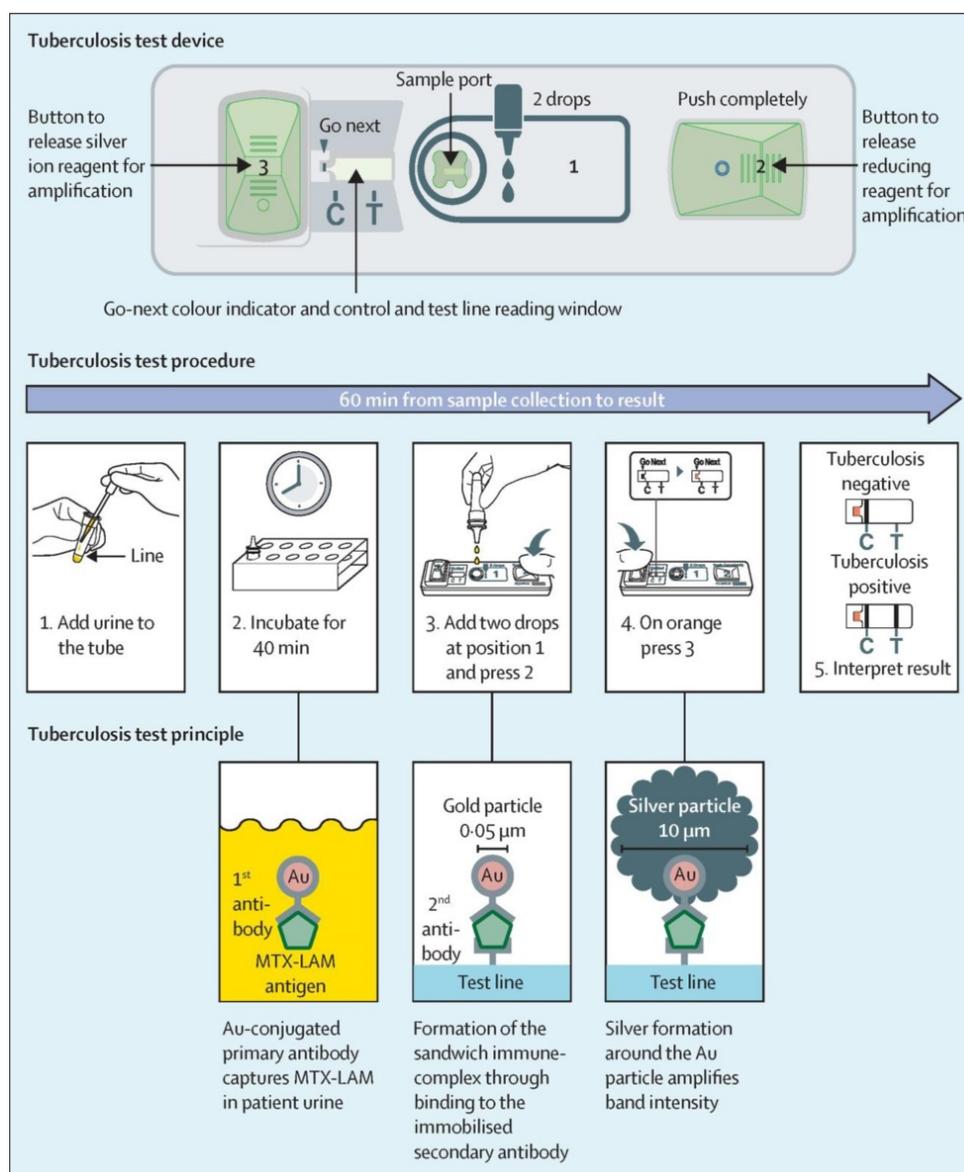
### 3. Nanoparticle shape

In addition to size, the shape of nanoparticles is

another important factor affecting their optical properties. NMNPs can be crafted into multifarious desired shapes with fascinating shape-dependent properties. In the last few decades, a myriad of strategies for the synthesis of shape-controlled NMNPs have been reported, and significant advances in this field have been obtained because of sustained contributions. To date, NMNPs are available in a wide variety of shapes (Figure 6A) [97], including zero-dimensional (0D) nanospheres; one-dimensional (1D) nanocrystals with circular, square cross-sections (e.g., nanorods and nanowires), and two-dimensional (2D) nanostructures with triangular, hexagonal, or circular projections (e.g., nanoplates, nanosheets, and nanotubes) [98, 99]. Compared with spherical nanostructures, these emerging morphologies of NMNPs allow for the fine tuning of their optical properties and functions that are difficult to obtain by simply adjusting the size of spherical nanoparticles. Therefore, the anisotropic growth of NMNPs has been considered as an effective method to modify their optical properties, thereby extending their applications in photocatalysis, optoelectronic devices, biosensing, bioimaging, and nanomedicine with tunable and luxuriant performances. Recently, investigating the influence of shape engineering in NMNPs on the LFIA performance has been enabled by advances in shape-controllable synthesis.



**Figure 4.** (A) The principle of the metal *in-situ* growth-mediated signal amplification in LFIA. (B) Schematic of the cascade signal amplification strategy based on the AuNP-LFIA platform for ultrasensitive detection of *E. coli* O157:H7 in milk. Adapted with permission from [58]. Copyright 2020 American Chemical Society. (C) Schematic illustration of the principle and process of PEI-CISG technology for enhancing AuNP-LFIA. Adapted with permission from [62]. Copyright 2021 Elsevier.



**Figure 5.** The principle, procedure, and test device of Fujifilm SILVAMP TB LAM. Adapted with permission from [96]. Copyright 2020 Elsevier.

### 3.1. Strategies for nanoparticle shape regulation

Shape control delivers great opportunities for the preparation of various novel NMNPs, thereby increasing their diversities. At present, NMNPs with different shapes are synthesized by two strategies of seed-mediated growth and heterogeneous nucleation. Among them, the seed-mediated growth has aroused wide concern because it has achieved great success in synthesizing different shapes of NMNPs [100]. In a typical seed-mediated growth, the shapes of nanoparticles are determined by three important synthetic parameters, including the crystal structures of seeds, the types of capping agents, and the nanocrystal growth kinetics. Controlling the seed crystallinity is prerequisite for high production of

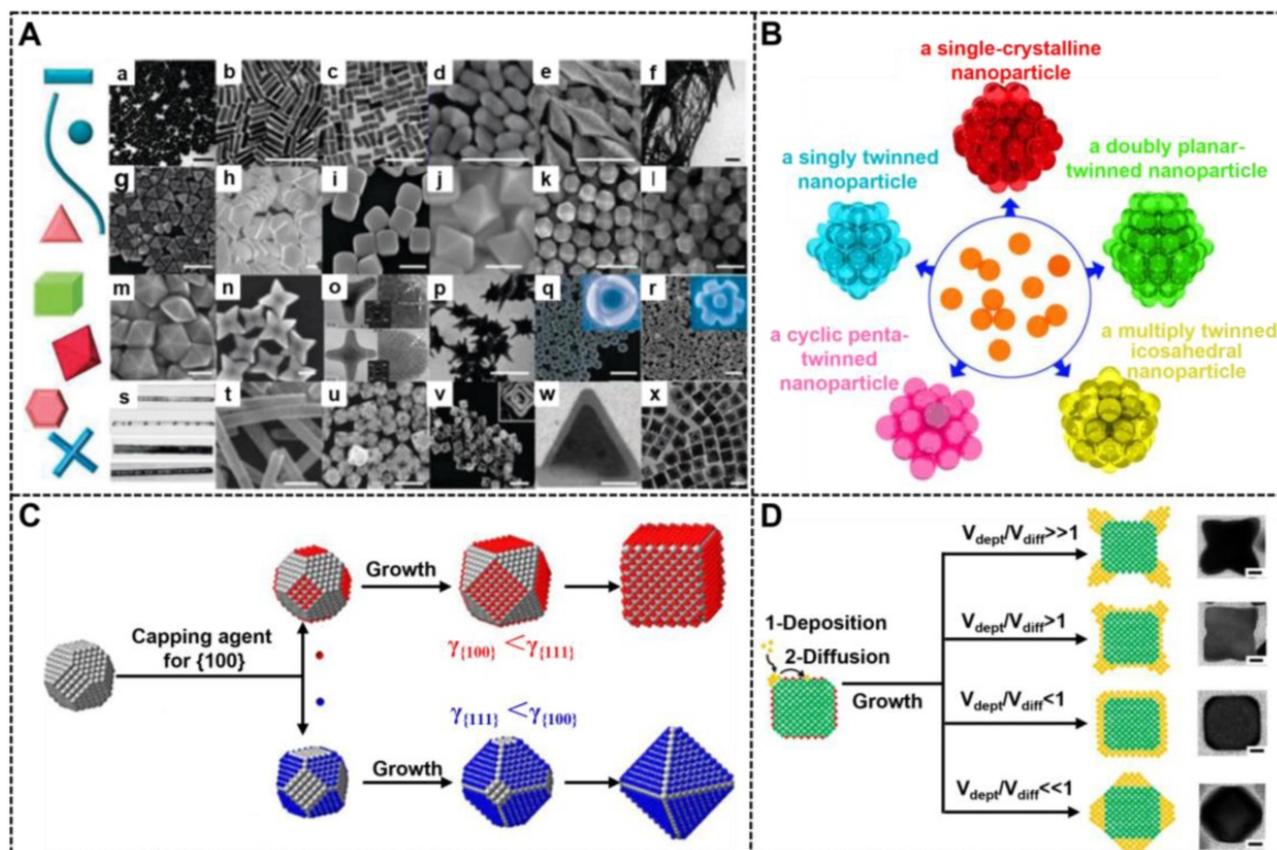
NMNPs with the desired shapes. Recently, the role of the seed shape on the structures of final nanocrystals has been systematically summarized by Xia et al [101]. **Figure 6B** illustrates the relationships between the seed crystallinity in single crystal; singly twinned, multiply twinned, and plate-like nanostructures; and nanocrystals of face-center cubic metals with different morphologies. Consequently, the recognition of the crystallinity of initial seeds can predict and direct the shapes of the resultant nanostructures. For example, single-crystal seeds can grow into cubes, octahedrons, tetrahedrons, octagonal rods, rectangular bars, and rectangular or octagonal wires; singly twinned seeds can evolve into right bipyramids and beams; multiply twinned seeds can generate icosahedrons, decahedrons, and pentagonal rods, and plate-like seeds can evolve into triangular and hexagonal

nanoplates. The internal crystal structures of NMNPs are primarily determined by the seeds, whereas their external crystal structures primarily depend on the growth rate of different seeds' facets. Facet-blocking strategy and growth kinetics control are the two effective approaches for controlling the shape of NMNPs. The facet-blocking strategy relies on the facet-specific capping agents, such as polymers, surfactants, small molecules, and ions, to selectively absorb onto a specific crystal facet of seeds to stabilize the surface atoms and reduce the surface energy ( $\gamma$ ) for lowered growth rates, thereby controlling the shapes of resultant NMNPs [102]. **Figure 6C** exhibits the role of capping agents in directing the growth of a single-crystal seed into nanocrystals with different shapes, wherein the (111) and (100) planes of a face-centered-cubic (*fcc*) crystal can be selectively blocked and passivated by the corresponding capping agents, thereby inducing seed growth along another unbound directions [103]. A detailed discussion of the role of surface capping agents in the shape-controlled synthesis of noble metal nanocrystals is recently reviewed elsewhere. Another common strategy for crystal plane control is to control the growth

dynamics of different crystal facets by varying reaction conditions, including reaction temperature, reactant species and concentrations, and reactant adding rate. Consequently, manipulating the deposition rates of atoms and surface diffusion on different planes can selectively facilitate the formation of certain facet, thereby controlling the shape development during seed growth (**Figure 6D**) [27]. Compared with the facet-blocking strategy, the kinetic control strategy is more advantageous in the preparation of unfavorable thermodynamic shapes of NMNPs.

### 3.2. Effect of nanoparticle shape on optical properties

The ability to control the optical properties of spherical NMNPs by the size of nanoparticles is limited, particularly when attempting to extend the LSPR maximum in the near infrared region. In comparison to size, the LSPR of NMNPs is sensitive to their shape variations. As mentioned earlier, the maximal LSPR peak of 50 nm silver nanospheres is located at 450 nm. When the nanospheres are remodeled with nanorods with long and short axes of



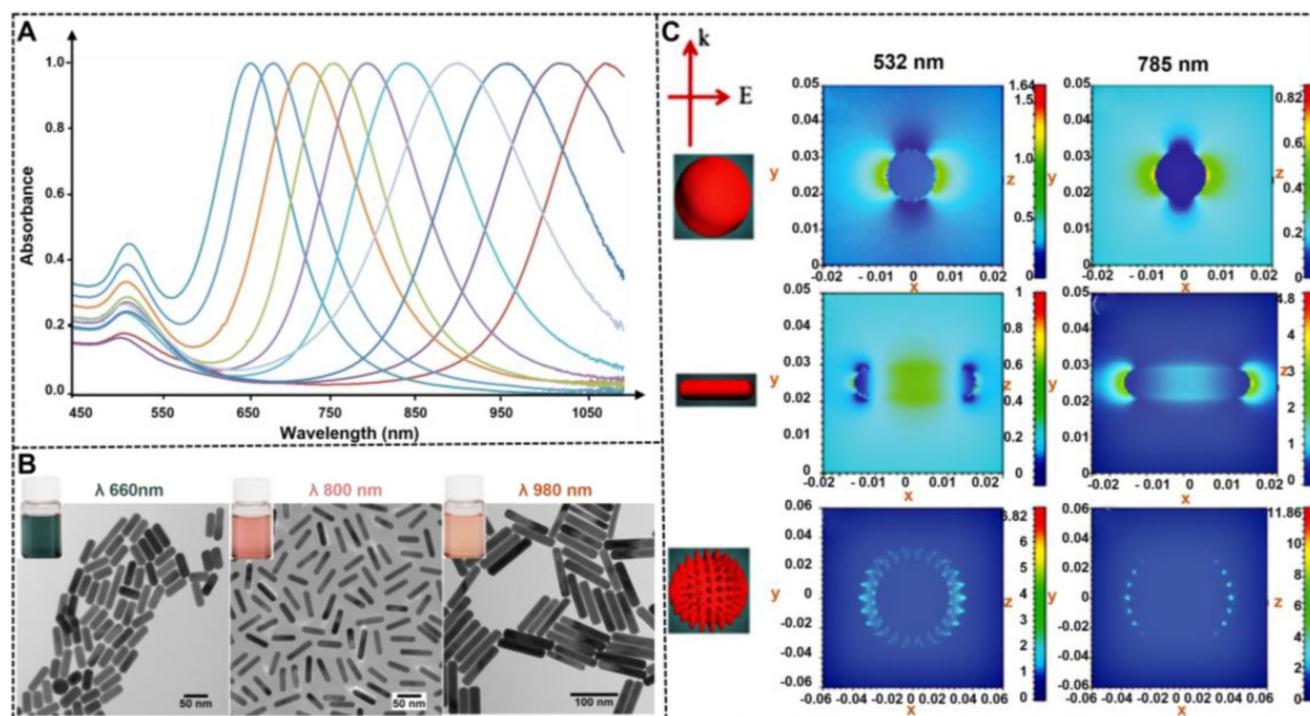
**Figure 6.** (A) Collage of scanning and transmission electron microscopy (SEM and TEM) images of NMNPs with different shapes. Adapted with permission from [97]. Copyright 2012 Elsevier. (B) Representation of NMNPs with different crystal structures. Adapted with permission from [101]. Copyright 2018 American Chemical Society. (C) Schematic illustrations showing the role of facet-specific capping agents in controlling the growth pathway of a single-crystal seed made of an *fcc* metal. Adapted with permission from [103]. Copyright 2015 American Chemical Society. (D) 2D models and TEM images (scale bars: 50 nm) showing the shape evolution of a cubic seed under four different kinetic conditions. The side faces of the cubic seed are covered by capping agents (red dots). Adapted with permission from [27]. Copyright 2013 National Academy of Sciences.

50 and 20 nm, respectively, their longitudinal LSPR peaks will be shifted to  $\sim 600$  nm. Consequently, the color of the solution changes from yellow to blue. Similar phenomena are observed when spherical AuNPs are reshaped to gold nanorods (AuNRs) with the same size. These observations indicate that the limitation to manipulate the LSPR of NMNPs by size can be easily surmounted by the nanocrystal shape as an important consideration when designing NMNPs, which is due to the fact that anisotropic NMNPs such as rods, triangular prisms, and cubes display multiple LSPRs originated from their reduced shape symmetry. A typical example is gold and silver nanorods, which exhibit tunable longitudinal and transverse LSPRs that are determined by their aspect ratios (Figures 7A–B) [104]. Moreover, reducing shape symmetry endows locations where the electric field strength is highly concentrated, namely, “hot spots” (Figure 7C) [105], thereby promoting highly sensitive detection by SERS. These unique shape-dependent optical properties of MNPNs are stimulating extensive and in-depth investigations in developing strategies to control their shape and expanding their application to a wider range. Collectively, the flexibility in controlling the NMNP shape largely increases the range of LSPR regulation, enriches the color of colloid solution, and improves

the electromagnetic field effect, thereby laying a solid foundation for their optical manipulation and sensing applications.

### 3.3. Shape engineering in LFIA

Given the diversities of shape-controlled NMNPs, numerous research groups have explored the use of various anisotropic NMNPs as LFIA reporters to improve the sensitivity. These available anisotropic NMNPs primarily involve multi-branched nanostructures (e.g., nanoflowers, nanostars, and nanopopcorns), hollow nanostructures or nanocages, nanorods, and nanourchins [106–108]. Compared with nanospheres, these nanostructures with anomalous morphologies show complex three-dimensional structures and enhanced physicochemical properties, such as good colloidal stability, high colorimetric signal intensity, strong electromagnetic field effects, and excellent photothermal conversion efficiency, thereby favoring the analytical performance of LFIA. Considering such superiorities, significant and tremendous progress in this aspect has been achieved in recent years. In future research, we will review the latest research achievements of the application of shape-controlled NMNPs in enhancing LFIA detection (Table 3).



**Figure 7.** UV-vis spectra (A) and TEM images (B) of Au nanorods with different aspect ratios. Adapted with permission from [104]. Copyright Fortis Life Sciences Company. (C) Electromagnetic field distributions and intensities for anisotropic NMNPs (e.g., nanorods and nanostars) compared to spherical NMNPs. The results indicating that the highest near field is generated at the LSPR wavelength and focused on the sharp tips of anisotropic NMNPs. Adapted with permission from [105]. Copyright 2017 the Royal Society of Chemistry.

**Table 3.** A summary of some representative LFIA by engineering the shape of noble metal nanoparticles.

Methods	Signal	Analyte	Dynamic range	LOD	Ref.
Multibranch nanostructures	Colorimetry	Aflatoxin B1	0.5-25 pg mL <sup>-1</sup>	4.17 pg mL <sup>-1</sup> (IC <sub>50</sub> )	[110]
	Colorimetry	<i>E. coli</i> O157:H7	No given	10 <sup>3</sup> CFU mL <sup>-1</sup>	[35]
	Colorimetry	OTA	No given	0.61 ng mL <sup>-1</sup> (IC <sub>50</sub> )	[111]
	Colorimetry	Influenza A	No given	67 ng mL <sup>-1</sup>	[113]
	SERS	-nucleoprotein		6.7 ng mL <sup>-1</sup>	
	Colorimetry	HCG	9-2304 mIU mL <sup>-1</sup>	9 mIU mL <sup>-1</sup>	[112]
Hollow nanostructures	Colorimetry	S-100β	0.1-100 ng mL <sup>-1</sup>	5.0 pg mL <sup>-1</sup>	[34]
	Colorimetry	Clenbuterol	No given	2 ng mL <sup>-1</sup>	[114]
	Colorimetry	IgG	0.5-50 ng mL <sup>-1</sup>	0.1 ng mL <sup>-1</sup>	[115]
Nanorods	LSPR shift	ErbB2 antigen	No given	No given	[118]
	Colorimetry	<i>E. coli</i> O157:H7	10 <sup>2</sup> -10 <sup>6</sup> CFU mL <sup>-1</sup>	100 CFU mL <sup>-1</sup>	[36]
	Colorimetry	<i>Campylobacter jejuni</i>	10 <sup>2</sup> -10 <sup>6</sup> CFU mL <sup>-1</sup>	75 CFU mL <sup>-1</sup>	[120]
	SERS	<i>Campylobacter jejuni</i>	10 <sup>2</sup> -5×10 <sup>6</sup> CFU mL <sup>-1</sup>	50 CFU mL <sup>-1</sup>	[42]
	Fluorescence	Prostate-specific antigen	3-10 ng mL <sup>-1</sup>	1.07 pg mL <sup>-1</sup>	[180]
Nanoprisms	Temperature	HCG	35-7000 mIU mL <sup>-1</sup>	2.8 mIU mL <sup>-1</sup>	[181]
	Multiplexed LFIA	Colorimetry (orange, red and green)	Dengue virus	No given	150 ng mL <sup>-1</sup>
		Yellow fever virus	No given		
		Ebola virus	No given		
Colorimetry (blue, yellow, and red)		Ovalbumin	No given	0.1 ng mL <sup>-1</sup>	[182]
		Hazelnut allergen	No given		
		Casein	No given		
Colorimetry (red, purple blue, and black)		Fumonisin B <sub>1</sub>	4-80 ng mL <sup>-1</sup>	3.27 ng mL <sup>-1</sup>	[123]
		Zearalenone	0.8-40 ng mL <sup>-1</sup>	0.70 ng mL <sup>-1</sup>	
		Ochratoxin A	0.2-2 ng mL <sup>-1</sup>	0.10 ng mL <sup>-1</sup>	
		Aflatoxin B <sub>1</sub>	0.1-1.25 ng mL <sup>-1</sup>	0.06 ng mL <sup>-1</sup>	

### Multi-branched nanostructures

Compared with spherical AuNPs with the same size, multi-branched AuNPs exhibit higher optical signal sensitivity, which benefits from their tips and core-tip interactions that can serve as an antenna to yield electromagnetic field enhancements. In addition, multi-branched AuNPs reveal better colloid stability and larger surface-to-volume ratio than those of spherical AuNPs because of their relatively rough and complex surface [34, 109]. Moreover, larger specific surface areas of multi-branched AuNPs are more favorable for improving antibody immobilization than spherical AuNPs with low dimension and ordinary shapes. Such advantages of hierarchical AuNPs make them well suitable as alternative labels of conventional spherical AuNPs with sizes of 20–40 nm to remarkably improve the detection performance of LFIA. For example, our group prepared multi-branched gold nanoflowers (AuNFs) for ultrasensitive and quantitative detection of aflatoxin B<sub>1</sub> (AFB<sub>1</sub>) in combination with the competitive LFIA method. The half maximal inhibitory of this method for AFB<sub>1</sub> at 4.17 pg mL<sup>-1</sup> was 10-fold lower than the traditional LFIA systems [110]. In the same year, Zhang et al. synthesized three hierarchical flower-like AuNPs, namely, tipped flower-like, popcorn-like, and large flower-like AuNPs, and performed a comparative study using these flower-like AuNPs labeled as probes for sandwich LFIA (**Figure 8A**) [35]. The results indicate that the tipped flower-like AuNPs exhibit the highest sensitivity of 10<sup>3</sup> CFU mL<sup>-1</sup> in testing *E. coli* O157:H7

among the three probes. Subsequently, our group further illustrated the role of the tip length and nanoparticle size in enhancing the performance of competitive and sandwich LFIA [111, 112]. In addition, the unique characteristics of multi-branched AuNPs, including multi-branches and surface roughness, result in high SERS activity, which can also increase the LFIA sensitivity. Using 4-aminothiophenol as a Raman reporter molecule and influenza A nucleoprotein as a model analyte, Maneeprakorn et al. demonstrated that the combination of SERS and LFIA could address the low sensitivity of traditional LFIA [113].

### Hollow nanostructures or nanocages

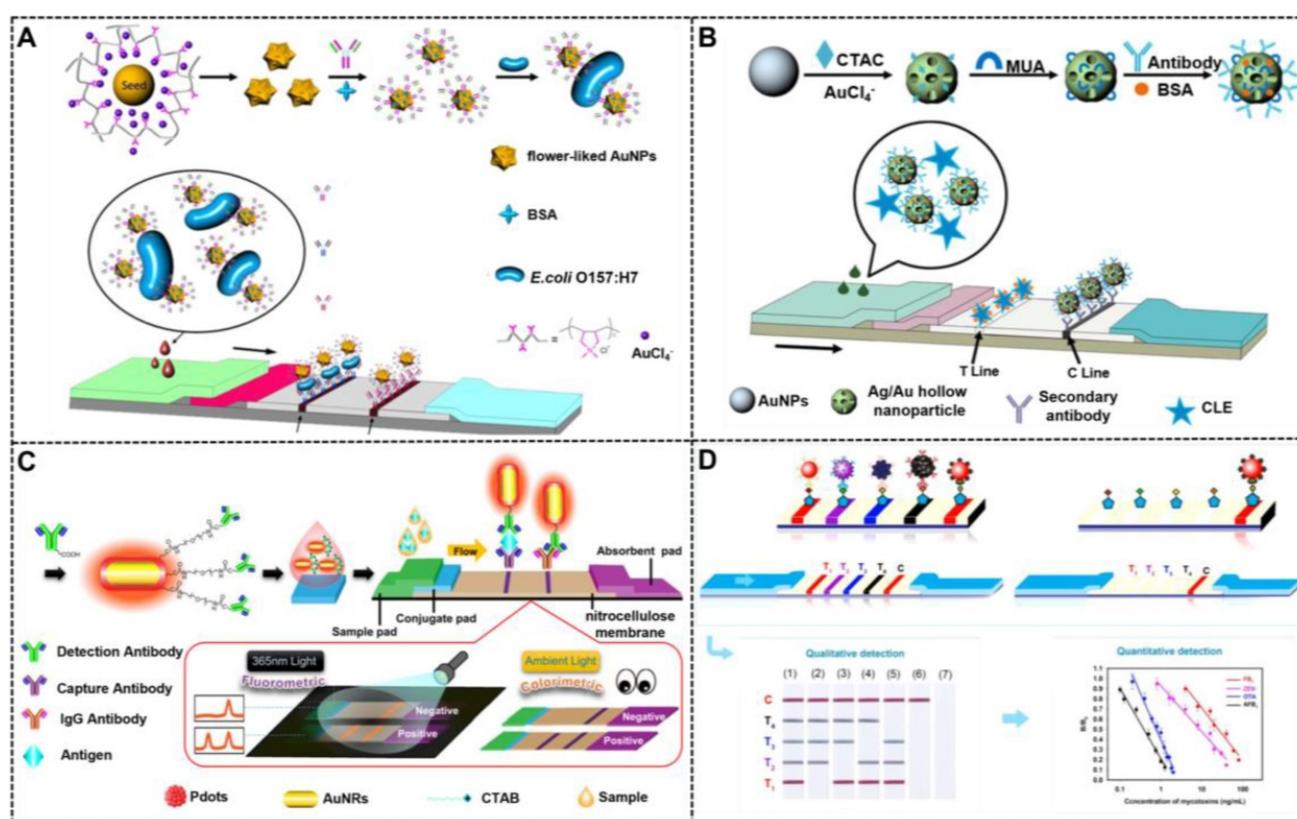
Except for flower-like nanoparticles, AuNPs with hollow structures were another glorious morphology with high specific surface area for increasing the strong surface affinity with antibodies and plasmonic activities for improving the LFIA sensitivity. Recently, Wang and co-workers optimized the synthesis of bimetallic hollow Ag/Au nanoparticles and investigated their potentials in improving the competitive detection of clenbuterol on the LFIA platform (**Figure 8B**) [114]. Under the optimal conditions, the LFIA method could detect low-concentration target with sensitivity at 2 ng mL<sup>-1</sup>, which is superior to that of the conventional LFIA strip using spherical AuNPs as labels. Gold nanocages, as an emerging gold nanomaterial, have received considerable attention because of their special structures with eight vertices and sharp corners/edges. These structural characteristics cause

them to serve as “hot spots” and be sensitive to the bulk and local dielectric changes. Given these excellent physicochemical properties, gold nanocages have a wide range of applications in optical sensing and biomedical fields. By combining a sandwich LFIA technology, Yang et al. proved that gold nanocages could serve as enhanced tags for the development of highly sensitive biosensors [115].

### Nanorods

Compared with spherical AuNPs, AuNRs show more advantages in optical properties, catalytic activity, stability, and biocompatibility. Based on previous reports, the extinction coefficient of AuNRs ( $\sim 10^9$  L mol<sup>-1</sup> cm<sup>-1</sup>) is  $\sim 10$ -fold higher than that of spherical AuNPs ( $\sim 10^8$  L mol<sup>-1</sup> cm<sup>-1</sup>) [116]. Given the anisotropic shape, AuNRs exhibit two distinct LSPR peaks that correspond to the electron oscillations along the transverse and longitudinal directions. Therefore, by adjusting the aspect ratios of AuNRs, they can present different LSPR peaks or rich color variations, thereby providing a favorable basis for rapid screening of visualization using the LFIA method. In addition, unlike nanospheres, nanorods have enhanced electric fields at the tips and edges,

which can achieve various enhanced optical properties, such as SERS activity, photothermal effect, and metal-enhanced fluorescence effect, thereby aiding other signal transduction models in LFIA, such as Raman, thermal contrast, and fluorescence. Given these outstanding properties, AuNRs have been widely used for photoacoustic imaging, photothermal therapy, and biosensing [117]. The fabrication and application of monodispersed AuNRs as signal reporters in LFIA were first reported by Venkataramasubramani and Tang in 2009 [118]. Afterward, most of the studies focused on investigating the optimization and use of AuNRs in improving the multiplexing and sensitivity of LFIA, two major challenges encountered by the conventional LFIA. Recently, using gold-silver core-shell bimetallic nanorods as a SERS substrate and 5,5'-dithiobis (2-nitrobenzoic acid) as a Raman reporter, Deng et al. developed a SERS-coupled LFIA strip for ultrasensitive detection of Sudan I with a sensitivity of 0.2 pg mL<sup>-1</sup> [119]. Similarly, He et al. developed a color/SERS dual-mode LFIA method for ultrasensitive detection of *Campylobacter jejuni* by using platinum-coated AuNRs (AuNR@Pt) as signal amplifiers. In this design, AuNR@Pt possesses



**Figure 8.** (A) Schematic illustration of surface functionalization of flowerlike AuNPs and their LFIA application for detection of *E. coli* O157:H7. Adapted with permission from [35]. Copyright 2015 American Chemical Society. (B) Schematic illustration of the synthesis and surface modification of hollow Au-Ag NPs and detection of CLE. Adapted with permission from [114]. Copyright 2017 Nature-Springer. (C) Schematic illustration of preparing colorimetric and fluorescent dual-mode LFIA. Adapted with permission from [120]. Copyright 2019 American Chemical Society. (D) Multiplex LFIA based on shape-controlled nanoparticles for simultaneous detection of fumonisin B1 (FB<sub>1</sub>), aflatoxin B1 (AFB<sub>1</sub>), ochratoxin A (OTA), and zearalenone (ZEN). Adapted with permission from [123]. Copyright 2020 Elsevier.

intrinsic peroxidase-mimicking activities and SERS enhancement properties, thereby facilitating dual-signal readout of color and SERS [120]. Under the optimal conditions, the sensitivities of the fabricated dual-mode LFIA are as low as 75 CFU mL<sup>-1</sup> for the colorimetric mode and 50 CFU mL<sup>-1</sup> for the SERS mode. By incorporating the fluorescence enhancement effect of AuNRs derived from the electromagnetic coupling with gold surface plasmons, You et al. designed semiconducting polymer dots (Pdots) coated with AuNRs (Au@Pdot) hybrid nanocomposites and demonstrated their uses as a colorimetric/fluorescent dual-modal signal probe in LFIA (Figure 8C). Given the plasmon-enhanced fluorescence of Pdots on AuNRs, this developed LFIA shows lower LOD of 1.07 pg mL<sup>-1</sup> for prostate specific antigen (PSA), which is at least two orders of magnitude better than that of the conventional fluorescent LFIA system. In addition, this dual-modal sensing technology in LFIA application can ensure detection accuracy and reliability [179].

#### Multiplexed LFIA based on shape-controlled NMNPs

Simultaneous detection of multiple target analytes has been a primary development direction in the LFIA area because of the increased detection efficiency and decreased test costs. The exciting progress of multiplexed LFIA has been achieved by integrating the multiline design with monochromatic signal labels. However, this multiplexed LFIA design can hardly provide indicators of line positioning, thereby resulting in the false interpretation of the results when multiple successive bands with the same color are present in a small test area [121]. By contrast, multicolored signal labels can effectively avoid these risks and enable intuitive visualization because each color corresponds to an analyte in a single strip. In recent years, increasing attempts have been devoted to constructing various multicolored LFIA strips by using different colored reporters as alternatives to traditional monochromatic ones. In this content, the shape or size-controlled NMNPs with different distinct colors are desirable signal probes for the development of multicolored LFIA. Emulating this principle, several multicolored LFIA strips were successfully developed for the determination of various target analytes, including proteins, mycotoxins, and viruses. Yen and co-workers presented a multiplexed LFIA design for multiplexed disease diagnostics using multicolored silver nanoparticles as labelling probes. In their work, three different silver nanoparticles with distinguishable colors (orange, red, and green) were synthesized using a seed-mediated growth strategy to control the morphological evolution. After coupling with

antibodies against dengue virus NS1 protein, Yellow Fever Virus NS1 protein, and Ebola virus Zaire strain glycoprotein, this design successfully achieves multiplexed determination of the three pathogens [122]. Similarly, our group explored the first application of gold nanospheres (red), gold nanocacti (purple), AuNFs (blue), and hyperbranched Au plasmonic blackbodies (black) in a multiplexed LFIA for the rapid and simultaneous detection of four common mycotoxins (Figure 8D) [123].

#### 4. Nanoparticle elemental composition

In general, the noble metals can be divided into two categories of coinage metals (e.g., Au and Ag) and platinum-group metals (e.g., Pd, Pt, Rh, Ir, and Ru) [124]. Noble metal nanomaterials consisting of coinage metals show tunable LSPR properties, but they have limited catalytic activities. By contrast, the nanostructures originated from platinum-group metals exhibit exactly opposite properties [27]. NMNPs with a single component can hardly meet the requirements with respect to high optical sensitivity, excellent colloid stability, and high catalytic activity. In addition, a small change in elemental composition of noble metal nanostructures can make a huge difference [124]. Accordingly, nanomaterial fabrication has gradually shifted toward the design and development of composite NMNPs containing two or more noble metal components or one noble metal incorporating non-noble metals with different physicochemical properties [40, 125]. Composite nanomaterials effectively combine the functions of each component while avoiding its limitations, thereby significantly improving their overall properties, such as tunable optical properties [126], increased colloid stability [127], and enhanced catalytic activities [36], and emerging new synergistic properties, such as magnetic [128] or fluorescent properties [39]. In recent years, composite noble metal nanostructures with controlled dimensions and tunable morphologies have been synthesized using various methods. Given their superior performances and remarkable synthesis, composite NMNPs have obtained numerous applications in a wide range of areas, including catalysis, optoelectronics, biomedical devices, sensing, and imaging [37]. As an improved signal reporter for LFIA, the composite NMNPs have been demonstrated with enhanced detection performances relative to traditional LFIA using single-component NMNPs as labels. Therefore, the following discussion will highlight the current state of the art of controlled synthetic strategies and performance improvements of composite noble metal nanostructures and their applications in LFIA. Table 4 summarized the representative LFIA using elemental

composition-controlled NMNPs.

**Table 4.** A summary of some representative LFIA using elemental composition-controlled noble metal nanoparticles.

Element	Analyte	Dynamic range	LOD	Ref.
Pt	HCG	0.1–9 ng mL <sup>-1</sup>	0.2 ng mL <sup>-1</sup>	[139]
	HCG	No given	0.3 ng mL <sup>-1</sup>	[183]
	Dehydroepiandrosterone	1–1000 ng mL <sup>-1</sup>	10.0 ng mL <sup>-1</sup>	[142]
IrO <sub>2</sub>	IgG	No given	0.07 µg mL <sup>-1</sup>	[184]
	Salbutamol	0.18–12 ng mL <sup>-1</sup>	0.002 ng mL <sup>-1</sup>	[127]
Au–Ag	Cadmium ion	0.05–25 ng mL <sup>-1</sup>	0.05 ng mL <sup>-1</sup>	[126]
	Penumolysin	No given	1 pg mL <sup>-1</sup>	[132]
	Chloramphenicol	1.36–123.21 ng mL <sup>-1</sup>	0.36 ng mL <sup>-1</sup>	[172]
Au–Pt	Thiamphenicol	0.80–95.29 ng mL <sup>-1</sup>	0.20 ng mL <sup>-1</sup>	
	Florfenicol	2.09–71.53 ng mL <sup>-1</sup>	0.78 ng mL <sup>-1</sup>	
	Prostate-specific antigen	0.3–10.00 ng mL <sup>-1</sup>	0.20 ng mL <sup>-1</sup>	[135]
	Prostate-specific antigen	10–200 pg mL <sup>-1</sup>	20 pg mL <sup>-1</sup>	[36]
	p24	1–10000 pg mL <sup>-1</sup>	0.8 pg mL <sup>-1</sup>	[24]
	Rabbit IgG	0.05–10 ng mL <sup>-1</sup>	5 pg mL <sup>-1</sup>	[185]
	<i>Clavibacter michiganensis</i>	No given	300 CFU mL <sup>-1</sup>	[186]
Pt–Ni(OH) <sub>2</sub>	Potato virus X	No given	4–8 pg mL <sup>-1</sup>	[187]
	Acetochlor	0.1–20 ng mL <sup>-1</sup>	0.63 ng mL <sup>-1</sup>	[143]
	Fenpropathrin	0.1–20 ng mL <sup>-1</sup>	0.24 ng mL <sup>-1</sup>	[143]
Pt–Pd	p53 Protein	0.1–10 ng mL <sup>-1</sup>	0.05 ng mL <sup>-1</sup>	[188]
	<i>E. coli</i> O157:H7	10–10 <sup>7</sup> CFU mL <sup>-1</sup>	34 CFU mL <sup>-1</sup>	[133]
	<i>E. coli</i> O157:H7	1×10 <sup>3</sup> –1×10 <sup>6</sup> CFU mL <sup>-1</sup>	9.0×10 <sup>2</sup> CFU mL <sup>-1</sup>	[189]
Au–Ag–Pt	Butyrylcholinesterase	0.05–6.4 nM	0.025 nM	[190]
	Myoglobin	6.67–150 ng mL <sup>-1</sup>	5.47 ng mL <sup>-1</sup>	[138]
FPNHs	H-FABP	No given	0.21 ng mL <sup>-1</sup>	[38]
	Dicofol	23.98–478.32 ng mL <sup>-1</sup>	9.9 ng mL <sup>-1</sup>	[39]
		(colorimetry)		
		3.97–91.47 ng mL <sup>-1</sup>	1.59 ng mL <sup>-1</sup>	
		(fluorescence)	(fluorescence)	
	Glycoprotein	2–1000 ng mL <sup>-1</sup>	0.18 ng mL <sup>-1</sup>	[141]
	Cystatin C	0.12–500 ng mL <sup>-1</sup>	0.61 ng mL <sup>-1</sup>	[40]
		(colorimetry)	(colorimetry)	
		0.12–500 ng mL <sup>-1</sup>	0.24 ng mL <sup>-1</sup>	
		(fluorescence)	(fluorescence)	
MPNHs	Anti-HCV	0.24–120 pg mL <sup>-1</sup>	0.24 pg mL <sup>-1</sup>	[37]
	Treponema pallidum antigens	No given	1 NCU mL <sup>-1</sup>	[140]
	Single nucleotide polymorphism	5 ng–1200 ng per test	5 ng per test	[191]
	Single nucleotide polymorphisms	0.02–2 pg µL <sup>-1</sup>	0.04 pg µL <sup>-1</sup>	[192]
	β-conglutinin	10 fM–100 pM	8 fM	[144]
	H1N1	No given	50 pfu mL <sup>-1</sup>	[41]
	HAdV	No given	10 pfu mL <sup>-1</sup>	
	HCG	0–50 mIU mL <sup>-1</sup>	0.2 mIU mL <sup>-1</sup>	[125]
	HCG	0.01–4 mIU mL <sup>-1</sup>	0.0094 mIU mL <sup>-1</sup>	[128]
	<i>E. coli</i> O157:H7	10 <sup>2</sup> –10 <sup>5</sup> CFU mL <sup>-1</sup>	9 × 10 <sup>1</sup> CFU mL <sup>-1</sup>	

#### 4.1. Strategies for nanoparticle elemental composition regulation

Given their advantages over corresponding monometallic nanoparticles, composite noble metal nanomaterials are particularly useful for diverse applications. At present, the synthesis of composite nanomaterials with core–shell, alloy, and bimetallic heterostructures has been achieved via various approaches, including atomic layer deposition, electrochemical deposition, templated growth, chemical reduction, thermal decomposition,

sonochemical method, and biosynthesis [124]. Among these methods, chemical reduction is the commonly used method. The procedure for synthesizing composite nanomaterials using this method is similar to that of monometallic nanoparticles, however controlling the co-reduction of mixed metal precursors is more challenging and complicated owing to their different reduction potential and inherent chemical properties. In general, the simultaneous reduction of mixed metal precursors in a homogeneous solution will produce alloyed nanocomposites, whereas a sequential reduction can lead to core–shell nanostructured composites [129]. Therefore, a series of synthetic parameters, such as the crystallization of each component, surface energy, relative bonding strength among different elements, relative atomic radius, and surface capping agent, should be considered to obtain the expected composite nanostructures with unexpected properties. In particular, some mild reducing agents, such as ethylene glycol and diethylene glycol, citrate and sodium citrate, ascorbic acid, formic acid, 2-thiopheneacetonitrile, polymers, and oleylamine, can be considered for use in synthesizing monodispersed composite nanomaterials in solution to achieve better control over the reaction kinetics and final product [130]. With all this in mind, core-shell nanoparticles or other nanohybrids of noble metals and non-noble metals are among the combinations that have been well studied [131]. To date, many composite noble metal nanomaterials, such as core-shell nanostructures (e.g., a metal shell surrounding a gold core or a gold shell surrounding another metal core) and alloyed bimetallic nanostructures (e.g., Au@Pt Co@Pt, Au@Ag, and Pt@Pb), serve as potential alternatives to traditional single-component AuNPs for the establishment of high-performance LFIA [24, 132, 133].

#### 4.2. Effect of elemental composition on the properties of composite NMNPs

The elemental composition of composite NMNPs plays a crucial role in their properties, wherein a slight change in the elemental composition can have a significant effect on the performance of composite nanomaterials in enhancing the optical signal intensity, increasing the colloidal stability, and breeding new functionalities [130]. Although the commercialized colorimetric signal labels have dominated by spherical AuNPs with sizes of 20–40 nm in LFIA, these citrate-modified AuNPs often suffer from low signal intensity and poor colloidal stability against variations in environmental factors, thereby resulting in low sensitivity and poor resistance to matrix interference in real practice. This

issue can be well addressed by introducing polydopamine coating to form ultra-stable core-shell nanostructured composites due to its high chemical reactivity, strong adhesion capacity, good biocompatibility, and excellent stability [134]. In another typical example, silver nanostructures show good LSPR activity, but they suffer from poor chemical and structural stability. Thus, increasing the stabilities of silver nanomaterials is the key to their wide applications. An available approach for this goal is through incorporating gold using galvanic replacement to produce Ag-Au nanocomposites [135, 136].

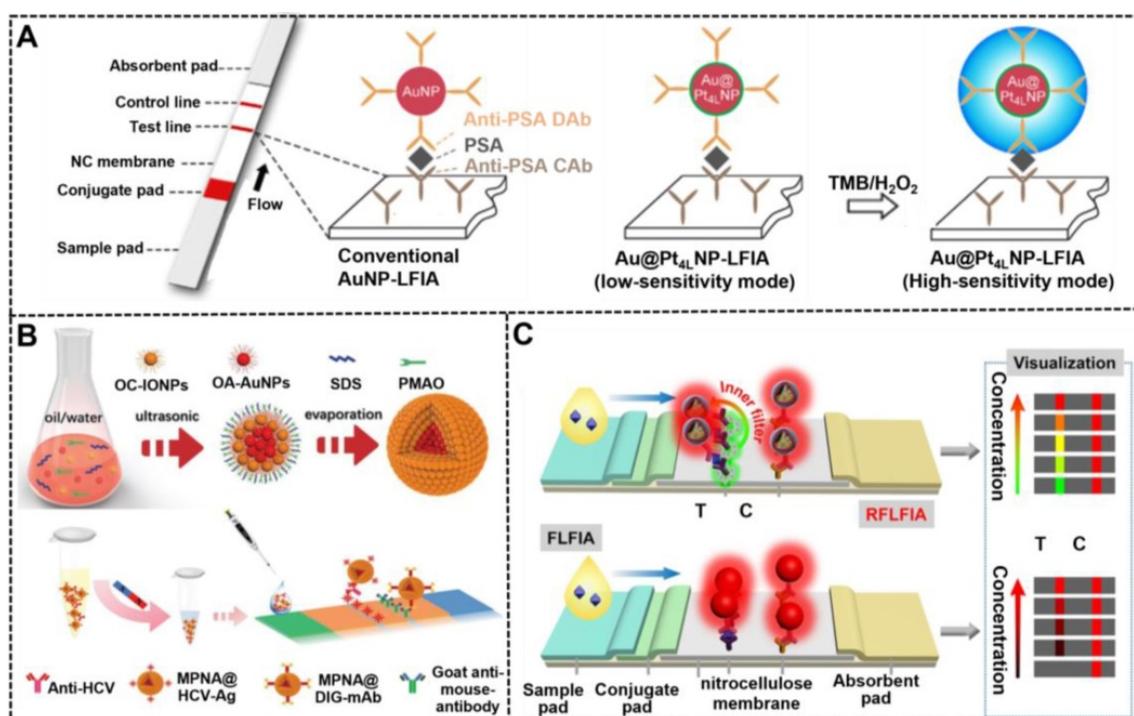
Noble metal nanomaterials with high catalytic activities have attracted extensive attention in enhancing the detection signal intensity of LFIA labels. Such catalytic bimetallic nanomaterials can be obtained by incorporating a catalytic noble metal into another metal within individual nanocomposite using the co-reduction or sequential reduction strategy [36]. The resultant multimetallic nanoparticles of different elementals, containing Au@Ag [135], Au@Pt [36], Pt@Pd [133], Pd@Ir [137], and Au@Ag@Pt [138], have been intensively studied in enhancing the colorimetric signal intensity due to their stronger catalytic activities compared with their parent monometallic nanoparticles. The catalytic constants of such noble metal nanozymes reach up to  $10^4$ – $10^5$  s<sup>-1</sup>, about one to two orders of magnitude higher than that of horseradish peroxidase ( $10^3$  s<sup>-1</sup>) [139]. In several recent studies, Xia's group has substantially improved the catalytic efficiencies of noble catalytic nanomaterials with a catalytic constant of  $10^6$ – $10^7$  s<sup>-1</sup> [36], which could serve as excellent substitutes for developing highly sensitive biosensors. In addition, multifunctional noble metal nanomaterials are emerging composite nanostructures that can simultaneously possess additional properties other than the functionalities of noble metal nanomaterials, which have attracted considerable interest in various fields. These multifunctional composite nanomaterials can be constructed by using the evaporation-induced self-assembly and the post-modification or post-growth method [37, 41]. For example, the combination of noble metal compositions and magnetic compositions to form composite magnetic NMNPs exhibits magnetic and plasmonic behavior, which can achieve simultaneous magnetic enrichment and colorimetric sensing [140]. Another notable example is the composition of noble metal materials and fluorescent materials, which allow the simultaneous generation or regulation of two signal transduction channels of colorimetry and fluorescence, thereby facilitating a novel dual-modal

sensing technology to achieve some synergistic effects on the detection performances [141]. In brief, composite NMNPs have advantages in at least two niche fields, which offer an elegant strategy for overcoming the unsolved bottlenecks encountered by single-component nanomaterials.

### 4.3. Elemental composition engineering in LFIA

#### Composite metallic nanozymes

Different from traditional colored nanomaterials, catalytic NMNPs exhibit dual roles for generating colorimetric signal transduction by intrinsic plasmonic activity and performing enzymatic deposition amplification by peroxidase-like activities. Leveraging these nanomaterials as signal probes for LFIA, about one order of magnitude improvement in sensitivity has been achieved compared with conventional LFIA without amplification [139, 142]. However, this enhancement is limited by the relatively low catalytic efficiency of monometallic nanozymes. As described earlier, composite metallic nanozymes have stronger catalytic efficiency than monometallic nanomaterials with similar sizes, which can further improve the detection sensitivity of LFIA when used as reporters. Recently, several multimetallic nano hybrids, such as Au@Pt [24], Pt@Pd [133], Pt@Ni [143], and Au@Ag@Pt [138], have improved the analytical performance of LFIA. For example, Gao et al. synthesized a series of difunctional Au@Pt<sub>nL</sub> (nL: n atomic layers of Pt) nano hybrids through engineering traditional ~40 nm AuNPs with ultrathin Pt coating of 1-10 atomic layers by varying the amount of Pt precursor during seed growth and then studied the impact of Pt shell thickness on their catalytic activity [36]. The results suggested that the catalytic efficiency of Au@Pt<sub>nL</sub> increased sharply with the increase of atomic layers and then reached a constant at n = 4. Using the synthesized Au@Pt<sub>4L</sub> nano hybrids as signal labels, the developed LFIA could achieve an ultrasensitive detection for PSA with an LOD of 20 pg mL<sup>-1</sup> in combination with Au@Pt<sub>4L</sub>-mediated enzymatic deposition amplification, which presents two orders of magnitude enhancement in sensitivity relative to that of Au@Pt<sub>4L</sub>-based LFIA without catalytic amplification (**Figure 9A**). Around the same time, Loynachan et al. reported a similar porous core-shell Au@Pt nanozyme and demonstrated its potential for improving the POC diagnostics of HIV coupled with the amplification of enzymatic deposition signal on the LFIA platform.



**Figure 9.** (A) The comparison between conventional AuNP-based LFIA and Au@Pt nanoparticle-based LFIA for PSA detection. Adapted with permission from [36]. Copyright 2019 American Chemical Society. (B) Schematic illustration for the synthetic procedures of magnetic-plasmonic nanoassemblies (MPNAs) and their application in a sandwich LFIA for the diagnosis of hepatitis C virus infection. Adapted with permission from [37]. Copyright 2019 Wiley-VCH GmbH. (C) Illustration of RFLFIA and traditional FLFIA for visual and quantitative detection of H-FABP. Adapted with permission from [38]. Copyright 2021 Wiley-VCH GmbH.

### Magnetic-plasmonic nanohybrids (MPNHs)

Composite MPNHs are a promising multifunctional nanomaterial because of their intrinsic plasmonic and magnetic properties, which support their various uses, such as magnetic separation and optical sensing. High-performance MPNHs should retain high magnetic-plasmonic activities simultaneously, thereby promoting fast magnetic response and sensitive colorimetric signal transduction. At present, most of MPNHs are prepared by growing Au shell or attaching isolated Au AuNPs onto the surface of magnetic nanomaterials to form core-shell “gold-coated magnetic” nanostructures [144]. However, given the inherent magnetic shielding effect of Au shell on the surface of magnetic nanomaterials, the saturation magnetization of such core-shell nanostructures decrease significantly with the increase of the plasmonic component. Although the shielding effect can be efficiently weakened via introducing a spacer layer between magnetic and plasmonic units, such as silicon and PDA layer, the synthesis of high-quality MPNHs with the maximized saturation magnetization and plasmonic activity remains a challenge. [125] In recent research, our group reported a facile synthesis of an improved MPNH, namely, MPNAs, through co-assembling oleylamine-coated AuNPs (OA-AuNPs) with oleic acid-coated iron oxide

nanoparticles (OC-IONPs) into polymer nanospheres (Figure 9B) [37]. The resultant MPNAs show a typical “magnetic-coated gold” core-shell nanostructure with OA-AuNPs aggregating into a core and OC-IONPs assembling into a magnetic shell, thereby achieving an efficient spatial separation of OA-AuNPs and OC-IONPs to minimize the interference between them. Thanks to the high loading of OA-AuNPs and reasonable spatial distribution of OC-IONPs, the obtained MPNAs were characterized with high saturation magnetization (~79.5% of initial OC-IONPs) and dramatically enhanced plasmonic activities. After covalently conjugating with recognition elements against hepatitis C virus antibody, the MPNAs can achieve synchronous magnetic enrichment and colorimetric sensing of target analytes on the magnetic-assisted LFIA platform based on their intrinsic dual functionality of plasmonic and magnetic. Under the optimized conditions, the LOD of this method was 0.24 pg mL<sup>-1</sup>, which was below those obtained by other control groups.

### Fluorescent-plasmonic nanohybrids (FPNHs)

Composite FPNHs are another multifunctional nanoprobe, which are extensively studied because of their intrinsic dual-mode signal transduction of plasmon and fluorescence [145]. Recently, several typical FPNHs, such as AuNPs/AgNPs-organic

fluorophore-based and AuNPs/AgNPs-quantum dot (QD) nanocomposite, have been reported for use in bioassay, photocatalysis, and imaging [40]. The available synthetic approaches for FPNHs primarily include the incorporation of plasmonic and fluorescent nanoparticle by layer-by-layer polyelectrolyte coating, the direct linkage of two nanomaterials using a chemical strategy, or the emulsion-based self-assembly technology [146, 147]. However, fluorescence may be quenched in the nanocomposite due to the plasmon-induced resonance energy transfer of plasmonic nanomaterials. The precise control of the distance between plasmonic units and fluorescent units and their spatial distribution in individual FPNH are critical to minimize fluorescence quenching and even obtain metal-enhanced fluorescence. Consequently, Huang et al. reported a synthetic method for high-quality FPNHs, namely, SASQS, by using the dendritic silica template to assemble directly with hydrophobic AuNPs via thiol-metal coordination. After silanization, controlled silica growth, and mercapto-group grafting, hydrophobic red-light-emitting QDs were then immobilized densely to form the nanocomposite of SASQS. Through further functionalization of antibodies against cystatin C (Cys C), this SASQS can perform the dual-mode colorimetric and fluorescent sensing of Cys C with LODs of 0.61 and 0.24 ng mL<sup>-1</sup>, respectively [40]. Subsequently, by integrating green-light-emitting QDs (denoted as gQDs) as a reference fluorescent signal, a ratiometric fluorescent LFIA strategy, namely, RFLFIA, was described by the same group for highly sensitive quantitative detection of heart-type fatty-acid-binding protein (H-FABP) integrated with a smartphone (**Figure 9C**) [38]. In this work, the SASQS conjugated with the detected antibody (SASQS-mAb1) was sprayed in the conjugate pad, whereas gQDs modified with the captured antibody (gQD-mAb2) were immobilized at the test line. Upon the addition of H-FABP, the sandwich immunocomplex was formed, thereby triggering the fluorescent change from green to yellow and then to red. This phenomenon may be due to the overlap of red fluorescence from SASQS and green fluorescence from gQDs and the inner filter effect of AuNPs from SASQS on the green emission. Compared with traditional FLFIA with only monochromatic fluorescent change, the proposed RFLFIA strip is more distinguishable due to its green-to-red color variance.

## 5. Nanoparticle external structure

The enhancement in the optical, photothermal, or catalytic properties of NMNPs largely depends on their external structure. NMNPs with unique external

structures can create plasmonic coupling for an intense electromagnetic field within the confined area, thereby significantly modifying the optical properties of NMNPs or other optical molecules adjacent to their surface [148]. Consequently, increasing researchers aimed to manipulate the optical activities of NMNPs, such as plasmonic, SERS, and fluorescent signal, to improve their application performance [27]. In addition to controlled nanocrystal synthesis, the optical properties of NMNPs can be enhanced by other methods. The LSPR property of NMNPs is closely associated with interparticle coupling interactions. Considering the LSPR, a significant enhancement in light absorption and local electromagnetic field is observed with the decrease of the interparticle distance. Thus, several high-quality plasmonic NMNPs with specific nanostructures of nanoaggregate [82], core-shell [149], and core-satellite characteristics [150] have shown potential applications in diverse areas, including biosensing, of such carefully crafted plasmonic nanostructures for enhancing the LFIA performance have been well investigated. **Table 5** summarized some representative LFIAs based on external structure-controlled NMNPs.

### 5.1. Strategies for the construction of structure-directed nanoparticles

Synthesizing NMNPs with related structures is crucial to achieve the fine tune of their optical properties and functions, which has motivated researchers to develop strategies for controlled preparation of such specific nanostructured NMNPs. For example, nanoaggregates can be prepared via chemical coupling and nucleic acid hybridization. For example, Hu et al. reported the simple synthesis of oligonucleotide-linked AuNP nanoaggregates by modifying a pair of complementary oligonucleotide sequences onto the surface of spherical AuNPs to form corresponding conjugates as crosslinking precursors [151]. Compared with individual AuNPs, AuNP nanoaggregates exhibit enhanced colorimetric signal strength, which is attributed to the collective molar extinctions of AuNPs. Nevertheless, the synthetic controllability and reproducibility of such methods are relatively poor. In addressing this issue, the controllable assembly strategy was recently reported to improve the synthesis of nanoaggregates and nanoassemblies. Recently, our group reported that assembled colloidal gold superparticles (abbreviated as GSPs) with remarkably increased light absorption and improved colloid stability were synthesized by the self-assembly of small hydrophobic AuNPs into large GSPs [82].

**Table 5.** A summary of external structure-controlled noble metal nanoparticles based LFIA.

Structure	Analyte	Dynamic range	LOD	Ref.	
Core-shell	Phenylethanolamine A	No given	0.32 pg mL <sup>-1</sup>	[173]	
	Salbutamol	No given	3.0 pg mL <sup>-1</sup>	[169]	
	<i>Salmonella enteritidis</i>	2.7-2.7×10 <sup>6</sup> CFU mL <sup>-1</sup>	27 CFU mL <sup>-1</sup>	[174]	
	Respiratory infection virus	1 pM-50 nM	0.03-0.041 pM	[193]	
	Pseudorabies virus	41-650 ng mL <sup>-1</sup>	5 ng mL <sup>-1</sup>	[175]	
	Pharmaceutical diclofenac	No given	0.07 pg mL <sup>-1</sup>	[194]	
	Clenbuterol	0-1 ng mL <sup>-1</sup>	5 ng mL <sup>-1</sup>	[171]	
	Myoglobin	0.01-500 ng mL <sup>-1</sup>	3.2 pg mL <sup>-1</sup>	[22]	
	Cardiac troponin I	0.01-50 ng mL <sup>-1</sup>	0.44 pg mL <sup>-1</sup>		
	Creatine kinase-MB isoenzymes	0.02-90 ng mL <sup>-1</sup>	0.55 pg mL <sup>-1</sup>		
	Cardiac troponin I	No given	0.1 ng mL <sup>-1</sup>	[149]	
	Mycoplasma pneumoniae (IgM)	0.1 ng -10 µg mL <sup>-1</sup>	0.1 ng mL <sup>-1</sup>	[176]	
	Mycoplasma pneumoniae	0.1-10 mg mL <sup>-1</sup>	0.1 ng mL <sup>-1</sup>		
	Cardiac troponin I	0.09-50 ng mL <sup>-1</sup>	0.09 ng mL <sup>-1</sup>	[158]	
	Core-satellite	Aflatoxin B <sub>2</sub>	No given	0.9 ng mL <sup>-1</sup>	[153]
		rabbit IgG	0.05-2 ng mL <sup>-1</sup>	0.01 ng mL <sup>-1</sup>	[154]
HCG		No given	0.039 mIU mL <sup>-1</sup>	[163]	
MicroRNA		No given	10 pM	[164]	
HCG		No given	1.6 mIU mL <sup>-1</sup>	[166]	
Clenbuterol		0.1-2 ng mL <sup>-1</sup>	0.1 ng mL <sup>-1</sup>	[157]	
C-reactive protein		No given	0.08 ng mL <sup>-1</sup>	[165]	
Influenza A		No given	2.5×10 <sup>-2</sup> HAU mL <sup>-1</sup>	[150]	
17β-estradiol		No given	0.5 ng mL <sup>-1</sup>	[155]	
HIV-1		No given	0.1 nM	[151]	
Nanoaggregates		Nucleoside	No given	20 µM	[195]
	p24 antigen	0.1 fg mL <sup>-1</sup> -10 ng mL <sup>-1</sup>	0.01 fg mL <sup>-1</sup>	[162]	
	Methamphetamine	0.023-375 ng mL <sup>-1</sup>	0.026 ng mL <sup>-1</sup>	[161]	
	HCG	0.49-1000 mIU mL <sup>-1</sup>	0.49 mIU mL <sup>-1</sup>	[82]	
	Hepatitis B surface antigen	0.46-1000 ng mL <sup>-1</sup>	0.45 ng mL <sup>-1</sup>		
	Troid-stimulating hormone	0.4-40 µIU mL <sup>-1</sup>	0.5 µIU mL <sup>-1</sup>	[196]	

Another effective approach to amplify the optical signal intensity to yield visual enhancement of NMNPs is through the design of core-satellite composite nanoarchitectures, wherein the core-satellite nanocomposite can be synthesized by attaching a large amount of isolated NMNPs onto the surface of large nanocarriers via the *in-situ* growth of NMNPs, and the post-modification of NMNPs, such as physical absorption and covalent coupling. To date, the available nanocarriers primarily include NMNPs, magnetic nanomaterials [152, 153], silica nanorods (SiNRs) [154], graphite-like carbon nitrides [155], latex nanocomposites [150], metal organic frameworks [156], and bacteria [157]. In addition, the core-shell feature of NMNPs benefits the SERS enhancement and thus allowing the SERS biosensing owing to the electronic ligand effect and enhanced electromagnetic field located in core-shell nanostructures, that can cause evident Raman signal enhancement for Raman reporter molecules deposited between interfaces. These core-shell NMNPs are usually synthesized by the sequential reduction growth method. Currently, the SERS activities of Ag@Au, Au@Ag, Au@Ag@Au, and hollow Au-Ag core-shell nanoparticles were investigated [149, 158]. In addition, several studies have attempted to elucidate the effect of gap size between the core and the shell on their SERS signal enhancement performance, and the results indicated that the gap size should match the expected thickness

of the monolayer of Raman reporter molecules [159]. The coupling of NMNP-based SERS tags and LFIA technologies improves the sensitivity and quantification, thereby increasing its actual application value in POC testing. Hence, the following section will summarize the typical applications such structure-directed NMNPs in improving the LFIA.

## 5.2. Structure engineering in LFIA

### Nanoaggregates and nanoassemblies

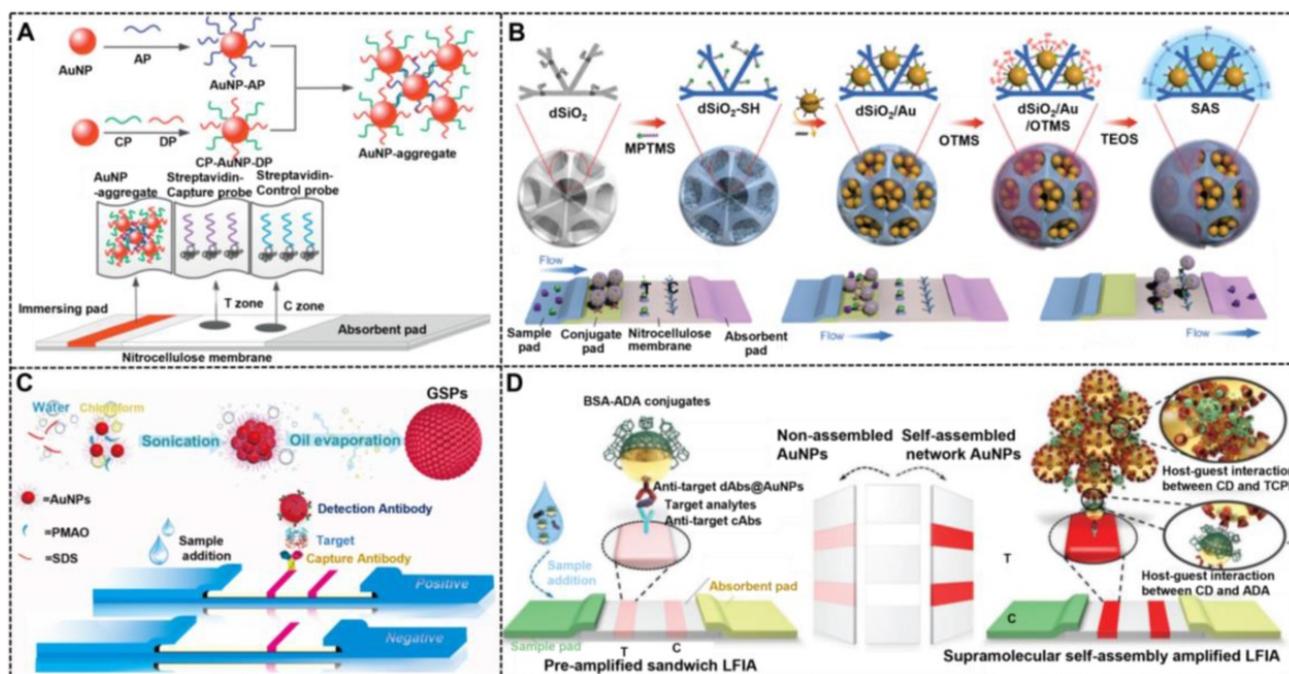
Increasing the accumulation of AuNPs on the T line has been considered as the straightforward strategy for enhancing the sensitivity of traditional AuNP-LFIA. Xu and co-workers used oligonucleotide-linked AuNP nanoaggregates as amplified signal probes to fabricate an improved LFIA for sensitive detection of a nucleic acid sequence of HIV (**Figure 10A**) [151]. The LOD of this developed lateral flow assay was 0.1 nM, thereby providing a 2.5-fold enhancement in detection sensitivity compared with that of traditional strip without signal amplification. Taking advantage of the immunoreaction to assist the synthesis of AuNP nanoaggregates for amplifying the plasmonic signal, Rivas et al. recently reported an enhanced LFIA methodology for the improved detection of *Leishmania* parasite DNA with a LOD of 0.038 parasites in each

DNA amplification reaction [160]. AuNP nanoassemblies consisting of numerous isolated AuNPs reveal markedly enhanced intensity, thereby increasing the LFIA sensitivity. Huang et al. recently reported the preparation of a controllable and high-quality nanoassembly, namely, SAS, by implanting high-density hydrophobic AuNPs into three-dimensional silica scaffolds (**Figure 10B**) [161]. The resultant SAS nanoassemblies were further functionalized with antibodies and used for highly sensitive POC testing of methamphetamine with a LOD of 0.026 ng mL<sup>-1</sup> coupled with the LFIA. Similarly, our group demonstrated the improved analytical performances of assembled AuNP nanomaterials (GSPs) with remarkably enhanced light absorption in monitoring proteins and pathogens (**Figure 10C**) [82], which resulted from the high loading capacity and weak interparticle plasmonic coupling in the nanoassemblies. Nevertheless, the signal amplification abilities of these methods are often compromised by the limited accumulation of nanoparticles at the T line, which only provide about one order of magnitude increase in sensitivity. Recently, our group developed a supramolecular self-assembly mediated multiple rounds of signal amplification strategy for enhancing the sensitivity of conventional AuNP-LFIA (**Figure 10D**) [162]. In this design, the smart host-guest supramolecular recognition between  $\beta$ -cyclodextrin ( $\beta$ -CD)-coated

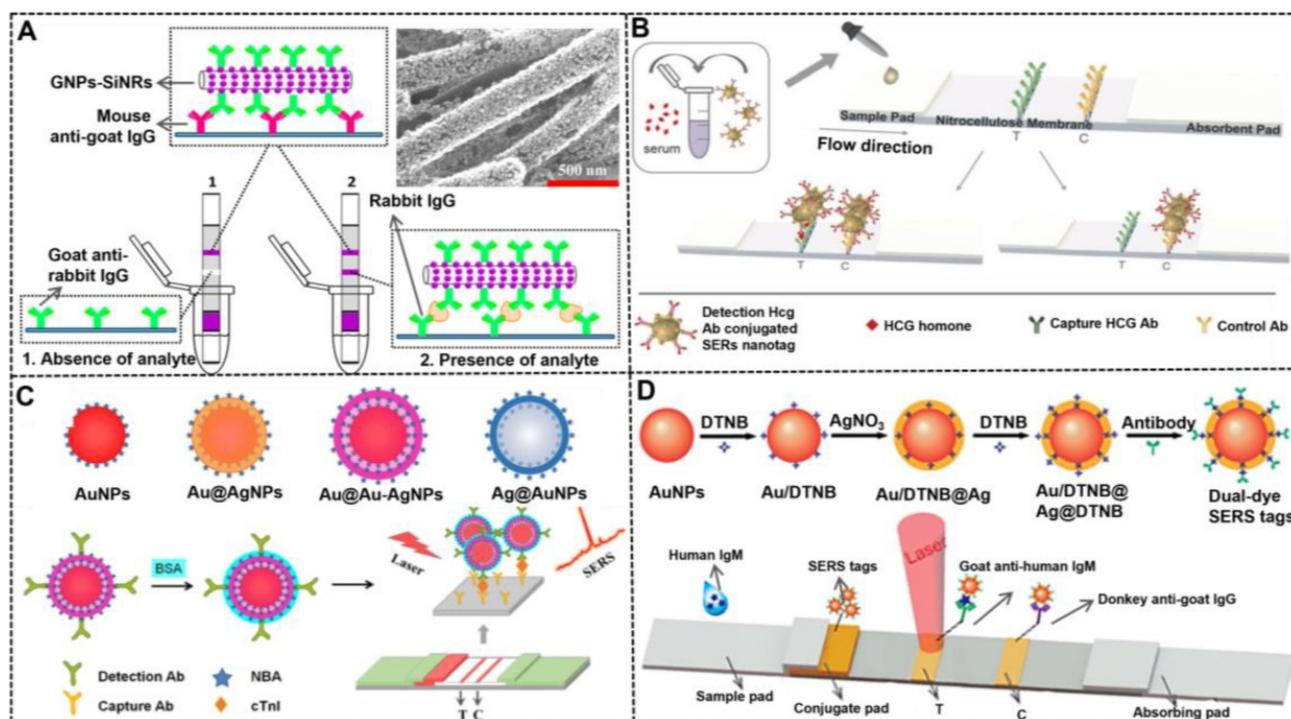
AuNPs and adamantane (ADA) or tetrakis(4-carboxyphenyl) porphyrin (TCPP) was applied to achieve the layer-by-layer self-assembly and massive accumulation of AuNPs at the T line. Under the optimized conditions, the amplified LFIA exhibited ultrahigh sensitivity with a LOD at the subattogram level and super-wide detection range covering seven orders of magnitude. In addition, the method can customize biomarker detection to meet the needs of clinicians by using a controllable cycle self-assembly strategy.

### Core-satellite nanostructures

Composite core-satellite nanostructured nanoparticles containing large numbers of AuNPs on their surface can produce intensive color signals when compared with pure AuNPs, thereby increasing the detection sensitivity of traditional AuNP-LFIA. Xu et al. pioneered the synthesis of AuNP-decorated SiNRs (AuNP-SiNRs) with enhanced colorimetric signal intensity and then used them as colored LFIA probes to improve protein detection (**Figure 11A**) [154]. In their work, AuNP-SiNRs were synthesized by using a two-step deposition process, including gold seed deposition and its growth. As shown in the inset of **Figure 11A**, a layer of AuNPs with a density at around 10<sup>4</sup> was deposited on the surface of a single SiNR, thereby resulting in a purple color that was darker than pure AuNP solution. After being



**Figure 10.** (A) The preparation of oligonucleotide linked AuNP aggregates and design of improved LFIA. Adapted with permission from [151]. Copyright 2013 the Royal Society of Chemistry. (B) Schematic illustration for the preparation of AuNP implanted nanospheres and their application in LFIA. Adapted with permission from [161]. Copyright 2019 the Royal Society of Chemistry. (C) Illustration of the synthetic strategy for GSPs by the microemulsion-based self-assembly process and their application in LFIA. Adapted with permission from [82]. Copyright 2020 Theranostics. (D) Schematic representation of the design and fabrication of supramolecular self-assembly amplified LFIA. Adapted with permission from [162]. Copyright 2019 Wiley-VCH GmbH.



**Figure 11.** (A) Schematic representation for the configuration and the measurement principle of the LFIA based on AuNPs loaded SiNR; Adapted with permission from [154]. Copyright 2014 American Chemical Society. (B) Schematic representation for the SERS-labeled Au/Ag satellites probes for detection of HCG in real serum sample. Adapted with permission from [166]. Copyright 2018 Wiley-VCH. (C) The structural schematic diagram of four different types of nanoprobes with core-shell structures, and the principle of the SERS-based LFIA for detection of cardiac troponin I (cTnI). Adapted with permission from [158]. Copyright 2018 Anal Bioanal Chem. (D) Synthetic route for dual dye-loaded SERS tags and schematic illustration of quantitative detection of human IgM using SERS-based LFIA. Adapted with permission from [176]. Copyright 2018 The Royal Society of Chemistry.

modified with antibodies, the AuNP-SiNRs can measure rabbit IgG at the concentration of  $0.01 \text{ ng mL}^{-1}$ . Consequently, increasing scholars have focused on the construction of various core-satellite nanostructures for the enhanced determination of other target analytes, involving aflatoxin B<sub>2</sub> [153, 157], human chorionic gonadotropin (HCG) [156, 163], microRNA [164], clenbuterol, 17 $\beta$ -estradiol [155], CRP [165], and influenza A antigen [150] with or without additional signal amplification.

Except for providing enhanced colorimetric signal transduction, the composite core-satellite nanostructures can also serve as improved SERS nanoprobes owing to their strong Raman signal enhancement efficiency originated from the formed "hot spots" between core and satellites. Tran et al. developed an Au/Au core-satellite nanocomposite as a SERS nanotag (Figure 11B) [166], which consisted of a 50 nm spherical AuNP core and 17 nm AuNP satellites. This nanocomposite was prepared through electrostatic assembly between the positively charged core and negatively charged satellites, wherein the core was pre-modified with the Raman molecule thio-2-naphthol and bridging molecule (11-mercapto-undecyl)-N,N,N-trimethyl-ammonium. Given the strong plasmonic coupling between core and satellites, many hot spots are generated, and the

Raman signal of reporter molecules in multiple narrow gaps is significantly enhanced. After the electrostatic adsorption of antibodies onto its surface, this Au@Au core-satellite nanoprobes can successfully measure HCG at low concentrations of  $1.6 \text{ mIU mL}^{-1}$  by combining with a home-made portable Raman strip reader.

### Core-shell nanostructures

Previous studies have indicated that the use of SERS signals to replace colorimetric signals of AuNPs is a potential strategy to produce high sensitivity of at least two orders of magnitude increase. The structure of SERS nanotags plays an important role in the LFIA. Plasmonic core-shell nanostructures have attracted great interest attributed to their unique tunable LSPR property, which have been widely adopted for the design and development of SERS nanoprobes [167, 168]. Compared with other nanostructures, the core-shell structure displays many inherent advantages. First, the Raman reporter molecules can be optionally placed at the surface of nanoparticles or embedded in the gap between the core and the shell, or both. Second, the outer metal shell layer can serve as not only a signal amplifier, but also a protective coating to prevent the leakage and degradation of Raman reporter molecules. Third, the multi-layer Raman molecules, multi-shelled nanostructures, and gap size

between the core and the shell in a core-shell nanocomposite are adjustable, following the requirement of the actual application. These characteristics make core-shell nanostructures an ideal option for manufacturing high-performance SERS nanotags. Since its first discovery in 2007, core-shell SERS nanoprobe has attracted considerable attention and extensive research [169]. Given the excellent stability and monodispersity of gold and high enhancement effect of silver, AgNPs@Au-shell [170], AuNPs@Au-shell [171], and AuNPs@Ag-shell [172] SERS nanoprobe has been reported. Blanco-Covián et al. synthesized AuNPs@Ag-shell with 34 nm AuNPs as a core coated with a 12 nm silver shell by using a seed-mediated growth process [132]. The resulting AuNPs@Ag-shell was then modified with the Raman reporter to prepare the SERS nanoprobe. Using this nanoprobe as a signal label, the LOD of this SERS-enhanced LFIA was  $1 \text{ pg mL}^{-1}$  for pneumolysin. As an improvement, Li et al. synthesized AuNPs@Ag-shell SERS nanoprobe (Au<sup>MBA</sup>@Ag) by embedding the Raman reporter (4-mercaptobenzoic acid, MBA) in the junction between the core and the shell, which can effectively protect the Raman molecules from the interference of environmental factors and possible leakage and degradation [173]. Subsequently, several similar AuNPs@Ag-shell SERS nanotags have been developed for the improved LFIA detection of salbutamol [169] and bacteria [174]. In addition, the metal shell number of core-shell nanostructures is increased to enhance the SERS performance. Shen et al. designed AuNPs@Ag-shell@Ag-shell SERS nanoprobe (AuAg<sup>4-ATP</sup>@AgNPs) as a highly sensitive signal to enable high sensitivity in the LFIA [175]. This enhanced SERS performance by increasing the metal shell was further confirmed by a recent comparative study from Wang's group, in which four different SERS nanoprobe, namely, AuNPs, AuNPs@Ag-shell, AgNPs@Au-shell, and AuNPs@Ag-shell@Au-shell, were comprehensively investigated by theoretical analysis and experimental measurement (Figure 11C). The results verified the advantage of AuNPs@Ag-shell@Au-shell in the following aspects, including SERS activity, simulated electromagnetic field, and LFIA sensitivity [158].

Apart from AuNPs@Ag-shell, AgNPs@Au-shell exhibits high sensitivity in SERS-based LFIA due to the higher enhancement effect of AgNPs than AuNPs. Zhang et al. synthesized AgNPs@Au-shell core-shell bimetallic SERS nanotags (AgNBA@Au) with the Raman reporter (methylene blue and Nile blue A) distributed in the interior gap between the two metals [170]. By optimizing the thickness of Au shell, the obtained core-shell SERS nanotags with the highest

intensity were used as labelled probes to improve the multiplex testing of cardiac biomarkers and respiratory tract infection pathogens on the lateral flow test strip. The introduction of multilayer Raman reporter molecules in the core-shell nanostructures has also been reported with improved sensitivity. Jia et al. used AgNPs@Au-shell as a carrier to load two layers of Raman dye 5,50-dithiobis-(2-nitrobenzoic acid) (DTNB) on the surface and in the interior gap to prepare SERS nanotags (Au<sup>DTNB</sup>@Ag<sup>DTNB</sup>, Figure 11D) [176]. Raman spectrum analysis indicates that Au<sup>DTNB</sup>@Ag<sup>DTNB</sup> shows 1.5- and twofold higher SERS signal than those of Au<sup>DTNB</sup>@Ag and Au@Ag<sup>DTNB</sup>, respectively. The LOD of this SERS nanotag for human IgM was  $0.1 \text{ ng mL}^{-1}$ , which was 100-fold more sensitive than the colorimetric strategy.

## 6. Summary and outlook

Conventional colorimetric LFIA using 20–40 nm spherical AuNP as labels has suboptimal sensitivity compared with laboratory-based immunoassays. The growing demands in highly sensitive detection of analytes have necessitated the improvements of the LFIA sensitivity. Various approaches focusing on five major core elements involved in the LFIA system, including sample, receptor, interaction, response, and signal output, have been enabled to reach lower LOD and higher sensitivity. Thanks to their excellent physicochemical properties, NMNPs have presented a wide range of applications in improving LFIA. In particular, the properties of NMNPs could be precisely controlled by tightly tuning their physicochemical parameters, including size, shape, composition, and external structure. Compared with traditional spherical AuNPs, the engineered NMNPs exhibit a series of enhanced performances in optical properties, colloid stabilities, catalytic activities, and multifunctional manipulations, thereby favoring the development of high-performance LFIA. Therefore, in this review, we discussed recently developed strategies using engineered NMNPs with desired properties to improve the sensitivity of LFIA. Despite the incredible progress made in this area, many scientific issues and technical challenges must be addressed prior to applications.

One of the challenges is the large-scale controlled synthesis of high-quality and high-performance engineered NMNPs. Achieving the high-yield and scaling-up synthesis protocol for industrial use is important. The uniformity of nanoparticles in size, shape, composition, and structure has been achieved using the existing synthesis technologies. However, the synthesis robustness and reproducibility of the currently available strategies are too low to meet the requirement of industrial implementations. Therefore,

further efforts should be devoted in developing new synthetic methods that allow nanoparticle products to be highly reproducible and controllable in yield, morphology, composition, and purity.

The analytical performance of NMNPs in LFIA is determined by their properties. In addition, the properties of NMNPs are closely associated with their physicochemical parameters. Thus, the precise control of the physicochemical parameters of NMNPs is crucial to obtain the optimal performance in LFIA applications. Benefiting from the rapid advances in nanoparticle synthesis and characterization, noble metal nanomaterials with controllable structure parameters and charming physicochemical properties have been obtained. Nevertheless, more advanced engineering methods and characterization tools should be introduced. Moreover, theoretical, and mechanistic studies on NMNP engineering should be conducted, thereby contributing to the understanding of spatio-temporal evolution variation of nanoparticles for the control of their structural design. Although several studies have focused on the relationships among the physical parameters of NMNPs, their physicochemical properties, and LFIA performances, further investigations of the correlations among these three factors are greatly encouraged, which can promote the application of the LFIA.

Noble metal nanomaterials with catalytic activities are regarded as potential alternatives to traditional AuNPs in the LFIA because they provide dual functions of plasmonic colorimetric sensing and nanozyme-catalyzed amplification. The catalytic activities of such nanomaterials are closely related to their composition, shape, size, and surface functionalization. For example, the nanozyme activities of catalytic nanomaterials will markedly decrease with surface modification of various ligands as compared with naked nanoparticles. Notably, surface functionalization of nanoparticles with recognition elements (e.g., antibodies) is the premise to ensure the stability and selectivity of labels in LFIA. Thus, the appropriate surface coating must be considered to retain the catalytic activities of nanomaterials and ensure good performance in LFIA. In addition, other structural parameters that affect the enzyme-mimicking activities of nanomaterials, such as size and shape, must be explored to ensure the superior performance of LFIA. Furthermore, the design and synthesis of novel noble metal nanostructures with ultrahigh catalytic activity and the exploration of their potential as catalytic tags for LFIA are good options.

Metal growth amplification is an important strategy for significantly enhancing the colorimetric

signal intensity to enable lower LOD in LFIA. However, most of the current strategies are uncontrollable and limited by the self-nucleating growth of metal ions, thereby resulting in high background signal and low reproducibility, and greatly reducing the accuracy and reliability of methodologies. In this regard, controllable growth techniques with improved robustness are necessary to broaden its application in practice. Analogous to the enzymatic deposition amplification, the metal growth amplification is also a post-amplification technique that is widely used to enhance the colorimetric signal strength after completing the strip. However, these two signal amplification strategies rely on two separate steps: running the strip with a sample solution and treating the completed strip with an enhancer solution, thereby leading to large batch-to-batch differences between strips. Therefore, the ingenious integration of these two independent operations into an entire strip device can reduce the variability and improve the reproducibility. For example, the combination of LFIA using a microfluidic technology can achieve simultaneous detection and signal amplification of samples in a single test system by controlling the direction of flow of different liquids.

Incorporating engineered NMNPs with other functional nanomaterials to increase functionalities has attracted increasing interest in developing various noble metal-based multifunctional composite nanostructures. Given their intrinsic multifunctionality, these hybrid nanomaterials have exhibited superior properties over their parent nanomaterials, thereby endowing traditional LFIA with additional performances, such as magnetic manipulation to separate and enrich analytes from the complex sample and multimodal sensing to improve the analytical efficiency and performance and increase the flexibility of application. Although various approaches have been successfully applied to synthesize these composite nanomaterials, the preparation of high-performance multifunctional nanohybrids remains a challenge, which might be due to the interaction of noble metal components and other functional components. For example, the noble metal nanomaterials can quench the emission of fluorescent materials by the inner filter effect and plasmon-induced resonance energy transfer. Interestingly, when the distance between the noble metal components and fluorescent component is appropriate, a metal-enhanced fluorescence effect can be observed. Therefore, during the synthesis of composite nanomaterials, we should focus on minimizing the adverse interferences and maximizing the beneficial effects between noble metal components

and other components.

Currently, the signal readout modes for noble metal nanomaterials mainly involve the qualitative screening by naked eyes and the quantitative analysis by the dedicated strip readers with multiple signal transduction modes, like fluorescence, photothermal, and SERS signals. Compared with the qualitative screening modes, these alternative signal-reading methods usually rely on the use of strip readers, which can provide better analytical performances and quantitative measurements, but increase the operational difficulty, testing complexity, and cost. Therefore, the exploitation of less sophisticated reader technology to allow the quantitative analysis in LFIA is highly desired.

In summary, this paper systematically reviews the role of noble metal nanoparticle label design in enhancing the LFIA sensitivity. However, it should be mentioned that in addition to the nanoparticle design, other important factors influencing the LFIA sensitivity should be considered including the screening of more efficient recognition molecules, the bioactivities of antibodies coupled onto the surface of NMNPs, the membrane selection (*e.g.*, aperture), the anti-fouling sensing ability, the sample pretreatment modification, the migration behavior of nanoparticles, the development of signal amplification strategies, and the strip device engineering. Several relevant research papers that focus on the above perspectives to enable sensitive or even ultrasensitive LFIA test strips have been authorized recently [43, 46, 47, 197-203]. Eventually, we hope that with these challenges well addressed, more engineered noble metal nanostructures can earn their place in LFIA applications in addition to traditional AuNPs.

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## Author Contributions

Conceptualization, X. Huang, Y. Xiong; Graphics, X. Chen and X. Huang; Resources (selection and review of literature papers), X. Chen, L. Ding; Writing (original draft), X. Chen, L. Ding; Writing (review & editing), X. Huang, Y. Xiong.

## Competing Interests

The authors have declared that no competing

interest exists.

## References

1. Miller BS, Bezinge L, Gliddon HD, Huang D, Dold G, Gray ER, et al. Spin-enhanced nanodiamond biosensing for ultrasensitive diagnostics. *Nature*. 2020; 587: 588-93.
2. Chen R, Ren C, Liu M, Ge X, Qu M, Zhou X, et al. Early Detection of SARS-CoV-2 seroconversion in humans with aggregation-induced near-infrared emission nanoparticle-labeled lateral flow immunoassay. *ACS Nano*. 2021; 15: 8996-9004.
3. Sciuotto G, Zangheri M, Anfossi L, Guardigli M, Prati S, Mirasoli M, et al. Miniaturized biosensors to preserve and monitor cultural heritage: from medical to conservation diagnosis. *Angew Chem Int Ed Engl*. 2018; 57: 7385-9.
4. Guo J, Chen S, Tian S, Liu K, Ni J, Zhao M, et al. 5G-enabled ultra-sensitive fluorescence sensor for proactive prognosis of COVID-19. *Biosens Bioelectron*. 2021; 181: 113160.
5. Ji T, Xu X, Wang X, Cao N, Han X, Wang M, et al. Background-free chromatographic detection of sepsis biomarker in clinical human serum through near-infrared to near-infrared upconversion immunolabeling. *ACS Nano*. 2020; 14: 16864-16874.
6. Zhou Y, Ding L, Wu Y, Huang X, Lai W, Xiong Y. Emerging strategies to develop sensitive AuNP-based ICTS nanosensors. *TrAC, Trends Anal Chem*. 2019; 112: 147-60.
7. de Puig H, Bosch I, Gehrke L, Hamad-schifferli K. Challenges of the nano-bio interface in lateral flow and dipstick immunoassays. *Trends Biotechnol*. 2017; 35: 1169-80.
8. Huang X, Aguilar ZP, Xu H, Lai W, Xiong Y. Membrane-based lateral flow immunochromatographic strip with nanoparticles as reporters for detection: A review. *Biosens Bioelectron*. 2016; 75: 166-80.
9. Znoyko SL, Orlov AV, Pushkarev AV, Mochalova EN, Guteneva NV, Lunin AV, et al. Ultrasensitive quantitative detection of small molecules with rapid lateral-flow assay based on high-affinity bifunctional ligand and magnetic nanolabels. *Anal Chim Acta*. 2018; 1034: 161-7.
10. Wang H, Rao H, Luo M, Xue X, Xue Z, Lu X. Noble metal nanoparticles growth-based colorimetric strategies: from monocolorimetric to multicolorimetric sensors. *Coord Chem Rev*. 2019; 398: 113003.
11. Ma X, He S, Qiu B, Luo F, Guo L, Lin Z. Noble metal nanoparticle-based multicolor immunoassays: an approach toward visual quantification of the analytes with the naked eye. *ACS Sens*. 2019; 4: 782-91.
12. Jakab A, Rosman C, Khalavka Y, Becker J, Trugler A, Hohenester U, et al. Highly sensitive plasmonic silver nanorods. *ACS Nano*. 2011; 5: 6880-5.
13. Xia X, Zhang J, Lu N, Kim MJ, Ghale K, Xu Y, et al. Pd-Ir core-shell nanocubes: a type of highly efficient and versatile peroxidase mimic. *ACS Nano*. 2015; 9: 9994-10004.
14. Kustner B, Gellner M, Schutz M, Schoppler F, Marx A, Strobel P, et al. SERS labels for red laser excitation: silica-encapsulated SAMs on tunable gold/silver nanoshells. *Angew Chem Int Ed Engl*. 2009; 48: 1950-3.
15. Pyo K, Thanthirige VD, Kwak K, Pandurangan P, Ramakrishna G, Lee D. Ultrabright luminescence from gold nanoclusters: rigidifying the Au(I)-thiolate shell. *J Am Chem Soc*. 2015; 137: 8244-50.
16. Kang X, Wang S, Song Y, Jin S, Sun G, Yu H, et al. Bimetallic Au<sub>2</sub>-Cu<sub>6</sub> nanoclusters: strong luminescence induced by the aggregation of copper(I) complexes with gold(0) species. *Angew Chem Int Ed Engl*. 2016; 55: 3611-4.
17. Yahia-Ammar A, Sierra D, Merola F, Hildebrandt N, Le Guevel X. Self-assembled gold nanoclusters for bright fluorescence imaging and enhanced drug delivery. *ACS Nano*. 2016; 10: 2591-9.
18. Goswami N, Yao Q, Luo Z, Li J, Chen T, Xie J. Luminescent metal nanoclusters with aggregation-induced emission. *J Phys Chem Lett*. 2016; 7: 962-75.
19. Chen L-Y, Wang C-W, Yuan Z, Chang H-T. Fluorescent gold nanoclusters: recent advances in sensing and imaging. *Anal Chem*. 2015; 87: 216-29.
20. Navlani-García M, Salinas-Torres D, Mori K, Kuwahara Y, Yamashita H. Tailoring the size and shape of colloidal noble metal nanocrystals as a valuable tool in catalysis. *Catal Surv Asia*. 2019; 23: 127-48.
21. Hong JW, Kang SW, Choi BS, Kim D, Lee SB, Han SW. Controlled synthesis of Pd-Pt alloy hollow nanostructures with enhanced catalytic activities for oxygen reduction. *ACS Nano*. 2012; 6: 2410-9.
22. Zhang D, Huang L, Liu B, Ni H, Sun L, Su E, et al. Quantitative and ultrasensitive detection of multiplex cardiac biomarkers in lateral flow assay with core-shell SERS nanotags. *Biosens Bioelectron*. 2018; 106: 204-11.
23. Peng T, Wang J, Zhao S, Zeng Y, Zheng P, Liang D, et al. Highly luminescent green-emitting Au nanocluster-based multiplex lateral flow immunoassay for ultrasensitive detection of clenbuterol and ractopamine. *Anal Chim Acta*. 2018; 1040: 143-9.
24. Loynachan CN, Thomas MR, Gray ER, Richards DA, Kim J, Miller BS, et al. Platinum nanocatalyst amplification: redefining the gold standard for lateral flow immunoassays with ultrabroad dynamic range. *ACS Nano*. 2018; 12: 279-88.
25. Ye H, Xi Z, Magloire K, Xia X. Noble-metal nanostructures as highly efficient peroxidase mimics. *Chem Nano Mat*. 2019; 5: 860-8.
26. Rycenga M, Cobley CM, Zeng J, Li W, Moran CH, Zhang Q, et al. Controlling the synthesis and assembly of silver nanostructures for plasmonic applications. *Chem Rev*. 2011; 111: 3669-712.

27. Xi Z, Ye H, Xia X. Engineered noble-metal nanostructures for *in vitro* diagnostics. *Chem mater.* 2018; 30: 8391-414.
28. Peng S, McMahon JM, Schatz GC, Gray SK, Sun Y. Reversing the size-dependence of surface plasmon resonances. *Proc Natl Acad Sci U S A.* 2010; 107: 14530-4.
29. Park J, Kim Y. Effect of shape of silver nanoplates on the enhancement of surface plasmon resonance (SPR) signals. *J Nanosci Nanotechnol.* 2008; 8: 5026-9.
30. Jha R, Sharma AK. Chalcogenide glass prism based SPR sensor with Ag-Au bimetallic nanoparticle alloy in infrared wavelength region. *J Opt A Pure Appl Opt* 2009; 11:045502.
31. Belhout SA, Baptista FR, Devereux SJ, Parker AW, Ward AD, Quinn SJ. Preparation of polymer gold nanoparticle composites with tunable plasmon coupling and their application as SERS substrates. *Nanoscale.* 2019; 11: 19884-94.
32. Khlebtsov BN, Tumskiy RS, Burov AM, Pylaev TE, Khlebtsov NG. Quantifying the numbers of gold nanoparticles in the test zone of lateral flow immunoassay strips. *ACS Appl Nano Mater.* 2019; 2: 5020-8.
33. Zhan L, Guo SZ, Song F, Gong Y, Xu F, Boulware DR, et al. The role of nanoparticle design in determining analytical performance of lateral flow immunoassays. *Nano Lett.* 2017; 17: 7207-12.
34. Gao X, Boryczka J, Zheng P, Kasani S, Yang F, Engler-Chiurazzi EB, et al. A "hot spot"-enhanced paper lateral flow assay for ultrasensitive detection of traumatic brain injury biomarker S-100 $\beta$  in blood plasma. *Biosens Bioelectron.* 2021; 177: 112967.
35. Zhang L, Huang Y, Wang J, Rong Y, Lai W, Zhang J, et al. Hierarchical flowerlike gold nanoparticles labeled immunochromatography test strip for highly sensitive detection of *Escherichia coli* O157:H7. *Langmuir.* 2015; 31: 5537-44.
36. Gao Z, Ye H, Tang D, Tao J, Habibi S, Minerick A, et al. Platinum-decorated gold nanoparticles with dual functionalities for ultrasensitive colorimetric *in vitro* diagnostics. *Nano Lett.* 2017; 17: 5572-9.
37. Hao L, Leng Y, Zeng L, Chen X, Chen J, Duan H, et al. Core-shell-heterostructured magnetic-plasmonic nanoassemblies with highly retained magnetic-plasmonic activities for ultrasensitive bioanalysis in complex matrix. *Adv Sci.* 2020; 7: 1902433.
38. Wang J, Jiang C, Jin J, Huang L, Yu W, Su B, et al. Ratiometric fluorescent lateral flow immunoassay for point-of-care testing of acute myocardial infarction. *Angew Chem Int Ed Engl.* 2021; 60: 13042-9.
39. Pan Y, Wei X, Guo X, Wang H, Song H, Pan C, et al. Immunoassay based on Au-Ag bimetallic nanoclusters for colorimetric/fluorescent double biosensing of dicofol. *Biosens Bioelectron.* 2021; 194: 113611.
40. Huang L, Jin J, Ao L, Jiang C, Zhang Y, Wen HM, et al. Hierarchical plasmonic-fluorescent labels for highly sensitive lateral flow immunoassay with flexible dual-modal switching. *ACS Appl Mater Interfaces.* 2020; 12: 58149-60.
41. Wang C, Wang C, Wang X, Wang K, Zhu Y, Rong Z, et al. Magnetic SERS strip for sensitive and simultaneous detection of respiratory viruses. *ACS Appl Mater Interfaces.* 2019; 11: 19495-505.
42. Scholz F, Ruttinger L, Heckmann T, Freund L, Gad AM, Fischer T, et al. Carboxyl functionalized gold nanorods for sensitive visual detection of biomolecules. *Biosens Bioelectron.* 2020; 164: 112324.
43. Liu Y, Zhan L, Qin Z, Sackrison J, Bischof JC. Ultrasensitive and highly specific lateral flow Assays for point-of-care diagnosis. *ACS Nano.* 2021; 15: 3593-611.
44. Huang Y, Xu T, Wang W, Wen Y, Li K, Qian L, et al. Lateral flow biosensors based on the use of micro- and nanomaterials: a review on recent developments. *Microchim Acta.* 2019; 187: 70.
45. Yang H, Xu W, Zhou Y. Signal amplification in immunoassays by using noble metal nanoparticles: a review. *Microchim Acta.* 2019; 186: 859.
46. Ye H, Liu Y, Zhan L, Liu Y, Qin Z. Signal amplification and quantification on lateral flow assays by laser excitation of plasmonic nanomaterials. *Theranostics.* 2020; 10: 4359-73.
47. Shirshahi V, Liu G. Enhancing the analytical performance of paper lateral flow assays: From chemistry to engineering. *TrAC, Trends Anal Chem.* 2021; 136:116200
48. Huang Z, Hu S, Xiong Y, Wei H, Xu H, Duan H, et al. Application and development of superparamagnetic nanoparticles in sample pretreatment and immunochromatographic assay. *TrAC, Trends Anal Chem.* 2019; 114: 151-70.
49. Jans H, Huo Q. Gold nanoparticle-enabled biological and chemical detection and analysis. *Chem Soc Rev.* 2012; 41: 2849-66.
50. Yang X, Yang M, Pang B, Vara M, Xia Y. Gold nanomaterials at work in biomedicine. *Chem Rev.* 2015; 115: 10410-88.
51. Swierczewska M, Lee S, Chen X. The design and application of fluorophore-gold nanoparticle activatable probes. *Phys Chem Chem Phys.* 2011; 13: 9929-41.
52. Jain PK, Lee KS, El-Sayed IH, El-Sayed MA. Calculated absorption and scattering properties of gold nanoparticles of different size, shape, and composition: applications in biological imaging and biomedicine. *J Phys Chem.* 2006; 110: 7238-48.
53. Li J, Duan H, Xu P, Huang X, Xiong Y. Effect of different-sized spherical gold nanoparticles grown layer by layer on the sensitivity of an immunochromatographic assay. *RSC Adv.* 2016; 6: 26178-85.
54. Kaur J, Singh KV, Boro R, Thampi K, Raje M, Varshney GC, et al. Immunochromatographic dipstick assay format using gold nanoparticles labeled protein-hapten conjugate for the detection of atrazine. *Environ Sci Technol.* 2007; 41: 5028-36.
55. Fu E, Liang T, Houghtaling J, Ramachandran S, Ramsey SA, Lutz B, et al. Enhanced sensitivity of lateral flow tests using a two-dimensional paper network format. *Anal Chem.* 2011; 83: 7941-6.
56. Rastogi SK, Gibson CM, Branan JR, Eric Aston D, Larry Branan A, Hrdlicka PJ. DNA detection on lateral flow test strips: enhanced signal sensitivity using LNA-conjugated gold nanoparticles. *Chem Commun.* 2012; 48: 7714-7716.
57. Bu T, Huang Q, Yan L, Huang L, Zhang M, Yang Q, et al. Ultra technically-simple and sensitive detection for *Salmonella enteritidis* by immunochromatographic assay based on gold growth. *Food Control.* 2018; 84: 536-43.
58. Fu J, Zhou Y, Huang X, Zhang W, Wu Y, Fang H, et al. Dramatically enhanced immunochromatographic assay using cascade signal amplification for ultrasensitive detection of *Escherichia coli* O157:H7 in milk. *J Agric Food Chem.* 2020; 68: 1118-25.
59. Cho I-H, Seo S-M, Paek E-H, Paek S-H. Immunogold-silver staining-on-a-chip biosensor based on cross-flow chromatography. *Journal of Chromatography B.* 2010; 878: 271-7.
60. Yang W, Li XB, Liu GW, Zhang BB, Zhang Y, Kong T, et al. A colloidal gold probe-based silver enhancement immunochromatographic assay for the rapid detection of abrin-a. *Biosens Bioelectron.* 2011; 26: 3710-3.
61. Tian M, Lei L, Xie W, Yang Q, Li CM, Liu Y. Copper deposition-induced efficient signal amplification for ultrasensitive lateral flow immunoassay. *Sens Actuators B.* 2019; 282: 96-103.
62. Zhou Y, Chen Y, Liu Y, Fang H, Huang X, Leng Y, et al. Controlled copper *in situ* growth-amplified lateral flow sensors for sensitive, reliable, and field-deployable infectious disease diagnostics. *Biosens Bioelectron.* 2021; 171: 112753.
63. de Oliveira PFM, Torresi RM, Emmerling F, Camargo PHC. Challenges and opportunities in the bottom-up mechanochemical synthesis of noble metal nanoparticles. *J Mater Chem A.* 2020; 8: 16114-41.
64. Ruan W, Lu Z, Zhou T, Zhao B, Niu L. Surface micropatterning technique for surface-enhanced Raman scattering analysis. *Anal Methods.* 2010; 2: 684-687.
65. Rival JV, Mymoona P, Lakshmi KM, Nonappa, Pradeep T, Shibu ES. Self-assembly of precision noble metal nanoclusters: hierarchical structural complexity, colloidal superstructures, and applications. *Small.* 2021; 17: 2005718.
66. Pelletier F, Thiébaud B. Improvement of noble metal based photocatalysts by spray pyrolysis processes. *Johnson Matthey Technol Rev.* 2016; 60: 39-54.
67. Suryanarayana C. Mechanical alloying: a novel technique to synthesize advanced materials. *Research.* 2019; 2019: 4219812.
68. Arakelyan SM, Veiko VP, Kutrovskaya SV, Kucherik AO, Osipov AV, Vartanyan TA, et al. Reliable and well-controlled synthesis of noble metal nanoparticles by continuous wave laser ablation in different liquids for deposition of thin films with variable optical properties. *J Nanopart Res.* 2016; 18: 155.
69. Ossi PM, Neri F, Santo N, Trusso S. Noble metal nanoparticles produced by nanosecond laser ablation. *Applied Physics A.* 2011; 104: 829-37.
70. Hoepfener S, Maoz R, Cohen SR, Chi L, Fuchs H, Sagiv J. Metal nanoparticles, nanowires, and contact electrodes self-assembled on patterned monolayer templates—a bottom-up chemical approach. *Adv Mater.* 2002; 14: 1036-41.
71. Dintinger J, Mühlig S, Rockstuhl C, Scharf T. A bottom-up approach to fabricate optical metamaterials by self-assembled metallic nanoparticles. *Opt Mater Express.* 2012; 2: 269-78.
72. Luechinger NA, Grass RN, Athanassiou EK, Stark WJ. Bottom-up fabrication of metal/metal nanocomposites from nanoparticles of immiscible metals. *Chem mater.* 2009; 22: 155-60.
73. Habibullah G, Viktorova J, Ruml T. Current strategies for noble metal nanoparticle synthesis. *Nanoscale Res Lett.* 2021; 16: 47.
74. Liu J, He F, Gunn TM, Zhao D, Roberts CB. Precise seed-mediated growth and size-controlled synthesis of palladium nanoparticles using a green chemistry approach. *Langmuir.* 2009; 25: 7116-28.
75. Niu J, Zhu T, Liu Z. One-step seed-mediated growth of 30-150 nm quasispherical gold nanoparticles with 2-mercaptosuccinic acid as a new reducing agent. *Nanotechnology.* 2007; 18: 325607.
76. Zheng Y, Zhong X, Li Z, Xia Y. Successive, Seed-mediated growth for the synthesis of single-crystal gold nanospheres with uniform diameters controlled in the range of 5-150 nm. *Part Part Syst Charact.* 2014; 31: 266-73.
77. Zhang Q, Li W, Moran C, Zeng J, Chen J, Wen L-P, et al. Seed-mediated synthesis of Ag nanocubes with controllable edge lengths in the range of 30-200 nm and comparison of their optical properties. *J Am Chem Soc.* 2010; 132: 11372-8.
78. Bastus NG, Comenge J, Puntes V. Kinetically controlled seeded growth synthesis of citrate-stabilized gold nanoparticles of up to 200 nm: size focusing versus ostwald ripening. *Langmuir.* 2011; 27: 11098-105.
79. Brown KR, Walter DG, Natan MJ. Seeding of colloidal Au nanoparticle solutions. 2. improved control of particle size and shape. *Chem Mater.* 2000; 12: 306-13.
80. Lu X, Rycenga M, Skrabalak SE, Wiley B, Xia Y. Chemical synthesis of novel plasmonic nanoparticles. *Annu Rev Phys Chem.* 2009; 60: 167-92.
81. Huang X, Jain PK, El-Sayed IH, El-Sayed MA. Gold nanoparticles: interesting optical properties and recent applications in cancer diagnostics and therapy. *Future Medicine.* 2007; 681-693.

82. Chen X, Leng Y, Hao L, Duan H, Yuan J, Zhang W, et al. Self-assembled colloidal gold superparticles to enhance the sensitivity of lateral flow immunoassays with sandwich format. *Theranostics*. 2020; 10: 3737-48.
83. Jeon J, Lee SH, Jeong Y, Kim K, Choi N, Choo J. Improvement of reproducibility and thermal stability of surface-enhanced Raman scattering-based lateral flow assay strips using silica-encapsulated gold nanoparticles. *Sens Actuators B*. 2020; 321.
84. Fang C, Chen Z, Li L, Xia J. Barcode lateral flow immunochromatographic strip for prostate acid phosphatase determination. *J Pharm Biomed Anal*. 2011; 56: 1035-40.
85. Laitinen MP, Vuento M. Affinity immunosensor for milk progesterone: identification of critical parameters. *Biosens Bioelectron*. 1996; 11: 1207-14.
86. Safenkova I, Zherdev A, Dzantiev B. Factors influencing the detection limit of the lateral-flow sandwich immunoassay: a case study with potato virus X. *Anal Bioanal Chem*. 2012; 403: 1595-605.
87. Wang J-Y, Chen M-H, Sheng Z-C, Liu D-F, Wu S-S, Lai W-H. Development of colloidal gold immunochromatographic signal-amplifying system for ultrasensitive detection of *Escherichia coli* O157:H7 in milk. *RSC Adv*. 2015; 5: 62300-5.
88. Wada A, Sakoda Y, Oyamada T, Kida H. Development of a highly sensitive immunochromatographic detection kit for H5 influenza virus hemagglutinin using silver amplification. *J Virol Methods*. 2011; 178: 82-6.
89. Li J, Zou M, Chen Y, Xue Q, Zhang F, Li B, et al. Gold immunochromatographic strips for enhanced detection of avian influenza and Newcastle disease viruses. *Anal Chim Acta*. 2013; 782: 54-8.
90. Horton J, Swinburne S, O'Sullivan M. A novel, rapid, single-step immunochromatographic procedure for the detection of mouse immunoglobulin. *J Immunol Methods*. 1991; 140: 131-4.
91. Yu Q, Li H, Li C, Zhang S, Shen J, Wang Z. Gold nanoparticles-based lateral flow immunoassay with silver staining for simultaneous detection of fumonisin B1 and deoxynivalenol. *Food Control*. 2015; 54: 347-52.
92. Panferov VG, Safenkova IV, Varitsev YA, Drenova NV, Kornev KP, Zherdev AV, et al. Development of the sensitive lateral flow immunoassay with silver enhancement for the detection of *Ralstonia solanacearum* in potato tubers. *Talanta*. 2016; 152: 521-30.
93. Rodriguez MO, Covian LB, Garcia AC, Blanco-Lopez MC. Silver and gold enhancement methods for lateral flow immunoassays. *Talanta*. 2016; 148: 272-8.
94. Panferov VG, Safenkova IV, Byzova NA, Varitsev YA, Zherdev AV, Dzantiev BB. Silver-enhanced lateral flow immunoassay for highly-sensitive detection of potato leafroll virus. *Food Agric Immunol*. 2017; 29: 445-57.
95. Kim W, Lee S, Jeon S. Enhanced sensitivity of lateral flow immunoassays by using water-soluble nanofibers and silver-enhancement reactions. *Sens Actuators B*. 2018; 273: 1323-7.
96. Broger T, Sossen B, du Toit E, Kerckhoff AD, Schutz C, Ivanova Reipold E, et al. Novel lipoarabinomannan point-of-care tuberculosis test for people with HIV: a diagnostic accuracy study. *Lancet Infect Dis*. 2019; 19: 852-61.
97. Motl NE, Smith AF, DeSantis CJ, Skrabalak SE. Engineering plasmonic metal colloids through composition and structural design. *Chem Soc Rev*. 2014; 43: 3823-34.
98. Xia Y, Xiong Y, Lim B, Skrabalak SE. Shape-controlled synthesis of metal nanocrystals: simple chemistry meets complex physics? *Angew Chem Int Ed Engl*. 2009; 48: 60-103.
99. Somorjai GA, Park JY. Colloid science of metal nanoparticle catalysts in 2D and 3D structures. challenges of nucleation, growth, composition, particle shape, size-control and their influence on activity and selectivity. *Top Catal*. 2008; 49: 126-35.
100. Grzelczak M, Perez-Juste J, Mulvaney P, Liz-Marzan LM. Shape control in gold nanoparticle synthesis. *Chem Soc Rev*. 2008; 37: 1783-91.
101. Niu W, Zhang L, Xu G. Seed-mediated growth of noble metal nanocrystals: crystal growth and shape control. *Nanoscale*. 2013; 5: 3172-81.
102. Yang TH, Shi Y, Janssen A, Xia Y. Surface capping agents and their roles in shape-controlled synthesis of colloidal metal nanocrystals. *Angew Chem Int Ed*. 2020; 59: 15378-401.
103. Xia Y, Xia X, Peng HC. Shape-controlled synthesis of colloidal metal nanocrystals: thermodynamic versus kinetic products. *J Am Chem Soc*. 2015; 137: 7947-66.
104. <https://nanocomposix.com/blogs/news/fortis-life-sciences-acquires-nanocomposix>
105. Reguera J, Langer J, Jimenez de Aberasturi D, Liz-Marzan LM. Anisotropic metal nanoparticles for surface enhanced Raman scattering. *Chem Soc Rev*. 2017; 46: 3866-85.
106. Wang W, Pang Y, Yan J, Wang G, Suo H, Zhao C, et al. Facile synthesis of hollow urchin-like gold nanoparticles and their catalytic activity. *Gold Bull*. 2012; 45: 91-8.
107. Xu Q, Guo X, Xu L, Ying Y, Wu Y, Wen Y, et al. Template-free synthesis of SERS-active gold nanopopcorn for rapid detection of chlorpyrifos residues. *Sens Actuators B*. 2017; 241: 1008-13.
108. Xie J, Zhang Q, Lee JY, Wang DI. The synthesis of SERS-active gold nanoflower tags for *in vivo* applications. *ACS Nano*. 2008; 2: 2473-80.
109. Serebrennikova K, Samsonova J, Osipov A. Hierarchical nanogold labels to improve the sensitivity of lateral flow immunoassay. *Nanomicro Lett*. 2018; 10: 24.
110. Ji Y, Ren M, Li Y, Huang Z, Shu M, Yang H, et al. Detection of aflatoxin B1 with immunochromatographic test strips: Enhanced signal sensitivity using gold nanoflowers. *Talanta*. 2015; 142: 206-12.
111. Xu P, Li J, Huang X, Duan H, Ji Y, Xiong Y. Effect of the tip length of multi-branched AuNFs on the detection performance of immunochromatographic assays. *Anal Methods*. 2016; 8: 3316-24.
112. Zhang W, Duan H, Chen R, Ma T, Zeng L, Leng Y, et al. Effect of different-sized gold nanoflowers on the detection performance of immunochromatographic assay for human chorionic gonadotropin detection. *Talanta*. 2019; 194: 604-10.
113. Maneprakorn W, Bamrungsap S, Apiwat C, Wiriyachaiyorn N. Surface-enhanced Raman scattering based lateral flow immunochromatographic assay for sensitive influenza detection. *RSC Adv*. 2016; 6: 112079-85.
114. Wang J, Zhang L, Huang Y, Dandapat A, Dai L, Zhang G, et al. Hollow Au-Ag nanoparticles labeled immunochromatography strip for highly sensitive detection of clenbuterol. *Sci Rep*. 2017; 7: 41419.
115. Yang Y, Ozsoz M, Liu G. Gold nanocage-based lateral flow immunoassay for immunoglobulin G. *Microchim Acta*. 2017; 184: 2023-9.
116. Near RD, Hayden SC, Hunter RE, Thackston D, El-Sayed MA. Rapid and efficient prediction of optical extinction coefficients for gold nanospheres and gold nanorods. *J Phys Chem C*. 2013; 117: 23950-5.
117. Perezjuste J, Pastorizasantos I, Lizmarzan L, Mulvaney P. Gold nanorods: synthesis, characterization and applications. *Coord Chem Rev*. 2005; 249: 1870-901.
118. Venkataramasubramani M, Tang L. Development of gold nanorod lateral flow test for quantitative multi-analyte detection. 25th Southern Biomedical Engineering Conference 2009, 15-17 May 2009, Miami, Florida, USA: Springer; 2009. p. 199-202.
119. Deng D, Yang H, Liu C, Zhao K, Li J, Deng A. Ultrasensitive detection of Sudan I in food samples by a quantitative immunochromatographic assay. *Food Chem*. 2019; 277: 595-603.
120. He D, Wu Z, Cui B, Xu E, Jin Z. Establishment of a dual mode immunochromatographic assay for *Campylobacter jejuni* detection. *Food Chem*. 2019; 289: 708-13.
121. Mohd Hanafiah K, Arifin N, Bustami Y, Noordin R, Garcia M, Anderson D. Development of multiplexed infectious disease lateral flow assays: challenges and opportunities. *Diagnostics (Basel)*. 2017; 7: 51.
122. Yen CW, de Puig H, Tam JO, Gomez-Marquez J, Bosch I, Hamad-Schifferli K, et al. Multicolored silver nanoparticles for multiplexed disease diagnostics: distinguishing dengue, yellow fever, and Ebola viruses. *Lab Chip*. 2015; 15: 1638-41.
123. Wu Y, Zhou Y, Huang H, Chen X, Leng Y, Lai W, et al. Engineered gold nanoparticles as multicolor labels for simultaneous multi-mycotoxin detection on the immunochromatographic test strip nanosensor. *Sens Actuators B*. 2020; 316: 128107.
124. Xu Y, Chen L, Wang X, Yao W, Zhang Q. Recent advances in noble metal based composite nanocatalysts: colloidal synthesis, properties, and catalytic applications. *Nanoscale*. 2015; 7: 10559-83.
125. Liu X, Wang K, Cao B, Shen L, Ke X, Cui D, et al. Multifunctional nano-sunflowers with color-magnetic-raman properties for multimodal lateralflow immunoassay. *Anal Chem*. 2021; 93: 3626-34.
126. Fu Q, Liu HL, Wu Z, Liu A, Yao C, Li X, et al. Rough surface Au@Ag core-shell nanoparticles to fabricating high sensitivity SERS immunochromatographic sensors. *J Nanobiotechnology*. 2015; 13: 81.
127. Zhao S, Bu T, Yang K, Xu Z, Bai F, He K, et al. Immunochromatographic assay based on polydopamine-decorated Iridium Oxide nanoparticles for the rapid detection of salbutamol in food samples. *ACS Appl Mater Interfaces*. 2021; 13: 28899-907.
128. Lai X, Zhang G, Zeng L, Xiao X, Peng J, Guo P, et al. Synthesis of pDA-mediated magnetic bimetallic nanozyme and Its application in immunochromatographic assay. *ACS Appl Mater Interfaces*. 2021; 13: 1413-23.
129. Xia Y, Gilroy KD, Peng HC, Xia X. Seed-mediated growth of colloidal metal nanocrystals. *Angew Chem Int Ed Engl*. 2017; 56: 60-95.
130. Lim B, Jiang M, Camargo PH, Cho EC, Tao J, Lu X, et al. Pd-Pt bimetallic nanodendrites with high activity for oxygen reduction. *Science*. 2009; 324: 1302-5.
131. Chen M, Wu B, Yang J, Zheng N. Small adsorbate-assisted shape control of Pd and Pt nanocrystals. *Adv Mater*. 2012; 24: 862-79.
132. Blanco-Covian L, Montes-Garcia V, Girard A, Fernandez-Abedul MT, Perez-Juste J, Pastoriza-Santos I, et al. Au@Ag SERRS tags coupled to a lateral flow immunoassay for the sensitive detection of pneumolysin. *Nanoscale*. 2017; 9: 2051-8.
133. Cheng N, Song Y, Zeinhom MMA, Chang YC, Sheng L, Li H, et al. Nanozyme-mediated dual immunoassay integrated with smartphone for use in simultaneous detection of pathogens. *ACS Appl Mater Interfaces*. 2017; 9: 40671-80.
134. Xu S, Zhang G, Fang B, Xiong Q, Duan H, Lai W. Lateral flow immunoassay based on polydopamine-coated gold nanoparticles for the sensitive detection of zearalenone in maize. *ACS Appl Mater Interfaces*. 2019; 11: 31283-90.
135. Kim HM, Kim J, An J, Bock S, Pham XH, Huynh KH, et al. Au-Ag assembled on silica nanopores for visual semi-quantitative detection of prostate-specific antigen. *J Nanobiotechnology*. 2021; 19: 73.

136. Liu R, Guo J, Ma G, Jiang P, Zhang D, Li D, et al. Alloyed crystalline Au–Ag hollow nanostructures with high chemical stability and catalytic performance. *ACS Appl Mater Interfaces*. 2016; 8: 16833–44.
137. Xia X, Zhang J, Lu N, Kim MJ, Ghale K, Xu Y, et al. Pd–Ir core-shell nanocubes: A type of highly efficient and versatile peroxidase mimic. *ACS Nano*. 2015; 9: 9994–10004.
138. Huang D, Lin B, Song Y, Guan Z, Cheng J, Zhu Z, et al. Staining traditional colloidal gold test strips with Pt nanoshell enables quantitative point-of-care testing with simple and portable pressure meter readout. *ACS Appl Mater Interfaces*. 2019; 11: 1800–6.
139. Kim M, Kim MS, Kweon SH, Jeong S, Kang MH, Kim MI, et al. Simple and sensitive point-of-care bioassay system based on hierarchically structured znyzyme-mimetic nanoparticles. *Adv Healthc Mater*. 2015; 4: 1311–6.
140. Yang D, Ma J, Zhang Q, Li N, Yang J, Raju PA, et al. Polyelectrolyte-coated gold magnetic nanoparticles for immunoassay development: toward point of care diagnostics for syphilis screening. *Anal Chem*. 2013; 85: 6688–95.
141. Hu J, Jiang YZ, Wu LL, Wu Z, Bi Y, Wong G, et al. Dual-signal readout nanospheres for rapid point-of-care detection of ebola virus glycoprotein. *Anal Chem*. 2017; 89: 13105–11.
142. Yang H, He Q, Chen Y, Shen D, Xiao H, Eremin SA, et al. Platinum nanoflowers with peroxidase-like property in a dual immunoassay for dehydroepiandrosterone. *Microchim Acta*. 2020; 187: 592.
143. Cheng N, Shi Q, Zhu C, Li S, Lin Y, Du D. Pt–Ni(OH)<sub>2</sub> nanosheets amplified two-way lateral flow immunoassays with smartphone readout for quantification of pesticides. *Biosens Bioelectron*. 2019; 142: 111498.
144. Wu Z, He D, Xu E, Jiao A, Chughtai MFJ, Jin Z. Rapid detection of beta-conglutinin with a novel lateral flow aptasensor assisted by immunomagnetic enrichment and enzyme signal amplification. *Food Chem*. 2018; 269: 375–9.
145. Schmidtke C, Klouft H, Bastús NG, Merkl J-P, Tran H, Flessau S, et al. A general route towards well-defined magneto- or fluorescent-plasmonic nanohybrids. *Nanoscale*. 2013; 5: 11783–94.
146. He X, Zhao Z, Xiong L-H, Gao PF, Peng C, Li RS, et al. Redox-active AIEgen-derived plasmonic and fluorescent core@shell nanoparticles for multimodality bioimaging. *J Am Chem Soc*. 2018; 140: 6904–11.
147. Shi R, Cao Y, Bao Y, Zhao Y, Waterhouse GIN, Fang Z, et al. Self-assembled Au/CdSe nanocrystal clusters for plasmon-mediated photocatalytic hydrogen evolution. *Adv Mater*. 2017; 29: 1700803.
148. Jain PK, El-Sayed MA. Universal scaling of plasmon coupling in metal nanostructures: extension from particle pairs to nanoshells. *Nano Lett*. 2007; 7: 2854–8.
149. Khlebtsov BN, Bratashov DN, Byzova NA, Dzantiev BB, Khlebtsov NG. SERS-based lateral flow immunoassay of troponin I by using gap-enhanced Raman tags. *Nano Res*. 2018; 12: 413–20.
150. Matsumura Y, Enomoto Y, Takahashi M, Maenosono S. Metal (Au, Pt) nanoparticle-latex nanocomposites as probes for immunochromatographic test strips with enhanced sensitivity. *ACS Appl Mater Interfaces*. 2018; 10: 31977–87.
151. Hu J, Wang L, Li F, Han YL, Lin M, Lu TJ, et al. Oligonucleotide-linked gold nanoparticle aggregates for enhanced sensitivity in lateral flow assays. *Lab Chip*. 2013; 13: 4352–7.
152. Chen H, Hu H, Tao C, Clauson RM, Moncion I, Luan X, et al. Self-assembled Au@Fe core/satellite magnetic nanoparticles for versatile biomolecule functionalization. *ACS Appl Mater Interfaces*. 2019; 11: 23858–69.
153. Tang D, Saucedo JC, Lin Z, Ott S, Basova E, Goryacheva I, et al. Magnetic nanogold microspheres-based lateral-flow immunodipstick for rapid detection of aflatoxin B<sub>2</sub> in food. *Biosens Bioelectron*. 2009; 25: 514–8.
154. Xu H, Chen J, Birrenkott J, Zhao JX, Takalkar S, Baryeh K, et al. Gold-nanoparticle-decorated silica nanorods for sensitive visual detection of proteins. *Anal Chem*. 2014; 86: 7351–9.
155. Yao X, Wang Z, Zhao M, Liu S, Su L, Dou L, et al. Graphite-like carbon nitride-laden gold nanoparticles as signal amplification label for highly sensitive lateral flow immunoassay of 17 $\beta$ -estradiol. *Food Chem*. 2021; 347: 129001.
156. Yuan J, Chen X, Duan H, Cai X, Li Y, Guo L, et al. Gold nanoparticle-decorated metal organic frameworks on immunochromatographic assay for human chorionic gonadotropin detection. *Microchim Acta*. 2020; 187: 640.
157. Huang Q, Bu T, Zhang W, Yan L, Zhang M, Yang Q, et al. An improved clenbuterol detection by immunochromatographic assay with bacteria@Au composite as signal amplifier. *Food Chem*. 2018; 262: 48–55.
158. Bai T, Wang M, Cao M, Zhang J, Zhang K, Zhou P, et al. Functionalized Au@Ag-Au nanoparticles as an optical and SERS dual probe for lateral flow sensing. *Anal Bioanal Chem*. 2018; 410: 2291–303.
159. Jiang HL, Akita T, Ishida T, Haruta M, Xu Q. Synergistic catalysis of Au@Ag core-shell nanoparticles stabilized on metal-organic framework. *J Am Chem Soc*. 2011; 133: 1304–6.
160. Rivas L, de la Escosura-Muñiz A, Serrano L, Altet L, Francino O, Sánchez A, et al. Triple lines gold nanoparticle-based lateral flow assay for enhanced and simultaneous detection of Leishmania DNA and endogenous control. *Nano Res*. 2015; 8: 3704–14.
161. Huang L, Jin J, Wang J, Jiang C, Xu M, Wen H, et al. Homogeneous and high-density gold unit implanted optical labels for robust and sensitive point-of-care drug detection. *Nanoscale*. 2019; 11: 16026–35.
162. Huang X, Zhou Y, Ding L, Yu G, Leng Y, Lai W, et al. Supramolecular recognition-mediated layer-by-layer self-assembled gold nanoparticles for customized sensitivity in paper-based strip nanobiosensors. *Small*. 2019; 15: e1903861.
163. Kim MS, Kweon SH, Cho S, An SSA, Kim MI, Doh J, et al. Pt-decorated magnetic nanozymes for facile and sensitive point-of-care bioassay. *ACS Applied Mater Interfaces*. 2017; 9: 35133–40.
164. Takalkar S, Xu H, Chen J, Baryeh K, Qiu W, Zhao JX, et al. Gold nanoparticle coated silica nanorods for sensitive visual detection of microRNA on a lateral flow strip biosensor. *Anal Sci*. 2016; 32: 617–22.
165. Le TS, He S, Takahashi M, Enomoto Y, Matsumura Y, Maenosono S. Enhancing the sensitivity of lateral flow immunoassay by magnetic enrichment using multifunctional nanocomposite probes. *Langmuir*. 2021; 37: 6566–77.
166. Tran V, Walkenfort B, König M, Salehi M, Schlucker S. Rapid, quantitative, and ultrasensitive point-of-care testing: A portable SERS reader for lateral flow assays in clinical chemistry. *Angew Chem Int Ed Engl*. 2019; 58: 442–6.
167. Zhao J, Zhang K, Li Y, Ji J, Liu B. High-resolution and universal visualization of latent fingerprints based on aptamer-functionalized core-shell nanoparticles with embedded SERS reporters. *ACS Appl Mater Interfaces*. 2016; 8: 14389–95.
168. Zhu R, Feng H, Li Q, Su L, Fu Q, Li J, et al. Asymmetric core-shell gold nanoparticles and controllable assemblies for SERS ratiometric detection of microRNA. *Angew Chem Int Ed Engl*. 2021; 60: 12560–8.
169. Zhang X, Chu Y, Yang H, Zhao K, Li J, Du H, et al. Ultrasensitive and specific detection of salbutamol in swine feed, meat, and urine samples by a competitive immunochromatographic test integrated with surface-enhanced Raman scattering. *Food Anal Methods*. 2016; 9: 3396–406.
170. Zhang D, Huang L, Liu B, Ni H, Sun L, Su E, et al. Quantitative and ultrasensitive detection of multiplex cardiac biomarkers in lateral flow assay with core-shell SERS nanotags. *Biosens Bioelectron*. 2018; 106: 204–11.
171. Su L, Hu H, Tian Y, Jia C, Wang L, Zhang H, et al. Highly sensitive colorimetric/surface-enhanced Raman spectroscopy immunoassay relying on a metallic core-shell Au/Au nanostar with clenbuterol as a target analyte. *Anal Chem*. 2021; 93: 8362–9.
172. Pan Y, Fei D, Liu P, Guo X, Peng L, Wang Y, et al. Surface-enhanced Raman scattering-based lateral flow immunoassay for the detection of chloramphenicol antibiotics using Au@Ag nanoparticles. *Food Anal Methods*. 2021; 126: 1–9.
173. Li M, Yang H, Li S, Zhao K, Li J, Jiang D, et al. Ultrasensitive and quantitative detection of a new beta-agonist phenylethanolamine A by a novel immunochromatographic assay based on surface-enhanced Raman scattering (SERS). *J Agric Food Chem*. 2014; 62: 10896–902.
174. Liu HB, Du XJ, Zang YX, Li P, Wang S. SERS-based lateral flow strip biosensor for simultaneous detection of listeria monocytogenes and salmonella enterica serotype enteritidis. *J Agric Food Chem*. 2017; 65: 10290–9.
175. Shen H, Xie K, Huang L, Wang L, Ye J, Xiao M, et al. A novel SERS-based lateral flow assay for differential diagnosis of wild-type pseudorabies virus and gE-deleted vaccine. *Sens Actuators B*. 2019; 282: 152–7.
176. Jia X, Wang C, Rong Z, Li J, Wang K, Qie Z, et al. Dual dye-loaded Au@Ag coupled to a lateral flow immunoassay for the accurate and sensitive detection of *Mycoplasma pneumoniae* infection. *RSC Adv*. 2018; 8: 21243–51.
177. Aveyard J, Mehrabi M, Cossins A, Braven H, Wilson R. One step visual detection of PCR products with gold nanoparticles and a nucleic acid lateral flow (NALF) device. *Chem Commun (Camb)*. 2007: 4251–3.
178. Lou S, Ye JY, Li KQ, Wu A. A gold nanoparticle-based immunochromatographic assay: the influence of nanoparticle size. *Analyst*. 2012; 137: 1174–81.
179. Kim DS, Kim YT, Hong SB, Kim J, Huh NS, Lee MK, et al. Development of lateral flow assay based on size-controlled gold nanoparticles for detection of hepatitis B surface antigen. *Sensors (Basel)*. 2016; 16: 2154.
180. You PY, Li FC, Liu MH, Chan YH. Colorimetric and fluorescent dual-mode immunoassay based on plasmon-enhanced fluorescence of polymer dots for detection of PSA in whole blood. *ACS Appl Mater Interfaces*. 2019; 11: 9841–9.
181. Qu Z, Wang K, Alfranca G, Jesús M, Cui D. A plasmonic thermal sensing based portable device for lateral flow assay detection and quantification. *Nanoscale Res Lett*. 2020; 15: 1–12.
182. Anfossi L, Di Nardo F, Russo A, Cavalera S, Giovannoli C, Spano G, et al. Silver and gold nanoparticles as multi-chromatic lateral flow assay probes for the detection of food allergens. *Anal Bioanal Chem*. 2019; 411: 1905–13.
183. Park JM, Jung HW, Chang YW, Kim HS, Kang MJ, Pyun JC. Chemiluminescence lateral flow immunoassay based on Pt nanoparticle with peroxidase activity. *Anal Chim Acta*. 2015; 853: 360–7.
184. Quesada-González D, Sena-Torralba A, Wicaksono WP, de la Escosura-Muñiz A, Ivardini TA, Merkoçi A. Iridium oxide (IV) nanoparticle-based lateral flow immunoassay. *Biosens Bioelectron*. 2019; 132: 132–5.
185. Zhang J, Yu Q, Qiu W, Li K, Qian L, Zhang X, et al. Gold-platinum nanoflowers as a label and as an enzyme mimic for use in highly sensitive lateral flow immunoassays: application to detection of rabbit IgG. *Microchim Acta*. 2019; 186: 357.
186. Panferov VG, Safenkova IV, Zherdev AV, Dzantiev BB. Urchin peroxidase-mimicking Au@Pt nanoparticles as a label in lateral flow immunoassay: impact of nanoparticle composition on detection limit of *Clavibacter michiganensis*. *Microchim Acta*. 2020; 187: 268.
187. Panferov VG, Safenkova IV, Zherdev AV, Dzantiev BB. The steadfast Au@Pt soldier: peroxide-tolerant nanozyme for signal enhancement in lateral flow immunoassay of peroxidase-containing samples. *Talanta*. 2021; 225: 121961.

188. Jiang T, Song Y, Du D, Liu X, Lin Y. Detection of p53 protein based on mesoporous Pt-Pd nanoparticles with enhanced peroxidase-like catalysis. *ACS Sensors*. 2016; 1: 717-24.
189. Han J, Zhang L, Hu L, Xing K, Lu X, Huang Y, et al. Nanozyme-based lateral flow assay for the sensitive detection of *Escherichia coli* O157:H7 in milk. *J Dairy Sci*. 2018; 101: 5770-9.
190. Zhao Y, Yang M, Fu Q, Ouyang H, Wen W, Song Y, et al. A nanozyme- and ambient light-based smartphone platform for simultaneous detection of dual biomarkers from exposure to organophosphorus pesticides. *Anal Chem*. 2018; 90: 7391-8.
191. Hui W, Zhang S, Zhang C, Wan Y, Zhu J, Zhao G, et al. A novel lateral flow assay based on GoldMag nanoparticles and its clinical applications for genotyping of MTHFR C677T polymorphisms. *Nanoscale*. 2016; 8: 3579-87.
192. Liu X, Zhang C, Liu K, Wang H, Lu C, Li H, et al. Multiple SNPs detection based on lateral flow assay for phenylketonuria diagnostic. *Anal Chem*. 2018; 90: 3430-6.
193. Zhang D, Huang L, Liu B, Ge Q, Dong J, Zhao X. Rapid and ultrasensitive quantification of multiplex respiratory tract infection pathogen via lateral flow microarray based on SERS nanotags. *Theranostics*. 2019; 9: 4849-59.
194. Deng D, Yang H, Liu C, Zhao K, Li J, Deng A. Ultrasensitive detection of diclofenac in water samples by a novel surface-enhanced Raman scattering (SERS)-based immunochromatographic assay using AgMBA@SiO<sub>2</sub>-Ab as immunoprobe. *Sens Actuators B*. 2019; 283: 563-70.
195. Liu J, Mazumdar D, Lu Y. A simple and sensitive "dipstick" test in serum based on lateral flow separation of aptamer-linked nanostructures. *Angew Chem Int Ed Engl*. 2006; 45: 7955-9.
196. Kim K, Han DK, Choi N, Kim SH, Joung Y, Kim K, et al. Surface-enhanced raman scattering-based dual-flow lateral flow assay sensor for the ultrasensitive detection of the thyroid-stimulating hormone. *Anal Chem*. 2021; 93: 6673-81.
197. Xing KY, Shan S, Liu DF, Lai WH. Recent advances of lateral flow immunoassay for mycotoxins detection. *TrAC, Trends Anal Chem*. 2020; 133: 116087.
198. Deng Y, Jiang H, Li X, Lv X. Recent advances in sensitivity enhancement for lateral flow assay. *Microchim Acta*. 2021; 188: 1-15.
199. Nguyen VT, Song S, Park S, Joo C. Recent advances in high-sensitivity detection methods for paper-based lateral-flow assay. *Biosens Bioelectron*. 2020; 152: 112015.
200. Sena-Torralba A, Ngo DB, Parolo C, Hu L, Álvarez-Diduk R, Bergua JF, et al. Lateral flow assay modified with time-delay wax barriers as a sensitivity and signal enhancement strategy. *Biosens Bioelectron*. 2020; 168: 112559.
201. Bishop JD, Hsieh HV, Gasperino DJ, Weigl BH. Sensitivity enhancement in lateral flow assays: A systems perspective. *Lab Chip*. 2019; 19: 2486-99.
202. Shen M, Chen Y, Zhu Y, Zhao M, Xu Y. Enhancing the sensitivity of lateral flow immunoassay by centrifugation-assisted flow control. *Anal Chem*. 2019; 91: 4814-20.
203. Soh JH, Chan H-M, Ying JY. Strategies for developing sensitive and specific nanoparticle-based lateral flow assays as point-of-care diagnostic device. *Nano Today*. 2020; 30: 100831.